

TECHNICAL REPORT

IEC TR 60788

Second edition
2004-02

Medical electrical equipment – Glossary of defined terms

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INTERNATIONAL ELECTROTECHNICAL COMMISSION

**MEDICAL ELECTRICAL EQUIPMENT –
GLOSSARY OF DEFINED TERMS**

FOREWORD

- 1) The International Electrotechnical Commission (IEC) is a worldwide organization for standardization comprising all national electrotechnical committees (IEC National Committees). The object of IEC is to promote international co-operation on all questions concerning standardization in the electrical and electronic fields. To this end and in addition to other activities, IEC publishes International Standards, Technical Specifications, Technical Reports, Publicly Available Specifications (PAS) and Guides (hereafter referred to as "IEC Publication(s)"). Their preparation is entrusted to technical committees; any IEC National Committee interested in the subject dealt with may participate in this preparatory work. International, governmental and non-governmental organizations liaising with the IEC also participate in this preparation. IEC collaborates closely with the International Organization for Standardization (ISO) in accordance with conditions determined by agreement between the two organizations.
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The main task of IEC technical committees is to prepare International Standards. However, a technical committee may propose the publication of a technical report when it has collected data of a different kind from that which is normally published as an International Standard, for example "state of the art".

IEC 60788, which is a technical report, has been prepared by IEC TC 62: Electrical EQUIPMENT in medical practice.

This second edition cancels and replaces the first edition of IEC 60788 published in 1984. This second edition constitutes a technical revision.

The text of this technical report is based on the following documents:

Enquiry draft	Report on voting
62/137/DTR	62/140/RVC

Full information on the voting for the approval of this technical report can be found in the report on voting indicated in the above table.

This publication does not follow the rules for structuring International Standards as given in Part 2 of the ISO/IEC Directives.

The committee has decided that the contents of this publication will remain unchanged until 2005. At this date, the publication will be

- reconfirmed;
- withdrawn;
- replaced by a revised edition, or
- amended.

INTRODUCTION

Purpose

- To provide an actual mirror of defined terms for all steps in the development of IEC standards under the scope of “MEDICAL ELECTRICAL EQUIPMENT”, IEC TC 62.
- To give guidance for harmonisation of the defined terms used in the IEC standards on “MEDICAL ELECTRICAL EQUIPMENT”.

Contents

- All DEFINED TERMS used in the General, Particular and Collateral Standards, recorded in the project files of the IEC for TC 62, SC 62A, 62B, 62C and 62D are mirrored.
- Recommendations to avoid existing redundancy are added as red text in the column “Definitions” in the table.

Maintenance

- An annual maintenance cycle for this TR is introduced. Closing date for the editorial input is the middle of December of a year.
- The annual editorial maintenance is done by the Secretaries of the IEC technical committee 62 and its subcommittees 62A, 62B, 62C and 62D.
- The compilation (addition of new terms and deletion of obsolete terms) is done by the Secretary of IEC TC 62.

Targets

- Represent the state-of-the-art in the definitions
- Harmonize the language of the IEC publications
- Ease translations of the IEC publications
- Enable self-control by the experts working in projects for MEDICAL ELECTRICAL EQUIPMENT.

Coded reference of the DEFINED TERMS

- In all cases – as appropriate – the reference codes “IEV xxx-xx-xx” of the International Electronic Vocabulary (IEV) are added in the “Reference” column of the table.
- For DEFINED TERMS used in RADIOLOGY the reference codes “rm-xx-xx” remain unchanged as initiated by IEC 60788 Ed.1.
- For main fields other than RADIOLOGY, the coded references will be generated in future annual editions.

Replacement

This technical report replaces IEC 60788 Ed.1, *Medical radiology – Terminology*.

MEDICAL ELECTRICAL EQUIPMENT – GLOSSARY OF DEFINED TERMS

1 Scope

This Technical report comprises all defined terms used in the IEC standards and technical reports which

- fall under the scope of MEDICAL ELECTRICAL EQUIPMENT, and
- are on the list of publications as stated in May 2003.

2 Normative references

The documents referenced in 2.2 are forming the sources for the defined terms in this document.

2.1 General

The defined terms listed in this glossary are mirrored as presented in the standards and technical reports. Only the recommendations are added for further harmonisation of multiple defined terms.

The glossary is prepared to ease the use of the electronic version by two search functions:

- Search in the alphabetic order, and
- Search by the technical and physical chapters in case of ionising radiation (rm-xx-xx).

2.2 List of the IEC publications mirrored in this edition 2004

The list of IEC Standards below comprises the defined terms as used in the latest consolidated version, comprising the amendments as applicable.

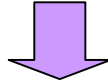
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2	60522	1999-02
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49	60601-2-45	2001-05
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51	60601-2-47	2001-07
52	60601-2-49	2001-07
53	60601-2-50	2000-07
54	60601-2-51	2003-02
55	60601-2-55	To be published
56	60601-3-1	1996-08
57	60613	1989-05
58	60627	2001-08
59	60731/A1	1997-07/ 2002-06
60	60789	1992-02
61	60806	1984-01
62	60976/A1	1989-06/ 2000-07
63	60977/A1	1989-10/ 2000-04
64	61168	1993-12
65	61170	1993-12
66	61217 Ed.1.1	2002-03
67	61223-1	1993-07
68	61223-2-1	1993-07
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91	61331-3	1998-11
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94	61675-2	1998-01
95	61675-3	1998-02
96	61676	2002-09
97	61852	1998-04
98	61859	1997-05
99	61948-1, TR	2001-02
100	61948-2, TR	2001-02
101	62083	2000-11
102	62266, TR	2002-03
103	ISO 14971	2000-11

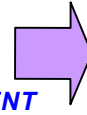
Glossary of DEFINED TERMS used for MEDICAL ELECTRICAL EQUIPMENT – Edition 2004

Search...

*...via chapters
for imaging EQUIPMENT*



*...by alphabetic index
for all medical EQUIPMENT*



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Physics	General	Ionizing RADIATION	Interactions	Quantities, units and related concepts				
Generation and emission of ionizing RADIATION	General	HIGH VOLTAGE generators	X-RAY TUBE assemblies	PARTICLE ACCELERATORS	Beam therapy, RADIONUCLIDE sources	Therapy EQUIPMENT with SEALED RADIOACTIVE SOURCES		
RADIOLOGICAL EQUIPMENT using ionizing RADIATION	General	EQUIPMENT for medical diagnostics	Images: Reception, transfer, recording	EQUIPMENT for RADIOTHERAPY	EQUIPMENT for nuclear medicine	Accessories	Operation of EQUIPMENT	Geometry of RADIATION BEAM
Medical RADIOLOGICAL techniques	General	Diagnosis using beams	Therapy using beams	Nuclear medicine				
Dosimetry	General	RADIATION DETECTORS	PHANTOMS					
Protection against ionizing RADIATION	General	Limits and factors	Groups of persons	Areas	Means of protection			
Testing of RADIOLOGICAL EQUIPMENT	General	Test EQUIPMENT	VERIFICATION of characteristics	Concepts in mathematics, metrics, statistics	Obligation & statement of compliance			
Technology	General	Docu-mentation	EQUIPMENT	Operation of EQUIPMENT	Persons			
Magnetic resonance EQUIPMENT	General							
ULTRASOUND EQUIPMENT	General							

PHYSICS General rm-10 RADIATION TYPE
PHYSICS Ionizing RADIATION rm-11 DOSE PROFILE EXTRA-FOCAL RADIATION FOCAL RADIATION INTRINSIC ENERGY RESOLUTION INTRINSIC ENERGY SPECTRUM IONIZING RADIATION LEAKAGE RADIATION MAXIMUM ENERGY NEUTRON PHOTON PRIMARY RADIATION RADIATION RADIONUCLIDE RESIDUAL RADIATION SCATTERED RADIATION STRAY RADIATION
PHYSICS Interactions rm-12 ABSORPTION BACK-SCATTERING BUILD UP FILTRATION INDUCED RADIOACTIVITY IRRADIATION RADIOACTIVITY TRANSMISSION
PHYSICS Quantities, units and related concepts rm-13 ABSORBED DOSE ABSORBED DOSE RATE ABSORBED DOSE RATE TO WATER

ABSORBED DOSE TO WATER ACTIVITY ADDITIONAL FILTRATION AIR KERMA AIR KERMA LENGTH AIR KERMA RATE ATTENUATION ATTENUATION COEFFICIENT ATTENUATION EQUIVALENT ATTENUATION RATIO AUTOMATIC CONTROL SYSTEM AUTOMATIC EXPOSURE CONTROL AUTOMATIC EXPOSURE RATE CONTROL AUTOMATIC INTENSITY CONTROL BUILD UP FACTOR DEPTH DOSE DOSE AREA PRODUCT DOSE AREA PRODUCT RATE DOSE EQUIVALENT DOSE MONITOR UNIT ELECTRON ENERGY FLUENCE RATE ENERGY RESOLUTION EXPOSURE EXPOSURE RATE HALF-VALUE LAYER INHERENT FILTRATION KERMA KERMA RATE LEAD EQUIVALENT NOMINAL ENERGY QUALITY EQUIVALENT FILTRATION RADIATION SPECTRUM RADIATION CONDITION RADIATION ENERGY RADIATION OUTPUT RADIATION QUALITY RADIATION QUANTITIES AND UNITS RADIATION QUANTITY
--

RADIOACTIVE HALF-LIFE RELATIVE SURFACE DOSE RESPONSE RESPONSE TIME SENSITIVITY PROFILE TENTH-VALUE LAYER TOTAL FILTRATION TRANSMISSION KERMA (TRANSMISSION KERMA RATE) TRANSMISSION OF PRIMARY RADIATION TRANSMISSION OF SCATTERED RADIATION TRANSMISSION OF TOTAL RADIATION TRANSMISSION RATIO UNATTENUATED BEAM UNATTENUATED BEAM QUALITY UNIFORMITY UNSCATTERED TRUE COINCIDENCE VARIATION VOXEL WATER KERMA
GENERATION & EMISSION OF IONIZING RADIATION General rm-20 ACTUAL FOCAL SPOT BLOOMING VALUE CAPSULE EFFECTIVE FOCAL SPOT EXAMINATION ROOM FOCAL SPOT NOMINAL FOCAL SPOT VALUE RADIATION HEAD RADIATION SOURCE RADIATION SOURCE ASSEMBLY RADIOACTIVE SOURCE RADIOACTIVE SOURCE TRAIN RADIOLOGICAL EQUIPMENT RADIOLOGICAL INSTALLATION

SEALED RADIOACTIVE SOURCE TARGET TARGET ANGLE TREATMENT ROOM X-RAY EQUIPMENT X-RAY GENERATOR X-RAY IMAGING ARRANGEMENT X-RAY TUBE HEAD
GENERATION & EMISSION OF IONIZING RADIATION High VOLTAGE generators rm-21 CAPACITOR DISCHARGE HIGH-VOLTAGE GENERATOR CONSTANT POTENTIAL HIGH-VOLTAGE GENERATOR HIGH-VOLTAGE CABLE CONNECTION HIGH-VOLTAGE GENERATOR HIGH-VOLTAGE TRANSFORMER ASSEMBLY NOMINAL SHORTEST IRRADIATION TIME ONE-PEAK HIGH-VOLTAGE GENERATOR PRIMARY TIMER PRIMARY/SECONDARY (TIMER) COMBINATION RADIATION QUANTITY FOR NOMINAL SHORTEST IRRADIATION TIME SIX-PEAK HIGH-VOLTAGE GENERATOR TWO-PEAK HIGH VOLTAGE GENERATOR
GENERATION & EMISSION OF IONIZING RADIATION X-RAY TUBE assemblies rm-22 ANODE ANODE ANGLE CATHODE FOCAL TRACK

MAXIMUM PEAK VOLTAGE
MEAN PEAK VOLTAGE
OPERATING CONDITIONS FOR
NOMINAL X-RAY TUBE VOLTAGE
PERMANENT FILTRATION
PRACTICAL PEAK POTENTIAL (PPP)
TUBE VOLTAGE (X-RAY)
TWELVE-PEAK HIGH VOLTAGE
GENERATOR
X-RAY TUBE
X-RAY TUBE ASSEMBLY
X-RAY TUBE HOUSING

**GENERATION & EMISSION
OF IONIZING RADIATION**
PARTICLE ACCELERATORS rm-23
PARTICLE ACCELERATOR
PRACTICAL RANGE
QUANTITY INDEX

**GENERATION & EMISSION
OF IONIZING RADIATION**
**Beam therapy, RADIONUCLIDE
sources rm-24**
DELINEATED LIGHT FIELD
DELINEATED RADIATION BEAM
DELINEATED RADIATION FIELD
DELINEATOR
RADIONUCLIDE BEAM THERAPY
EQUIPMENT
SHUTTER
SOURCE CARRIER

**GENERATION & EMISSION
OF IONIZING RADIATION**
**Therapy EQUIPMENT with SEALED
RADIOACTIVE SOURCES rm-25**
CHANNEL
SOURCE APPLICATOR
SOURCE DRIVE MECHANISM

STORAGE CONTAINER

**RADIOLOGICAL EQUIPMENT
USING IONIZING RADIATION**
General rm-30
ASSOCIATED EQUIPMENT
GANTRY
IRRADIATION SWITCH
PATIENT SUPPORT
QUALITY ASSURANCE
QUALITY ASSURANCE PROGRAMME
REFERENCE AIR KERMA

**RADIOLOGICAL EQUIPMENT
USING IONIZING RADIATION**
**EQUIPMENT for medical
diagnosis rm-31**
CASSETTE CHANGER
CT SCANNER
EFFECTIVE LENGTH
EFFECTIVE RANGE (OF INDICATED
VALUES)
FILM CHANGER
INTERVENTIONAL X-RAY EQUIPMENT
POSITRON EMISSION TOMOGRAPH
RADIOSCOPICALLY GUIDED
INTERVENTIONAL PROCEDURE
SERIAL CHANGER
SPEED INDEX
SPOTFILM DEVICE

**RADIOLOGICAL EQUIPMENT
USING IONIZING RADIATION**
**Reception, recording and
transfer of images rm-32**
ANTI-SCATTER GRID
ARTEFACT
AXIAL FIELD OF VIEW
AXIAL POINT SPREAD FUNCTION
AXIAL RESOLUTION

AXIAL SLICE WIDTH
BEST FOCUS
CENTRAL AXIS
CENTRAL LINE INDICATION
CENTRAL MAGNIFICATION
CENTRE OF THE ENTRANCE FIELD
CENTRE OF THE OUTPUT IMAGE
COINCIDENCE DETECTION
COINCIDENCE WINDOW
CONTRAST IMPROVEMENT RATIO
CONTRAST INDEX
CONTRAST RATIO (ABBREVIATION
CR)
CONVERSION FACTOR
CROSS GRID
CT DETECTOR
CT DOSIMETER
DAS CONTRAST SENSITIVITY
DAS VISUAL SPATIAL RESOLUTION
DECENTRING OF A FOCUSED GRID
DEFOCUSING OF A FOCUSED GRID
DETECTIVE QUANTUM EFFICIENCY
(ABBREVIATION DQE)
DETECTOR ASSEMBLY
DETECTOR FIELD OF VIEW (FOV)
DIFFERENTIAL RADIAL IMAGE
DISTORTION
DIRECT RADIOGRAM
DOUBLE EMULSION FILM
DYNAMIC RANGE
EDGE FILTER
EFFECTIVE IMAGE RECEPTION AREA
ELECTRO-OPTICAL X-RAY IMAGE
INTENSIFIER
ENTRANCE FIELD
ENTRANCE FIELD SIZE
ENTRANCE PLANE
FLUORESCENT SCREEN
FOCUSED GRID
FOCUSING DISTANCE

GRID EXPOSURE FACTOR
GRID RATIO
GRID SELECTIVITY
IMAGE DISTORTION
IMAGE MATRIX
IMAGE RECEPTOR PLANE IN X-RAY
IMAGE INTENSIFIER TUBES
INPUT SCREEN
INTEGRAL IMAGE DISTORTION
INTEGRAL MAGNIFICATION
INTENSIFYING SCREEN
INTERRUPTION
LINEAR GRID
LINEAR RANGE
LINEARITY
LINE PAIR RESOLUTION
LOCAL RADIAL MAGNIFICATION
LOW CONTRAST RESOLUTION
LOW-FREQUENCY DROP (LFD)
LUMINANCE DISTRIBUTION
LUMINANCE NON-UNIFORMITY
MAMMOGRAPHIC ANTI-SCATTER GRID
MATRIX ELEMENT
MEAN CT NUMBER
MOVING GRID
NET OPTICAL DENSITY
NOMINAL ENTRANCE FIELD SIZE
NOMINAL FOCAL SPOT VALUE
NOMINAL IMAGE SIZE
NOMINAL TOMOGRAPHIC SECTION
THICKNESS
NOMINAL TOMOGRAPHIC SLICE
THICKNESS
NON-SCREEN FILM
OBJECT SLICE
OBLIQUE CROSS GRID
ORTHOGONAL CROSS GRID
OUTPUT IMAGE
OUTPUT SCREEN
PARALLEL GRID

PIXEL PROJECTION PROJECTION ANGLE QUANTUM ABSORPTION EFFICIENCY RADIOGRAPHIC CASSETTE RADIOGRAPHIC CASSETTE HOLDER RADIOGRAPHIC FILM RADIOLOGICAL IMAGE RADIOSCOPIC SCREEN REGION OF INTEREST (ROI) RESOLUTION OF THE DISPLAY SINOGRAM SPATIAL RESOLUTION SPOTFILM DEVICE STATIONARY GRID STRIP FREQUENCY STRIPS PER CENTIMETRE TAPERED GRID THREE-DIMENSIONAL RECONSTRUCTION TRIxel TRUE CENTRAL LINE TWO-DIMENSIONAL RECONSTRUCTION USEFUL ENTRANCE FIELD SIZE VEILING GLARE INDEX (VGI) X-RAY IMAGE INTENSIFIER X-RAY IMAGE INTENSIFIER TUBE X-RAY IMAGE RECEPTOR X-RAY PATTERN XRii
RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION EQUIPMENT for RADIOTHERAPY rm-33 CONTINUATION DOSE RATE MONITORING SYSTEM DOSE RATE MONITORING SYSTEM ELECTRON BEAM APPLICATOR

EQUILIBRATION TIME EQUIPMENT MODEL / EQUIPMENT MODELLING EXIT SURFACE FIELD SIZE INTERRUPTION (OF IRRADIATION)/TO INTERRUPT (IRRADIATION) IRRADIATION TREATMENT PRESCRIPTION ISOCENTRIC EQUIPMENT ISOCENTRIC TREATMENT LINE SOURCE LINE SPREAD FUNCTION (LSF) LINEAR GRID LINEAR RANGE LINEARITY LIQUID SCINTILLATION COUNTER NORMAL TREATMENT DISTANCE (NTD) PATIENT ANATOMY MODEL / ANATOMY MODELLING PENETRATIVE QUALITY PRIMARY/SECONDARY DOSE MONITORING COMBINATION PRIMARY-SECONDARY DOSE MONITORING SYSTEM RADIOTHERAPY SIMULATOR RADIOTHERAPY TREATMENT PLANNING SYSTEM (RTPS) REDUNDANT DOSE MONITORING COMBINATION REDUNDANT DOSE MONITORING SYSTEMS REDUNDANT (TIMER) COMBINATION SECONDARY DOSE MONITORING SYSTEM TERMINATION (OF IRRADIATION) TERMINATION OF IRRADIATION /TO TERMINATE IRRADIATION TRANSMISSION DETECTOR

TREATMENT CONTROL PANEL WEDGE FILTER ANGLE WEDGE FILTER FACTOR ZERO APPLICATOR
RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION EQUIPMENT for nuclear medicine rm-34 CENTRE OF ROTATION (COR) CERENKOV COUNTER COLLIMATOR (FOR GAMMA CAMERAS) COLLIMATOR AXIS COLLIMATOR BACK FACE COLLIMATOR FRONT FACE CONVERGING COLLIMATOR COUNT LOSS COUNT RATE COUNT RATE CHARACTERISTIC DETECTOR HEAD DETECTOR HEAD TILT DETECTOR LINE SPREAD FUNCTION DETECTOR SHIELD DIVERGING COLLIMATOR EMISSION COMPUTED TOMOGRAPHY (ECT) ENTRANCE FIELD OF A COLLIMATOR EQUIVALENT WIDTH (EW) EXIT FIELD OF A COLLIMATOR FIXED COORDINATE SYSTEM GAMMA CAMERA GAMMA CAMERA BASED WHOLEBODY IMAGING SYSTEM IN VIVO COUNTING SYSTEM LINE OF RESPONSE (LOR) LIQUID SCINTILLATION COUNTER MULTIPLE WINDOW SPATIAL REGISTRATION NON-UNIFORMITY OF RESPONSE NORMALIZED SLICE SENSITIVITY

NORMALIZED VOLUME SENSITIVITY OFFSET ORGAN COUNTING SYSTEM PARALLEL HOLE COLLIMATOR PHYSICAL POINT SPREAD FUNCTION PILE UP EFFECT PIN-HOLE COLLIMATOR POINT SOURCE POINT SPREAD FUNCTION (PSF) POSITIONING TIME POSITRON EMISSION TOMOGRAPHY (PET) PROJECTION BEAM PULSE AMPLITUDE ANALYZER PULSE WINDOW RADIAL RESOLUTION RADIATION DETECTOR ASSEMBLY RADIUS OF ROTATION RANDOM COINCIDENCE RECOVERY COEFFICIENT RESOLVING TIME SAMPLE CHANGER SCATTER FRACTION (SF) SCATTERED TRUE COINCIDENCE SENSITIVITY SINGLE GAMMA-RAY PHOTON PULS SINGLES RATE SLICE SENSITIVITY SLICE THICKNESS SPATIAL NONLINEARITY SYSTEM AXIS SYSTEM NON-UNIFORMITY OF RESPONSE SYSTEM SENSITIVITY TANGENTIAL RESOLUTION TOTAL COINCIDENCES TRANSVERSE FIELD OF VIEW TRANSVERSE POINT SPREAD FUNCTION TRANSVERSE RESOLUTION

<p>TRANSVERSE TOMOGRAPHY TREATMENT FIELD TREATMENT PARAMETER TREATMENT PLAN/ TREATMENT PLANNING TRUE COINCIDENCE TRUE COUNT RATE VOLUME SENSITIVITY WELL-COUNTER WELL-TYPE DETECTOR WHOLE BODY COUNTER WHOLE BODY IMAGING DEVICE</p>
<p>RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION Accessories rm-35 ADDED FILTER BACK POINTER BEAM SCATTERING FILTER COMPRESSION DEVICE CORE BIOPSY GUN EFFECTIVE APERTURE FIELD FLATTENING FILTER FILTER FRONT POINTER IONIZING RADIATION SHIELD MAMMOGRAPHIC STEREOTACTIC DEVICE RADIOGRAM TISSUE EQUIVALENT MATERIAL WEDGE FILTER ZERO FILTER</p>
<p>RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION Operation of EQUIPMENT rm-36 ANODE COOLING CURVE ANODE HEAT CONTENT ANODE HEATING CURVE ANODE INPUT POWER ANODE SPEED</p>

<p>APPARENT RESISTANCE OF SUPPLY MAINS CATHODE EMISSION CHARACTERISTIC CONTINUOUS MODE CONTROLLED AREA CT CONDITIONS OF OPERATION CT PITCH FACTOR CURRENT TIME PRODUCT DECREASING INPUT POWER RATING DEFAULT SETTING EQUIVALENT ANODE INPUT POWER FILAMENT CURRENT INDIRECT RADIOGRAM INITIAL X-RAY TUBE VOLTAGE INITIATION INTERMITTENT MODE IRRADIATION TIME LIMITED X-RAY TUBE VOLTAGE LOADING LOADING FACTOR LOADING STATE LOADING TIME MAXIMUM ANODE HEAT CONTENT MAXIMUM CONTINUOUS HEAT DISSIPATION MAXIMUM X-RAY TUBE ASSEMBLY HEAT CONTENT MODES OF OPERATION WITH CONTINUED DISPLAY NOMINAL ANODE INPUT POWER NOMINAL ELECTRIC POWER NOMINAL X-RAY TUBE VOLTAGE NON- ISOCENTRIC OBJECT PROGRAMMED CONTROL PERCENTAGE RIPPLE PERCENTAGE RIPPLE IN CONSTANT POTENTIAL HIGH-VOLTAGE GENERATORS PRUDENT USE STATEMENT</p>

<p>RADIOGRAPHIC RATING SERIAL LOAD RATING SINGLE LOAD RATING TREATMENT TIME X-RAY TUBE ASSEMBLY COOLING CURVE X-RAY TUBE ASSEMBLY HEAT CONTENT X-RAY TUBE ASSEMBLY HEATING CURVE X-RAY TUBE ASSEMBLY INPUT POWER X-RAY TUBE CURRENT X-RAY TUBE LOAD X-RAY TUBE VOLTAGE</p>
<p>RADIOLOGICAL EQUIPMENT USING IONIZING RADIATION Geometry of RADIATION BEAM rm-37 BEAM APPLICATOR BEAM LIMITING DEVICE BEAM LIMITING SYSTEM BOUNDARY AND DIMENSIONS OF THE X-RAY FIELD BROAD BEAM BROAD BEAM CONDITION DETECTOR HEAD TILT DIAPHRAGM ENTRANCE SURFACE FOCAL SPOT TO IMAGE RECEPTOR DISTANCE FOCAL SPOT TO SKIN DISTANCE GEOMETRICAL FIELD SIZE GEOMETRICAL RADIATION FIELD IMAGE PLANE IMAGE RECEPTION AREA IMAGE RECEPTION PLANE INPUT APERTURE IRRADIATION FIELD SIZE ISOCENTRE</p>

<p>ISOCENTRIC LIGHT DETECTOR LIGHT FIELD LIGHT FIELD -INDICATOR NARROW BEAM NARROW BEAM CONDITION OUTPUT BEAM AREA OUTPUT BEAM DIMENSIONS (NON- UNIFORM EXCITATION) PATIENT SURFACE PENUMBRA RADIATION SOURCE TO SKIN DISTANCE RADIATION APERTURE RADIATION BEAM RADIATION BEAM AXIS RADIATION FIELD RATED FIELD SIZE RATED RANGE REFERENCE AXIS REFERENCE DIRECTION REFERENCE PLANE SOURCE TO ENTRANCE PLANE DISTANCE (SED) TARGET VOLUME TREATMENT VOLUME USEFUL BEAM USEFUL FIELD VIRTUAL SOURCE</p>
<p>MEDICAL RADIOLOGICAL TECHNIQUES General rm-40 MEDICAL DIAGNOSTIC RADIOLOGY MEDICAL RADIOLOGICAL EXAMINATION MEDICAL RADIOLOGY NUCLEAR MEDICINE RADIOLOGICAL RADIOLOGY</p>

RADIOTHERAPY TREATMENT
MEDICAL RADIOLOGICAL TECHNIQUES Diagnosis using beams rm-41 CINERADIOGRAPHY COMPUTED TOMOGRAPHY DENTAL PANORAMIC RADIOGRAPHY DIRECT RADIOGRAPHY DIRECT RADIOSCOPY INDIRECT RADIOGRAPHY INDIRECT RADIOSCOPY RADIOGRAPHY RADIOSCOPY RADIOSCOPICALLY GUIDED INVASIVE PROCEDURE RECONSTRUCTIVE TOMOGRAPHY SERIAL RADIOGRAPHY SINGLE PHOTON EMISSION COMPUTED TOMOGRAPHY (SPECT) TOMOGRAPHIC PLANE TOMOGRAPHIC SECTION TOMOGRAPHIC SECTION THICKNESS TOMOGRAPHIC VOLUME TOMOGRAPHY TOTAL FIELD OF VIEW
MEDICAL RADIOLOGICAL TECHNIQUES Therapy using beams rm-42 ANNIHILATION RADIATION BEAM OFF BEAM ON BRACHYRADIOTHERAPY BRACHYTHERAPY SOURCE MODEL / BRACHYTHERAPY SOURCE MODELING INTERSTITIAL RADIOTHERAPY

INTRACAVITARY RADIOTHERAPY MOVING BEAM RADIOTHERAPY STATIONARY RADIOTHERAPY SUPERFICIAL RADIOTHERAPY TELERADIOTHERAPY X-RAY THERAPY
MEDICAL RADIOLOGICAL TECHNIQUES Nuclear medicine rm-43
DOSIMETRY General rm-50 DOSEMETER DOSEMETER (PATIENT CONTACT) DOSIMETER (DIAGNOSTIC) DOSIMETER (RADIOTHERAPY) RADIATION METER
DOSIMETRY RADIATION DETECTORS rm-51 CHAMBER (IONIZATION) CHAMBER ASSEMBLY DOSE AREA PRODUCT METER EFFECTIVE RANGE EXPOSURE METER IONIZATION CHAMBER LEAKAGE CURRENT (CHAMBER ASSEMBLY) RADIATION DETECTOR SENSITIVE VOLUME TRANSMISSION CHAMBER
DOSIMETRY PHANTOMS rm-52 PHANTOM

PROTECTION AGAINST IONIZING RADIATION General rm-60 RADIATION PROTECTION RADIOLOGICAL PROTECTION
PROTECTION AGAINST IONIZING RADIATION Limits and factors rm-61 DOSE EQUIVALENT LIMIT WORKLOAD
PROTECTION AGAINST IONIZING RADIATION Groups of persons rm-62
PROTECTION AGAINST IONIZING RADIATION Areas rm-63 PROTECTED AREA SIGNIFICANT ZONE OF OCCUPANCY
PROTECTION AGAINST IONIZING RADIATION Means of protection rm-64 OVARY SHIELD PROTECTIVE BARRIER PROTECTIVE DEVICE PROTECTIVE GLASS PLATE PROTECTIVE GLASS PLATE TYPE SC PROTECTIVE GLASS PLATE TYPE VI PROTECTIVE GONAD APRON PROTECTIVE MITTEN PRIMARY PROTECTIVE SHIELDING PROTECTIVE SHIELDING SCROTUM SHIELD SHADOW SHIELD STRUCTURAL SHIELDING

TESTING OF RADIOLOGICAL EQUIPMENT General rm-70 ACCEPTANCE TEST CONSTANCY TEST FILM ILLUMINATOR FILM PROCESSOR HYDRAULIC TEST PRESSURE INSTRUMENT PARAMETER INVASIVE MEASUREMENT QUALITY ASSURANCE QUALITY ASSURANCE PROGRAMME QUALITY CONTROL REFERENCE CONDITIONS REFERENCE DATA REFERENCE INDICATED VALUE REFERENCE SCALE READING REFERENCE VOLUME SITE TEST SPEED INDEX STANDARD TEST CONDITIONS STATUS TEST TYPE TEST VALIDATION VERIFICATION
TESTING OF RADIOLOGICAL EQUIPMENT Test EQUIPMENT rm-71 AIR-DENSITY CHARACTERISTIC BASE DEPTH CALIBRATION FACTOR CERTIFIED RADIOACTIVE STANDARD SOURCE COMPOSITION OF REFERENCE MATERIALS EFFECTIVE RADIATED POWER (ERP) FIELD-CLASS DOSIMETER HALF VALUE LAYER TEST DEVICE INITIAL CONSTANCY TEST FILM

INITIAL REFERENCE FILM
 INSTRUMENT ACCURACY
 IONIZATION CHAMBER TEST SOURCE
 MEASURING ASSEMBLY
 MTF ANALYZER
 MULTI-DETECTOR COUNTER
 NON-INVASIVE MEASUREMENT
 NON-IRRADIATED CONSTANCY TEST
 FILM
 PINHOLE CAMERA
 RADIOACTIVE IMPURITY
 RADIOACTIVE STANDARD SOURCE
 RADIONUCLIDE CALIBRATOR
 RADIONUCLIDE FACTOR
 RATED LENGTH (OF USE)
 REFERENCE POINT (OF A CHAMBER)
 REFERENCE POINT (OF A RADIATION
 DETECTOR)
 REFERENCE-CLASS DOSIMETER
 SAMPLE VOLUME CHARACTERISTIC
 SLIT CAMERA
 STANDARD TEST VALUES
 STAR PATTERN CAMERA
 TEST DEVICE
 TRACEABLE RADIOACTIVE STANDARD
 SOURCE
 UNIFORM CONSTANCY TEST FILM

**TESTING OF RADIOLOGICAL
 EQUIPMENT**
Verification of characteristics
rm-72

ENERGY CALIBRATION
 FILM BASE PLUS FOG DENSITY
 FOCAL SPOT PINHOLE RADIOGRAM
 FOCAL SPOT SLIT RADIOGRAM
 FOCAL SPOT STAR RADIOGRAM
 INTRINSIC LINE SPREAD FUNCTION
 INTRINSIC NON-UNIFORMITY OF
 RESPONSE

INTRINSIC SPATIAL NON-LINEARITY
 IMMUNITY LEVEL
 IMMUNITY TEST LEVEL
 MINIMUM EFFECTIVE RANGE
 MINIMUM RATED RANGE
 ROUTINE TEST
 SPATIAL RESOLUTION (IN CT
 EQUIPMENT)
 SPECIFIED ENERGY RESPONSE
 STABILITY CHECK DEVICE
 STABILIZATION TIME
 STANDARD
 STANDARD MEASUREMENT DEPTH
 STAR PATTERN RESOLUTION LIMIT
 SYSTEM LINEARITY
 ZERO DRIFT (MEASURING ASSEMBLY)
 ZERO SHIFT (MEASURING ASSEMBLY)

**TESTING OF RADIOLOGICAL
 EQUIPMENT**

**Concepts in mathematics,
 metrics and statistics** **rm-73**

BASELINE VALUE
 COEFFICIENT OF VARIATION
 COMBINED STANDARD UNCERTAINTY
 COMPUTED TOMOGRAPHY DOSE
 INDEX (CTDI)
 COMPUTED TOMOGRAPHY DOSE
 INDEX 100 (CTDI100)
 COMPUTED TOMOGRAPHY NUMBER
 (CT NUMBER)
 CONVENTIONAL TRUE VALUE
 COORDINATE SYSTEM OF PROJECTION
 CORRECTION FACTOR
 ERROR OF MEASUREMENT
 EXPANDED UNCERTAINTY
 FULLWIDTH AT HALF MAXIMUM
 (FWHM)
 FULL WIDTH AT TENTH MAXIMUM
 (FWTM)

HAZARD ANALYSIS
 INDICATED VALUE
 INTERVENTIONAL REFERENCE POINT
 INTRINSIC ERROR
 ISOPLANATIC REGION
 LIMITS OF VARIATION
 LINE SOURCE
 LINE SPREAD FUNCTION (LSF)
 MAXIMUM TOLERABLE RISK
 MEASURED VALUE
 MODULATION TRANSFER FUNCTION
 (MTF)
 NOISE
 NOMINAL (VALUE)
 NON- LINEARITY
 OPTICAL TRANSFER FUNCTION (OTF)
 OVERALL UNCERTAINTY
 RANDOM UNCERTAINTY
 REFERENCE VALUE
 RELATIVE INTRINSIC ERROR
 RESIDUAL RISK
 RISK
 SAFETY
 SAFETY FACTOR
 SAFETY HAZARD
 SAFETY INTEGRITY
 SCALE READING
 SEVERITY
 SINGLE FAULT CONDITION
 TRUE VALUE

**TESTING OF RADIOLOGICAL
 EQUIPMENT**

**Obligation and statement of
 compliance** **rm-74**

COMPLIANCE LEVEL OF IMMUNITY
 COMPLIANCE LEVEL
 SPECIFIC
 SPECIFIED

TECHNOLOGY

General **rm-80**

DESIGNED FOR
 DEVELOPMENT LIFE-CYCLE
 EMERGENCY TROLLEY
 EQUIPMENT
 HAND-HELD EQUIPMENT
 HARD COPY CAMERA
 HIGH VOLTAGE
 IEC 60601 TEST LEVEL
 IMAGE DISPLAY DEVICE
 INFORMATION TECHNOLOGY
 EQUIPMENT (ITE)
 LIFE SUPPORTING EQUIPMENT OR
 SYSTEM
 LOW VOLTAGE
 MEDICAL ELECTRICAL EQUIPMENT
 (REFERRED TO AS EQUIPMENT)
 MEDICAL ELECTRICAL SYSTEM
 MOBILE EQUIPMENT
 MODEL OR TYPE REFERENCE
 NATIONAL STANDARD
 PASSWORD
 PERFORMANCE CHARACTERISTIC
 PROGRAMMABLE ELECTRICAL
 MEDICAL SYSTEM (PEMS)
 PROGRAMMABLE ELECTRONIC
 SUBSYSTEM (PESS)
 PROGRAMMABLE ELECTRONIC
 SYSTEM (PES)
 PROPERLY INSTALLED
 PUBLIC MAINS NETWORKS
 RATED (VALUE)
 RADIO FREQUENCY (RF)
 TOOL
 VOLTAGE RIPPLE

TECHNOLOGY
Documentation **rm-82**
 ACCOMPANYING DOCUMENTS
 ASSEMBLING INSTRUCTIONS
 ESTABLISHED CRITERIA
 INSTRUCTIONS FOR USE
 NORMAL USE
 RISK MANAGEMENT FILE
 RISK MANAGEMENT SUMMARY
 WORKING STANDARD

TECHNOLOGY
EQUIPMENT **rm-83**
 ACCESS COVER
 ACCESSIBLE CONDUCTIVE PARTS
 ACCESSIBLE METAL PART
 ACCESSIBLE PART
 ACCESSIBLE SURFACE
 ACCESSORY
 ADDRESS PILE UP
 AIR CLEARANCE
 BASIC INSULATION
 CATEGORY AP EQUIPMENT
 CATEGORY APG EQUIPMENT
 CLASS I EQUIPMENT
 CLASS II EQUIPMENT
 COLD CONDITION
 CONDUCTIVE CONNECTION
 CONTINUOUS OPERATION
 CONTINUOUS OPERATION WITH
 INTERMITTENT LOADING
 CONTINUOUS OPERATION WITH SHORT-
 TIME LOADING
 CONTROL PANEL
 CONTROLLING TIMER
 CREEPAGE DISTANCE
 DEFIBRILLATION-PROOF APPLIED
 PART
 DETACHABLE POWER SUPPLY CORD
 DIRECT CARDIAC APPLICATION

DISINFECTABLE EQUIPMENT
 DOUBLE INSULATION
 EARTH LEAKAGE CURRENT
 ELECTROMAGNETIC COMPATIBILITY
 (ABBREVIATION EMC)
 ELECTROMAGNETIC DISTURBANCE
 ELECTROMAGNETIC EMISSION
 ELECTROMAGNETIC ENVIRONMENT
 ELECTROMAGNETIC NOISE
 ELECTROSTATIC DISCHARGE: (ESD)
 EMISSION (ELECTROMAGNETIC)
 ENCLOSURE
 ENCLOSURE LEAKAGE CURRENT
 EXTERNAL TERMINAL DEVICE
 EXCLUSION BAND
 FIXED EQUIPMENT
 FIXED MAINS SOCKET OUTLET
 FIXED SETTING (OF A CONTROL OR
 LIMITING DEVICE)
 FLAMMABLE ANAESTHETIC MIXTURE
 WITH AIR
 FLAMMABLE ANAESTHETIC MIXTURE
 WITH OXYGEN OR NITROUS OXIDE
 F-TYPE ISOLATED (FLOATING) APPLIED
 PART (F-TYPE APPLIED PART)
 FUNCTION (OF AN EQUIPMENT
 AND/OR SYSTEM)
 FUNCTIONAL EARTH CONDUCTOR
 FUNCTIONAL EARTH TERMINAL
 HARD-WIRED
 IMMUNITY (TO A DISTURBANCE)
 INTERCONNECTION TERMINAL
 DEVICE
 INTERLOCK
 INTERNAL ELECTRICAL POWER
 SOURCE
 INTERNALLY POWERED EQUIPMENT
 LARGE EQUIPMENT AND/OR SYSTEM
 LEAKAGE CURRENT
 LIVE

MAINS CONNECTOR
 MAINS PART
 MAINS PLUG
 MAINS TERMINAL DEVICE
 OVER-CURRENT RELEASE
 OPERATING FREQUENCY
 PATIENT AUXILIARY CURRENT
 PATIENT CIRCUIT
 PATIENT CONNECTION
 PATIENT ENVIRONMENT
 PATIENT LEAKAGE CURRENT
 PERMANENTLY INSTALLED
 EQUIPMENT
 PHYSIOLOGICAL SIMULATION
 FREQUENCY
 PORTABLE EQUIPMENT
 POTENTIAL EQUALIZATION
 CONDUCTOR
 POWER SUPPLY CORD
 PRESSURE (OVERPRESSURE)
 PROTECTIVE COVER
 PROTECTIVE EARTH CONDUCTOR
 PROTECTIVE EARTH TERMINAL
 PROTECTIVELY EARTHED
 QUENCH
 REINFORCED INSULATION
 SAFETY DEVICE
 SAFETY EXTRA-LOW VOLTAGE
 (SELV)
 SAFETY EXTRA-LOW VOLTAGE
 TRANSFORMER
 SECONDARY TIMER
 SELF-RESETTING THERMAL CUT-OUT
 SEPARATION DEVICE
 SERIAL NUMBER
 SHORT-TIME OPERATION
 SIGNAL INPUT PART
 SIGNAL OUTPUT PART
 STATIC LOAD
 STATIONARY EQUIPMENT

STERILIZABLE EQUIPMENT
 SUPPLEMENTARY INSULATION
 SUPPLY EQUIPMENT
 SUPPLY MAINS
 SURFACE DOSE
 TERMINAL DEVICE
 THERMAL CUT-OUT
 THERMOSTAT
 TIMING DEVICE
 TOTAL LOAD
 TRANSPORTABLE EQUIPMENT
 TYPE B APPLIED PART
 TYPE BF APPLIED PART
 TYPE CF APPLIED PART

TECHNOLOGY
Operation of
EQUIPMENT **rm-84**
 ADJUSTABLE SETTING (OF A CONTROL
 OR LIMITING DEVICE)
 APPLIED PART
 AUXILIARY MAINS SOCKET-OUTLET
 DEGRADATION (OF PERFORMANCE)
 DISPLAY
 DUTY CYCLE
 INFLUENCE QUANTITY
 INTERMITTENT OPERATION
 MAXIMUM PERMISSIBLE WORKING
 PRESSURE
 MEDICAL SUPERVISION
 MODE OF OPERATION
 PREPARATORY STATE
 READY STATE
 SAFE WORKING LOAD
 STAND-BY STATE
 TRANSFER

TECHNOLOGY
Persons **rm-85**
 MANUFACTURER
 OPERATOR

PATIENT
 QUALIFIED PERSON
 USER

MAGNETIC RESONANCE
General rm-90
 COMPLIANCE VOLUME
 CONTROLLED ACCESS AREA
 EFFECTIVE STIMULATION DURATION (TS)
 EMERGENCY FIELD SHUT DOWN UNIT
 FIRST LEVEL CONTROLLED
 OPERATING MODE
 GRADIENT OUTPUT
 GRADIENT UNIT
 HEAD RF TRANSMIT COIL
 HEAD SAR
 LOCAL RF TRANSMIT COIL
 LOCAL SAR
 MAGNETIC RESONANCE (MR)
 MAGNETIC RESONANCE EQUIPMENT
 (MR EQUIPMENT)
 MAGNETIC RESONANCE EXAMINATION
 (MR EXAMINATION)
 MAGNETIC RESONANCE SYSTEM
 (MR SYSTEM)
 NORMAL OPERATING MODE
 PARTIAL BODY SAR
 ROUTINE MONITORING
 SEARCH COIL
 SECOND LEVEL CONTROLLED
 OPERATING MODE
 SPECIAL PURPOSE GRADIENT
 SYSTEM
 SPECIFIC ABSORPTION RATE(SAR)
 TIME RATE OF CHANGE OF THE
 MAGNETIC FIELD (dB/dt)
 TRANSVERSE FIELD MAGNET
 VOLUME RF TRANSMIT COIL
 WHOLE BODY GRADIENT SYSTEM
 WHOLE BODY MAGNET

WHOLE BODY MAGNETIC RESONANCE
 EQUIPMENT (WHOLE BODY MR
 EQUIPMENT)
 WHOLE BODY RF TRANSMIT COIL
 WHOLE BODY SAR

ULTRASOUND
General rm-100
 -12 dB OUTPUT BEAM AREA
 -12 dB OUTPUT BEAM DIMENSIONS
 ACOUSTIC ATTENUATION
 COEFFICIENT
 ACOUSTIC WORKING FREQUENCY
 APPLIANCE COUPLER
 APPLIANCE INLET
 APPLICATION DISTANCE
 APPLICATION LIMITS
 APPLICATION PLANE
 ATTENUATED BEAM
 ATTENUATED BEAM QUALITY
 ATTENUATED OUTPUT POWER
 ATTENUATED PEAK-RAREFACTIONAL
 ACOUSTIC PRESSURE
 ATTENUATED PULSE-AVERAGE
 INTENSITY
 ATTENUATED PULSE-INTENSITY
 INTEGRAL
 ATTENUATED SPATIAL-PEAK
 TEMPORAL-AVERAGE INTENSITY
 ATTENUATED TEMPORAL-AVERAGE
 INTENSITY
 BEAM ALIGNMENT AXIS
 BEAM AREA
 BONE THERMAL INDEX
 BOUNDED OUTPUT POWER
 BREAK-POINT DEPTH
 COMBINED-OPERATING MODE
 CRANIAL-BONE THERMAL INDEX
 DEPTH FOR TIB
 DEPTH FOR TIS

DEPTH OF DOSE MAXIMUM
 DISCRETE-OPERATING MODE
 EQUIVALENT BEAM DIAMETER
 EQUIVALENT APERTURE DIAMETER
 EQUIVALENT BEAM AREA
 FULL SOFTWARE CONTROL OF
 ACOUSTIC OUTPUT
 MAXIMUM GRADIENT SLEW RATE
 MECHANICAL INDEX
 MULTI-PURPOSE ULTRASONIC
 EQUIPMENT
 NON-SCANNING MODE
 OUTPUT POWER
 PEAK-RAREFACTIONAL ACOUSTIC
 PRESSURE
 PULSE AVERAGE INTENSITY
 PULSE BEAM-WIDTH
 PULSE DURATION
 PULSE-INTENSITY INTEGRAL
 PULSE REPETITION RATE
 PULSE-PRESSURE-SQUARED
 INTEGRAL
 SCANNING MODE
 SOFT TISSUE THERMAL IINDEX
 SPATIAL-PEAK TEMPORAL-AVERAGE
 INTENSITY
 THERMAL INDEX
 TRANSDUCER ASSEMBLY
 TRANSMIT PATTERN
 ULTRASONIC DIAGNOSTIC
 EQUIPMENT
 ULTRASONIC TRANSDUCER

-12 DB OUTPUT BEAM AREA
-12 DB OUTPUT BEAM DIMENSIONS

A

ABSORBED DOSE
ABSORBED DOSE RATE
ABSORBED DOSE RATE TO WATER
ABSORBED DOSE TO WATER
ABSORPTION
ACCEPTANCE TEST
ACCESS COVER
ACCESSIBLE CONDUCTIVE PARTS
ACCESSIBLE METAL PART
ACCESSIBLE PART
ACCESSIBLE SURFACE
ACCESSORY
ACCOMPANYING DOCUMENTS
ACOUSTIC ATTENUATING COEFFICIENT
ACOUSTIC WORKING FREQUENCY
ACTIVE ELECTRODE
ACTIVITY
ACTUAL FOCAL SPOT
ADDED FILTER
ADDITIONAL FILTRATION
ADDRESS PILE UP
ADJUSTABLE SETTING (OF A CONTROL
OR LIMITING DEVICE)
ADMINISTRATION SET
ADMINISTRATION SET CHANGE
INTERVAL
AFTERLOADING
AIR CLEARANCE
AIR CONTROLLED INCUBATOR
AIR CONTROLLED TRANSPORT
INCUBATOR
AIR KERMA
AIR KERMA LENGTH
AIR KERMA RATE
AIR-DENSITY CHARACTERISTIC
ALARM
ALARM CONDITION
ALARM LIMIT
ALARM SIGNAL
ALARM SYSTEM

AMBULATORY
ELECTROCARDIOGRAPHIC SYSTEM
(EQUIPMENT)
AMBULATORY RECORDER
ANAESTHETIC GAS DELIVERY SYSTEM
ANAESTHETIC GAS DELIVERY SYSTEM
PIPING
ANAESTHETIC SYSTEM (ANAESTHETIC
WORKSTATION)
ANAESTHETIC VAPOUR DELIVERY
DEVICE
ANAESTHETIC VENTILATOR
ANALYSING ELECTROCARDIOGRAPH
ANNIHILATION RADIATION
ANNUNCIATION
ANODE
ANODE COOLING CURVE
ANODE ANGLE
ANODE HEAT CONTENT
ANODE HEATING CURVE
ANODE INPUT POWER
ANODE SPEED
ANTI-SCATTER GRID
APPARENT RESISTANCE OF SUPPLY
MAINS
APPLIANCE COUPLER
APPLIANCE INLET
APPLICATION DISTANCE
APPLICATION LIMITS
APPLICATION PLANE
APPLICATOR
APPLIED PART
APPLIED PART INTERFACE
ARTEFACT
ARTIFACT
ARTERIAL PRESSURE
ASSEMBLING INSTRUCTIONS
ASSOCIATED EQUIPMENT
ATTACHMENT HEAD
ATTENUATED BEAM
ATTENUATED BEAM QUALITY
ATTENUATED OUTPUT POWER

ATTENUATED PEAK-RAREFACTIONAL
ACOUSTIC PRESSURE
ATTENUATED PULSE-AVERAGE
INTENSITY
ATTENUATED PULSE-INTENSITY
INTEGRAL
ATTENUATED SPATIAL-PEAK
TEMPORAL-AVERAGE INTENSITY
ATTENUATED TEMPORAL-AVERAGE
INTENSITY
ATTENUATION
ATTENUATION COEFFICIENT
ATTENUATION EQUIVALENT
ATTENUATION RATIO
AUDITORY STIMULATOR
AUDITORY STIMULATOR
AUTOMATIC CONTROL SYSTEM
AUTOMATIC CYCLING NON-INVASIVE
BLOOD PRESSURE MONITORING
EQUIPMENT
AUTOMATIC EXPOSURE CONTROL
AUTOMATIC EXPOSURE RATE
CONTROL
AUTOMATIC INTENSITY CONTROL
AUXILIARY MAINS SOCKET-OUTLET
AVERAGE INCUBATOR TEMPERATURE
AVERAGE TEMPERATURE
AVERAGE TRANSPORT INCUBATOR
TEMPERATURE
AXIAL FIELD OF VIEW
AXIAL POINT SPREAD FUNCTION
AXIAL RESOLUTION
AXIAL SLICE WIDTH

B

BABY COMPARTMENT
BABY CONTROLLED INCUBATOR
BABY CONTROLLED MODE
BABY CONTROLLED TRANSPORT
INCUBATOR
BACK POINTER
BACK-SCATTERING

BACTERIAL FILTER
BASE DEPTH
BASELINE VALUE
BASIC INSULATION
BEAM ALIGNMENT AXIS
BEAM AREA
BEAM APPLICATOR
BEAM LIMITING DEVICE
BEAM LIMITING SYSTEM
BEAM NON-UNIFORMITY RATIO
BEAM OFF
BEAM ON
BEAM SCATTERING FILTER
BEAM TYPE
BEAM-AREA
BEST FOCUS
BIOPOTENTIAL INPUT PART
BIPOLAR ELECTRODE
BLANKET
BLOOD LEAK
BLOOMING VALUE
BOLUS
BONE THERMAL INDEX
BOUNDARY AND DIMENSIONS OF THE
X-RAY FIELD
BOUNDED OUTPUT POWER
BRACHYRADIOTHERAPY
BRACHYTHERAPY SOURCE MODEL
BREAK-POINT DEPTH
BROAD BEAM
BROAD BEAM CONDITION
BUILD UP
BUFFER-FREE HAEMODIAFILTRATION
BUILD UP FACTOR
BURST

C

CALIBRATION ("CAL")
CALIBRATION FACTOR
CALIBRATION INTERVAL
CALIBRATION VOLTAGE
CAPACITIVELY COUPLED HF CURRENT

CAPACITOR DISCHARGE HIGH-VOLTAGE GENERATOR
CAPSULE
CARDIAC DEFIBRILLATOR
CARDIAC DEFIBRILLATOR-MONITOR
CASSETTE CHANGER
CATEGORY AP EQUIPMENT
CATEGORY APG EQUIPMENT
CATHETER TIP TRANSDUCER
CATHODE
CATHODE EMISSION CHARACTERISTIC
CENTRAL AXIS
CENTRAL ILLUMINANCE
CENTRAL LINE INDICATION
CENTRAL MAGNIFICATION
CENTRAL TERMINAL ACCORDING TO WILSON (CT)
CENTRE OF ROTATION (COR)
CENTRE OF THE ENTRANCE FIELD
CENTRE OF THE OUTPUT IMAGE
CERENKOV COUNTER
CERTIFIED RADIOACTIVE STANDARD SOURCE
CHAMBER (IONIZATION)
CHAMBER ASSEMBLY
CHANNEL
CHARGING CIRCUIT
CINERADIOGRAPHY
CLASS I EQUIPMENT
CLASS II EQUIPMENT
CLEARLY LEGIBLE
COAGULATION
COEFFICIENT OF VARIATION
COINCIDENCE DETECTION
COINCIDENCE WINDOW
COLD CONDITION
COLLIMATOR (FOR GAMMA CAMERAS)
COLLIMATOR AXIS
COLLIMATOR BACK FACE
COLLIMATOR FRONT FACE
COMBINED-OPERATING MODE
COMBINED STANDARD UNCERTAINTY
COMMON MODE DC OFFSET VOLTAGE

COMMON MODE REJECTION
COMPLIANCE VOLUME
COMPOSITION OF REFERENCE MATERIALS
COMPRESSION DEVICE
COMPUTED TOMOGRAPHY
COMPUTED TOMOGRAPHY DOSE INDEX (CTDI)
COMPUTED TOMOGRAPHY DOSE INDEX 100 (CTDI100)
COMPUTED TOMOGRAPHY NUMBER (CT NUMBER)
CONDITIONS OF ADEQUATE HEAT DISCHARGE
CONDUCTIVE CONNECTION
CONSTANCY TEST
CONSTANT POTENTIAL HIGH-VOLTAGE GENERATOR
CONTACT SURFACE TEMPERATURE
CONTINUATION
CONTINUOUS MODE
CONTINUOUS OPERATION
CONTINUOUS OPERATION WITH INTERMITTENT LOADING
CONTINUOUS OPERATION WITH SHORT-TIME LOADING
CONTINUOUS RECORDER
CONTRAST IMPROVEMENT RATIO
CONTRAST INDEX
CONTRAST RATIO
CONTROL PANEL
CONTROL SIDE RAIL
CONTROL TEMPERATURE
CONTROLLED ACCESS AREA
CONTROLLED AREA
CONTROLLING TIMER
CONVENTIONAL TRUE VALUE
CONVERGING COLLIMATOR
CONVERSION FACTOR
COORDINATE SYSTEM OF PROJECTION
CORE BIOPSY GUN
CORRECTION FACTOR
COUNT LOSS

COUNT RATE
COUNT RATE CHARACTERISTIC
CRANIAL-BONE THERMAL INDEX
CREEPAGE DISTANCE
CROSS GRID
CT CONDITIONS OF OPERATION
CT DETECTOR
CT DOSIMETER
CT PITCH FACTOR
CT SCANNER
CURRENT TIME PRODUCT
CUTTING

D
DAS CONTRAST SENSITIVITY
DAS VISUAL SPATIAL RESOLUTION
DECENTRING OF A FOCUSED GRID
DECREASING INPUT POWER RATING
DEFAULT SETTING
DEFIBRILLATION-PROOF APPLIED PART
DEFOCUSING OF A FOCUSED GRID
DEGRADATION (OF PERFORMANCE)
DELINEATED LIGHT FIELD
DELINEATED RADIATION BEAM
DELINEATED RADIATION FIELD
DELINEATOR
DELIVERED ENERGY
DENTAL PANORAMIC RADIOGRAPHY
DEPTH DOSE
DEPTH FOR BONE THERMAL INDEX
DEPTH FOR SOFT TISSUE THERMAL INDEX
DEPTH OF DOSE MAXIMUM
DEPTH OF ILLUMINATION
DESIGNED FOR
DETACHABLE POWER SUPPLY CORD
DETECTIVE QUANTUM EFFICIENCY (ABBREVIATION DQE)
DETECTOR ASSEMBLY
DETECTOR FIELD OF VIEW (FOV)
DETECTOR HEAD
DETECTOR HEAD TILT

DETECTOR LINE SPREAD FUNCTION
DETECTOR POSITIONING TIME
DETECTOR SHIELD
DEVELOPMENT LIFE-CYCLE
DIAPHRAGM
DIALYSER
DIALYSING FLUID
DIALYSING FLUID CONCENTRATE
DIALYSING SOLUTION
DIFFERENTIAL RADIAL IMAGE
DISTORTION
DIRECT CARDIAC APPLICATION
DIRECT FOCAL DISTANCE
DIRECT RADIOGRAM
DIRECT RADIOGRAPHY
DIRECT RADIOSCOPY
DISABLE
DISCHARGE CIRCUIT
DISCHARGE CONTROL CIRCUIT
DISCRETE-OPERATING MODE
DISINFECTABLE EQUIPMENT
DISPLAY
DIVERGING COLLIMATOR
DOME
DOSE AREA PRODUCT
DOSE AREA PRODUCT METER
DOSE AREA PRODUCT RATE
DOSE EQUIVALENT
DOSE EQUIVALENT LIMIT
DOSE MONITOR UNIT
DOSE MONITORING SYSTEM
DOSE PROFILE
DOSE RATE MONITORING SYSTEM
DOSEMETER
DOSEMETER (PATIENT CONTACT)
DOSIMETER (DIAGNOSTIC)
DOSIMETER (RADIOTHERAPY)
DOUBLE EMULSION FILM
DOUBLE INSULATION
DRIFT
DRIP-RATE INFUSION CONTROLLER
DRIP-RATE INFUSION PUMP
DUMMY COMPONENT

DUTY CYCLE
DUTY FACTOR
DYNAMIC RANGE

E
EARTH LEAKAGE CURRENT
ECG RECORD
EDGE FILTER
EFFECTIVE APERTURE
EFFECTIVE FOCAL SPOT
EFFECTIVE IMAGE RECEPTION AREA
EFFECTIVE INTENSITY
EFFECTIVE LENGTH
EFFECTIVE RADIATED POWER (ERP)
EFFECTIVE RADIATING AREA
EFFECTIVE RANGE
EFFECTIVE RANGE (OF INDICATED VALUES)
EFFECTIVE RECORDING WIDTH
EFFECTIVE SURFACE AREA
ELECTRICAL STIMULATOR
ELECTRICALLY OPERATED HOSPITAL BED
ELECTROCARDIOGRAM (ECG)
ELECTROCARDIOGRAPH (ECG)
ELECTROCARDIOGRAPHIC (ECG) MONITORING EQUIPMENT
ELECTRODE
ELECTROENCEPHALOGRAM (EEG)
ELECTROENCEPHALOGRAPH (EEG)
ELECTROMAGNETIC COMPATIBILITY (ABBREVIATION EMC)
ELECTROMAGNETIC DISTURBANCE
ELECTROMAGNETIC EMISSION
ELECTROMAGNETIC ENVIRONMENT
ELECTROMAGNETIC NOISE
ELECTROMYOGRAPH
ELECTRON
ELECTRON BEAM APPLICATOR
ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER
ELECTROSTATIC DISCHARGE: (ESD)
EMERGENCY AIR INTAKE PORT

EMERGENCY FIELD SHUT DOWN UNIT
EMERGENCY TROLLEY
EMISSION (ELECTROMAGNETIC)
EMISSION COMPUTED TOMOGRAPHY (ECT)
ENCLOSURE
ENCLOSURE LEAKAGE CURRENT
ENDOSCOPE
ENDOSCOPIC EQUIPMENT
ENDOSCOPICALLY-USED ACCESSORY
ENERGY CALIBRATION
ENERGY FLUENCE RATE
ENERGY METER/DEFIBRILLATOR TESTER
ENERGY RESOLUTION
ENTRANCE FIELD
ENTRANCE FIELD OF A COLLIMATOR
ENTRANCE FIELD SIZE
ENTRANCE PLANE
ENERGY STORAGE DEVICE
ENTRANCE SURFACE
EQUILIBRATION TIME
EQUIPMENT
EQUIVALENT BEAM DIAMETER
EQUIPMENT ELECTRODE
EQUIPMENT FOR EXTRACORPOREALLY INDUCED LITHOTRIPSY
EQUIPMENT MODEL / EQUIPMENT MODELLING
EQUIVALENT ANODE INPUT POWER
EQUIVALENT APERTURE DIAMETER
EQUIVALENT BEAM AREA
EQUIVALENT WIDTH (EW)
ESSENTIAL PERFORMANCE (OF AN EQUIPMENT OR SYSTEM)
ERROR OF MEASUREMENT
ESTABLISHED CRITERIA
EVOKED RESPONSE EQUIPMENT
EXAMINATION ROOM
EXCLUSION BAND
EXIT FIELD OF A COLLIMATOR
EXIT SURFACE
EXPANDED UNCERTAINTY

EXPOSURE
EXPOSURE METER
EXPOSURE RATE
EXTERNAL PACEMAKER
EXTERNAL TERMINAL DEVICE
EXTRACORPOREAL CIRCUIT
EXTRACORPOREALLY INDUCED LITHOTRIPSY
EXTRA-FOCAL RADIATION

F
FAIL SAFE
FIELD FLATTENING FILTER
FIELD SIZE
FIELD-CLASS DOSIMETER
FILAMENT CURRENT
FILM BASE PLUS FOG DENSITY
FILM CHANGER
FILM ILLUMINATOR
FILM PROCESSOR
FILTER
FILTRATION
FIRST LEVEL CONTROLLED OPERATING MODE
FIXED COORDINATE SYSTEM
FIXED EQUIPMENT
FIXED MAINS SOCKET OUTLET
FIXED SETTING (OF A CONTROL OR LIMITING DEVICE)
FLAMMABLE ANAESTHETIC MIXTURE WITH AIR
FLAMMABLE ANAESTHETIC MIXTURE WITH OXYGEN OR NITROUS OXIDE
FLOW-DIRECTION-SENSITIVE COMPONENT
FLUORESCENT SCREEN
FOCAL RADIATION
FOCAL SPOT
FOCAL SPOT PINHOLE RADIOGRAM
FOCAL SPOT SLIT RADIOGRAM
FOCAL SPOT STAR RADIOGRAM
FOCAL SPOT TO IMAGE RECEPTOR DISTANCE

FOCAL SPOT TO SKIN DISTANCE
FOCAL TRACK
FOCAL VOLUME
FOCUSED GRID
FOCUSING DISTANCE
FREE FLOW
FREQUENT USE DEFIBRILLATOR
FRESH GAS
FRESH GAS INTAKE PORT
FRONT POINTER
F-TYPE ISOLATED (FLOATING) APPLIED PART (F-TYPE APPLIED PART)
FULL SOFTWARE CONTROL OF ACOUSTIC OUTPUT
FULLWIDTH AT HALF MAXIMUM (FWHM)
FULL WIDTH AT TENTH MAXIMUM (FWTM)
FUNCTION (OF AN EQUIPMENT OR SYSTEM)
FUNCTIONAL EARTH CONDUCTOR
FUNCTIONAL EARTH TERMINAL

G
GAMMA CAMERA
GAMMA CAMERA BASED WHOLEBODY IMAGING SYSTEM
GANTRY
GAS CONCENTRATION
GAS EXHAUST PORT
GAS INTAKE PORT
GAS OUTPUT PORT
GEOMETRICAL FIELD SIZE
GEOMETRICAL RADIATION RADIATION FIELD
GRADIENT OUTPUT
GRADIENT UNIT
GRID EXPOSURE FACTOR
GRID RATIO
GRID SELECTIVITY

H
 HAEMODIALYSIS,
 HAEMODIAFILTRATION AND/OR
 HAEMOFILTRATION EQUIPMENT
 HAEMODIALYSIS (HD)
 HAEMOFILTRATION (HF)
 HAEMODIAFILTRATION (HDF)
 HALF VALUE LAYER TEST DEVICE
 HALF-VALUE LAYER
 HAND-HELD EQUIPMENT
 HARD COPY CAMERA
 HARD-WIRED
 HARM
 HAZARD
 HAZARD ANALYSIS
 HAZARDOUS SITUATION
 HEAD/FOOT PANEL ASSEMBLY
 HEAD RF TRANSMIT COIL
 HEAD SAR
 HEATING DEVICE
 HIGH-CONTRAST RESOLUTION
 HIGH FREQUENCY SURGICAL
 EQUIPMENT
 HIGH HEAT TRANSFER
 HIGH PRESSURE GAS INPUT PORT
 HIGH VOLTAGE
 HIGH-VOLTAGE CABLE CONNECTION
 HIGH-VOLTAGE GENERATOR
 HIGH-VOLTAGE TRANSFORMER
 ASSEMBLY
 HYDRAULIC TEST PRESSURE

I
 IEC 60601 TEST LEVEL
 IMAGE DISPLAY DEVICE
 IMAGE DISTORTION
 IMAGE MATRIX
 IMAGE PLANE
 IMAGE RECEPTION AREA
 IMAGE RECEPTION PLANE
 IMAGE RECEPTOR PLANE IN X-RAY
 IMAGE INTENSIFIER TUBES
 IMMUNITY (TO A DISTURBANCE)

IMMUNITY COMPLIANCE LEVEL
 IMMUNITY LEVEL
 IMMUNITY TEST LEVEL
 IN VITRO COUNTING SYSTEM
 IN VIVO COUNTING SYSTEM
 INCUBATOR
 INCUBATOR TEMPERATURE
 INDICATED VALUE
 INDIRECT RADIOGRAM
 INDIRECT RADIOGRAPHY
 INDIRECT RADIOSCOPY
 INDUCED RADIOACTIVITY
 INFANT PHOTOTHERAPY EQUIPMENT
 INFANT RADIANT WARMER
 INFLATING GAS
 INFLATING GAS INPUT PORT
 INFLOW
 INFLUENCE QUANTITY
 INFORMATION TECHNOLOGY
 EQUIPMENT (ABBREVIATION ITE)
 INFREQUENT USE DEFIBRILLATOR
 INFUSION CONTROLLER
 INFUSION PUMP
 INFUSION PUMP FOR AMBULATORY USE
 INHERENT FILTRATION
 INHIBITION
 INITIAL CONSTANCY TEST FILM
 INITIAL REFERENCE FILM
 INITIAL X-RAY TUBE VOLTAGE
 INITIATION
 INPUT APERTURE
 INPUT SCREEN
 INSTRUCTIONS FOR USE
 INSTRUMENT ACCURACY
 INSTRUMENT PARAMETER
 INTEGRAL IMAGE DISTORTION
 INTEGRAL MAGNIFICATION
 INTEGRATED PATIENT
 MONITORING/COMMUNICATIONS
 SYSTEMS CONTROL SIDE RAIL
 INTENDED USE / INTENDED PURPOSE
 INTENSIFYING SCREEN

INTERCHANGEABLE ANAESTHETIC
 VAPOUR DELIVERY DEVICE
 INTERCONNECTION CONDITIONS
 INTERCONNECTION TERMINAL DEVICE
 INTERLOCK
 INTERMEDIATE RATE
 INTERMITTENT MODE
 INTERMITTENT OPERATION
 INTERNAL DISCHARGE CIRCUIT
 INTERNAL ELECTRICAL POWER
 SOURCE
 INTERNALLY POWERED EQUIPMENT
 INTERRUPTION
 INTERRUPTION (OF IRRADIATION)/TO
 INTERRUPT (IRRADIATION)
 INTERSTITIAL RADIOTHERAPY
 INTERVENTIONAL REFERENCE POINT
 INTERVENTIONAL X-RAY EQUIPMENT
 INTRACAVITARY RADIOTHERAPY
 INTRINSIC ENERGY RESOLUTION
 INTRINSIC ENERGY SPECTRUM
 INTRINSIC ERROR
 INTRINSIC LINE SPREAD FUNCTION
 INTRINSIC NON-UNIFORMITY OF
 RESPONSE
 INTRINSIC SPATIAL NON-LINEARITY
 INVASIVE MEASUREMENT
 IONIZATION CHAMBER
 IONIZATION CHAMBER TEST SOURCE
 IONIZING RADIATION
 IONIZING RADIATION SHIELD
 IRRADIATION
 IRRADIATION FIELD SIZE
 IRRADIATION SWITCH
 IRRADIATION TIME
 IRRADIATION TREATMENT
 PRESCRIPTION
 ISOCENTRE
 ISOCENTRIC
 ISOCENTRIC EQUIPMENT
 ISOCENTRIC TREATMENT
 ISOPLANATIC REGION

K
 KEEP OPEN RATE (KOR)
 KERMA
 KERMA RATE

L
 LARGE EQUIPMENT OR SYSTEM
 LATCHED ALARM
 LEAD (S)LEAD EQUIVALENT
 LEAD SELECTOR
 LEAD WIRE(S)
 LEAKAGE CURRENT
 LEAKAGE CURRENT (CHAMBER
 ASSEMBLY)
 LEAKAGE RADIATION
 LEGIBLE
 LIFE SUPPORTING EQUIPMENT OR
 SYSTEM
 LIFTING POLE
 LIGHT DETECTOR
 LIGHT EMISSION PART
 LIGHT FIELD
 LIGHT FIELD CENTRE
 LIGHT FIELD DIAMETER
 LIGHT FIELD -INDICATOR
 LIMITED X-RAY TUBE VOLTAGE
 LIMITS OF VARIATION
 LINE OF RESPONSE (LOR)
 LINE PAIR RESOLUTION
 LINE SOURCE
 LINE SPREAD FUNCTION (LSF)
 LINEAR GRID
 LINEAR RANGE
 LINEARITY
 LIQUID SCINTILLATION COUNTER
 LITHOTRIPSY
 LIVE
 LOADING
 LOADING FACTOR
 LOADING STATE
 LOADING TIME

LOCAL RADIAL MAGNIFICATION
LOCAL RF TRANSMIT COIL
LOCAL SAR
LOCALIZATION DEVICE
LONG TERM AUTOMATIC MODE
LOW CONTRAST RESOLUTION
LOW HEAT TRANSFER
LOW-FREQUENCY DROP (LFD)
LOW POWER EQUIPMENT
LOW-PRESSURE GAS INPUT PORT
LOW VOLTAGE
LUMINAIRE FOR DIAGNOSIS
LUMINANCE DISTRIBUTION
LUMINANCE NON-UNIFORMITY

M

MAGNETIC RESONANCE
MAGNETIC RESONANCE EQUIPMENT
(MR EQUIPMENT)
MAGNETIC RESONANCE EXAMINATION
(MR EXAMINATION)
MAGNETIC RESONANCE SYSTEM (MR
SYSTEM)
MAINS CONNECTOR
MAINS PART
MAINS PLUG
MAINS TERMINAL DEVICE
MAINS VOLTAGE
MAJOR SURGICAL LUMINAIRE
MAMMOGRAPHIC ANTI SCATTER GRID
MAMMOGRAPHIC STEREOTACTIC
DEVICE
MANUAL DEFIBRILLATOR
MANUAL MODE
MANUAL VENTILATION PORT
MANUFACTURER
MATCHED LOAD
MATTRESS
MATTRESS SUPPORT PLATFORM
MATRIX ELEMENT
MAXIMUM ANODE HEAT CONTENT

MAXIMUM CONTINUOUS HEAT
DISSIPATION
MAXIMUM ENERGY
MAXIMUM GRADIENT SLEW RATE
MAXIMUM INFUSION PRESSURE
MAXIMUM LIMITED PRESSURE
(P_{limmax})
MAXIMUM PEAK VOLTAGE
MAXIMUM PERMISSIBLE WORKING
PRESSURE
MAXIMUM TOLERABLE RISK
MAXIMUM TRACKING RATE
MAXIMUM WORKING PRESSURE
(P_{wmax})
MAXIMUM X-RAY TUBE ASSEMBLY
HEAT CONTENT
MEAN CT NUMBER
MEAN PEAK VOLTAGE
MEASURED VALUE
MEASURING ASSEMBLY
MECHANICAL INDEX
MEDICAL DEVICE
MEDICAL DIAGNOSTIC RADIOLOGY
MEDICAL ELECTRICAL EQUIPMENT
(REFERRED TO AS EQUIPMENT)
MEDICAL ELECTRICAL SYSTEM
MEDICAL RADIOLOGICAL EXAMINATION
MEDICAL RADIOLOGY
MEDICAL SUPERVISION
MICROWAVE THERAPY EQUIPMENT
MID POINT AVERAGE TEMPERATURE
MINIMUM BREAKING LOAD
MINIMUM EFFECTIVE RANGE
MINIMUM LIMITED PRESSURE (P_{limmin})
MINIMUM RATE
MINIMUM RATED RANGE
MINOR SURGICAL LUMINAIRE
(TREATMENT LUMINAIRE)
MINUTE VOLUME (\dot{V})
MOBILE EQUIPMENT
MOBILE OPERATING TABLE
MODE OF OPERATION
MODEL OR TYPE REFERENCE

MODES OF OPERATION WITH
CONTINUED DISPLAY
MODULATION TRANSFER FUNCTION
(MTF)
MOMENTARY CONTACT SWITCH
MONITOR
MONITORING DEVICE
MOVING BEAM RADIOTHERAPY
MOVING GRID
MTF ANALYZER
MULTI-DETECTOR COUNTER
MULTIPLE WINDOW SPATIAL
REGISTRATION
MULTI-DETECTOR COUNTER
MULTI-PURPOSE ULTRASONIC
EQUIPMENT
MULTICHANNEL ELECTRO-
CARDIOGRAPH
MULTIFUNCTION PATIENT MONITORING
EQUIPMENT
MULTIPLE FUNCTION
MULTIPARAMETER PATIENT
MONITORING EQUIPMENT

N

NARROW BEAM
NARROW BEAM CONDITION
NATIONAL STANDARD
NET OPTICAL DENSITY
NEUTRAL ELECTRODE
NEUTRON
NOISE
NOMINAL (VALUE)
NOMINAL ANODE INPUT POWER
NOMINAL ELECTRIC POWER
NOMINAL ENERGY
NOMINAL ENTRANCE FIELD SIZE
NOMINAL FOCAL SPOT VALUE
NOMINAL IMAGE SIZE
NOMINAL SENSITIVITY

NOMINAL SHORTEST IRRADIATION
TIME
NOMINAL TOMOGRAPHIC SECTION
THICKNESS
NOMINAL TOMOGRAPHIC SLICE
THICKNESS
NOMINAL X-RAY TUBE VOLTAGE
NON-ISOCENTRIC
NON-LINEARITY
NON-FLAMMABLE ANAESTHETIC
AGENTS
NON-INVASIVE MEASUREMENT
NON-IRRADIATED CONSTANCY TEST
FILM
NON-INTERCHANGEABLE
ANAESTHETIC VAPOUR DELIVERY
DEVICE
NON-LATCHED ALARM
NON-IMPLANTABLE PULSE GENERATOR
NON-LATCHING ALARM SIGNAL
NON-SCANNING MODE
NON-SCREEN FILM
NON-UNIFORMITY OF RESPONSE
NORMAL CONDITION
NORMAL OPERATING MODE
NORMAL POSITION
NORMAL SENSITIVITY
NORMAL TREATMENT DISTANCE (NTD)
NORMAL USE
NORMALIZED SLICE SENSITIVITY
NORMALIZED VOLUME SENSITIVITY
NUCLEAR MEDICINE

O

OBJECT PROGRAMMED CONTROL
OBJECT SLICE
OBJECTIVE EVIDENCE
OBLIQUE CROSS GRID
OCCLUSION ALARM THRESHOLD
(PRESSURE)
OFFSET
ONE-PEAK HIGH-VOLTAGE
GENERATOR

OPERATING CABLE
OPERATING CONDITIONS FOR
NOMINAL X-RAY TUBE VOLTAGE
OPERATING FREQUENCY
OPERATOR
OPERATOR'S POSITION
OPTICAL TRANSFER FUNCTION (OTF)
ORGAN COUNTING SYSTEM
ORTHOGONAL CROSS GRID
OUTFLOW
-12 dB OUTPUT BEAM AREA
-12 dB OUTPUT BEAM DIMENSIONS
(NON-UNIFORM EXCITATION)
OUTPUT CIRCUIT
OUTPUT IMAGE
OUTPUT POWER
OUTPUT SCREEN
OVARY SHIELD
OVERALL UNCERTAINTY
OVER-CURRENT RELEASE
OVERLOAD TOLERANCE
OVER-BLANKET
OXYGEN RICH ENVIRONMENT

P

PAD
PARALLEL GRID
PARALLEL HOLE COLLIMATOR
PART LEAKAGE CURRENT
PARTIAL BODY SAR
PARTICLE ACCELERATOR
PASSWORD
PATIENT
PATIENT ANATOMY MODEL / ANATOMY
MODELLING
PATIENT AUXILIARY CURRENT
PATIENT CABLE
PATIENT CIRCUIT
PATIENT CONNECTION
PATIENT CONNECTION PORT (OF THE
VENTILATOR BREATHING SYSTEM)
PATIENT ELECTRODE

PATIENT END
PATIENT ENVIRONMENT
PATIENT EXTRAPMENT
PATIENT LEAKAGE CURRENT
PATIENT LINE
PATIENT SUPPORT
PATIENT SURFACE
PEAK-RAREFACTIONAL ACOUSTIC
PRESSURE
PENDANT CONTROL
PENETRATIVE QUALITY
PENUMBRA
PERCENTAGE RIPPLE
PERCENTAGE RIPPLE IN CONSTANT
POTENTIAL HIGH-VOLTAGE
GENERATORS
PERFORMANCE CHARACTERISTIC
PERITONEAL DIALYSIS
PERITONEAL DIALYSIS EQUIPMENT
PERMANENT FILTRATION
PERMANENTLY INSTALLED EQUIPMENT
PHANTOM
PHOTON
PHYSICAL POINT SPREAD FUNCTION
PHYSIOLOGICAL ALARM
PHYSIOLOGICAL MONITORING UNIT
PHYSIOLOGICAL SIMULATION
FREQUENCY
PILE-UP EFFECT
PINHOLE CAMERA
PIN-HOLE COLLIMATOR
PIXEL
PLAYBACK EQUIPMENT
POINT SOURCE
POINT SPREAD FUNCTION (PSF)
PORTABLE EQUIPMENT
POSITIONING DEVICE
POSITIONING TIME
POSITRON EMISSION TOMOGRAPH
POSITRON EMISSION TOMOGRAPHY
(PET)
POST-VENTRICULAR ATRIAL
REFRACTOR PERIOD (PVARP)

POTENTIAL EQUALIZATION
CONDUCTOR
POWER SUPPLY
POWER SUPPLY CORD
PRACTICAL PEAK POTENTIAL (PPP)
PRACTICAL RANGE
PREPARATORY STATE
PRESSURE (OVERPRESSURE)
PRESSURE PULSE
PRESSURE PULSE COUPLING
PRIMARY DOSE MONITORING SYSTEM
PRIMARY PROTECTIVE SHIELDING
PRIMARY RADIATION
PRIMARY TIMER
PRIMARY/SECONDARY (TIMER)
COMBINATION
PRIMARY/SECONDARY DOSE
MONITORING COMBINATION
PRIMARY-SECONDARY DOSE
MONITORING SYSTEM
PROCEDURE
PROCESS
PROFILE PUMP
PROGRAMMABLE ELECTRICAL
MEDICAL SYSTEM (PEMS)
PROGRAMMABLE ELECTRONIC
SUBSYSTEM (PESS)
PROGRAMMABLE ELECTRONIC SYSTEM
(PES)
PROJECTION
PROJECTION ANGLE
PROJECTION BEAM
PROPERLY INSTALLED
PROTECTED AREA
PROTECTION DEVICE
PROTECTIVE BARRIER
PROTECTIVE COVER
PROTECTIVE DEVICE
PROTECTIVE EARTH CONDUCTOR
PROTECTIVE EARTH TERMINAL
PROTECTIVE GLASS PLATE
PROTECTIVE GLASS PLATE TYPE SC
PROTECTIVE GLASS PLATE TYPE VI

PROTECTIVE GONAD APRON
PROTECTIVE MITTEN
PROTECTIVE SHIELDING
PROTECTIVE SYSTEM
PROTECTIVELY EARTHED
PRUDENT USE STATEMENT
PUBLIC MAINS NETWORKS
PULSE AMPLITUDE ANALYZER PULSE
WINDOW
PULSE-AVERAGE INTENSITY
PULSE BEAM-WIDTH
PULSE DURATION
PULSE-INTENSITY INTEGRAL
PULSE REPETITION PERIOD
PULSE REPETITION RATE
PULSE-PRESSURE-SQUARED
INTEGRAL

Q

QUALIFIED PERSON
QUALITY ASSURANCE
QUALITY ASSURANCE PROGRAMME
QUALITY CONTROL
QUALITY EQUIVALENT FILTRATION
QUANTITY INDEX
QUANTUM ABSORPTION EFFICIENCY
QUENCH

R

RADIATION SOURCE TO SKIN
DISTANCE
RADIATION SPECTRUM
RADIATION TYPE
RADIAL RESOLUTION
RADIATION
RADIATION APERTURE
RADIATION BEAM
RADIATION BEAM AXIS
RADIATION CONDITION
RADIATION DETECTOR
RADIATION DETECTOR ASSEMBLY
RADIATION ENERGY

RADIATION FIELD
RADIATION HEAD
RADIATION METER
RADIATION OUTPUT
RADIATION PROTECTION
RADIATION QUALITY
RADIATION QUANTITIES AND UNITS
RADIATION QUANTITY
RADIATION QUANTITY FOR NOMINAL
SHORTEST IRRADIATION TIME
RADIATION SOURCE
RADIATION SOURCE ASSEMBLY
RADIOACTIVE HALF-LIFE
RADIOACTIVE IMPURITY
RADIOACTIVE SOURCE
RADIOACTIVE SOURCE TRAIN
RADIOACTIVE STANDARD SOURCE
RADIOACTIVITY
RADIO FREQUENCY (RF)
RADIOGRAM
RADIOGRAPHIC CASSETTE
RADIOGRAPHIC CASSETTE HOLDER
RADIOGRAPHIC FILM
RADIOGRAPHIC RATING
RADIOGRAPHY
RADIOLOGICAL
RADIOLOGICAL EQUIPMENT
RADIOLOGICAL INSTALLATION
RADIOLOGICAL IMAGE
RADIOLOGICAL PROTECTION
RADIOLOGY
RADIOMETRIC PARAMETERS
RADIONUCLIDE
RADIONUCLIDE BEAM THERAPY
EQUIPMENT
RADIONUCLIDE CALIBRATOR
RADIONUCLIDE FACTOR
RADIOSCOPIC SCREEN
RADIOSCOPICALLY GUIDED
INTERVENTIONAL PROCEDURE
RADIOSCOPY
RADIOTHERAPY
RADIOTHERAPY SIMULATOR

RADIOTHERAPY TREATMENT PLANNING
SYSTEM (RTPS)
RADIUS OF ROTATION
RANDOM COINCIDENCE
RANDOM UNCERTAINTY
RATED (VALUE)
RATED FIELD SIZE
RATED LENGTH
RATED LOAD
RATED OUTPUT POWER
RATED RANGE (OF USE)
READY STATE
RECONSTRUCTIVE TOMOGRAPHY
RECORD
RECORDING ELECTROCARDIOGRAPH
RECOVERY COEFFICIENT
REDUNDANT (TIMER) COMBINATION
REDUNDANT DOSE MONITORING
COMBINATION
REDUNDANT DOSE MONITORING
SYSTEMS
REFERENCE AIR KERMA
REFERENCE AXIS
REFERENCE CONDITIONS
REFERENCE DATA
REFERENCE DIRECTION
REFERENCE INDICATED VALUE
REFERENCE PLANE
REFERENCE POINT (OF A CHAMBER)
REFERENCE POINT (OF A RADIATION
DETECTOR)
REFERENCE POINT ACCORDING TO
GOLDBERGER
REFERENCE SCALE READING
REFERENCE VALUE
REFERENCE VOLUME
REFERENCE-CLASS DOSIMETER
REGION OF CONTROL
REGION OF INTEREST (ROI)
REINFORCED INSULATION
RELATIVE INTRINSIC ERROR
RELATIVE SURFACE DOSE

RESERVE ELECTRICAL POWER
SOURCE
RESIDUAL RADIATION
RESIDUAL RISK
RESOLUTION OF THE DISPLAY
RESOLVING TIME
RESPONSE
RESPIRATORY PRESSURE
RESPONSE TIME
RHYTHM RECOGNITION DETECTOR
RISK
RISK ANALYSIS
RISK ASSESSMENT
RISK CONTROL
RISK EVALUATION
RISK MANAGEMENT
RISK MANAGEMENT FILE
RISK MANAGEMENT SUMMARY
ROUTINE MONITORING
ROUTINE TEST
RUCK-RESISTANT BLANKET

S

SAFE WORKING LOAD
SAFETY
SAFETY DEVICE
SAFETY EXTRA-LOW VOLTAGE (SELV)
SAFETY EXTRA-LOW VOLTAGE
TRANSFORMER
SAFETY FACTOR
SAFETY HAZARD
SAFETY INTEGRITY
SAMPLE CHANGER
SAMPLE VOLUME CHARACTERISTIC
SCALE READING
SCANNING MODE
SCATTER FRACTION (SF)
SCATTERED RADIATION
SCATTERED TRUE COINCIDENCE
SCATTERING
SCREEN FILM
SCROTUM SHIELD
SEALED RADIOACTIVE SOURCE

SEARCH COIL
SECOND LEVEL CONTROLLED
OPERATING MODE
SECONDARY DOSE MONITORING
SYSTEM
SECONDARY TIMER
SELECTED ENERGY
SELF-RESETTING THERMAL CUT-OUT
SENSITIVE VOLUME
SENSITIVITY
SENSITIVITY PROFILE
SEPARATE MONITORING ELECTRODES
SEPARATION DEVICE
SERIAL CHANGER
SERIAL LOAD RATING
SERIAL NUMBER
SERIAL RADIOGRAPHY
SET TEMPERATURE
SEVERITY
SHADOW SHIELD
SHORT-TIME OPERATION
SHUTTER
SIDE RAIL
SIGNAL INPUT PART
SIGNAL OUTPUT PART
SIGNIFICANT ZONE OF OCCUPANCY
SILENCE
SILENCE/RESET
SILENCING
SILENCING/RESET
SINGLE CHAMBER
SINGLE CHANNEL
ELECTROCARDIOGRAPH
SINGLE FUNCTION
SINGLE FAULT CONDITION
SINGLE GAMMA-RAY PHOTON PULS
SINGLE LOAD RATING
SINGLE PHOTON EMISSION COMPUTED
TOMOGRAPHY (SPECT)
SINGLES RATE
SINOGRAM
SITE TEST
SIX-PEAK HIGH-VOLTAGE GENERATOR

SHADOW DILUTION
SHORT TERM AUTOMATIC MODE
SHORT-WAVE THERAPY EQUIPMENT
SKIN TEMPERATURE
SKIN TEMPERATURE SENSOR
SLICE SENSITIVITY
SLICE THICKNESS
SLIT CAMERA
SOFT TISSUE THERMAL INDEX
SOURCE APPLICATOR
SOURCE CARRIER
SOURCE DRIVE MECHANISM
SOURCE TO ENTRANCE PLANE
DISTANCE (SED)
SPATIAL NONLINEARITY
SPATIAL RESOLUTION
SPATIAL RESOLUTION (IN CT
EQUIPMENT)
SPATIAL-PEAK TEMPORAL-AVERAGE
INTENSITY
SPECIAL PURPOSE GRADIENT SYSTEM
SPECIAL USE EQUIPMENT
SPECIFIC
SPECIFIC ABSORPTION RATE(SAR)
SPECIFIED
SPECIFIED ENERGY RESPONSE
SPEED INDEX
SPOTFILM DEVICE
SQUEEZING AND SHEARING POINTS
(FOR FINGERS AND HANDS)
STABILITY CHECK DEVICE
STABILIZATION TIME
STANDARDIZATION VOLTAGE
STANDARD
STANDARD MEASUREMENT DEPTH
STANDARD TEST CONDITIONS
STANDARD TEST VALUES
STAND-BY
STAND-BY STATE
STAR PATTERN CAMERA
STAR PATTERN RESOLUTION LIMIT
STATIC LOAD
STATIONARY EQUIPMENT

STATIONARY GRID
STATIONARY RADIOTHERAPY
STATUS TEST
STEADY TEMPERATURE CONDITION
STERILE HANDLE
STERILIZABLE EQUIPMENT
STIMULATOR
STORAGE CONTAINER
STORED ENERGY
STRAY RADIATION
STRIP FREQUENCY
STRIPS PER CENTIMETRE
STRUCTURAL SHIELDING
SUBSTITUTION FLUID
SUPERFICIAL RADIOTHERAPY
SUPPLEMENTARY INSULATION
SUPPLY EQUIPMENT
SUPPLY LINE
SUPPLY MAINS
SUPPLY UNIT
SURFACE DOSE
SURGICAL LUMINAIRE
SURGICAL LUMINAIRE SYSTEM
SUSPENDED
SUSPENSION
SYNCHRONIZER
SYRINGE PUMP
SYSTEM AXIS
SYSTEM LINEARITY
SYSTEM NON-UNIFORMITY OF
RESPONSE
SYSTEM SENSITIVITY

T
TANGENTIAL RESOLUTION
TAPERED GRID
TARGET
TARGET ANGLE
TARGET MARKER
TARGET LOCATION
TARGET VOLUME
TECHNICAL ALARM
TELERADIOTHERAPY

TEMPERATURE LIMITER
TEMPORAL-AVERAGE INTENSITY
TEMPORAL-MAXIMUM INTENSITY
TEMPORAL MAXIMUM OUTPUT POWER
TENTH-VALUE LAYER
TERMINAL DEVICE
TERMINATION (OF IRRADIATION)
TERMINATION OF IRRADIATION /TO
TERMINATE IRRADIATION
TEST
TEST DEVICE
TEST DEVICE AVERAGE TEMPERATURE
TEST LOAD
THERMAL CUT-OUT
THERMAL INDEX
THERMOSTAT
THREE-DIMENSIONAL
RECONSTRUCTION
TIME CONSTANT
TIME RATE OF CHANGE OF MAGNETIC
FIELD (dB/dt)
TIMING DEVICE
TISSUE EQUIVALENT MATERIAL
TOMOGRAPHIC PLANE
TOMOGRAPHIC SECTION
TOMOGRAPHIC SECTION THICKNESS
TOMOGRAPHIC VOLUME
TOMOGRAPHY
TOOL
TOTAL COINCIDENCES
TOTAL FIELD OF VIEW
TOTAL FILTRATION
TOTAL IRRADIANCE FOR BILIRUBIN
TOTAL LOAD
TRACEABLE RADIOACTIVE STANDARD
SOURCE
TRANSDUCER ASSEMBLY
TRANSFER
TRANSCUTANEOUS OXYGEN AND
CARBON DIOXIDE PARTIAL
PRESSURE MONITORING EQUIPMENT
TRANSCUTANEOUS PARTIAL
PRESSURE MONITORING EQUIPMENT

TRANSDUCER
TRANSMEMBRANE PRESSURE (TMP)
TRANSMISSION
TRANSMISSION CHAMBER
TRANSMISSION DETECTOR
TRANSMISSION KERMA
(TRANSMISSION KERMA RATE)
TRANSMISSION OF PRIMARY
RADIATION
TRANSMISSION OF SCATTERED
RADIATION
TRANSMISSION OF TOTAL RADIATION
TRANSMISSION RATIO
TRANSMIT PATTERN
TRANSPORT INCUBATOR
TRANSPORT INCUBATOR
TEMPERATURE
TRANSPORTABLE ELECTRICAL POWER
SOURCE
TRANSPORTABLE EQUIPMENT
TRANSPORTER
TRANSVERSE FIELD MAGNET
TRANSVERSE FIELD OF VIEW
TRANSVERSE POINT SPREAD
FUNCTION
TRANSVERSE RESOLUTION
TRANSVERSE TOMOGRAPHY
TREATMENT
TREATMENT CONTROL PANEL
TREATMENT FIELD
TREATMENT HEAD
TREATMENT PARAMETER
TREATMENT PLAN/ TREATMENT
PLANNING
TREATMENT ROOM
TREATMENT VOLUME
TRENDELENBURG
TRIXEL
TRUE CENTRAL LINE
TRUE COINCIDENCE
TRUE COUNT RATE
TRUE VALUE
TUBE VOLTAGE (X-RAY)

TWELVE-PEAK HIGH VOLTAGE
GENERATOR
TWO- PEAK HIGH VOLTAGE
GENERATOR
TWO-DIMENSIONAL RECONSTRUCTION
TYPE B APPLIED PART
TYPE B EQUIPMENT
TYPE BF APPLIED PART
TYPE CF APPLIED PART
TYPE TEST

U

ULTRAFILTRATION
ULTRASONIC DIAGNOSTIC EQUIPMENT
ULTRASONIC PHYSIOTHERAPY
EQUIPMENT
ULTRASONIC TRANSDUCER
ULTRASOUND
UNATTENUATED BEAM
UNATTENUATED BEAM QUALITY
UNDER-BLANKET
UNIFORM CONSTANCY TEST FILM
UNIFORMITY
UNIFORMITY G2 OF THE TOTAL
IRRADIANCE FOR BILIRUBIN
UNSCATTERED TRUE COINCIDENCE
UNWANTED RADIATION
USEFUL BEAM
USEFUL ENTRANCE FIELD SIZE
USEFUL FIELD
USER

V

VALIDATION
VARIATION
VEILING GLARE INDEX (VGI)
VENOUS PART
VENOUS PRESSURE
VENTILATOR
VENTILATOR BREATHING SYSTEM
(VBS)
VERIFICATION

VIRTUAL SOURCE
VISUAL STIMULATOR
VOLTAGE RIPPLE
VOLUME RF TRANSMIT COIL
VOLUME SENSITIVITY
VOLUMETRIC INFUSION CONTROLLER
VOLUMETRIC INFUSION PUMP
VOXEL

W

WARNING SIGNAL
WATER KERMA
WAVE RECOGNITION POINTS
WAVEFORM
WEDGE FILTER
WEDGE FILTER ANGLE
WEDGE FILTER FACTOR
WELL-COUNTER
WELL-TYPE DETECTOR
WHOLE BODY COUNTER
WHOLE BODY GRADIENT SYSTEM
WHOLE BODY IMAGING DEVICE
WHOLE BODY MAGNET
WHOLE BODY MAGNETIC RESONANCE
EQUIPMENT (WHOLE BODY MR
EQUIPMENT)
WHOLE BODY RF TRANSMIT COIL
WHOLE BODY SAR
WORKING STANDARD
WORKLOAD

X

X-RAY EQUIPMENT
X-RAY GENERATOR
X-RAY IMAGE INTENSIFIER
X-RAY IMAGE INTENSIFIER TUBE
X-RAY IMAGE RECEPTOR
X-RAY IMAGING ARRANGEMENT
X-RAY PATTERN
X-RAY THERAPY
X-RAY TUBE
X-RAY TUBE ASSEMBLY

X-RAY TUBE ASSEMBLY COOLING
CURVE
X-RAY TUBE ASSEMBLY HEAT
CONTENT
X-RAY TUBE ASSEMBLY HEATING
CURVE
X-RAY TUBE ASSEMBLY INPUT POWER
X-RAY TUBE CURRENT
X-RAY TUBE HEAD
X-RAY TUBE HOUSING
X-RAY TUBE LOAD
X-RAY TUBE VOLTAGE
XRII

Z

ZERO APPLICATOR
ZERO DRIFT (MEASURING ASSEMBLY)
ZERO FILTER
ZERO SHIFT (MEASURING ASSEMBLY)

Term	Definition	Reference	Used in IEC
-12 DB OUTPUT BEAM AREA	Area of the ultrasonic beam derived from the -12 dB OUTPUT BEAM DIMENSIONS. Symbol: A_{aprt} . Unit: centimetre squared, cm ² .		IEC 60601-2-37:2001
-12 DB OUTPUT BEAM DIMENSIONS	Dimensions of the ultrasonic beam (-12 dB PULSE BEAM WIDTH) in specified directions normal to the BEAM ALIGNMENT AXIS and at the TRANSDUCER output face. NOTE 1 For reasons of measurement accuracy the -12 dB OUTPUT BEAM DIMENSIONS can be derived from measurements at a distance chosen to be as close as possible to the face of the TRANSDUCER, and if possible no more than 1 mm from the face. NOTE 2 For contact TRANSDUCERS, these dimensions can be taken as the dimensions of the radiating element. Symbol: X, Y. Unit: centimetres, cm.		IEC 60601-2-37:2001
ABSORBED DOSE	Letter symbol: D . Mean energy imparted by IONIZING RADIATION to matter. ABSORBED DOSE is determined as the quotient of $d\bar{\varepsilon}$ by dm , where $d\bar{\varepsilon}$ is the mean energy imparted by IONIZING RADIATION to matter of mass dm : $D = \frac{d\bar{\varepsilon}}{dm}$ The unit of ABSORBED DOSE is the joule per kilogram (J.kg ⁻¹). The special name of the unit of ABSORBED DOSE is the gray (Gy). The earlier unit of ABSORBED DOSE was the rad, 1 rad being equal to 10 ⁻² J.kg ⁻¹ .	rm-13-08	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976/ A1:2000 IEC 62083:2000
ABSORBED DOSE RATE	Letter symbol: \dot{D} . ABSORBED DOSE per unit time. ABSORBED DOSE RATE is determined as the quotient of dD by dt , where dD is the increment of ABSORBED DOSE in the time interval dt : $\dot{D} = \frac{dD}{dt}$ A unit of ABSORBED DOSE RATE is any quotient of the gray or its multiples or submultiples by a suitable unit of time (Gy.s ⁻¹ , mGy.h ⁻¹ , etc.).	rm-13-09	60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60976/ A1:2000 IEC 62083:2000
ABSORBED DOSE RATE TO WATER	Letter symbol: \dot{D} . Following the definition in C.5 of ICRU 33, ABSORBED DOSE RATE to water is the quotient of dD by dt , where dD is the increment of ABSORBED DOSE to water in the time interval dt . The unit of ABSORBED DOSE RATE to water is Gy · s ⁻¹ (Gy · min ⁻¹ ; Gy · h ⁻¹).		IEC 60731/A1:2002
ABSORBED DOSE TO WATER	Letter symbol: D . Following the definition in C.4 of ICRU 33, ABSORBED DOSE to water is the quotient of $d\bar{\varepsilon}$ by dm where $d\bar{\varepsilon}$ is the mean energy imparted by IONIZING RADIATION to water of mass dm . The unit of ABSORBED DOSE to water is Gy (where 1 Gy = 1 J · kg ⁻¹).		IEC 60731/A1:2002

Term	Definition	Reference	Used in IEC
ABSORPTION	Phenomenon in which incident RADIATION transfers to the matter which it traverses some or all its energy. NOTE SCATTERING accompanied by energy loss, for example the compton effect and NEUTRON slowing down, is considered to be ENERGY ABSORPTION.	rm-12-05	IEC 61223-3-1:1999
ACCEPTANCE TEST	TEST carried out after new EQUIPMENT has been installed, or major modifications have been made to existing EQUIPMENT, in order to verify compliance with contractual specifications.	rm-70-01	IEC 60627:2001 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61267:1994 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000
ACCEPTANCE TEST	TEST carried out at the request and with the participation of the user or his representative to ascertain by determination of proper performance parameters that the instrument meets the specifications claimed by the vendor. NOTE An ACCEPTANCE TEST should be carried out at the time of installation and when appropriate after major service. During or immediately after ACCEPTANCE TESTING, REFERENCE DATA are collected to be used as a standard for comparison with future ROUTINE TESTS.		IEC 61948-1:2001 IEC 61948-2:2001
ACCESS COVER	Part of an ENCLOSURE or guard providing the possibility of access to EQUIPMENT parts for the purpose of adjustment, inspection, replacement or repair.	NG.01.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
ACCESSIBLE CONDUCTIVE PARTS	Conducting parts of EQUIPMENT which can be touched without the use of a TOOL.		IEC 60601-2-9:1996
ACCESSIBLE METAL PART	Metal part of EQUIPMENT which can be touched without the use of a TOOL. See also NG.01.22.	NG.01.02	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60731/A1:2002 IEC 61674/ A1:2002

Term	Definition	Reference	Used in IEC
ACCESSIBLE PART	Part of EQUIPMENT which can be touched without the use of a TOOL.	NG.01.22	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-26:2002 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
ACCESSIBLE SURFACE	Surface of EQUIPMENT or of an EQUIPMENT part that can be easily or accidentally touched by persons without the use of a TOOL.	rm-84-07	IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-33:2002
ACCESSORY	<p>Additional component for use with an EQUIPMENT in order:</p> <ul style="list-style-type: none"> – to perform its intended use; – to adapt the EQUIPMENT to some special use; – to facilitate the use of the EQUIPMENT; – to enhance the performance of the EQUIPMENT; – to enable the functions of the EQUIPMENT to be integrated with those of other EQUIPMENT. 	rm-83-06	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/ A1:2000 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61267:1994

Term	Definition	Reference	Used in IEC
ACCESSORY	<p>Additional component for use with an EQUIPMENT in order:</p> <ul style="list-style-type: none"> – to perform its intended use; – to adapt the EQUIPMENT to some special use; – to facilitate the use of the EQUIPMENT; – to enhance the performance of the EQUIPMENT; – to enable the functions of the EQUIPMENT to be integrated with those of other EQUIPMENT. <p>Separate programmers are regarded as accessories and therefore a component part of the EQUIPMENT.</p>		IEC 60601-2-24:1998
ACCESSORY	Optional component necessary and/or suitable to be used with EQUIPMENT in order to enable, facilitate or improve the intended use of EQUIPMENT or to integrate additional functions.	NG.01.03	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-29:1999
ACCOMPANYING DOCUMENT	<p>Document accompanying a medical device, or an ACCESSORY, and containing important information for the USER, OPERATOR, installer or assembler of the medical device particularly regarding SAFETY.</p> <p>NOTE Based on IEC 60601-1:1988, definition 2.1.4.</p>		ISO 14971:2000

Term	Definition	Reference	Used in IEC
ACCOMPANYING DOCUMENTS	Documents provided with an installation, EQUIPMENT, ASSOCIATED EQUIPMENT or ACCESSORY and containing important information for the assembler, installer and USER, particularly regarding SAFETY.	rm-82-01	IEC 60336:1993 IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-37:2001 IEC 60601-2-43:2000 IEC 60601-2-44: 2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60731/A1:2002 IEC 60976/ A1:2000 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61303:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998 IEC 61674/ A1:2002 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998 IEC 62083:2000

Term	Definition	Reference	Used in IEC
ACCOMPANYING DOCUMENTS	Documents accompanying EQUIPMENT or an ACCESSORY and containing all important information for the USER, OPERATOR, installer or assembler of EQUIPMENT, particularly regarding SAFETY. Recommended replacement: rm-82-01	NG.01.04	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-1-4:2000 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-12:2001 IEC 60601-2-17/ A1: 1996 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
ACCOMPANYING DOCUMENTS	Documents provided with an installation, EQUIPMENT, ASSOCIATED EQUIPMENT or ACCESSORY, containing important information for the assembler, installer and USER, particularly regarding SAFETY (IEC 60788 rev., MR-128-01). Recommended replacement: NG.01.04		IEC 60580:2000
ACOUSTIC ATTENUATING COEFFICIENT	Coefficient intended to account for ultrasonic ATTENUATION of tissue between the source and a specified point. Symbol: α . Unit: decibels per centimetre per megahertz, dB cm ⁻¹ MHz ⁻¹ .		IEC 60601-2-37:2001
ACOUSTIC WORKING FREQUENCY	Arithmetic mean of the most widely separated frequencies f_1 and f_2 at which the amplitude of the pressure spectrum of the acoustic signal is 3 dB lower than the peak amplitude. Symbol: f_{awf} . Unit: megahertz, MHz.		IEC 60601-2-37:2001
ACOUSTIC WORKING FREQUENCY	Frequency of an acoustic signal based on the observation of the output of a hydrophone placed in an acoustic field. The signal is analysed using the zero-crossing frequency technique (see 3.4.1 of IEC 61102). [IEC 61689, definition 3.3]		IEC 60601-2-5:2000
ACTIVE ELECTRODE	Electrode intended to produce certain physical effects required in electrosurgery, for example CUTTING and coagulation.		IEC 60601-2-2:1998
ACTIVITY	Letter symbol: A. Quantitative indication of the RADIOACTIVITY of an amount of RADIONUCLIDE in a particular energy state at a given time. ACTIVITY is determined as the quotient of dN by dt , where dN is the expectation value of the number of spontaneous nuclear transitions from that energy state in the time interval dt : $A = \frac{dN}{dt}$ The unit of ACTIVITY is the reciprocal second (s ⁻¹). The special name of the unit of ACTIVITY is the becquerel (Bq), 1 Bq being equal to one transition per second. The earlier unit of ACTIVITY was the curie (Ci), 1 Ci being equal to 3.7 x 10 ¹⁰ transitions per second.	rm-13-18	IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60789:1992 IEC 61262-5:1994 IEC 61303:1994 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998 IEC 61948-1:2001 IEC 61948-2:2001
ACTUAL FOCAL SPOT	Area on the surface of the TARGET that intercepts the beam of accelerated particles.	rm-20-12	IEC 60336:1993 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-7:1995

Term	Definition	Reference	Used in IEC
ADDED FILTER	Removable or irremovable FILTER positioned in the RADIATION BEAM to provide part or all of the ADDITIONAL FILTRATION.	rm-35-02	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60806:1984 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-2:1996 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61267:1994
ADDITIONAL FILTRATION	QUALITY EQUIVALENT FILTRATION due to ADDED FILTERS and other removable materials in the RADIATION BEAM which are between the RADIATION SOURCE and the PATIENT or a specified plane.	rm-13-47	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-44:2002 IEC 60627:2001 IEC 60806:1984 IEC 61223-3-1:1999
ADDRESS PILE-UP	For imaging devices false address calculation of an artificial event which passes the PULSE amplitude analyzer window, but is formed from two or more events by the pile-up effect.		IEC 61675-1:1998
ADJUSTABLE SETTING (of a control or limiting device)	Setting which can be altered by the OPERATOR without the use of a TOOL.	NG.09.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
ADMINISTRATION SET	Device(s) that convey(s) liquid from the supply via the EQUIPMENT to the PATIENT.		IEC 60601-2-24:1998
ADMINISTRATION SET CHANGE INTERVAL	Time recommended by the MANUFACTURER of the EQUIPMENT for using the ADMINISTRATION SET.		IEC 60601-2-24:1998
AFTERLOADING	Manual or remotely-controlled transfer of one or more SEALED RADIOACTIVE SOURCES between a STORAGE CONTAINER and pre-positioned SOURCE APPLICATORS for BRACHYRADIOTHERAPY.	rm-42-54	IEC 60601-2-17 A1:1996

Term	Definition	Reference	Used in IEC
AIR CLEARANCE	Shortest path in air between two conductive parts.	NG.03.01	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-44: 2002 IEC 60601-2-45:2001
AIR CONTROLLED INCUBATOR	INCUBATOR in which the air temperature is automatically controlled by an air temperature sensor close to a value set by the USER.		IEC 60601-2-19 A1:1996
AIR CONTROLLED TRANSPORT INCUBATOR	TRANSPORT INCUBATOR in which the air temperature is automatically controlled by an air temperature sensor close to a value set by the USER.		IEC 60601-2-20 A1:1996
AIR KERMA	Letter symbol: K . Quotient of dE_{tr} by dm , where dE_{tr} is the sum of the initial kinetic energies of all the charged particles in a mass dm of air, thus $K = \frac{dE_{tr}}{dm}$. Unit: J kg ⁻¹ . The special name for the unit of AIR KERMA is gray (Gy) (ICRU 60).	rm-13-11	IEC 60580:2000
AIR KERMA	Letter symbol: K . Following the definition in C.6 of ICRU 33, AIR KERMA is the quotient of dE_{tr} by dm where dE_{tr} is the sum of the initial kinetic energies of all the charged ionizing particles liberated by uncharged ionizing particles in air of mass dm . The unit of AIR KERMA is Gy (where 1 Gy = 1 J · kg ⁻¹). Recommended replacement: precise definition in IEC 60580 (2000)		IEC 60731/A1:2002
AIR KERMA	KERMA measured in a mass of air. Recommended replacement: precise definition in IEC 60580 (2000)	rm-13-11	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-17 /A1: 1996 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61267:1994 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
AIR KERMA	Letter symbol: K . Quotient of dE_{tr} by dm , where dE_{tr} is the sum of the initial kinetic energies of all the charged ionizing particles liberated by uncharged ionizing particles in air of mass dm . The unit of AIR KERMA is Gy (where $1 \text{ Gy} = 1 \text{ J} \cdot \text{kg}^{-1}$), (see C.6 of ICRU 33). Recommended replacement: precise definition in IEC 60580 (2000)		IEC 61674 /A1:2002
AIR KERMA LENGTH	Letter symbol: $K.l$. For any straight line passing through the cross sectional X-ray scan of a CT machine, AIR KERMA LENGTH is the infinite integral of the product of AIR KERMA and elemental length along this line. The unit of AIR KERMA LENGTH is Gy·m (mGy·m).		IEC 61674 /A1:2002
AIR KERMA RATE	Letter symbol: \dot{K} . Quotient of dK by dt , where dK is the increment of AIR KERMA in the time interval dt , thus $\dot{K} = \frac{dK}{dt}$. Unit: $\text{J kg}^{-1} \text{ s}^{-1}$. If the special name gray is used, the unit of AIR KERMA RATE is gray per second (Gy s^{-1}) (ICRU).	rm-13-54	IEC 60580:2000
AIR KERMA RATE	Letter symbol: \dot{K} . Following the definition in C.7 of ICRU 33, AIR KERMA RATE is the quotient of dK by dt , where dK is the increment of AIR KERMA in the time interval dt . The unit of AIR KERMA RATE is $\text{Gy} \cdot \text{s}^{-1}$ ($\text{Gy} \cdot \text{min}^{-1}$; $\text{Gy} \cdot \text{h}^{-1}$). Recommended replacement see IEC 60580 (2000)		IEC 60731/A1:2002
AIR KERMA RATE	Letter symbol: \dot{K} . Quotient of dK by dt , where dK is the increment of AIR KERMA in the time interval dt . The unit of AIR KERMA RATE is Gy/s (Gy/min; Gy/h), (see C.7 of ICRU 33). Recommended replacement see IEC 60580 (2000)		IEC 61674/ A1:2002
AIR-DENSITY CHARACTERISTIC	Two-dimensional function relating the instrument reading with temperature and PRESSURE.		IEC 61303:1994
ALARM	Signal which indicates abnormal events occurring to the PATIENT or EQUIPMENT.		IEC 60601-2-23:1999 IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-49:2001 IEC 60601-2-51:2003
ALARM CONDITION	A condition that occurs when a variable that is being monitored by an ALARM SYSTEM equals or falls outside the set ALARM LIMIT(S).		IEC 60601-2-13:2003
ALARM LIMIT	Value(s) which are set by the MANUFACTURER, the device, the USER or OPERATOR which define the threshold range of the ALARM CONDITION.		IEC 60601-2-13:2003
ALARM SIGNAL	A signal the purpose of which is to alert the OPERATOR to an abnormal condition in the PATIENT or the EQUIPMENT that may develop into a SAFETY HAZARD which requires OPERATOR awareness or action.		IEC 60601-2-13:2003
ALARM SYSTEM	A system that is intended to make the OPERATOR(S) aware of an ALARM CONDITION, in the PATIENT or EQUIPMENT, by means of its ALARM SIGNAL(S).		IEC 60601-2-13:2003
AMBULATORY ELECTROCARDIOGRAPHIC SYSTEM (EQUIPMENT)	AMBULATORY RECORDER and a PLAYBACK EQUIPMENT, both of which may contain an analysis function. NOTE This EQUIPMENT is often referred to as Holter monitoring EQUIPMENT after its inventor, Dr. Norman Holter.		IEC 60601-2-47:2001
AMBULATORY RECORDER	Recording EQUIPMENT worn or carried by the PATIENT including associated ELECTRODES and cables for recording or recording and analysing heart action potentials.		IEC 60601-2-47:2001

Term	Definition	Reference	Used in IEC
ANAESTHETIC GAS DELIVERY SYSTEM	Assembly of components which controls and delivers the fresh gas into the ANAESTHETIC BREATHING SYSTEM. NOTE It may include a flow control system, flow meters and/or a gas mixing system and ANAESTHETIC GAS DELIVERY SYSTEM PIPING.		IEC 60601-2-13:2003
ANAESTHETIC GAS DELIVERY SYSTEM PIPING	All pipework, including unions, from unidirectional valves in the pipeline inlets and from the outlets of the pressure regulator(s) to the flow control system, as well as the PIPING connecting the flow control system and the piping connecting the ANAESTHETIC VAPOUR DELIVERY DEVICE to the FRESH GAS OUTLET. It includes piping leading to and from pneumatic ALARM SYSTEM(s), pressure indicators, oxygen flush and gas power outlets.		IEC 60601-2-13:2003
ANAESTHETIC SYSTEM (ANAESTHETIC WORKSTATION)	Inhalational ANAESTHETIC SYSTEM that contains an ANAESTHETIC GAS DELIVERY SYSTEM, an ANAESTHETIC BREATHING SYSTEM and the required MONITORING DEVICE(S), ALARM SYSTEM(s), and PROTECTION DEVICES. NOTE The ANAESTHETIC SYSTEM may include, but is not limited to, ANAESTHETIC VAPOUR DELIVERY DEVICE(S) and ANAESTHETIC VENTILATOR(S) and their associated MONITORING DEVICE(S), ALARM SYSTEM(s) and PROTECTION DEVICE(S).		IEC 60601-2-13:2003
ANAESTHETIC VAPOUR DELIVERY DEVICE	Device which provides the vapour of an anaesthetic agent in a controllable concentration.		IEC 60601-2-13:2003
ANAESTHETIC VENTILATOR	Automatic device, which is connected via the ANAESTHETIC BREATHING SYSTEM to the PATIENT'S airway and is designed to augment or provide ventilation of the PATIENT during anaesthesia.		IEC 60601-2-13:2003
ANALYSING ELECTROCARDIOGRAPH	ELECTROCARDIOGRAPH capable of analysing heart action potentials, deriving measurements from them and/or making interpretative statements. These may be also capable of communicating ECGs and/or analysis results.		IEC 60601-2-51:2003
ANNIHILATION RADIATION	IONIZING RADIATION that is produced when a particle and its antiparticle interact and cease to exist.		IEC 61675-1:1998
ANNUNCIATION	Communication of ALARM SIGNALS to the OPERATOR.		IEC 60601-2-13:2003
ANODE	In an X-RAY TUBE, electrode to which ELECTRONS forming a beam are accelerated and which usually contains the TARGET.	rm-22-06	IEC 60336:1993 IEC 60601-2-28:1993 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60806:1984 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996
ANODE COOLING CURVE	Curve showing the ANODE HEAT CONTENT as a function of time with zero ANODE INPUT POWER, beginning after a LOADING when the ANODE HEAT CONTENT is equal to the maximum ANODE HEAT CONTENT.	rm-36-29	IEC 60601-2-28:1993 IEC 60613:1989
ANODE ANGLE	TARGET ANGLE in an X-RAY TUBE or in an X-RAY TUBE ASSEMBLY.	rm-22-07	IEC 60336:1993
ANODE HEAT CONTENT	Momentary value of the heat contained in the ANODE of an X-RAY TUBE accumulated during, or retained after, LOADINGS.	rm-36-26	IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989

Term	Definition	Reference	Used in IEC
ANODE HEATING CURVE	Curve showing the ANODE HEAT CONTENT as a function of LOADING TIME for specified ANODE INPUT POWER.	rm-36-28	IEC 60601-2-28:1993 IEC 60613:1989
ANODE INPUT POWER	Power applied to the ANODE of an X-RAY TUBE to produce X-radiation.	rm-36-22	IEC 60601-2-28:1993 IEC 60613:1989
ANODE SPEED	In a rotating ANODE X-RAY TUBE, angular velocity at which the ANODE rotates, usually expressed in revolutions per minute.	rm-36-35	IEC 60336:1993 IEC 60601-2-28:1993 IEC 60613:1989
ANTI-SCATTER GRID	Device to be placed before the IMAGE RECEPTION AREA in order to reduce the incidence of SCATTERED RADIATION upon that area and thus increase the contrast in the X-RAY PATTERN.	rm-32-06	IEC 60601-1-3:1994 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994
ANTI-SCATTER GRID	Device with a fixed periodic arrangement of materials with different X-RAY ATTENUATION properties to be placed in front of the IMAGE RECEPTION AREA in order to reduce the incidence of SCATTERED RADIATION upon that area and thus increase the contrast in the X-RAY PATTERN. Recommended replacement: rm-32-06		IEC 60627:2001
APPARENT RESISTANCE OF SUPPLY MAINS	For diagnostic X-RAY GENERATOR, resistance of the SUPPLY MAINS determined under specific load conditions.	rm-36-16	IEC 60601-2-7:1998 IEC 60601-2-44: 2002 IEC 60601-2-45:2001
APPLIANCE COUPLER	Means enabling the connection of a flexible cord to EQUIPMENT without the use of a TOOL, consisting of two parts: a MAINS CONNECTOR and an APPLIANCE INLET.	NG.07.01	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-13:2003

Term	Definition	Reference	Used in IEC
APPLIANCE INLET	Part of an APPLIANCE COUPLER incorporated in or fixed to EQUIPMENT.	NG.07.02	IEC 60601-1:1988 IEC 60601-1/A2:1995
APPLICATION DISTANCE	Distance from the EFFECTIVE FOCAL SPOT to the APPLICATION PLANE.		IEC 61267:1994
APPLICATION LIMITS	Letter symbols: f_1 , f_2 , unit: cm. Lower, f_1 , and upper, f_2 , limits of the distance from the FOCAL SPOT to the incident face of a FOCUSED GRID or a PARALLEL GRID between which the obtained RADIOLOGICAL information can be considered acceptable for many purposes.		IEC 60627:2001
APPLICATION LIMITS	Letter symbols: lower limit: f_1 , upper limit: f_2 . For a FOCUSED GRID, limits of the distance from the FOCAL SPOT to the incident face between which the RADIOLOGICAL information obtained can generally be expected to be acceptable.	rm-32-19	IEC 60601-2-7:1998
APPLICATION PLANE	Plane perpendicular to the REFERENCE AXIS, where the standard RADIATION CONDITION is defined.		IEC 61267:1994
APPLICATOR	An ACCESSORY or part of the EQUIPMENT intended to be used to couple the r.f. power to the PATIENT, but excluding the associated connecting cables.		IEC 60601-2-3/ A1:1998
APPLICATOR	Radiator, i.e., an aerial with a directional effect, such as a dipole with reflector, a dipole array, open waveguide or dielectric radiator for local application of microwave energy to the PATIENT.		IEC 60601-2-6:1984
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. 	NG.01.05	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-17/A1:1996 IEC 60601-2-26:2002 IEC 60601-2-29:1999 IEC 60601-2-37:2001 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
APPLIED PART	A part of a DOSEMETER, the RADIATION DETECTOR (for example CHAMBER ASSEMBLY) together with any additional PROTECTIVE COVER provided by the MANUFACTURER, intended for physical contact (not electrical contact) with the PATIENT (for example for intracavitary use).		IEC 60601-2-9:1996
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. <p>Accessible parts of APPLICATORS.</p>		IEC 60601-2-3/ A1:1998

Term	Definition	Reference	Used in IEC
APPLIED PART	<p>A part of the EQUIPMENT which in NORMAL USE:</p> <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. <p>Accessible parts of APPLICATORS and their associated connecting cables or waveguides and their connectors.</p>		IEC 60601-2-6:1984
APPLIED PART	<p>A part of the EQUIPMENT which in NORMAL USE:</p> <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. <p>The STIMULATOR ELECTRODES and all parts conductively connected to them.</p>		IEC 60601-2-10 /A1: 2001
APPLIED PART	<p>A part of the EQUIPMENT which in NORMAL USE:</p> <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT, <p>or any part of the VENTILATOR intended to be connected to the breathing system.</p>		IEC 60601-2-12:2001
APPLIED PART	The EXTRACORPOREAL CIRCUIT and the DIALYSING FLUID circuit and/or all parts permanently and conductively connected to it.		IEC 60601-2-16:1998
APPLIED PART	<p>A part of the EQUIPMENT which in NORMAL USE:</p> <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. <p>For some ENDOSCOPIC EQUIPMENT, the APPLIED PART extends, as seen from the PATIENT, into the SUPPLY UNIT(S) to the point(s) where the required separation is provided (see 17a) of the General Standard).</p>		IEC 60601-2-18 /A1: 2000
APPLIED PART	<p>A part of the EQUIPMENT which in NORMAL USE:</p> <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. <p>For some ENDOSCOPIC EQUIPMENT, the APPLIED PART extends, as seen from the PATIENT, into the SUPPLY UNIT(S) to the point(s) where the required separation is provided (see 17a) and 17 c) of the General Standard).</p>		IEC 60601-2-18/ A1: 2000
APPLIED PART	The definition of IEC 60601-1 (see amendment 2) applies.		IEC 60601-2-19 /A1: 1996 IEC 60601-2-20/ A1: 1996
APPLIED PART	TRANSDUCER and its connecting lead.		IEC 60601-2-23:1999

Term	Definition	Reference	Used in IEC
APPLIED PART	Entirety of all parts of the EQUIPMENT including the infusion liquid pathway that is intentionally in contact with the PATIENT being treated in NORMAL USE.		IEC 60601-2-24:1998
APPLIED PART	The occluding cuff and any integral TRANSDUCERS, their connecting leads and pressure tubes.		IEC 60601-2-30:1999
APPLIED PART	The TRANSDUCER, including any fluid filled system.		IEC 60601-2-34:2000
APPLIED PART	All parts of the BED which can intentionally or unintentionally come into contact with the PATIENT, are considered an APPLIED PART. (See Figure 111.)		IEC 60601-2-38 /A1: 1999
APPLIED PART	The part of the DIALYSING SOLUTION circuit that conveys DIALYSING SOLUTION from the EQUIPMENT to the peritoneal cavity of the PATIENT, and subsequently to a drainage bag or drain, or parts permanently and conductively connected to it, shall be considered as the APPLIED PART.		IEC 60601-2-39:1999
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – can be brought into contact with the PATIENT, or – needs to be touched by the PATIENT. NOTE Except if intended for such purpose, a SURGICAL LUMINAIRE or LUMINAIRE FOR DIAGNOSIS has no APPLIED PART on the PATIENT.		IEC 60601-2-41:2000
APPLIED PART	A part of the EQUIPMENT which in NORMAL USE: <ul style="list-style-type: none"> – necessarily comes into physical contact with the PATIENT for the EQUIPMENT to perform its function, or – needs to be touched by the PATIENT. 		IEC 60601-2-49:2001
APPLIED PART INTERFACE	That portion of the APPLIED PART intended to come into contact with the PATIENT'S skin.		IEC 60601-2-23:1999
ARTERIAL PRESSURE	The PRESSURE measured in the EXTRACORPOREAL CIRCUIT between the PATIENT and the arterial blood pump.		IEC 60601-2-16:1998
ARTEFACT / ARTIFACT	Apparent structure visible in the image which does not represent a structure within the object and which cannot be explained by NOISE or the MODULATION TRANSFER FUNCTION of the system.	rm-32-67	IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996
ARTEFACT	Apparent structure visible in the image which does not represent a structure within the object.		IEC 61223-3-4:2000
ASSEMBLING INSTRUCTIONS	Those parts of ACCOMPANYING DOCUMENTS giving information enabling an assembler to observe necessary precautions with respect to SAFETY and functional performance when assembling EQUIPMENT, equipment parts or sub-assemblies according to their specified purpose.	rm-82-03	IEC 60601-1-3:1994

Term	Definition	Reference	Used in IEC
ASSOCIATED EQUIPMENT	In a RADIOLOGICAL INSTALLATION, EQUIPMENT other than those for the production and control of IONIZING RADIATION, but essential for its application.	rm-30-01	IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-1:1993 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
ATTACHMENT HEAD	ACCESSORY intended to be attached to the TREATMENT HEAD for the purpose of modifying the ultrasonic beam characteristics.		IEC 60601-2-5:2000
ATTENUATED BEAM	X-ray beam exiting the PATIENT or PHANTOM.		IEC 61674 /A1:2002
ATTENUATED BEAM QUALITY	RADIATION QUALITY of the X-ray beam exiting the PATIENT or PHANTOM.		IEC 61674/ A1:2002
ATTENUATED OUTPUT POWER	Value of the acoustic OUTPUT POWER after ATTENUATION and at a specified distance from the TRANSDUCER, and given by: $P_{\alpha} = P10^{(-\alpha z f_{awf} / 10)}$ where α is the ACOUSTIC ATTENUATION COEFFICIENT in decibels per centimetre per megahertz; z is the distance from the source to the point of interest in centimetres; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz; P_{α} is the ATTENUATED OUTPUT POWER in milliwatts; P is the OUTPUT POWER in milliwatts measured in water. Symbol: P_{α} . Unit: milliwatts, mW.		IEC 60601-2-37:2001
ATTENUATED PEAK-RAREFACTIONAL ACOUSTIC PRESSURE	Value of the PEAK-RAREFACTIONAL ACOUSTIC PRESSURE after ATTENUATION and at a specified point, and given by $p_{ra}(z) = p_r(z)10^{(-\alpha z f_{awf} / 20)}$ where α is the ACOUSTIC ATTENUATING COEFFICIENT in decibels per centimetre per megahertz; z is the distance from the source to the point of interest, in centimetres; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz; $p_r(z)$ is the PEAK-RAREFACTIONAL ACOUSTIC PRESSURE measured in water. Symbol: p_{ra} . Unit: megapascals, MPa.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
ATTENUATED PULSE-AVERAGE INTENSITY	<p>Value of the acoustic PULSE-AVERAGE INTENSITY after ATTENUATION and at a specified point, and given by</p> $I_{pa,\alpha} = I_{pa}(z)10^{(-\alpha z f_{awf} / 10)}$ <p>where</p> <p>α is the ACOUSTIC ATTENUATING COEFFICIENT in decibels per centimetre per megahertz;</p> <p>z is the distance from the source to the point of interest in centimetres;</p> <p>f_{awf} is the ACOUSTIC WORKING FREQUENCY, at distance z in megahertz;</p> <p>$I_{pa}(z)$ is the PULSE-AVERAGE INTENSITY measured in water, in milliwatts per centimetre squared.</p> <p>Symbol: $I_{pa,\alpha}$. Unit: watts per centimetre squared, W cm⁻².</p>		IEC 60601-2-37:2001
ATTENUATED PULSE-INTENSITY INTEGRAL	<p>Value of the PULSE-INTENSITY INTEGRAL after ATTENUATION and at a specified point, and given by</p> $I_{pi,\alpha} = I_{pi}10^{(-\alpha z f_{awf} / 10)}$ <p>where</p> <p>α is the ACOUSTIC ATTENUATION COEFFICIENT in decibels per centimetre per megahertz;</p> <p>z is the distance from the source to the point of interest in centimetres;</p> <p>f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz;</p> <p>$I_{pi,\alpha}$ is the ATTENUATED PULSE-INTENSITY INTEGRAL in millijoules per centimetre squared;</p> <p>I_{pi} is the PULSE-INTENSITY INTEGRAL measured in water in millijoules per centimetre squared.</p> <p>Symbol: $I_{pi,\alpha}$. Unit: millijoules per centimetre squared, mJ/cm².</p>		IEC 60601-2-37:2001
ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY	<p>Value of the SPATIAL-PEAK TEMPORAL AVERAGE INTENSITY after ATTENUATION and at a specified distance z, and given by</p> $I_{zpta,\alpha}(z) = I_{zpta}(z)10^{(-\alpha z f_{awf} / 10)}$ <p>where</p> <p>α is the ACOUSTIC ATTENUATING COEFFICIENT in decibels per centimetre per megahertz;</p> <p>z is the distance from the source to the point of interest in centimetres;</p> <p>f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz;</p> <p>$I_{zpta}(z)$ is the SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY, at a specified distance z in milliwatts per centimetre squared measured in water.</p> <p>Symbol: $I_{zpta,\alpha}(z)$. Unit: milliwatts per centimetre squared, mW cm².</p>		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
ATTENUATED TEMPORAL-AVERAGE INTENSITY	<p>Value of the TEMPORAL-AVERAGE INTENSITY after ATTENUATION and at a specified point, and given by</p> $I_{ta,\alpha}(z) = I_{ta}(z)10^{(-\alpha z f_{awf} / 10)}$ <p>where</p> <p>α is the ACOUSTIC ATTENUATING COEFFICIENT in decibels per centimetre per megahertz;</p> <p>z is the distance from the source to the point of interest in centimetres;</p> <p>f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz;</p> <p>$I_{ta,\alpha}(z)$ is the ATTENUATED TEMPORAL-AVERAGE INTENSITY in milliwatts per centimetre squared;</p> <p>$I_{ta}(z)$ is the TEMPORAL-AVERAGE INTENSITY measured in water in milliwatts per centimetre squared.</p> <p>Symbol: $I_{ta,\alpha}(z)$. Unit: milliwatts per centimetre squared, mW cm².</p>		IEC 60601-2-37:2001
ATTENUATION	<p>Reduction of a RADIATION QUANTITY upon passage of the RADIATION through matter resulting from all types of interaction with this matter. The RADIATION QUANTITY may be, for example, the particle flux density or the energy density.</p> <p>NOTE ATTENUATION does not include the geometric reduction of the RADIATION QUANTITY with distance from the RADIATION SOURCE.</p>	rm-12-08	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-17/ A1: 1996 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998 IEC 61675-1:1998 IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
ATTENUATION COEFFICIENT	<p>Letter symbol: μ. For a material in a beam of uncharged ionizing particles, quotient $\frac{dN}{N}$ by dl, where $\frac{dN}{N}$ is the fraction of particles that experience interactions in traversing a distance dl in the material.</p> $\mu = -\frac{1}{N} \frac{dN}{dl}$	rm-13-39	IEC 60601-1-3:1994 IEC 61267:1994
ATTENUATION EQUIVALENT	<p>Letter symbol: δ. Thickness of a layer of reference material which, if substituted for the material under consideration in a beam of specified RADIATION QUALITY and under specified geometrical conditions, gives the same degree of ATTENUATION. The ATTENUATION EQUIVALENT is expressed in suitable submultiples of the metre together with the reference material and the RADIATION QUALITY of the incident beam.</p>	rm-13-37	IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-29:1999 IEC 60601-2-45:2001 IEC 61262-1:1994 IEC 61262-4:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998
ATTENUATION RATIO	<p>Ratio of the value of a specified RADIATION QUANTITY in the centre of a BROAD BEAM of specified RADIATION QUALITY with the attenuating material under consideration outside the beam, to the value at the same position and under the same conditions with this attenuating material placed in the beam.</p>	rm-13-40	IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61331-1:1994
AUDITORY STIMULATOR	<p>Parts of EQUIPMENT for the application of sound pressure from a TRANSDUCER (headphone, bone conductor or free-field) to the ear(s) of the PATIENT, for the evoking of biopotentials or other action.</p>		IEC 60601-2-40:1998
AUTOMATED EXTERNAL DEFIBRILLATOR (AED)	<p>A DEFIBRILLATOR that, once activated by the OPERATOR, analyses the ECG obtained from ELECTRODES placed on the chest surface, identifies shockable cardiac rhythms, and automatically operates the DEFIBRILLATOR when a shockable rhythm is detected, hereinafter referred to as an AED.</p> <p>NOTE AEDs may provide varying levels of automation and be referred to by various terms.</p>		IEC 60601-2-4:2002
AUTOMATIC CONTROL SYSTEM	<p>In an X-RAY GENERATOR, system in which the control or limitation of the electric energy delivered to an X-ray tub assembly depends upon the measurement of one or more radiation quantities or corresponding physical quantities.</p>	rm-36-45	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999

Term	Definition	Reference	Used in IEC
AUTOMATIC CYCLING NON-INVASIVE BLOOD PRESSURE MONITORING EQUIPMENT	A device, or part of a physiological monitoring or measuring system, including its associated accessories used for intermittent assessment of a PATIENT'S blood pressure by an externally applied means.		IEC 60601-2-30:1999
AUTOMATIC CYCLING NON-INVASIVE BLOOD PRESSURE MONITORING EQUIPMENT	Stand alone measuring EQUIPMENT or part of a physiological monitoring or measuring system, including associated TRANSDUCERS, that is used for the internal measurement of circulatory system pressures.		IEC 60601-2-34:2000
AUTOMATIC EXPOSURE CONTROL	In an X-RAY GENERATOR, mode of operation in which one or more LOADING FACTORS are controlled automatically in order to obtain at a pre-selected location a desired quantity of RADIATION.	rm-36-46	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61267:1994
AUTOMATIC EXPOSURE RATE CONTROL	In an X-RAY GENERATOR, mode of operation in which the rate of emitted RADIATION is controlled automatically by control of one or more LOADING FACTORS in order to obtain at a pre-selected location and in a pre-selected LOADING TIME a desired quantity of RADIATION.	rm-36-47	IEC 61223-3-1:1999
AUTOMATIC INTENSITY CONTROL	In an X-RAY GENERATOR, mode of operation in which one or more LOADING FACTORS are controlled automatically in order to obtain at a pre-selected location a desired rate of a RADIATION QUANTITY.	rm-36-48	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 61223-2-9:1999
AUXILIARY MAINS SOCKET-OUTLET	Socket-outlet with MAINS VOLTAGE on EQUIPMENT, accessible without the use of a TOOL and intended for provision of mains supply to other EQUIPMENT or to other separate parts of the EQUIPMENT.	NG.07.04	IEC 60601-1/A2:1995 IEC 60601-2-12:2001 IEC 60601-2-13:2003
AVERAGE INCUBATOR TEMPERATURE	The average of the INCUBATOR TEMPERATURE readings taken at regular intervals achieved during STEADY TEMPERATURE CONDITION (see Figure 101).		IEC 60601-2-19/A1:1996
AVERAGE TEMPERATURE	The average of temperature readings taken at regular intervals at any specified point in the BABY COMPARTMENT achieved during STEADY TEMPERATURE CONDITION.		IEC 60601-2-19/A1:1996
AVERAGE TEMPERATURE	The average of the maximum and minimum temperatures at any specified point in the BABY COMPARTMENT achieved during STEADY TEMPERATURE CONDITION.		IEC 60601-2-20/A1:1996
AVERAGE TRANSPORT INCUBATOR TEMPERATURE	The average of the maximum and minimum TRANSPORT INCUBATOR TEMPERATURES achieved during STEADY TEMPERATURE CONDITION (see Figure 101).		IEC 60601-2-20/A1:1996
AXIAL FIELD OF VIEW	Dimensions of a slice through the TOMOGRAPHIC VOLUME parallel to and including the SYSTEM AXIS. In practice it is specified only by its axial dimension given by the distance between the centres of the outermost defined IMAGE PLANES plus the average of the measured AXIAL SLICE WIDTH measured as EQUIVALENT WIDTH (EW).	rm-32-51	IEC 61675-1:1998 IEC 61675-2:1998
AXIAL POINT SPREAD FUNCTION	Profile passing through the peak of the PHYSICAL POINT SPREAD FUNCTION in a plane parallel to the SYSTEM AXIS.	rm-32-52	IEC 61675-1:1998 IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
AXIAL RESOLUTION	For tomographs with sufficiently fine axial sampling fulfilling the sampling theorem, SPATIAL RESOLUTION along a line parallel to the SYSTEM AXIS.	rm-32-53	IEC 61675-1:1998 IEC 61675-2:1998
AXIAL SLICE WIDTH	For tomographs, the width of the AXIAL POINT SPREAD FUNCTION.	rm-33-54	IEC 61675-1:1998 IEC 61675-2:1998
BABY COMPARTMENT	An environmentally-controlled ENCLOSURE intended to contain a baby and with transparent section(s) which allows for viewing of the baby.		IEC 60601-2-19/A1:1996
BABY CONTROLLED INCUBATOR	An AIR CONTROLLED INCUBATOR which has additional capability of automatically controlling the INCUBATOR air temperature in order to maintain the temperature as measured by a SKIN TEMPERATURE SENSOR close to a value set by the USER.		IEC 60601-2-19/A1:1996
BABY CONTROLLED MODE	A mode of operation in which the power output varies automatically in response to the temperature of the baby, to achieve a temperature close to a value set by the USER.		IEC 60601-2-21/A1:1996
BABY CONTROLLED TRANSPORT INCUBATOR	An air controlled TRANSPORT INCUBATOR which has the additional capability of automatically controlling the INCUBATOR air temperature in order to maintain the temperature as measured by a SKIN TEMPERATURE SENSOR close to a value set by the USER.		IEC 60601-2-20/A1:1996
BACK POINTER	Luminous or mechanical device intended to indicate the RADIATION BEAM AXIS and its point of exit from the PATIENT.	rm-35-13	IEC 60976/ A1:2000
BACK-SCATTERING	SCATTERING of particles or RADIATION by material through angles greater than 90° with respect to their initial direction.	rm-12-04	IEC 60806:1984
BACTERIAL FILTER	Device that removes bacteria and particulate matter from the gas stream. [ISO 4135:1995, definition 4.1.7 modified]		IEC 60601-2-12:2001
BASE DEPTH	Depth in a PHANTOM of the plane containing the distal point of 90 % of the maximum ABSORBED DOSE on the RADIATION BEAM AXIS.		IEC 60976/A1:2000
BASELINE VALUE	REFERENCE VALUE of functional parameter: – either the value obtained for this parameter in the initial CONSTANCY TEST immediately following a STATUS TEST, or – where described in a corresponding particular standard, the mean value of values obtained in a series of initial CONSTANCY TESTS, immediately following a STATUS TEST.	rm-73-11	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
BASIC INSULATION	Insulation applied to LIVE parts to provide basic protection against electric shock.	NG.03.02	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
BEAM ALIGNMENT AXIS	Straight line joining the points of maximum PULSE-INTENSITY INTEGRAL measured at several different distances in the far field. For the purposes of alignment, this line may be projected to the face of the ULTRASONIC TRANSDUCER.		IEC 60601-2-37:2001
BEAM APPLICATOR	<p>In MEDICAL RADIOLOGY, device usually attached to the RADIATION SOURCE ASSEMBLY performing at least one of the following functions:</p> <ul style="list-style-type: none"> - to indicate the RADIATION BEAM AXIS; <p>to indicate the RADIATION FIELD;</p> <ul style="list-style-type: none"> - to ensure a minimum distance from the RADIATION SOURCE to the ENTRANCE SURFACE; - to serve as COMPRESSION DEVICE. <p>NOTE 1 A BEAM APPLICATOR may include PROTECTIVE SHIELDING and serve as a BEAM LIMITING DEVICE.</p> <p>NOTE 2 As BEAM APPLICATORS may be mentioned: pointing APPLICATOR, open-ended APPLICATOR, dental BEAM APPLICATOR, therapeutic BEAM APPLICATOR.</p>	rm-37-30	IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60976/A1:2000 IEC 61223-2-7:1999 IEC 61223-3-4:2000 IEC 62083:2000
BEAM AREA	<p>Area in the specified plane perpendicular to the BEAM-ALIGNMENT AXIS consisting of all points at which the PULSE-INTENSITY INTEGRAL is greater than a specified fraction of the maximum PULSE-INTENSITY INTEGRAL in that plane.</p> <p>NOTE For measurement purposes the PULSE-INTENSITY INTEGRAL can be taken as being proportional to the PULSE PRESSURE-SQUARED INTEGRAL.</p>		IEC 60601-2-37:2001
BEAM LIMITING DEVICE	Device to limit the RADIATION FIELD.	rm-37-28	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60976/A1:2000 IEC 61217:2002 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 62083:2000

Term	Definition	Reference	Used in IEC
BEAM LIMITING SYSTEM	Entirety of parts and their geometrical configuration contributing to the limitation of the RADIATION BEAM.	rm-37-27	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60976/ A1:2000 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61331-1:1994
BEAM NON-UNIFORMITY RATIO	Ratio of the square of the maximum r.m.s. acoustic pressure to the spatial average of the square of the r.m.s. acoustic pressure where the spatial average is taken over the EFFECTIVE RADIATING AREA, determined in accordance with IEC 61689. [IEC 61689, definition 3.9, modified]		IEC 60601-2-5:2000
BEAM OFF	The condition in which the RADIATION SOURCE (S) is fully shielded, and is also in a position in which it can be secured.		IEC 60601-2-11:1997
BEAM ON	The condition in which the RADIATION SOURCE (S) is fully exposed for RADIOTHERAPY.		IEC 60601-2-11:1997
BEAM SCATTERING FILTER	FILTER used in order to scatter a beam of ELECTRONS.	rm-35-09	IEC 60601-2-1/A1:2002 IEC 60976/A1:2000
BEAM TYPE	Descriptive classification for the ultrasonic beam in one of three types: collimated, convergent or divergent. [IEC 61689, definition 3.11]		IEC 60601-2-5:2000
BEST FOCUS	Setting of focusing potentials resulting in maximum integrated area under the MTF curve for the given slit orientation. NOTE This setting of focusing potentials is chosen to reduce ambiguity and may slightly deviate from settings in practical use of the XRII.		IEC 61262-7:1995
BIOPOTENTIAL INPUT PART	APPLIED PART(s) of EQUIPMENT or SYSTEM for the collection of biopotentials.		IEC 60601-2-40:1998
BIPOLAR ELECTRODE	Assembly of two ACTIVE ELECTRODES on the same support, so constructed that, when energised, the hf current flows mainly between these two ELECTRODES.		IEC 60601-2-2:1998
BLANKET	Flexible HEATING DEVICE, which may be folded, for use under or over a PATIENT.		IEC 60601-2-35:1996
BLOOD LEAK	A leakage of blood from the blood compartment to the DIALYSING FLUID compartment of the DIALYSER due to a rupture of the semi-permeable membrane.		IEC 60601-2-16:1998
BLOOMING VALUE	As a characteristic of the EFFECTIVE FOCAL SPOT of an X-RAY TUBE, ratio of two resolution limits obtained under specific LOADING conditions.	rm-20-15	IEC 60336:1993
BOLUS	Discrete quantity of liquid which is delivered in a short time.		IEC 60601-2-24:1998
BONE THERMAL INDEX	THERMAL INDEX for applications, such as foetal (second and third trimester) or neonatal cephalic (through the fontanelle), in which the ULTRASOUND beam passes through soft tissue and a focal region is in the immediate vicinity of bone. Symbol: <i>TIB</i> . Unit: None. NOTE See DD.4.2 and DD.5.2 for methods of determining the BONE THERMAL INDEX.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
BOUNDARY AND DIMENSIONS OF THE X-RAY FIELD	In this collateral standard IEC 60601-1-3:1994, the boundary of an X-ray field (see rm-37-07), is described by the locus of points at which the AIR KERMA RATE is 25 % of the mean of the AIR KERMA RATE at the approximate centres of the quarters of the area enclosed. The dimensions of an X-ray field are described in terms of the lengths of its intercepts on each of two orthogonal major axes in the plane of interest. Unless otherwise stated, it is to be assumed that the plane of interest is at right angles to the REFERENCE AXIS; also that the major axes intersect on the REFERENCE AXIS and are oriented so that one axis is collinear with the PROJECTION of the longitudinal axis of the X-RAY TUBE lying in the plane and passing through this point of intersection.		IEC 60601-1-3:1994
BOUNDED OUTPUT POWER	OUTPUT POWER emitted in SCANNING MODE from a region of the active area of the TRANSDUCER whose width in the scan plane is limited to 1 cm. Symbol: P_1 . Unit: milliwatts, mW.		IEC 60601-2-37:2001
BRACHYRADIOTHERAPY	Intracavitary, interstitial or SUPERFICIAL RADIOTHERAPY using one or more SEALED RADIOACTIVE SOURCES.	rm-42-52	IEC 62083:2000
BRACHYTHERAPY SOURCE MODEL/BRACHYTHERAPY SOURCE MODELING	All physical, geometric and radiation parameters required to plan a course of RADIOTHERAPY for a particular BRACHYTHERAPY RADIOACTIVE SOURCE. The process of establishing the BRACHYTHERAPY SOURCE MODEL is referred to as "BRACHYTHERAPY SOURCE MODELING".		IEC 62083:2000
BREAK-POINT DEPTH	Value equal to 1,5 times the EQUIVALENT APERTURE DIAMETER, and given by $z_{bd} = 1,5 D_{eq}$ where D_{eq} is the EQUIVALENT APERTURE DIAMETER. Symbol: z_{bp} . Unit: centimetres, cm.		IEC 60601-2-37:2001
BROAD BEAM	RADIATION BEAM of such a solid angle that a further increase of the solid angle does not appreciably increase a measured RADIATION QUANTITY, thus including the contribution of SCATTERED RADIATION.	rm-37-24	IEC 60627:2001 IEC 61331-1:1994
BROAD BEAM CONDITION	Arrangement for the measurement of a RADIATION QUANTITY in a BROAD BEAM of IONIZING RADIATION.	rm-37-25	IEC 60627:2001 IEC 61267:1994
BUFFER-FREE HAEMODIAFILTRATION	A specific form of HDF where the buffer is not given to the PATIENT with the DIALYSING FLUID, but with the SUBSTITUTION FLUID.		IEC 60601-2-16:1998
BUILD UP	Phenomenon of the increase with depth of the ABSORBED DOSE RATE due to the release of secondary charged particles and to SCATTERED RADIATION in matter beyond the ENTRANCE SURFACE.	rm-12-12	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60976/ A1:2000
BUILD UP FACTOR	Letter symbol: B . For a material irradiated, ratio of the value of a RADIATION QUANTITY in the centre of a BROAD BEAM of specified RADIATION QUALITY and the corresponding value of the RADIATION QUANTITY in the centre of a NARROW BEAM, both values measured in the material under consideration.	rm-13-49	IEC 61331-1:1994
CALIBRATION ("CAL")	Facility enabling the CALIBRATION VOLTAGE and zero voltage to be recorded in place of the ELECTROCARDIOGRAM.		IEC 60601-2-51:2003
CALIBRATION FACTOR	For a CHAMBER ASSEMBLY with an associated MEASURING ASSEMBLY it is the factor which converts the INDICATED VALUE, corrected to stated REFERENCE CONDITIONS, to the CONVENTIONAL TRUE VALUE at the position of the REFERENCE POINT of the IONIZATION CHAMBER. For an IONIZATION CHAMBER calibrated on its own without a specified MEASURING ASSEMBLY, the CALIBRATION FACTOR converts the ionization charge or current, corrected to REFERENCE CONDITIONS, to the CONVENTIONAL TRUE VALUE at the position of the REFERENCE POINT of the CHAMBER (this is the reciprocal of RESPONSE under REFERENCE CONDITIONS).		IEC 60731/A1:2002
CALIBRATION INTERVAL	Recommended time between calibrations as described in the ACCOMPANYING DOCUMENTS.		IEC 60601-3-1:1996
CALIBRATION VOLTAGE	Voltage step recorded for amplitude CALIBRATION PURPOSES.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
CAPACITIVELY COUPLED HF CURRENT	Unavoidable high frequency current flowing from an ENDOSCOPICALLY-USED ACCESSORY to the ENDOSCOPE.		IEC 60601-2-18 A1:2000
CAPACITOR DISCHARGE HIGH-VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR in which the electrical energy is stored in a HIGH VOLTAGE capacitor to be supplied to an X-RAY TUBE by discharge in a single LOADING.	rm-21-08	IEC 60601-1-3:1994 IEC 60601-2-7:1998
CAPSULE	Of a SEALED RADIOACTIVE SOURCE, container in which the radioactive material is hermetically sealed for its intended use.	rm-20-16	IEC 60601-2-17/A1:1996
CARDIAC DEFIBRILLATOR	MEDICAL ELECTRICAL EQUIPMENT intended to defibrillate the heart by an electrical PULSE via ELECTRODES applied either to the PATIENT'S skin (external ELECTRODES), or to the exposed heart (internal ELECTRODES). May be referred to as DEFIBRILLATOR or EQUIPMENT. NOTE Such EQUIPMENT may also include other monitoring or therapeutic functions.		IEC 60601-2-4:2002
CASSETTE CHANGER	SERIAL CHANGER in which each RECORD is taken upon a RADIOGRAPHIC FILM in a separate RADIOGRAPHIC CASSETTE.	rm-31-06	IEC 61223-2-11:1999
CATEGORY AP EQUIPMENT	EQUIPMENT or EQUIPMENT part complying with specified requirements on construction, marking and documentation in order to avoid sources of ignition in a FLAMMABLE ANAESTHETIC MIXTURE WITH AIR.	NG.02.02	IEC 60601-1:1988 IEC 60601-1/A2:1995
CATEGORY APG EQUIPMENT	EQUIPMENT or EQUIPMENT part complying with specified requirements on construction, marking and documentation in order to avoid sources of ignition in a FLAMMABLE ANAESTHETIC MIXTURE WITH OXYGEN OR NITROUS OXIDE.	NG.02.03	IEC 60601-1:1988 IEC 60601-1/A2:1995
CATHETER TIP TRANSDUCER	TRANSDUCER mounted at or close to the tip of a catheter and intended for insertion into the cardiovascular system.		IEC 60601-2-34:2000
CATHODE	In an X-RAY TUBE, source of the ELECTRONS.	rm-22-05	IEC 60613:1989
CATHODE EMISSION CHARACTERISTIC	Dependence of the X-RAY TUBE CURRENT on variables, for example filament heating current, X-RAY TUBE VOLTAGE.	rm-36-20	IEC 60601-2-28:1993 IEC 60613:1989
CENTRAL AXIS	The line perpendicular to the ENTRANCE PLANE passing through the CENTRE OF THE ENTRANCE FIELD.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
CENTRAL ILLUMINANCE	(E_c) Illuminance at 1 m distance from the light-emitting area of the EQUIPMENT in THE LIGHT FIELD CENTRE (LFC) without any obstruction of the light beam.		IEC 60601-2-41:2000
CENTRAL LINE INDICATION	Marking on the incident face of a LINEAR GRID, which is intended to indicate the position and direction of the TRUE CENTRAL LINE. NOTE In most cases, this marking coincides with the geometric centre line of the grid's incident face.		IEC 60627:2001
CENTRAL MAGNIFICATION	As a characteristic of XRIIs, the ratio of the length in the OUTPUT IMAGE of the actual length of a small object placed in the ENTRANCE PLANE symmetrically about the CENTRAL AXIS.		IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995

Term	Definition	Reference	Used in IEC
CENTRAL TERMINAL ACCORDING TO WILSON (CT)	Terminal at the average potential of the R, L and F potentials.		IEC 60601-2-51:2003
CENTRE OF ROTATION (COR)	Origin of that coordinate system, which describes the PROJECTIONS of a transverse slice with respect to their orientation in space. NOTE The CENTRE OF ROTATION of a transverse slice is given by the intersection of the SYSTEM AXIS with the mid-plane of the corresponding OBJECT SLICE.		IEC 61675-2:1998
CENTRE OF THE ENTRANCE FIELD	That point in the ENTRANCE PLANE which is imaged at the CENTRE OF THE OUTPUT IMAGE.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
CENTRE OF THE OUTPUT IMAGE	The centre of the smallest circle circumscribing the OUTPUT IMAGE.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
CERENKOV COUNTER	Counting system which detects the Cerenkov radiation emitted from the sample. NOTE CERENKOV COUNTERS are used for measuring samples with β -emitting RADIONUCLIDES that have a particle energy larger than the Cerenkov threshold. Under special conditions, a LIQUID SCINTILLATION COUNTER can be used as a CERENKOV COUNTER.		IEC 61948-1:2001
CERTIFIED RADIOACTIVE STANDARD SOURCE	RADIOACTIVE SOURCE hat has been calibrated by a laboratory recognized as a country's national standardizing laboratory for RADIOACTIVITY measurements and has been so certified by the aforementioned laboratory.		IEC 61303:1994

Term	Definition	Reference	Used in IEC
CHAMBER (ionization)	<p>An IONIZING RADIATION DETECTOR consisting of a CHAMBER filled with air, in which an electric field insufficient to produce gas multiplication is provided for the collection at the ELECTRODES of charges associated with the ions and the ELECTRONS produced in the measuring volume of the detector by IONIZING RADIATION.</p> <p>NOTE For this standard IEC 60731/ A1:2002, the IONIZATION CHAMBER is considered to consist of the measuring volume, the collecting electrode, the guard electrode (if any) the outer electrode (which consists of the CHAMBER wall and possibly a conducting coating), those parts of the insulator adjacent to the measuring volume, the build-up cap and water-proof housing (if any).</p> <p>There are several categories of IONIZATION CHAMBER:</p> <p>Shell CHAMBER: an IONIZATION CHAMBER with a measuring volume of between 0,1 cm³ and 1,0 cm³ bounded by a rigid outer electrode mounted on a supporting stem. The measuring volume is usually symmetrical about the axis of the stem and the CHAMBER is intended to be used with the axis of symmetry perpendicular to the axis of the RADIATION BEAM. There are two types of shell CHAMBER:</p> <ol style="list-style-type: none"> 1) thimble CHAMBER: the outer electrode takes the form of a rigid cylindrical wall closed at one end and mounted at the other on the supporting stem; 2) spherical CHAMBER: the outer electrode takes the form of a rigid spherical wall mounted on the supporting stem; <p>Parallel-plate CHAMBER: an IONIZATION CHAMBER with a measuring volume of between 0,01 cm³ and 0,5 cm³ bounded by parallel ELECTRODES. The CHAMBER is intended to be used with the ELECTRODES perpendicular to the axis of the RADIATION BEAM;</p> <p>Vented CHAMBER: an IONIZATION CHAMBER constructed in such a way as to allow the air inside the measuring volume to communicate freely with the atmosphere such that corrections to the RESPONSE for changes in air density need to be made;</p> <p>Sealed CHAMBER: an IONIZATION CHAMBER constructed in such a way as to restrict the pathway between the air inside the measuring volume and the atmosphere sufficiently to ensure that the RESPONSE of the CHAMBER is independent of changes in ambient conditions over a period of time stated by the MANUFACTURER;</p> <p>Unguarded IONIZATION CHAMBER: an IONIZATION CHAMBER in which the guard conductor in the cable surrounding the centre (signal) conductor terminates in the cable and does not extend into the stem or body of the CHAMBER ASSEMBLY;</p> <p>Partially guarded IONIZATION CHAMBER: an IONIZATION CHAMBER in which the guard conductor in the cable surrounding the centre (signal) conductor extends well into the stem or body of the CHAMBER ASSEMBLY but does not enter the air in the CHAMBER;</p> <p>Guarded IONIZATION CHAMBER: an IONIZATION CHAMBER in which the guard conductor in the stem or body of the CHAMBER ASSEMBLY is continuous with a guard electrode that is in contact with the air inside the CHAMBER.</p>		IEC 60731/A1:2002
CHAMBER ASSEMBLY	The IONIZATION CHAMBER and all other parts to which the CHAMBER is permanently attached, except the MEASURING ASSEMBLY. It includes the electrical fitting and any permanently attached cable.	rm-51-08	IEC 60601-2-9:1996 IEC 60731/A1:2002
CHANNEL	In EQUIPMENT for remotely controlled after-loading, tubing in which a particular SEALED RADIOACTIVE SOURCE or assembly of SEALED RADIOACTIVE SOURCES is moved.	rm-25-02	IEC 60601-2-17/A1:1996
CHANNEL	Complete system for the amplification and conditioning of potential differences between a pair or combination of ELECTRODES.		IEC 60601-2-26:2002
CHANNEL	Hardware and/or software selection of a particular ELECTROCARDIOGRAPHIC LEAD for purposes of display, recording, or TRANSMISSION.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
CHARGING CIRCUIT	Circuit within the DEFIBRILLATOR intended for charging the ENERGY STORAGE DEVICE. This circuit includes all parts conductively connected to the ENERGY STORAGE DEVICE during the charging period.		IEC 60601-2-4:2002
CINERADIOGRAPHY	INDIRECT RADIOGRAPHY of moving objects usually in rapid series on cine film.	rm-41-14	IEC 60601-2-7:1998 IEC 61223-1:1993 IEC 61223-3-1:1999
CLASS I EQUIPMENT	EQUIPMENT in which protection against electric shock does not rely on BASIC INSULATION only, but which includes an additional SAFETY precaution in that means are provided for the connection of the EQUIPMENT to the PROTECTIVE EARTH CONDUCTOR in the fixed wiring of the installation in such a way that ACCESSIBLE METAL PARTS cannot become LIVE in the event of a failure of the BASIC INSULATION.	NG.02.04	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
CLASS II EQUIPMENT	EQUIPMENT in which protection against electric shock does not rely on BASIC INSULATION only, but in which additional SAFETY precautions such as DOUBLE INSULATION or REINFORCED INSULATION are provided, there being no provision for protective earthing or reliance upon installation conditions.	NG.02.05	IEC 60601-1:1988 IEC 60601-1/A2:1995
CLEARLY LEGIBLE	Visual attribute of information displayed by the EQUIPMENT that allows the OPERATOR to discern (or identify) qualitative or quantitative values or functions under a specific set of environmental conditions.		IEC 60601-2-12:2001
COAGULATION	Sealing of small blood vessels or of body tissue caused by the passage of high frequency current at the ACTIVE ELECTRODE(S).		IEC 60601-2-2:1998
COEFFICIENT OF VARIATION	Standard deviation of a set of readings expressed as a percentage of the mean value of these readings.	rm-73-12	IEC 60580:2000 IEC 61674/ A1:2002
COINCIDENCE DETECTION	A method which checks whether two opposing detectors have detected one PHOTON each simultaneously. By this method the two PHOTONS are concatenated into one event. NOTE THE COINCIDENCE DETECTION between two detector elements serves as an electronic collimation to define the corresponding PROJECTION BEAM or LINE OF RESPONSE (LOR), respectively.		IEC 61675-1:1998
COINCIDENCE WINDOW	Time interval during which tow detected PHOTONS are considered being simultaneous.		IEC 61675-1:1998
COLD CONDITION	The condition obtained if EQUIPMENT is de-energized for a sufficiently long time to attain the ambient temperature.	NG.10.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
COLLIMATOR (for GAMMA CAMERAS)	In a RADIONUCLIDE imaging device, block of radiation attenuating material with one or more APERTURES defining the field of view and limiting the angular spread of the RADIATION that can reach the RADIATION DETECTOR ASSEMBLY.	rm-34-05	IEC 60789:1992 IEC 61675-2:1998 IEC 61675-3:1998

Term	Definition	Reference	Used in IEC
COLLIMATOR AXIS	Straight line which passes through the geometrical centre of the exit and ENTRANCE FIELDS of the COLLIMATOR.	rm-34-32	IEC 60789:1992 IEC 61948-2:2001
COLLIMATOR BACK FACE	Surface of the COLLIMATOR which is closest to the radiation detection assembly.		IEC 60789:1992
COLLIMATOR FRONT FACE	Surface of the COLLIMATOR which is closest to the object being imaged.		IEC 60789:1992
COMBINED STANDARD UNCERTAINTY	Defined in ISO: Guide to the expression of uncertainty in measurement (1993)		IEC 60580:2000
COMBINED-OPERATING MODE	Mode of operation of an EQUIPMENT which combines more than one DISCRETE-OPERATING MODE.		IEC 60601-2-37:2001
COMMON MODE DC OFFSET VOLTAGE	DC voltage appearing on LEAD ELECTRODES with respect to the NEUTRAL ELECTRODE resulting from ELECTRODE-skin voltages.		IEC 60601-2-51:2003
COMMON MODE REJECTION	Ability of the ELECTROCARDIOGRAPH including the PATIENT CABLE and LEAD ELECTRODES, high frequency filters, protection networks, LEAD networks, amplifier input, etc., to discriminate between signals with differences between amplifier inputs (differential signal) and signals common to both amplifier inputs (common signal), in the presence of LEAD ELECTRODE impedance imbalance.		IEC 60601-2-51:2003
(IMMUNITY) COMPLIANCE LEVEL	Level less than or equal to the IMMUNITY LEVEL for which the EQUIPMENT or SYSTEM meets the requirements of the applicable subclause of 36.202. NOTE Additional requirements for COMPLIANCE LEVELS are specified in 6.8.201.1.		IEC 60601-1-2:2001
COMPLIANCE VOLUME	Area of PATIENT accessible space in which compliance of GRADIENT OUTPUT is inspected In MR EQUIPMENT with a cylindrical WHOLE BODY MAGNET, the COMPLIANCE VOLUME is a cylinder with its axis coinciding with the magnet axis and with a radius of 0,20 m. In MR EQUIPMENT with a TRANSVERSE FIELD MAGNET and a WHOLE BODY GRADIENT SYSTEM, the COMPLIANCE VOLUME is a volume bound by planes parallel to the magnet poles and separated by a distance that is either the largest dimension of the accessible space between the poles of the magnet, or 0,40 m, whichever is less. In all other MR EQUIPMENT the COMPLIANCE VOLUME is the volume where any part of a PATIENT body can be properly located according to the intended use of the MR EQUIPMENT.		IEC 60601-2-33:2002
COMPOSITION OF REFERENCE MATERIALS	Values of ATTENUATION EQUIVALENT, HALF-VALUE LAYER and QUALITY EQUIVALENT FILTRATION expressed in this collateral standard IEC 60601-1-3:1994 as thickness of aluminum or lead, apply to reference materials of the following composition: – aluminum of purity 99,99 % or higher and density 2,70 g cm ⁻³ ; – lead of purity 99,99 % or higher and density 11,35 g cm ⁻³ .		IEC 60601-1-3:1994

Term	Definition	Reference	Used in IEC
COMPRESSION DEVICE	In MEDICAL RADIOLOGY, device used to exert pressure upon a part of a PATIENT during either examination or TREATMENT.	rm-35-15	IEC 60601-1-3:1994 IEC 60601-2-45:2001 IEC 61223-2-10:1999
COMPUTED TOMOGRAPHY	RECONSTRUCTIVE TOMOGRAPHY in which recording and processing is effected by a computing system.	rm-41-20	IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-3-1:1999 IEC 62083:2000
COMPUTED TOMOGRAPHY DOSE INDEX (CTDI)	<p>Integral of the DOSE PROFILE along a line perpendicular to the TOMOGRAPHIC PLANE from -7 times T to $+7$ times T (where T is the NOMINAL TOMOGRAPHIC SLICE THICKNESS), divided by the product of the NOMINAL TOMOGRAPHIC SLICE THICKNESS and the number of tomograms N produced in a single scan.</p> $CTDI = \frac{1}{NxT} \int_{-7xT}^{+7xT} D(z) dz$ <p>where</p> <p>T is the NOMINAL TOMOGRAPHIC SLICE THICKNESS;</p> <p>N is the number of tomograms produced in a single scan;</p> <p>$D(z)$ is the DOSE PROFILE along a line z perpendicular to the TOMOGRAPHIC PLANE.</p> <p>NOTE A scan can consist of a number of tomograms (slices).</p>		IEC 61223-2-6:1994

Term	Definition	Reference	Used in IEC
COMPUTED TOMOGRAPHY DOSE INDEX 100 (CTDI ₁₀₀)	<p>The integral of the DOSE PROFILE produced in a single axial scan along a line perpendicular to the TOMOGRAPHIC PLANE from -50 mm to $+50$ mm, divided by the product of the number of TOMOGRAPHIC SECTIONS N and the NOMINAL TOMOGRAPHIC SECTION THICKNESS T</p> $CTDI_{100} = \frac{1}{N \times T} \int_{-50mm}^{+50mm} D(z) dz$ <p>where</p> <p>$D(z)$ is the DOSE PROFILE along a line z perpendicular to the TOMOGRAPHIC PLANE, where dose is reported as ABSORBED DOSE to air;</p> <p>N is the number of TOMOGRAPHIC SECTIONS produced in a single axial scan of the X-RAY SOURCE;</p> <p>T is the NOMINAL TOMOGRAPHIC SECTION THICKNESS.</p> <p>NOTE 1 The term $CTDI_{vol}$ has been introduced as a more representative value for dose than the traditional $CTDI$ integrated from $-7T$ to $+7T$ as defined by the FDA in 21 CFR 1020.331.</p> <p>NOTE 2 The dose is reported as ABSORBED DOSE to air. This is required in order to avoid present confusion, as some MANUFACTURERS of CT SCANNERS express dose values calculated as ABSORBED DOSE to air and others as ABSORBED DOSE to polymethyl-methacrylate (PMMA).</p> <p>Although $CTDI_{100}$ refers to ABSORBED DOSE to air, for practical purposes the evaluation of ABSORBED DOSE to air within a PMMA dosimetry PHANTOM is well approximated by measurement of the AIR KERMA with an IONIZATION CHAMBER in the PHANTOM.</p> <p>NOTE 3 This definition assumes that the DOSE PROFILE is centred on $z = 0$.</p> <p>NOTE 4 A single axial scan is typically a 360° rotation of the X-RAY SOURCE.</p>		IEC 60601-2-44:2002
COMPUTED TOMOGRAPHY NUMBER (CT NUMBER)	<p>Number used to represent the mean X-RAY ATTENUATION associated with each elemental area of the COMPUTED TOMOGRAPHY image.</p> <p>NOTE The COMPUTED TOMOGRAPHY NUMBER is normally expressed in Hounsfield units. MEASURED VALUES of ATTENUATION are transformed INTO COMPUTED TOMOGRAPHY NUMBERS using the international Hounsfield scale, using the expression:</p> $CT \text{ number of material} = \frac{\mu_{material} - \mu_{water}}{\mu_{water}} \times 1000$ <p>where</p> <p>μ is the linear ATTENUATION COEFFICIENT.</p> <p>The CT number scale is defined so that water has a value of 0 and air a value of 1000.</p>		IEC 61223-2-6:1994
CONDITIONS OF ADEQUATE HEAT DISCHARGE	The conditions achieved when a HEATING DEVICE is supported and covered as specified in Annex EE.		IEC 60601-2-35:1996

Term	Definition	Reference	Used in IEC
CONDUCTIVE CONNECTION	Connection through which a current can flow exceeding the allowable LEAKAGE CURRENT.	NG.07.05	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-17/A1:1996 IEC 60601-2-51:2003
CONSTANCY TEST	Each of a series of tests, carried out: <ul style="list-style-type: none"> – to ensure that the functional performance of EQUIPMENT meets ESTABLISHED CRITERIA; or – to enable the early recognition of changes in the properties of components of the EQUIPMENT. 	rm-70-03	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
CONSTANT POTENTIAL HIGH-VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR with a PERCENTAGE RIPPLE of the output voltage not exceeding a specific value.	rm-21-06	IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001
CONTACT SURFACE TEMPERATURE	The temperature T_R at the reference point of the heated APPLIED PART (see Figures 101a and 101b).		IEC 60601-2-35:1996
CONTINUATION	In RADIOTHERAPY, re-starting IRRADIATION after INTERRUPTION of IRRADIATION without re-selection of operating conditions.		IEC 60601-2-17 /A1:1996
CONTINUOUS MODE	For an X-RAY GENERATOR, mode of LOADING an X-RAY TUBE continuously as in RADIOTHERAPY or in RADIOSCOPY.	rm-36-42	IEC 60601-1-3:1994 IEC 60601-2-7:1998
CONTINUOUS OPERATION	Operation under normal load for an unlimited period, without the specified limits of temperature being exceeded.	NG.10.02	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-17/A1:1996 IEC 60601-2-51:2003
CONTINUOUS OPERATION WITH INTERMITTENT LOADING	Operation in which EQUIPMENT is connected continuously to the SUPPLY MAINS. The stated permissible LOADING TIME is so short that the long term on-load operating temperature is not attained. The ensuing interval in LOADING is, however, not sufficiently long for cooling down to the long term no-load operating temperature.	NG.10.03	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997

Term	Definition	Reference	Used in IEC
CONTINUOUS OPERATION WITH SHORT-TIME LOADING	Operation in which EQUIPMENT is connected continuously to the SUPPLY MAINS. The stated permissible LOADING TIME is so short that the long term on-load operating temperature is not attained. The ensuing interval is, however, sufficiently long for cooling down to the long term no-load operating temperature.	NG.10.04	IEC 60601-1:1988 IEC 60601-1/A2:1995
CONTINUOUS RECORDER	EQUIPMENT which performs continuous analysis and/or recording of the ECG.		IEC 60601-2-47:2001
CONTRAST IMPROVEMENT RATIO	Letter symbol: <i>K</i> . Characteristic of an ANTI-SCATTER GRID, evaluated as the ratio of the TRANSMISSION OF PRIMARY RADIATION to the TRANSMISSION OF TOTAL RADIATION, under specific measuring conditions.		IEC 60627:2001
CONTRAST INDEX	For CONSTANCY TESTS in X-RAY EQUIPMENT, difference between the SPEED INDEX and the value of optical density produced by a constant EXPOSURE from a light source, greater than that used for producing the SPEED INDEX. NOTE 1 This EXPOSURE is normally aimed at an optical density in the range from 1,6 to 2,0 above that of film base plugs fog density. NOTE 2 SPEED INDEX and CONTRAST INDEX are used as constancy parameters and are intended to facilitate the routine checks described in Technical report IEC 61223-2-1:1993. They must not be confused with the sensitometric definitions of SENSITIVITY in terms of speed and average gradient.		IEC 61223-2-1:1993 IEC 61223-2-10:1999
CONTRAST RATIO (abbreviation CR)	The ratio of the luminance at the CENTRE OF THE OUTPUT IMAGE with an unblocked X-ray beam to the luminance at the CENTRE OF THE OUTPUT IMAGE when the X-ray beam is blocked at the CENTRE OF THE ENTRANCE FIELD, under specific conditions.		IEC 61262-6:1994
CONTROL PANEL	Part of EQUIPMENT in which one or more manually operated devices are mounted for the purpose of controlling all, or some, of the functions of the EQUIPMENT. The CONTROL PANEL may contain devices for indicating and displaying operating factors.	rm-83-02	IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-37:2001 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-3-1:1999
CONTROL SIDE RAIL	SIDE RAIL which incorporates BED function controls for PATIENT activation.		IEC 60601-2-38 /A1:1999
CONTROL TEMPERATURE	Temperature selected at the temperature control.		IEC 60601-2-19/A1:1996 IEC 60601-2-20/A1:1996
CONTROL TEMPERATURE	The temperature set at the temperature control.		IEC 60601-2-21/A1:1996
CONTROLLED ACCESS AREA	Area to which access is controlled for SAFETY reasons.		IEC 60601-2-33:2002
CONTROLLED AREA	Defined area which is part of an area under surveillance and for which access, occupancy and working conditions are regulated and controlled in order to protect persons against IONIZING RADIATION.	rm-63-05	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-45:2001
CONTROLLING TIMER	TIMING DEVICE changing a state of operation at the end of a predetermined time interval or of a predetermined total time that may consist of separate time intervals.	rm-83-04	IEC 60601-2-17 /A1:1996
CONTROLLING TIMER (abbreviation: timer)	Device to measure the time during which IRRADIATION occurs and, when a predetermined time is reached, to terminate IRRADIATION.		IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997

Term	Definition	Reference	Used in IEC
CONVENTIONAL TRUE VALUE	Value used instead of the TRUE VALUE when calibrating or determining the performance of an instrument, since in practice the TRUE VALUE is unknown and unknowable. NOTE The CONVENTIONAL TRUE VALUE will usually be the value determined by the STANDARD with which the instrument under test is compared.	rm-73-13	IEC 60580:2000 IEC 61674/A1:2002 IEC 60731/A1:2002
CONVERGING COLLIMATOR	Focused COLLIMATOR the geometrical focal plane of which lies before its entrance face.	rm-34-07	IEC 60789:1992
CONVERSION FACTOR	The ratio of the luminance in the CENTRE OF THE OUTPUT IMAGE of a specific zone in the OUTPUT IMAGE to the AIR KERMA RATE in the CENTRE OF THE ENTRANCE FIELD.		IEC 61262-2:1994
COORDINATE SYSTEM OF PROJECTION	Cartesian system of the IMAGE MATRIX of each two-dimensional PROJECTION with axes X_p and Y_p (defined by the axis of the IMAGE MATRIX). The Y_p axis and the PROJECTION of the SYSTEM AXIS onto the detector front face have to be in parallel. The origin of the COORDINATE SYSTEM OF PROJECTION is the centre of the IMAGE MATRIX.		IEC 61675-2:1998
COORDINATE SYSTEM OF PROJECTION	Recommended replacement: IEC 61675-2:1998		IEC 61675-2:1998
CORE BIOPSY GUN	Automatic needle device for performing core biopsy.		IEC 60601-2-45:2001
CORRECTION FACTOR	Dimensionless multiplier which corrects the INDICATED VALUE of an instrument from its value when operated under particular conditions to its value when operated under stated REFERENCE CONDITIONS.	rm-73-14	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/A1:2002 IEC 61676:2002
COUNT LOSS	Difference between measured COUNT RATE and TRUE COUNT RATE, which is caused by the finite RESOLVING TIME of the instrument.		IEC 61675-1:1998
COUNT RATE	Number of counts per unit of time.	rm-34-33	IEC 61675-1:1998 IEC 61675-3:1998
COUNT RATE	Recommended replacement: IEC 61675-1:1998, IEC 61675-3:1998		IEC 61675-2:1998
COUNT RATE CHARACTERISTIC	Function giving the relationship between observed COUNT RATE and TRUE COUNT RATE.	rm-34-21	IEC 60789:1992 IEC 61675-1:1998
CRANIAL-BONE THERMAL INDEX	THERMAL INDEX for applications, such as paediatric and adult cranial applications, in which the ULTRASOUND beam passes through bone near the beam entrance into the body. Symbol: <i>TIC</i> . Unit: None. NOTE See DD.4.3 for methods of determining the CRANIAL BONE THERMAL INDEX.		IEC 60601-2-37:2001
CREEPAGE DISTANCE	Shortest path along the surface of insulating material between two conductive parts.	NG.03.03	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
CROSS-GRID	ANTI-SCATTER GRID composed of two LINEAR GRIDS built together in such a way that the directions of their absorbing strips form an angle.		IEC 60627:2001

Term	Definition	Reference	Used in IEC
CUTTING	Resection or DISSECTION of body tissue caused by the passage of high frequency current of high current density at the ACTIVE ELECTRODE(S).		IEC 60601-2-2:1998
CT CONDITIONS OF OPERATION	All selectable parameters governing the operation of a CT SCANNER, for example NOMINAL TOMOGRAPHIC SECTION THICKNESS, PITCH FACTOR, FILTRATION, PEAK X-RAY TUBE VOLTAGE and either X-RAY TUBE CURRENT and LOADING TIME or CURRENT TIME PRODUCT.		IEC 60601-2-44:2002
CT DETECTOR	RADIATION DETECTOR which is used for CT DOSIMETRY.		IEC 61674/A1:2002
CT DOSIMETER	Diagnostic DOSIMETER which uses long narrow IONIZATION CHAMBERS and/or semi-conductor detectors for the measurement of AIR KERMA integrated along the length of the detector when the detector is exposed to a cross-sectional X-ray scan of a computed tomographic machine. A CT DOSIMETER contains the following components: <ul style="list-style-type: none"> – one or more detector assemblies; – a MEASURING ASSEMBLY. 		IEC 61674/ A1:2002
CT PITCH FACTOR	The ratio of the PATIENT SUPPORT travel Δd along the z direction per rotation of the X-RAY SOURCE divided by the product of the NOMINAL TOMOGRAPHIC SECTION THICKNESS T and the number of TOMOGRAPHIC SECTIONS N . $CT \text{ pitch factor} = \frac{\Delta d}{N \times T}$ where Δd is the PATIENT SUPPORT travel along the z direction per rotation of the X-RAY SOURCE; T is the NOMINAL TOMOGRAPHIC SECTION THICKNESS; N is the number of TOMOGRAPHIC SECTIONS produced by a single axial scan of the X-RAY SOURCE.		IEC 60601-2-44:2002
CT SCANNER	X-RAY EQUIPMENT for COMPUTED TOMOGRAPHY (CT). A computed TOMOGRAPHY X-ray system is a diagnostic X-ray system intended to generate cross-sectional images of the body by computer reconstruction of X-ray transmission data from the same axial plane at different angles. This generic type of device may include signal analysis and display EQUIPMENT, PATIENT and EQUIPMENT supports, support parts and accessories. NOTE Secondary imaging processing is not included in the scope of this standard.		IEC 60601-2-44:2002
CT SCANNER	X-RAY EQUIPMENT for COMPUTED TOMOGRAPHY (CT). A computed TOMOGRAPHY X-ray system is a diagnostic X-ray system intended to generate cross-sectional images of the body by computer reconstruction of X-ray transmission data obtained at different angles. This generic type of device may include signal analysis and display EQUIPMENT, PATIENT SUPPORT, support parts and ACCESSORIES. NOTE Secondary imaging processing is not included in the scope of this standard		IEC 60601-2-44:2002

Term	Definition	Reference	Used in IEC
CURRENT TIME PRODUCT	In MEDICAL RADIOLOGY, quantity of electricity resulting from the LOADING of an X-RAY TUBE, expressed in milliampere seconds, as the product of the mean X-RAY TUBE CURRENT in milliamperes and the duration of the LOADING in seconds.	rm-36-13	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
DAS CONTRAST SENSITIVITY	Ability of the DAS system to display low contrast vessels against background.		IEC 61223-3-3:1996
DAS VISUAL SPATIAL RESOLUTION	Ability of the DAS system to display small structures of high contrast. NOTE DAS VISUAL SPATIAL RESOLUTION depends both on technical and observer performance.		IEC 61223-3-3:1996
DECENTRING OF A FOCUSED GRID	Distance from the FOCAL SPOT of an X-RAY TUBE to the plane through the TRUE CENTRAL LINE of a FOCUSED GRID and perpendicular to the incident face of the grid.		IEC 60627:2001
DECREASING INPUT POWER RATING	Highest permitted X-RAY TUBE LOAD given as a function of LOADING TIME for single LOADINGS during which the ANODE INPUT POWER is decreased in steps or continuously.	rm-36-39	IEC 60613:1989
DEFAULT SETTING	Specific state of control, THE ULTRASONIC DIAGNOSTIC EQUIPMENT will enter upon power-up, new PATIENT select or change from non-foetal to foetal applications.		IEC 60601-2-37:2001
DEFIBRILLATOR ELECTRODES	ELECTRODES intended to deliver an electrical PULSE to the PATIENT for the purpose of cardiac defibrillation. NOTE DEFIBRILLATOR ELECTRODES may also provide other monitoring (e.g. ECG acquisition) or therapeutic (e.g. transcutaneous pacing) functions and may be disposable or reusable.		IEC 60601-2-4:2002
DEFIBRILLATION-PROOF APPLIED PART	APPLIED PART having protection against the effects of a discharge of a cardiac DEFIBRILLATOR to the PATIENT.	NG.01.27	IEC 60601-1/A2:1995 IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-51:2003
DEFOCUSING OF A FOCUSED GRID	Difference between the distance from the FOCAL SPOT of an X-RAY TUBE to the incident face of a FOCUSED GRID and the FOCUSING DISTANCE of that grid.		IEC 60627:2001
DEGRADATION (OF PERFORMANCE)	Undesired departure in the operational performance of an EQUIPMENT or SYSTEM from its intended performance. NOTE The term "DEGRADATION" can apply to temporary or permanent failure. [IEV 161-01-19, modified]		IEC 60601-1-2:2001
DELINEATED LIGHT FIELD	For RADIOTHERAPY SIMULATORS, the area of the LIGHT FIELD bounded by the DELINEATOR shadow and in a plane perpendicular to the X-ray beam axis.		IEC 61168:1993
DELINEATED RADIATION BEAM	That part of the RADIATION BEAM bordered by the shadow cast by the DELINEATORS.		IEC 60601-2-29:1999
DELINEATED RADIATION FIELD	Interception of the DELINEATED RADIATION BEAM by a perpendicular plane to the RADIATION BEAM AXIS.		IEC 61217:2002

Term	Definition	Reference	Used in IEC
DELINEATED RADIATION FIELD	Area of the DELINEATED RADIATION BEAM intercepted on a plane perpendicular to the REFERENCE AXIS.		IEC 60601-2-29:1999
DELINEATOR	A means for defining the border which outlines the simulated RADIATION FIELD.		IEC 61217:2002
DELINEATOR(S)	Means for defining the border(s) of the simulated RADIATION FIELD.		IEC 60601-2-29:1999 IEC 61217:2002
DELIVERED ENERGY	Energy which is delivered through the DEFIBRILLATOR ELECTRODES and dissipated in the PATIENT or in a resistance of specified value.		IEC 60601-2-4:2002
DENTAL PANORAMIC RADIOGRAPHY	DIRECT RADIOGRAPHY of a part of or the complete dentition by the use of an intraoral X-RAY TUBE.	rm-41-11	IEC 61223-1:1993
DENTAL PANORAMIC TOMOGRAPHY	DIRECT RADIOGRAPHY of a part or of the complete dentition by the application of a slit-DIAPHRAGM in combination with the relative motion of the X-RAY TUBE and the X-RAY IMAGE RECEPTOR.	rm-41-12	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61223-3-4:2000
DEPTH DOSE	ABSORBED DOSE at a specified depth beneath the ENTRANCE SURFACE or the irradiated object, usually on the RADIATION BEAM AXIS.	rm-13-51	IEC 62083:2000
DEPTH FOR BONE THERMAL INDEX	Distance from the plane where the -12 dB OUTPUT BEAM DIMENSIONS are determined along the BEAM ALIGNMENT AXIS to the plane where the product of ATTENUATED OUTPUT POWER and attenuated PULSE-INTENSITY INTEGRAL is maximum. Symbol: z_b . Unit: centimetres, cm.		IEC 60601-2-37:2001
DEPTH FOR SOFT-TISSUE THERMAL INDEX	Distance from the plane where the -12 dB OUTPUT BEAM DIMENSIONS are determined along the BEAM ALIGNMENT AXIS to the plane at which the lower value of the ATTENUATED OUTPUT POWER and the product of the ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY and 1 cm^2 is maximized over the distance range equal to, or more than, 1,5 times the EQUIVALENT APERTURE DIAMETER. Symbol: z_s . Unit: centimetres, cm. NOTE In this particular standard, the restricted definition of SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY from 3.49 of IEC 61102 relating to a specified plane is used where SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY is replaced by ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY.		IEC 60601-2-37:2001
DEPTH OF ILLUMINATION	Working distance around 1 m below the emitting surface of the EQUIPMENT, in which the illuminance reaches at least 20 % of CENTRAL ILLUMINANCE (E_c). (See Figure 115.)		IEC 60601-2-41:2000
DEPTH OF DOSE MAXIMUM	Depth in a PHANTOM of the maximum ABSORBED DOSE on the RADIATION BEAM AXIS with the surface of the PHANTOM at a specified distance.		IEC 60976/ A1:2000
DESIGNED FOR	When used in standards to characterize EQUIPMENT, devices, components or arrangements: designates an intended and usually apparent purpose or use for the product.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
DETACHABLE POWER SUPPLY CORD	Flexible cord intended to be connected to EQUIPMENT by means of a suitable APPLIANCE COUPLER.	NG.07.06	IEC 60601-1:1988 IEC 60601-1/A2:1995
DETECTIVE QUANTUM EFFICIENCY (DQE)	The ratio of the squared signal-to-noise ratio present at the output of a RADIATION DETECTOR to the squared signal-to-noise ratio present at the input of that RADIATION DETECTOR.		IEC 61262-5:1994

Term	Definition	Reference	Used in IEC
DETECTOR ASSEMBLY	The RADIATION DETECTOR and all other parts to which the RADIATION DETECTOR is permanently attached, except the MEASURING ASSEMBLY.		IEC 60601-2-9:1996
DETECTOR ASSEMBLY	RADIATION DETECTOR and all other parts to which the RADIATION DETECTOR is permanently attached, except the MEASURING ASSEMBLY. NOTE The DETECTOR ASSEMBLY normally includes: – the RADIATION DETECTOR and the stem (or body) on which the RADIATION DETECTOR is permanently mounted (or embedded); – the electrical fitting and any permanently attached cable or pre-amplifier.		IEC 61674/A1:2002
DETECTOR FIELD OF VIEW (FOV)	Region of the detector within which events are included in the display image. This region shall be specified by the MANUFACTURER.		IEC 60789:1992 IEC 61675-3:1998
DETECTOR FIELD OF VIEW	Region of the detector within which events are included in the displayed image. This region has to be specified by the MANUFACTURER.		IEC 61948-2:2001
DETECTOR HEAD	Assembly of the RADIATION DETECTOR ASSEMBLY, the COLLIMATOR and the DETECTOR SHIELD.	rm-34-09	IEC 60789:1992 IEC 61675-2:1998 IEC 61675-3:1998
DETECTOR HEAD	Consists of the RADIATION DETECTOR, the COLLIMATOR and the radiation shield.		IEC 61948-2:2001
DETECTOR HEAD TILT	Deviation of the COLLIMATOR AXIS from orthogonality with the SYSTEM AXIS.	rm-34-34	IEC 61675-2:1998 IEC 61948-2:2001
DETECTOR LINE SPREAD FUNCTION	The LSF measured with an uncollimated LINE SOURCE at a specified distance Z from the COLLIMATOR FRONT FACE.		IEC 60789:1992
DETECTOR POSITIONING TIME	Fraction of the total time spent on an acquisition which is not used in collecting data.		IEC 61675-2:1998
DETECTOR SHIELD	Component for attenuating IONIZING RADIATION outside the ENTRANCE FIELD of the COLLIMATOR.	rm-34-10	IEC 60789:1992
DEVELOPMENT LIFE-CYCLE	Necessary activities occurring during a period of time that starts at the concept phase of a project and finishes when the VALIDATION of the PEMS is complete.	rm-80-01	IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
DIALYSER	For the purpose of this Particular Standard, the term DIALYSER is used to describe any device containing a semi-permeable membrane that is used to perform HD/HDF/HF.		IEC 60601-2-16:1998
DIALYSING FLUID	A solution which is intended to exchange solutes and/or water with blood during HD/HDF. NOTE The words dialysate and dialysis fluid are commonly used as supplicated synonyms of DIALYSING FLUID.		IEC 60601-2-16:1998
DIALYSING FLUID CONCENTRATE	A solution of chemicals which, when appropriately diluted, produces DIALYSING FLUID.		IEC 60601-2-16:1998
DIALYSING SOLUTION	Pharmaceutical preparation (solution), according to the relevant Pharmacopoeia monograph for use with PERITONEAL DIALYSIS EQUIPMENT.		IEC 60601-2-39:1999

Term	Definition	Reference	Used in IEC
DIAPHRAGM	BEAM LIMITING DEVICE with either a fixed or an adjustable aperture in practically one plane.	rm-37-29	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60806:1984 IEC 60976/A1:2000 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994
DIFFERENTIAL RADIAL IMAGE DISTORTION	IMAGE DISTORTION for a small, radially oriented TEST DEVICE of constant length placed in any position in the ENTRANCE PLANE. DIFFERENTIAL RADIAL IMAGE DISTORTION is a function of position of this TEST DEVICE in the ENTRANCE PLANE.		IEC 61262-4:1994
DIRECT CARDIAC APPLICATION	Use of APPLIED PART which may come in direct CONDUCTIVE CONNECTION to the PATIENT'S heart.	NG.02.07	IEC 60601-1:1988 IEC 60601-1/A2:1995
DIRECT FOCAL DISTANCE	Shortest distance from the X-RAY IMAGE RECEPTOR to the position of the FOCAL SPOT.		IEC 60601-2-45:2001
DIRECT RADIOGRAM	RADIOGRAM obtained directly at the IMAGE RECEPTION AREA.	rm-32-03	IEC 60601-2-1/A1:2002 IEC 60806:1984
DIRECT RADIOGRAPHY	RADIOGRAPHY in which the recording is effected at an IMAGE RECEPTION AREA.	rm-41-07	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 61223-1:1993 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000
DIRECT RADIOSCOPY	RADIOSCOPY in which the visible images are presented at the IMAGE RECEPTION AREA, or close to it, in the RADIATION BEAM.	rm-41-02	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61331-2:1994
DISABLE	State of indefinite duration in which the ALARM SYSTEM or part of the ALARM SYSTEM does not annunciate an auditory ALARM SIGNAL.		IEC 60601-2-13:2003
DISCHARGE CIRCUIT	Circuit within the DEFIBRILLATOR which connects the ENERGY STORAGE DEVICE to the DEFIBRILLATOR ELECTRODES. This circuit includes all switching connections between that device and the DEFIBRILLATOR ELECTRODES.		IEC 60601-2-4:2002
DISCHARGE CONTROL CIRCUIT	Circuit including the manually operated discharge controls and all parts conductively connected to them.		IEC 60601-2-4:2002

Term	Definition	Reference	Used in IEC
DISCRETE-OPERATING MODE	Mode of operation of ULTRASONIC DIAGNOSTIC EQUIPMENT in which the purpose of the excitation of the ULTRASONIC TRANSDUCER or ULTRASONIC TRANSDUCER element group is to utilize only one diagnostic methodology.		IEC 60601-2-37:2001
DISINFECTABLE EQUIPMENT	EQUIPMENT parts which come into contact with the PATIENT during NORMAL USE and which may be disinfected in accordance with the MANUFACTURER'S instructions.		IEC 60601-2-9:1996
DISPLAY	Visual presentation of information.	rm-84-01	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-37:2001 IEC 60601-2-43:2000 IEC 61217:2002 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 62083:2000
DIVERGING COLLIMATOR	Focused COLLIMATOR, the geometrical focal plane of which lies behind its entrance face.	rm-34-08	IEC 60789:1992
DOME	The means for hydraulically coupling the PATIENT'S blood pressure to the TRANSDUCER, where a TRANSDUCER external to the PATIENT is used.		IEC 60601-2-34:2000
DOSE AREA PRODUCT	Product of the area of the cross-section of an X-ray beam and the averaged AIR KERMA over that cross-section. The unit is the Gray square metre (Gy.m ²). Dose area product rate, with the unit Gy.m ² .s ⁻¹ ; Dose area product (rate), used for brevity where either dose area product or dose area product rate apply, according to the context. NOTE The SI unit Gy.m ² may be expressed with a prefix, e.g. as μGy.m ² , to retain earlier used numeric dimensions of values displayed to the OPERATOR. Recommended replacement: rm-13-54		IEC 60601-2-43:2000
DOSE AREA PRODUCT	Letter symbol: <i>K.A.</i> Product of the area of the USEFUL BEAM and the AIR KERMA over the cross-section of the USEFUL BEAM, both quantities being measured at the same distance from the FOCAL SPOT. The unit of DOSE AREA PRODUCT is Gy.m ² .	rm-13-54	IEC 60580:2000
DOSE AREA PRODUCT METER	EQUIPMENT which uses IONIZATION CHAMBERS for the measurement of DOSE AREA PRODUCT or DOSE AREA PRODUCT RATE in the beam of an X-ray machine used for diagnostic MEDICAL RADIOLOGICAL EXAMINATIONS. A DOSE AREA PRODUCT METER contains the following components: – IONIZATION CHAMBER; – MEASURING ASSEMBLY; – STABILITY CHECK DEVICE.	rm-51-09	IEC 60580:2000

Term	Definition	Reference	Used in IEC
DOSE AREA PRODUCT RATE	Letter symbol: $\dot{K} \cdot A$. Quotient of an increment of DOSE AREA PRODUCT by the corresponding increment of time. The unit of DOSE AREA PRODUCT RATE is Gym^2/s .	rm-13-55	IEC 60580:2000
DOSE EQUIVALENT	Letter symbol: H . Quantity used to express the RISK of the deleterious effects of IONIZING RADIATION upon living organisms, given by the product of D , Q and N , at the point of interest in tissue: $H = Q N D$ where: D is the ABSORBED DOSE, Q is the quality factor and N is the product of any other modifying factors. The unit of DOSE EQUIVALENT is the joule per kilogram (J.kg^{-1}). The special name of the unit of DOSE EQUIVALENT is the sievert (Sv). The earlier unit of DOSE EQUIVALENT was the rem, 1 rem being equal to 10^{-2}J.kg^{-1} .	rm-13-24	IEC 60601-1-3:1994 IEC 60601-2-11:1997
DOSE EQUIVALENT LIMIT	Value, accumulated within a stated time, of effective dose equivalent to the body or of DOSE EQUIVALENT to parts of it, other than from natural IONIZING RADIATION and from IONIZING RADIATION due to medical procedures, which has been fixed as a limit for enforcement of RADIOLOGICAL PROTECTION.	rm-61-01	IEC 61331-3:1998
DOSE MONITOR UNIT	In a DOSE MONITORING SYSTEM, arbitrary unit in which a quantity is displayed and from which ABSORBED DOSE can be calculated.	rm-13-26	IEC 60601-2-1/A1:2002 IEC 60976/ A1:2000 IEC 62083:2000
DOSE MONITORING SYSTEM	System of devices for the measurement and display of a RADIATION QUANTITY directly related to the ABSORBED DOSE. It may include means for terminating IRRADIATION when a pre-selected value is reached.	rm-33-01	IEC 60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60976/ A1:2000
DOSE PROFILE	The representation of the dose as a function of position along a line.		IEC 60601-2-44:2002
DOSE PROFILE	Representation of the dose as a function of position along a line perpendicular to the TOMOGRAPHIC PLANE.		IEC 61223-2-6:1994
DOSE RATE MONITORING SYSTEM	System of devices for the measurement and display of a RADIATION QUANTITY directly related to the ABSORBED DOSE RATE.	rm-33-02	IEC 60601-2-1/A1:2002
DOSEMETER	RADIATION METER intended to measure the ABSORBED DOSE.	rm-50-02	IEC 60601-2-9:1996 IEC 60601-2-43:2000 IEC 61223-2-10:1999
DOSEMETER (PATIENT contact)	RADIATION METER used for the measurement on or in the PATIENT of ABSORBED DOSE, ABSORBED DOSE RATE, or any dose-related quantities in IONIZING RADIATION, such as EXPOSURE or KERMA. This EQUIPMENT usually consists of one or more RADIATION DETECTOR assemblies (for example CHAMBER assemblies) and a MEASURING ASSEMBLY.		IEC 60601-2-9:1996
DOSIMETER (diagnostic)	EQUIPMENT which uses IONIZATION CHAMBERS and/or semi-conductor detectors for the measurement of AIR KERMA, AIR KERMA LENGTH and/or KERMA, AIR KERMA RATE in the beam of an X-ray machine used for diagnostic MEDICAL RADIOLOGICAL EXAMINATIONS. A diagnostic DOSIMETER contains the following components: <ul style="list-style-type: none">– one or more detector assemblies which may or may not be an integral part of the MEASURING ASSEMBLY;– a MEASURING ASSEMBLY;– one or more STABILITY CHECK DEVICES (optional).		IEC 61674/ A1:2002

Term	Definition	Reference	Used in IEC
DOSIMETER (RADIOTHERAPY)	EQUIPMENT which uses IONIZATION CHAMBERS for the measurement of AIR KERMA, ABSORBED DOSE, or the corresponding rates, in PHOTON and ELECTRON radiation as used in radiation therapy. A RADIOTHERAPY DOSIMETER contains the following components: <ul style="list-style-type: none"> – one or more CHAMBER assemblies; – a MEASURING ASSEMBLY (including possibly a separate display device); – one or more STABILITY CHECK DEVICES (optional); – one or more PHANTOMS or build-up caps (optional). 	rm-33-07	IEC 60601-2-9:1996 IEC 60731/A1:2002
DOUBLE EMULSION FILM	For use in DIRECT RADIOGRAPHY, RADIOGRAPHIC FILM covered with radiation-sensitive emulsion on both sides of its carrier.	rm-32-34	IEC 61223-2-1:1993
DOUBLE INSULATION	Insulation comprising both BASIC INSULATION and SUPPLEMENTARY INSULATION.	NG.03.04	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-51:2003
DRIFT	Change of the GAS READING of a RGM, for a given GAS LEVEL over a stated period of time, under REFERENCE CONDITIONS that remain constant.		IEC 60601-2-55:To be published
DRIP-RATE INFUSION CONTROLLER	INFUSION CONTROLLER in which the delivery rate is set by the OPERATOR and indicated by the EQUIPMENT as a number of drops per unit of time.		IEC 60601-2-24:1998
DRIP-RATE INFUSION PUMP	INFUSION PUMP in which the delivery rate is set by the OPERATOR and indicated by the EQUIPMENT as a number of drops per unit of time.		IEC 60601-2-24:1998
DUMMY COMPONENT	Test replacement for moulded components like transformers, semiconductors etc. The DUMMY COMPONENT has a geometry equal to that of the component it will replace during the TEST. The moulded volume does not incorporate parts of the original components (ex-semiconductor dye, transformer cores and windings). The DUMMY COMPONENT makes it possible to test creepage, clearance and dielectric strength with the correct geometry without exceeding the internal maximum voltage of the part being replaced.		IEC 60601-2-4:2002
DUTY CYCLE	Ratio of the operating time to the sum of the operating time and the ensuing interval. In the case of operating times and intervals of varying duration, it is calculated as a mean value over a sufficiently long time.	NG.10.05	IEC 60601-1:1988 IEC 60601-1/A2:1995
DUTY FACTOR	Ratio of the PULSE DURATION to the PULSE REPETITION PERIOD (see 5.3.2.4 of IEC 60469-1). [IEC 61689, definition 3.17]		IEC 60601-2-5:2000
DYNAMIC RANGE	Range of ATTENUATION that can be used for subtraction.		IEC 61223-3-3:1996

Term	Definition	Reference	Used in IEC
EARTH LEAKAGE CURRENT	Current flowing from the MAINS PART through or across the insulation into the PROTECTIVE EARTH CONDUCTOR.	NG.05.01	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
ECG RECORD	A registration (e.g. a hard copy write-out or a display) of an ECG signal including the associated data such as date and time of the registration, name and identification of the PATIENT, etc.		IEC 60601-2-51:2003
EDGE FILTER	FILTER whose ABSORPTION characteristic as a function of RADIATION ENERGY shows a discontinuity.	rm-35-05	IEC 60601-1-3:1994
EFFECTIVE APERTURE	The area of the INPUT SCREEN of the XRII which is irradiated by the RADIATION SOURCE through the INPUT APERTURE. NOTE Due to geometrical enlargement and the source size, the diameter of this area is always larger than the diameter of the INPUT APERTURE itself.		IEC 61262-5:1994
EFFECTIVE FOCAL SPOT	Perpendicular PROJECTION of the ACTUAL FOCAL SPOT on the REFERENCE PLANE. NOTE The shortened term FOCAL SPOT refers to the EFFECTIVE FOCAL SPOT (IEC 60806:1984).	rm-20-13	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60806:1984 IEC 61262-1:1994 IEC 61267:1994
EFFECTIVE IMAGE RECEPTION AREA	The term IMAGE RECEPTION AREA defined in IEC 60788 (rm-37-16) is taken in this collateral standard IEC 60601-1-3:1994 to include only those parts of the surface that are configured at the relevant time to be able to receive an X-RAY PATTERN and have at the same time appropriate means of processing for display or storage of the information contained. NOTE In accordance with this convention, the IMAGE RECEPTION AREA of a multi-field X-RAY IMAGE INTENSIFIER TUBE is considered to be restricted by the selection of magnification modes, to exclude any portion of the INPUT SCREEN from which the X-RAY PATTERN cannot be electronically processed.	rm-37-16	IEC 60601-1-3:1994
EFFECTIVE INTENSITY	Ratio of the OUTPUT POWER to the EFFECTIVE RADIATING AREA. It is expressed in watts per square centimetre. [IEC 61689, definition 3.18, modified]		IEC 60601-2-5:2000
EFFECTIVE LENGTH	Length along the axis of the CT DETECTOR between the two points at which the RESPONSE has fallen to 50 % of its maximum value (at the centre).		IEC 61674/A1:2002

Term	Definition	Reference	Used in IEC
EFFECTIVE RADIATED POWER (ERP)	Power required at the input of a lossless reference antenna to produce, in a given direction at any specified distance, the same power flux density as that radiated by a given device. NOTE As used by the ITU and as used in IEC 60050 (712), the term “effective radiated power” appears without qualification only when the reference antenna is a half-wave dipole. [IEV 161-04-16, modified]		IEC 60601-1-2:2001
EFFECTIVE RADIATING AREA	Beam cross-sectional area extrapolated to the front face of the TREATMENT HEAD and multiplied by a dimensionless factor according to IEC 61689. [IEC 61689, definition 3.20, modified] NOTE This may be thought of as the area of the face of the TREATMENT HEAD which contains 100 % of the total mean square acoustic power.		IEC 60601-2-5:2000
EFFECTIVE RANGE	Range of INDICATED VALUES for which an instrument complies with a stated performance. The maximum (minimum) effective INDICATED VALUE is the highest (lowest) in this range.		IEC 61676:2002
EFFECTIVE RANGE (of INDICATED VALUES)	Range of INDICATED VALUES for which an instrument complies with a stated performance, the maximum (minimum) effective INDICATED VALUE is the highest (lowest) in this range. The concept of EFFECTIVE RANGE may also be applied to SCALE READINGS and to related quantities that are not directly indicated by the instrument, for example the input signal. NOTE 1 The EFFECTIVE RANGE of INDICATED VALUES is referred to as EFFECTIVE RANGE in this standard IEC 61674. NOTE 2 For CT DOSIMETERS the EFFECTIVE RANGE of AIR KERMA LENGTH need not be stated as the largest range of which is of practical interest to the USER, e.g. 1μGy·m to 2mGy·m.		IEC 61674/ A1:2002
EFFECTIVE RANGE (of INDICATED VALUES)	The range of INDICATED VALUES for which an instrument complies with a stated performance; the maximum (minimum) effective INDICATED VALUE is the highest (lowest) in this range. The concept of EFFECTIVE RANGE may, for example, also be applied to SCALE READINGS and to related quantities not directly indicated by the instrument e.g. input current. NOTE Referred to as EFFECTIVE RANGE in this standard IEC 60731/A1:2002. Recommended replacement: IEC 61674		IEC 60731/A1:2002
EFFECTIVE RANGE (of INDICATED VALUES)	Range of INDICATED VALUES for which an instrument complies with a stated performance; the maximum (minimum) effective INDICATED VALUE is the highest (lowest) in this range. The concept of EFFECTIVE RANGE may, for example, also be applied to SCALE READINGS and to related quantities that are not directly indicated by the instrument, e.g. input current. NOTE The EFFECTIVE RANGE of INDICATED VALUES is referred to as EFFECTIVE RANGE in this standard IEC 60580. Recommended replacement: IEC 61674		IEC 60580:2000
EFFECTIVE RECORDING WIDTH	Width of the recording paper within which the signal of a CHANNEL can be recorded according to this performance standard.		IEC 60601-2-51:2003
EFFECTIVE STIMULATION DURATION ($t_{s,eff}$)	Duration of any period of the monotonic increasing or decreasing gradient, used to describe its limits for cardiac or peripheral nerve stimulation. It is defined as the ratio of the peak-to-peak field variation and the maximum value of the time derivative of the gradient in that period.		IEC 60601-2-33:2002

Term	Definition	Reference	Used in IEC
EFFECTIVE SURFACE AREA	Surface on which the PATIENT rests according to the intended position and which is radiated by the PHOTOTHERAPY EQUIPMENT. NOTE The EFFECTIVE SURFACE AREA is the intended TREATMENT surface which is illuminated by the phototherapy light. The area of 60 cm x 30 cm is used as a standard sized surface unless specified differently in the ACCOMPANYING DOCUMENTS.		IEC 60601-2-50:2000
ELECTRICAL STIMULATOR	Parts of EQUIPMENT for the application of electric currents via ELECTRODES in direct contact with the PATIENT, for the evoking of biopotentials or other action.		IEC 60601-2-40:1998
ELECTRICALLY OPERATED HOSPITAL BED	BED and its accessories intended for use in the diagnosis, TREATMENT or monitoring of an adult PATIENT while under medical supervision.		IEC 60601-2-38 /A1:1999
ELECTROCARDIOGRAM (ECG)	Visible RECORD of heart action potentials.		IEC 60601-2-25/A1:1999 IEC 60601-2-26:2002
ELECTROCARDIOGRAM (ECG)	Visual RECORD of heart action potentials. [IEC 60601-2-25:1999, definition 2.101] Recommendation: unify with IEC 60601-2-25		IEC 60601-2-47:2001
ELECTROCARDIOGRAM (ECG)	Visible recording of heart action potentials as measured at the body surface (see also the definition of 'ECG RECORD'). Recommendation: unify with IEC 60601-2-25		IEC 60601-2-51:2003
ELECTROCARDIOGRAPH (ECG)	MEDICAL ELECTRICAL EQUIPMENT and associated ELECTRODES intended for the production of detachable ELECTROCARDIOGRAMS for diagnostic purposes. Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999		IEC 60601-2-25/A1:1999
ELECTROCARDIOGRAPH (ECG)	MEDICAL ELECTRICAL EQUIPMENT and associated ELECTRODES intended for the production of ELECTROCARDIOGRAMS for diagnostic purposes. Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999		IEC 60601-2-51:2003
ELECTROCARDIOGRAPHIC (ECG) MONITORING EQUIPMENT	EQUIPMENT and associated ELECTRODES for the monitoring and/or recording of heart action potentials and displaying the resultant data locally and/or transmitting to a central station. Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999		IEC 60601-2-27:1994
ELECTRODE	ELECTRODE attached to a specified part of the body to detect heart action voltages in combination with another ELECTRODE or ELECTRODES. Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999		IEC 60601-2-25/A1:1999
ELECTRODE	Conductor attached to a specified part of the body to detect heart action voltages in combination with another ELECTRODE or ELECTRODES. Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999		IEC 60601-2-27:1994
ELECTRODE(S)	Means (typically, an electrical sensor) in contact with a specified part of the body to detect heart action voltage in combination with another means (see also Table 109). Both means (electrical sensors) are connected to the ELECTROCARDIOGRAPH via a PATIENT CABLE. Recommendation: unify IEC 60601-2-27:1994, IEC 60601-2-51, IEC 60601-2-25:1999		IEC 60601-2-51:2003
ELECTROENCEPHALOGRAM (EEG)	Display or RECORD of the variation with time of voltages taken from ELECTRODES on the scalp, whose positions are specified. [IEV 891-04-23, modified]		IEC 60601-2-26:2002

Term	Definition	Reference	Used in IEC
ELECTROENCEPHALOGRAPH (EQUIPMENT)	Device to produce an ELECTROENCEPHALOGRAM. [IEV 891-04-24]	IEV 891-04-24	IEC 60601-2-26:2002
ELECTROMAGNETIC COMPATIBILITY (abbreviation EMC)	The ability of an EQUIPMENT or system to function satisfactorily in its ELECTROMAGNETIC ENVIRONMENT without introducing intolerable ELECTROMAGNETIC DISTURBANCES to anything in that environment (IEV 161-01-07).	IEV 161-01-07	IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-29:1999 IEC 62083:2000
ELECTROMAGNETIC COMPATIBILITY (EMC)	Ability of an EQUIPMENT or SYSTEM to function satisfactorily in its ELECTROMAGNETIC ENVIRONMENT without introducing intolerable ELECTROMAGNETIC DISTURBANCES to anything in that environment. [IEV 161-01-07]		IEC 60601-1-2:2001
ELECTROMAGNETIC DISTURBANCE	Any electromagnetic phenomenon which may degrade the performance of an EQUIPMENT and/or system (IEV 161-01-05, modified). NOTE An ELECTROMAGNETIC DISTURBANCE may be an electromagnetic NOISE, an unwanted signal or a change in the propagation medium itself.		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
ELECTROMAGNETIC DISTURBANCE	Any electromagnetic phenomenon that may degrade the performance of a device, EQUIPMENT or system. NOTE An ELECTROMAGNETIC DISTURBANCE may be an ELECTROMAGNETIC NOISE, an unwanted signal or a change in the propagation medium itself. [IEV 161-01-05, modified].		IEC 60601-1-2:2001
(ELECTROMAGNETIC) EMISSION	Phenomenon by which electromagnetic energy emanates from a source. [IEV 161-01-08]	IEV 161-01-08	IEC 60601-1-2:2001
ELECTROMAGNETIC ENVIRONMENT	Totality of electromagnetic phenomena existing at a given location. NOTE In general, the ELECTROMAGNETIC ENVIRONMENT is time dependent and its description may need a statistical approach. [IEV 161-01-01, modified]		IEC 60601-1-2:2001
ELECTROMAGNETIC NOISE	Time-varying electromagnetic phenomenon apparently not conveying information and which may be superimposed on or combined with a wanted signal. [IEV 161-01-02]	IEV 161-01-02	IEC 60601-1-2:2001
ELECTROMYOGRAPH	MEDICAL ELECTRICAL EQUIPMENT for the detection and analysis of biopotentials accompanying nerve and muscle action, originating either spontaneously, intentionally or by electrical or other stimulation.		IEC 60601-2-40:1998
ELECTRON	Stable elementary particle having an electric charge of $\pm 1,60219 \times 10^{-19}$ C and a rest mass of $9,10956 \times 10^{-31}$ kg.	rm-11-18	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997
ELECTRON BEAM APPLICATOR	BEAM LIMITING DEVICE for ELECTRON RADIATION BEAMS.		IEC 60601-2-1/A1:2002

Term	Definition	Reference	Used in IEC
ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER	X-RAY IMAGE INTENSIFIER incorporating an electro-optical vacuum device.	rm-32-40	IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
ELECTROSTATIC DISCHARGE (ESD)	A transfer of electric charge between bodies of different electrostatic potential in proximity or through direct contact. (IEV 161-01-22).		IEC 60601-1-2:2001
EMERGENCY AIR INTAKE PORT	Dedicated intake port through which ambient air may be drawn when the supply of FRESH GAS is insufficient or absent. [ISO 4135:1995, definition 4.2.2 modified]		IEC 60601-2-12:2001
EMERGENCY FIELD SHUT DOWN UNIT	Device for de-energizing a superconducting or resistive magnet in case of an emergency situation.		IEC 60601-2-33:2002
EMERGENCY TROLLEY	Wheeled trolley intended to support and convey life-supporting and resuscitation EQUIPMENT for cardio-respiratory emergencies.	NG.12.14	IEC 60601-1:1988 IEC 60601-1/A2:1995
EMISSION (electromagnetic)	The phenomenon by which electromagnetic energy emanates from a source (IEV 161-01-08).		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
EMISSION COMPUTED TOMOGRAPHY (ECT)	Imaging method for the representation of the spatial distribution of incorporated RADIONUCLIDES in selected two-dimensional slice through the object.	rm-34-35	IEC 61675-1:1998 IEC 61675-2:1998
ENCLOSURE	Exterior surface of EQUIPMENT including: <ul style="list-style-type: none"> – all ACCESSIBLE METAL PARTS, knobs, grips and the like; – accessible shafts; – for the purpose of tests, metal foil, with specified dimensions, applied in contact with parts of the exterior surface made of material with low conductivity or made of insulating material. 	NG.01.06	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
ENCLOSURE LEAKAGE CURRENT	Current flowing from the ENCLOSURE or from parts thereof, excluding APPLIED PARTS, accessible to the OPERATOR or PATIENT in NORMAL USE, through an external CONDUCTIVE CONNECTION other than the PROTECTIVE EARTH CONDUCTOR to earth or to another part of the ENCLOSURE.	NG.05.02	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002
ENDOSCOPE	An APPLIED PART of MEDICAL EQUIPMENT introduced into a PATIENT to provide an internal view or image for examination, diagnosis and/or therapy.		IEC 60601-2-18/ A1:2000
ENDOSCOPIC EQUIPMENT	An ENDOSCOPE together with its SUPPLY UNIT(S), as required for its intended use.		IEC 60601-2-18 /A1:2000
ENDOSCOPICALLY-USED ACCESSORY	An ACCESSORY, which may be the APPLIED PART of MEDICAL ELECTRICAL EQUIPMENT that is not ENDOSCOPIC EQUIPMENT, introduced into a PATIENT through the same orifice in the PATIENT as the ENDOSCOPE.		IEC 60601-2-18 /A1:2000
ENDOSCOPICALLY USED ACCESSORY	See definition in IEC 60601-2-18:1996. NOTE The reader is referred to IEC 60601-2-18 to ensure that a consistent definition is used.		IEC 60601-2-2:1998
ENERGY CALIBRATION	Process of establishing a relation between the window setting of the PULSE height analyzer and the energy of the PHOTONS.		IEC 61948-1:2001
ENERGY FLUENCE RATE	Letter symbol: ψ . Increment of energy fluence during a suitably small interval of time dt divided by that interval of time. $\psi = \frac{d\Psi}{dt}$	rm-13-05	IEC 60627:2001
ENERGY METER/DEFIBRILLATOR TESTER	An INSTRUMENT capable of measuring the energy output from a CARDIAC DEFIBRILLATOR while generating a simulated ECG output to the CARDIAC DEFIBRILLATOR.		IEC 60601-2-4:2002
ENERGY RESOLUTION	A term used to characterize the ability of a RADIATION DETECTOR to distinguish between PHOTONS of different energies. NOTE The ENERGY RESOLUTION can be expressed as the ratio of the photopeak FULLWIDTH AT HALF MAXIMUM (FWHM) to photopeak energy expressed as a percentage.		IEC 61948-1:2001
ENERGY STORAGE DEVICE	The component (for example a capacitor) that is charged with the energy necessary to deliver an electrical defibrillation PULSE to the PATIENT.		IEC 60601-2-4:2002

Term	Definition	Reference	Used in IEC
ENTRANCE FIELD	For an XRII, the area in the ENTRANCE PLANE that can be used for the TRANSMISSION of an X-RAY PATTERN under specific conditions.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
ENTRANCE FIELD	For a COLLIMATOR, area on the entrance face bounded by the shortest perimeter tangential to the outside edges of the peripheral apertures on its entrance face.	rm-34-12	IEC 61223-3-3:1996
ENTRANCE FIELD OF A COLLIMATOR	Area bounded by the shortest line which is tangential to the outside edges of the peripheral COLLIMATOR apertures on the COLLIMATOR FRONT FACE.		IEC 60789:1992
ENTRANCE FIELD SIZE	For an ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER, diameter of the field in the ENTRANCE PLANE that can be used for the TRANSMISSION of an X-RAY PATTERN under specific conditions.	rm-32-43	IEC 60601-2-43:2000 IEC 61223-3-3:1996
ENTRANCE FIELD SIZE	For an XRII, the diameter of the field in the ENTRANCE PLANE that can be used at a specified SED for the TRANSMISSION of an X-RAY PATTERN. For an XRII with more than one magnification mode, the ENTRANCE FIELD SIZE for each of the magnification modes shall correspond to the same diameter of the XRII OUTPUT IMAGE occurring with the largest ENTRANCE FIELD SIZE. Recommended replacement: rm-32-43		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995
ENTRANCE PLANE	For an ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER, plane perpendicular to its axis of symmetry and grazing the part which protrudes most in the direction of the RADIATION SOURCE.	rm-32-42	IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996
ENTRANCE PLANE	The plane perpendicular to the axis of symmetry of the XRII and grazing the part of the XRII, including its housing, that protrudes most in the direction of the RADIATION SOURCE. Recommended replacement: rm-32-42		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
ENTRANCE SURFACE	In RADIOLOGY, plane or curved surface through which the radiation enters an irradiated object including any bolus which is present.	rm-37-17	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 61223-2-7:1999 IEC 61223-2-11:1999 IEC 61267:1994 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
EQUILIBRATION TIME	The time taken for a SCALE READING to reach and remain within a specified deviation from its final steady value after a sudden change in an INFLUENCE QUANTITY has been applied to the instrument.		IEC 60731/A1:2002
EQUILIBRATION TIME	Time taken for a SCALE READING to reach and remain within a specified deviation from its final steady value, after a sudden change in an INFLUENCE QUANTITY has been applied to the instrument. Recommended replacement: IEC 60731/A1:2002		IEC 61674/ A1:2002
EQUIPMENT	(see NG.02.15)	NG.02.11	IEC 60522:1999 IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-17 /A1:1996 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 62083:2000
EQUIPMENT ELECTRODE	Conductor applied over, or inserted into, a region of the scalp or brain to detect electrical ACTIVITY of the brain in combination with another ELECTRODE or ELECTRODES.		IEC 60601-2-26:2002
EQUIPMENT FOR EXTRACORPOREALLY INDUCED LITHOTRIPSY	Device for TREATMENT with extracorporeally generated PRESSURE PULSES.		IEC 60601-2-36:1997
EQUIPMENT MODEL/EQUIPMENT MODELLING	All physical, geometric and radiation parameters required to plan a course of RADIOTHERAPY for particular EQUIPMENT. The process of establishing the EQUIPMENT model is referred to as "EQUIPMENT MODELLING".		IEC 62083:2000
EQUIVALENT ANODE INPUT POWER	Value of ANODE INPUT POWER which, if applied continuously under specified ambient conditions, would maintain a specific level of ANODE HEAT CONTENT.	rm-36-24	IEC 60613:1989

Term	Definition	Reference	Used in IEC
EQUIVALENT APERTURE DIAMETER	<p>Diameter of a circle whose area is the –12 dB OUTPUT BEAM AREA and given by</p> $D_{eq} \equiv \sqrt{\frac{4}{\pi}} A_{aprt}$ <p>where</p> <p>A_{aprt} is the –12 dB OUTPUT BEAM AREA. Symbol: D_{eq}. Unit: centimetres, cm.</p> <p>NOTE This formula gives the diameter of a circle whose area is the –12 dB OUTPUT BEAM AREA. It is used in the calculation of the CRANIAL-BONE THERMAL INDEX and the SOFT TISSUE THERMAL INDEX.</p>		IEC 60601-2-37:2001
EQUIVALENT BEAM AREA	<p>Value of the area of the acoustic beam at the distance z in terms of power and intensity, and given by</p> $A_{eq}(z) \equiv \frac{P_{\alpha}(z)}{I_{zpta,\alpha}(z)} = \frac{P}{I_{zpta}(z)}$ <p>where</p> <p>$P_{\alpha}(z)$ is the ATTENUATED OUTPUT POWER, at the distance z, in milliwatts,</p> <p>$I_{zpta,\alpha}(z)$ is the ATTENUATED SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY, at the distance z, in milliwatts per square centimetre,</p> <p>P is the OUTPUT POWER in milliwatts,</p> <p>$I_{zpta}(z)$ is the SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY, at the distance z, in milliwatts per square centimetre, and</p> <p>z is the distance from the source to the specified point in centimetres.</p> <p>Symbol: $A_{eq}(z)$. Unit: centimetres squared, cm².</p>		IEC 60601-2-37:2001
EQUIVALENT BEAM DIAMETER	<p>Value of the diameter of the acoustic beam at the distance z in terms of the EQUIVALENT BEAM AREA, and given by</p> $d_{eq}(z) \equiv \sqrt{\frac{4}{\pi}} A_{eq}(z)$ <p>where</p> <p>$A_{eq}(z)$ is the EQUIVALENT BEAM AREA;</p> <p>z is the distance from the source to the specified point.</p> <p>Symbol: $d_{eq}(z)$. Unit: centimetres, cm.</p>		IEC 60601-2-37:2001
EQUIVALENT WIDTH (EW)	Width of that rectangle having the same area and the same height as the RESPONSE function, e.g. the POINT SPREAD FUNCTION.	rm-34-45	IEC 61675-1:1998 IEC 61675-2:1998
EQUIVALENT WIDTH (EW)	The width of a rectangle having the same area as the LSF and a height equal to the maximum value of the LSF. Recommended replacement: IEC 61675-1:1998, IEC 61675-2:1998		IEC 60789:1992
ERROR OF MEASUREMENT	Difference between the MEASURED VALUE of a quantity and the TRUE VALUE of that quantity.		IEC 61674/ A1:2002

Term	Definition	Reference	Used in IEC
ERROR OF MEASUREMENT	The difference remaining between the MEASURED VALUE of a quantity and the TRUE VALUE of that quantity.		IEC 60731/A1:2002
ESSENTIAL PERFORMANCE (of an EQUIPMENT or SYSTEM)	PERFORMANCE CHARACTERISTICS necessary to maintain the RESIDUAL RISK within acceptable limits. NOTE See also 3.201.2. This definition will be inserted in the 3rd edition of IEC 60601-1 (in preparation).		IEC 60601-1-2:2001
ESTABLISHED CRITERIA	In a QUALITY ASSURANCE PROGRAMME, acceptable VARIATIONS in results of a CONSTANCY TEST which signal satisfactory functional performance of the EQUIPMENT tested.	rm-70-04	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
EVOKED RESPONSE EQUIPMENT	MEDICAL ELECTRICAL EQUIPMENT for the detection and analysis of biopotentials resulting from an evoking stimulus. The stimulus may be electrical, tactile, auditory, visual, olfactory etc.		IEC 60601-2-40:1998
EXAMINATION ROOM	In MEDICAL DIAGNOSTIC RADIOLOGY, room in which IONIZING RADIATION is applied to the PATIENT or measured on the PATIENT, and which has the required structural means for RADIATION PROTECTION and for mechanical support.	rm-20-22	IEC 60601-2-7:1998 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61331-3:1998
EXCLUSION BAND	Frequency band for intentional receivers of RF electromagnetic energy that extends from – 5 % to + 5 % of the frequency, or frequency band, of reception for frequencies of reception greater than or equal to 80 MHz and from –10 % to + 10 % of the frequency, or frequency band, of reception for frequencies of reception less than 80 MHz. NOTE Other definitions of this term are sometimes used for other purposes in national radio regulations.		IEC 60601-1-2:2001
EXIT FIELD OF A COLLIMATOR	Area bounded by the shortest line which is tangential to the outside edges of the peripheral COLLIMATOR apertures on the COLLIMATOR BACK FACE.		IEC 60789:1992
EXIT SURFACE	In RADIOLOGY, plane or curved surface through which the RADIATION BEAM emerges from an irradiated object.		IEC 61267:1994
EXPANDED UNCERTAINTY	Quantity defining the interval about the result of a measurement within which the values that could reasonably be attributed to the measure and may be expected to lie with a higher degree of confidence.	rm-73-15	IEC 60580:2000 IEC 61674/A1:2002

Term	Definition	Reference	Used in IEC
EXPOSURE	<p>Letter symbol: X. Electric charge produced by IONIZING RADIATION in air. EXPOSURE is determined as the quotient of dQ by dm, where the value of dQ is the absolute value of the total charge of the ions of one sign produced in air when all the ELECTRONS (negatrons and positrons) liberated by PHOTONS in air of mass dm are completely stopped in air:</p> $X = \frac{dQ}{dm}$ <p>The unit of EXPOSURE is the coulomb per kilogram ($C \cdot kg^{-1}$). The earlier unit of EXPOSURE was the roentgen (R), being equal to $2,58 \times 10^{-4} C \cdot kg^{-1}$.</p>	rm-13-14	IEC 60601-1-3:1994 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1993 IEC 61223-3-1:1999
EXPOSURE	<p>Letter symbol: X. Following the definition in C.8 of ICRU 33 EXPOSURE is the quotient of dQ by dm where dQ is the absolute value of the total charge of the ions of one sign produced in air when all the ELECTRONS (negatrons and positrons) liberated by PHOTONS in air of mass dm are completely stopped in air. The unit of EXPOSURE is $C \cdot kg^{-1}$.</p> <p>Recommended replacement: rm-13-14</p>		IEC 60731/A1:2002
EXPOSURE RATE	<p>Letter symbol: \dot{X}. EXPOSURE per unit time. EXPOSURE RATE is determined as the quotient of dX by dt, where dX is the increment of EXPOSURE in the time interval dt:</p> $\dot{X} = \frac{dX}{dt}$ <p>A unit of EXPOSURE RATE is any quotient of the unit of EXPOSURE or its multiples or submultiples by a suitable unit of time ($C \cdot kg^{-1} \cdot s^{-1}$, $mC \cdot kg^{-1} \cdot h^{-1}$, etc.).</p>	rm-13-15	IEC 60601-1-3:1994 IEC 61223-2-9:1999 IEC 61262-2:1994
EXPOSURE RATE	<p>Letter symbol: \dot{X}. Following the definition in C.9 of ICRU 33 EXPOSURE RATE is the quotient of dX by dt, where dX is the increment of EXPOSURE in the time interval dt. The unit of EXPOSURE RATE is $C \cdot kg^{-1} \cdot s^{-1}$ ($C \cdot kg^{-1} \cdot min^{-1}$; $C \cdot kg^{-1} \cdot h^{-1}$).</p> <p>Recommended replacement: rm-13-15</p>		IEC 60731/A1:2002
EXTERNAL PACEMAKER	Pacemaker with a NON-IMPLANTABLE PULSE GENERATOR and PATIENT CABLE(S) (if used).		IEC 60601-2-31/A1:1998
EXTERNAL TERMINAL DEVICE	TERMINAL DEVICE by which electrical connection to other EQUIPMENT is made.	NG.07.07	IEC 60601-1:1988 IEC 60601-1/A2:1995
EXTRA-FOCAL RADIATION	In an X-ray source assembly, X-radiation emitted from the RADIATION SOURCE other than that emitted from the ACTUAL FOCAL SPOT.	rm-11-11	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60627:2001 IEC 61223-3-2:1996
EXTRACORPOREAL CIRCUIT	Blood lines and any integral ACCESSORY thereof.		IEC 60601-2-16:1998
EXTRACORPOREALLY INDUCED LITHOTRIPSY	LITHOTRIPSY inside the PATIENT by PRESSURE PULSES generated outside the PATIENT.		IEC 60601-2-36:1997
FAIL SAFE	Capability of an EQUIPMENT to provide a minimum illuminance and to be directed on the operation area even in SINGLE FAULT CONDITION.		IEC 60601-2-41:2000

Term	Definition	Reference	Used in IEC
FIELD FLATTENING FILTER	FILTER used to homogenize the ABSORBED DOSE RATE over the RADIATION FIELD.	rm-35-07	IEC 60601-2-11:1997 IEC 60601-2-1/A1:2002 IEC 60976/ A1:2000
FIELD SIZE	Abbreviation for IRRADIATION FIELD SIZE.		IEC 60601-2-11:1997
FIELD-CLASS DOSIMETER	Dosimeter whose performance and stability are sufficient for it to be used to make ordinary routine measurements.	rm-71-05	IEC 60601-2-9:1996 IEC 60731/A1:2002
FILAMENT CURRENT	For an X-RAY TUBE, electric current applied to the filament for control of the thermionic emission from the CATHODE.	rm-36-08	IEC 60613:1989
FILM BASE PLUS FOG DENSITY	For CONSTANCY TESTS in X-RAY EQUIPMENT, the optical density in an area of the RADIOGRAM, on the processed control film, that has not been exposed to light from a sensitometer.	rm-72-04	IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-7:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
FILM CHANGER	SERIAL CHANGER in which each RECORD is taken upon a separate RADIOGRAPHIC FILM not contained in an individual RADIOGRAPHIC CASSETTE.	rm-31-07	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61223-3-1:1999
FILM ILLUMINATOR	Luminous surface in combination with additional provisions for the observation of transparent objects such as RADIOGRAMS on RADIOGRAPHIC FILM.	rm-70-10	IEC 60601-2-45:2001 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999
FILM PROCESSOR	For use in MEDICAL DIAGNOSTIC RADIOLOGY, a combination of EQUIPMENT and device to process the latent RADIOLOGICAL information, recorded on, or transferred to, radiographic material, into a permanent, visible image.	rm-70-11	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999

Term	Definition	Reference	Used in IEC
FILTER	In RADIOLOGICAL EQUIPMENT, material or device provided to effect FILTRATION of the RADIATION BEAM.	rm-35-01	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976/ A1:2000 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61262-5:1994
FILTER(S)	Means, realised in hardware, firmware or software, to attenuate unwanted components in the signal being recorded, e.g. muscle action voltages in ECG signal.		IEC 60601-2-51:2003
FILTRATION	Modification of characteristics of IONIZING RADIATION on passing through matter. NOTE FILTRATION may be: – preferential ABSORPTION of certain components of polyenergetic X or gamma radiation accompanying its ATTENUATION; – a modification of the distribution of radiation intensity over the cross-section of a RADIATION BEAM.	rm-12-11	IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61331-3:1998
FILTRATION	Modification of characteristics of IONIZING RADIATION on passing through matter. NOTE FILTRATION includes: – modification of the energy spectrum of IONIZING RADIATION by preferential ABSORPTION of components; – modification of the spatial distribution of radiation intensity over the cross section of a RADIATION BEAM, by differential ATTENUATION. Recommended replacement: rm-12-11		IEC 60580:2000
FIRST LEVEL CONTROLLED OPERATING MODE	Mode of operation of the MR EQUIPMENT in which one or more outputs reach a value that may cause physiological stress to PATIENTS which needs to be controlled by MEDICAL SUPERVISION.		IEC 60601-2-33:2002
FIXED COORDINATE SYSTEM	Cartesian system with axes X, Y, and Z, Z being the SYSTEM AXIS. The origin of the FIXED COORDINATE SYSTEM is defined by the centre of the TOMOGRAPHIC VOLUME. The SYSTEM AXIS is orthogonal to all transverse slices.		IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
FIXED EQUIPMENT	EQUIPMENT which is fastened or otherwise secured at a specified location in a building or a vehicle and can only be detached by means of a TOOL.	NG.02.12	IEC 60601-1:1988 IEC 60601-1/A2:1995
FIXED MAINS SOCKET OUTLET	Mains socket-outlet installed in a fixed wiring system in a building or a vehicle. According to IEC 60601-1/A1:1991 modify title in IEC 60601-1:1988 to read: Fixed mains socket-outlet	NG.07.08	IEC 60601-1:1988 IEC 60601-1/A1:1991 IEC 60601-1/A2:1995
FIXED SETTING (of a control or limiting device)	Setting not intended to be altered by the OPERATOR and which can only be altered by means of a TOOL.	NG.09.04	IEC 60601-1:1988 IEC 60601-1/A2:1995
FLAMMABLE ANAESTHETIC MIXTURE WITH AIR	Mixture of a flammable anaesthetic vapour with air in such a concentration that ignition may occur under specified conditions. A mixture of the vapour of a flammable disinfection or cleaning agent with air may be treated as a FLAMMABLE ANAESTHETIC MIXTURE with air subject to national or local regulations.	NG.12.15	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999
FLAMMABLE ANAESTHETIC MIXTURE WITH OXYGEN OR NITROUS OXIDE	Mixture of a flammable anaesthetic vapour with oxygen or with nitrous oxide in such a concentration that ignition may occur under specified conditions.	NG.12.16	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999
FLOW-DIRECTION-SENSITIVE COMPONENT	VENTILATOR component through which the gas flow has to be in one direction only for its proper functioning and/or PATIENT SAFETY. [ISO 4135:1995, definition 4.1.13]		IEC 60601-2-12:2001
FLUORESCENT SCREEN	Layer of a fluorescent substance on a carrier, emitting light when irradiated with IONIZING RADIATION.	rm-32-30	IEC 60601-1-3:1994 IEC 60627:2001 IEC 61331-2:1994
FOCAL RADIATION	In an X-ray source assembly, X-radiation emitted from the ACTUAL FOCAL SPOT.	rm-11-10	IEC 60627:2001

Term	Definition	Reference	Used in IEC
FOCAL SPOT	Shortened term (see EFFECTIVE FOCAL SPOT).	rm-20-13s	IEC 60336:1993 IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994
FOCAL SPOT PINHOLE RADIOGRAM	RADIOGRAM obtained by means of a PINHOLE CAMERA, showing the shape and orientation of an EFFECTIVE FOCAL SPOT, and the spatial distribution of intensity of radiation across it.	rm-72-02	IEC 60336:1993
FOCAL SPOT SLIT RADIOGRAM	RADIOGRAM obtained by means of a SLIT CAMERA, showing the distribution, across an EFFECTIVE FOCAL SPOT, in the direction normal to the length of the slit, of the intensity of the radiation emitted.	rm-72-01	IEC 60336:1993
FOCAL SPOT STAR RADIOGRAM	Radiogram obtained by means of a STAR PATTERN CAMERA for the determination of the STAR PATTERN RESOLUTION LIMIT in one or more directions across an EFFECTIVE FOCAL SPOT.	rm-72-03	IEC 60336:1993

Term	Definition	Reference	Used in IEC
FOCAL SPOT TO IMAGE RECEPTOR DISTANCE	Distance from the REFERENCE PLANE of an EFFECTIVE FOCAL SPOT to the point at which the REFERENCE AXIS intersects with the image receptor plane.	rm-37-13	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996
FOCAL SPOT TO SKIN DISTANCE	In MEDICAL DIAGNOSTIC RADIOLOGY, distance from the REFERENCE PLANE of an EFFECTIVE FOCAL SPOT to a plane normal to the REFERENCE DIRECTION and containing the point on the PATIENT SURFACE nearest to the RADIATION SOURCE. In RADIOTHERAPY, distance from the REFERENCE PLANE of an EFFECTIVE FOCAL SPOT to the point at which the REFERENCE AXIS intersects with the ENTRANCE SURFACE.	rm-37-12	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 61223-3-4:2000
FOCAL TRACK	In a rotating ANODE X-RAY TUBE, part of the ANODE which is struck by the beam of ELECTRONS during rotation of the ANODE.	rm-22-08	IEC 60336:1993 IEC 60806:1984
FOCAL VOLUME	Volume in space contained within the surface defined by the –6 dB isobar of the maximum peak compressional acoustic pressure.		IEC 60601-2-36:1997
FOCUSED GRID	LINEAR GRID where the planes of the absorbing strips converge at the FOCUSING DISTANCE to a straight line.	rm-32-09	IEC 60601-2-7:1998 IEC 61223-3-1:1999
FOCUSED GRID	LINEAR GRID in which the planes of the absorbing strips converge to a straight line at the FOCUSING DISTANCE. Recommended replacement: rm-32-09		IEC 60627:2001
FOCUSING DISTANCE	Letter symbol: f_0 , unit: cm. Distance between the incident face of a FOCUSED GRID and the line into which the planes of the absorbing strips of the grid converge. NOTE Attention is drawn to the differences between FOCUSING DISTANCE, FOCAL SPOT to grid distance and “FOCAL SPOT to film distance”.		IEC 60627:2001
FREE FLOW	Flow in an ADMINISTRATION SET which is not controlled by the EQUIPMENT, for example, due to the unintended effects of gravity by the removal of the ADMINISTRATION SET from the EQUIPMENT.		IEC 60601-2-24:1998
FREQUENT USE DEFIBRILLATOR	Term used to describe a DEFIBRILLATOR designed to endure more than 2 500 discharges.		IEC 60601-2-4:2002

Term	Definition	Reference	Used in IEC
FRESH GAS	Gas supplied to the VENTILATOR BREATHING SYSTEM. It excludes the following: <ul style="list-style-type: none"> – air drawn through the EMERGENCY AIR INTAKE PORT; – air drawn through leaks in the VENTILATOR BREATHING SYSTEM; – expired gas from the PATIENT. 		IEC 60601-2-12:2001
FRESH GAS INTAKE PORT	Intake port, other than the EMERGENCY AIR INTAKE PORT, through which FRESH GAS may be drawn into the VENTILATOR BREATHING SYSTEM. [ISO 4135:1995, definition 4.2.6 modified]		IEC 60601-2-12:2001
FRONT POINTER	Luminous or mechanical device intended to indicate the RADIATION BEAM AXIS and its point of entry into the PATIENT.	rm-35-12	IEC 60976 /A1:2000
F-TYPE ISOLATED (floating) APPLIED PART (hereinafter referred to as F-type APPLIED PART)	APPLIED PART isolated from other parts of the EQUIPMENT to such a degree that no current higher than the PATIENT LEAKAGE CURRENT allowable in SINGLE FAULT CONDITION flows if an unintended voltage originating from an external source is connected to the PATIENT, and thereby applied between the APPLIED PART and earth. F-type APPLIED PARTS are either TYPE BF APPLIED PARTS or TYPE CF APPLIED PARTS.	NG.01.07	IEC 60601-1:1998 IEC 60601-1/A2:1995 IEC 60601-2-47:2001 IEC 60601-2-51:2003
FULL SOFTWARE CONTROL OF ACOUSTIC OUTPUT	Means by which the EQUIPMENT establishes values of the acoustic output quantities independent of direct OPERATOR control.		IEC 60601-2-37:2001
FULLWIDTH AT HALF MAXIMUM (FWHM)	For a bell shaped curve, distance parallel to the abscissa axis between the points where the ordinate has half of its maximum value.	rm-73-02	IEC 60601-2-44:2002 IEC 60789:1992 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998
FULL WIDTH AT TENTH MAXIMUM (FWTM)	For a bell shaped curve, distance parallel to the abscissa axis between the points where the ordinate has one tenth of its maximum value.	rm-73-03	IEC 60789:1992
FUNCTION (OF AN EQUIPMENT OR SYSTEM)	Clinically significant feature that the EQUIPMENT or SYSTEM is intended to provide.		IEC 60601-1-2:2001
FUNCTIONAL EARTH CONDUCTOR	Conductor to be connected to a FUNCTIONAL EARTH TERMINAL.	NG.06.03	IEC 60601-1:1988 IEC 60601-1/A2:1995
FUNCTIONAL EARTH TERMINAL	Terminal directly connected to a point of a measuring supply or control circuit or to a screening part which is intended to be earthed for functional purposes.	NG.06.04	IEC 60601-1:1988 IEC 60601-1/A2:1995
GAMMA CAMERA	EQUIPMENT for scintigraphy, which produces an image by simultaneous detection of radiation emitted from the object.	rm-34-03	IEC 60789:1992 IEC 61675-2:1998 IEC 61675-3:1998
GAMMA CAMERA BASED WHOLEBODY IMAGING SYSTEM	EQUIPMENT for scintigraphy, employing one or two DETECTOR HEAD(S), in which the image is formed by moving the DETECTOR HEAD(S) and the object relative to each other and relating output information of the RADIOLOGICAL IMAGE.		IEC 61675-3:1998
GANTRY	That part of the EQUIPMENT supporting the RADIATION HEAD.	rm-30-04	IEC 60601-2-1/A1:2002 IEC 62083:2000

Term	Definition	Reference	Used in IEC
GANTRY	That part of the EQUIPMENT supporting and allowing possible movements of the RADIATION HEAD. Recommended replacement: IEC 60601-2-1:2002		IEC 60601-2-11:1997
GANTRY	In EQUIPMENT for RADIOTHERAPY, part of the EQUIPMENT supporting and allowing possible movements of the RADIATION HEAD. Recommended replacement: IEC 60601-2-1:2002		IEC 60601-2-29:1999 IEC 60976/A1:2000 IEC 61217:2002
GAS CONCENTRATION	Volume fraction of the gas expressed as a percentage referred to dry conditions and constant barometric pressure.		IEC 60601-3-1:1996
GAS EXHAUST PORT	That part of a VENTILATOR from which gas is discharged to the atmosphere either directly or via a gas scavenging system. [ISO 4135:1995, definition 4.2.7]		IEC 60601-2-12:2001
GAS INTAKE PORT	Port through which gas is drawn into the VENTILATOR BREATHING SYSTEM.		IEC 60601-2-12:2001
GAS OUTPUT PORT	Port through which gas is delivered at RESPIRATORY PRESSURES via the inspiratory limb to the PATIENT CONNECTION PORT. [ISO 4135:1995, definition 4.2.8 modified]		IEC 60601-2-12:2001
GAS RETURN PORT	Port through which gas is returned at RESPIRATORY PRESSURES via the expiratory limb from the PATIENT CONNECTION PORT. [ISO 4135:1995, definition 4.2.9 modified]		IEC 60601-2-12:2001
GEOMETRICAL FIELD SIZE	Geometrical PROJECTION as seen from the centre of the front surface of the RADIATION SOURCE on a plane perpendicular to the axis of the beam of the distal end of the BEAM LIMITING DEVICE. The field is thus of the same shape as the aperture of the BEAM LIMITING DEVICE. The GEOMETRICAL FIELD SIZE may be defined at any distance from the VIRTUAL SOURCE.		IEC 60976/ A1:2000
GEOMETRICAL FIELD SIZE	Geometrical projection of the distal end of the BEAM LIMITING DEVICE on a plane orthogonal to the RADIATION BEAM AXIS, as seen from the centre of the front surface of the RADIATION SOURCE. The RADIATION FIELD is thus of the same shape as the aperture of the BEAM LIMITING DEVICE. The GEOMETRICAL FIELD SIZE may be defined at any distance from the RADIATION SOURCE. Recommended replacement: IEC 60976		IEC 60601-2-11:1997
GEOMETRICAL RADIATION FIELD	Geometrical projection of the distal end of the BEAM LIMITING DEVICE on a plane orthogonal to the REFERENCE AXIS, as seen from the centre of the front surface of the TARGET/ELECTRON radiation window. The geometrical RADIATION FIELD may be defined at any distance from the front surface of the TARGET for X-RADIATION, or from the ELECTRON radiation window for ELECTRON radiation.		IEC 60601-2-1/A1:2002
GRADIENT OUTPUT	Parameter characterizing gradient performance such as rate of change of the magnitude of the magnetic field, or electric field induced by one or more GRADIENT UNITS under specified conditions and at a specified position.		IEC 60601-2-33:2002
GRADIENT UNIT	All gradient coils and amplifiers that together generate a magnetic field gradient along one of the axes of the coordinate system of the MR EQUIPMENT.		IEC 60601-2-33:2002
GRID EXPOSURE FACTOR	Letter symbol: <i>B</i> . For an ANTI-SCATTER GRID, ratio of the INDICATED VALUE of the rate of total RADIATION without the ANTI-SCATTER GRID in a specified beam to that with the ANTI-SCATTER GRID placed in the beam, under specific measuring conditions.	rm-32-26	IEC 61223-3-3:1996

Term	Definition	Reference	Used in IEC
GRID EXPOSURE FACTOR	Letter symbol: <i>B</i> . Characteristic of an ANTI-SCATTER GRID, evaluated as the ratio of the MEASURED VALUE of the quantity or rate of total RADIATION without the ANTI-SCATTER GRID in a RADIATION BEAM to that with the ANTI-SCATTER GRID placed in the beam, under specific measuring conditions. Recommended replacement: rm-32-26		IEC 60627:2001
GRID RATIO	Letter symbol: <i>r</i> . Ratio between the height of the absorbing strips and the distance between the absorbing strips in the centre of a LINEAR GRID.		IEC 60627:2001
GRID SELECTIVITY	Letter symbol: Σ . Characteristic of an ANTI-SCATTERED GRID, evaluated as the ratio of the TRANSMISSION OF PRIMARY RADIATION to the TRANSMISSION OF SCATTERED RADIATION, under specific measuring conditions.		IEC 60627:2001
HAEMODIALYSIS, HAEMODIAFILTRATION AND/OR HAEMOFILTRATION EQUIPMENT	A system or combination of units used to perform HAEMODIALYSIS, HAEMODIAFILTRATION and/or HAEMOFILTRATION (also refer to 2.2.15).		IEC 60601-2-16:1998
HAEMODIALYSIS (HD)	Process whereby solute imbalances in a PATIENT'S blood are corrected, mainly by diffusion across a semi-permeable membrane. NOTE This process normally includes fluid removal.		IEC 60601-2-16:1998
HAEMOFILTRATION (HF)	A process whereby solute imbalances of a PATIENT'S blood are corrected, mainly by FILTRATION across a semi-permeable membrane. NOTE This process includes fluid exchange and normally fluid removal.		IEC 60601-2-16:1998
HAEMODIAFILTRATION (HDF)	A process whereby solute imbalances in a PATIENT'S blood are corrected by means of simultaneous FILTRATION and diffusion across a semi-permeable membrane. NOTE This process includes fluid exchange and normally fluid removal.		IEC 60601-2-16:1998
HALF VALUE LAYER TEST DEVICE	Device of known X-RAY ATTENUATION properties, normally shaped as foil or plate, which, when applied in the proper thickness, attenuates AIR KERMA RATE to one half of the value that is measured without the device.		IEC 61267:1994
HALF-VALUE LAYER	Thickness of a specified material which attenuates under NARROW BEAM CONDITIONS X- radiation or gamma radiation with a particular RADIATION ENERGY or with a particular spectrum to an extent such that the KERMA RATE, EXPOSURE RATE or ABSORBED DOSE RATE is reduced to one half of the value that is measured without the material. The HALF-VALUE LAYER is expressed in suitable submultiples of the metre together with the material.	rm-13-42	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994

Term	Definition	Reference	Used in IEC
HALF-VALUE LAYER	Thickness of a specified material which under NARROW BEAM CONDITIONS attenuates PHOTON radiation according to its energy spectrum to an extent such that the AIR KERMA RATE is reduced to one half of the value that is measured without the material. Recommended replacement: rm-13-42		IEC 60580:2000
HAND-HELD EQUIPMENT	EQUIPMENT intended to be supported by the hand during NORMAL USE.	NG.02.13	IEC 60601-1:1988 IEC 60601-1/A2:1995
HARD COPY CAMERA	Device producing non-erasable images on a sheet of material from an input signal provided by an imaging system. NOTE Definition from IEC 61223-2-5: IMAGE display device: Device capable of displaying images from an input signal provided by an imaging system.	rm-80-07	IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-3-3:1996
HARD-WIRED	Term used where the features of a system can be modified only by physically removing and re-routing wires.		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
HARM	Physical injury or damage to the health of people, or damage to property or the environment. [ISO/IEC Guide 51:1999, definition 3.1]		ISO 14971:2000
HAZARD	Potential source of HARM. [ISO/IEC Guide 51:1999, definition 3.5]		ISO 14971:2000
HAZARD ANALYSIS	Identification of hazards and their initiating causes. NOTE The quantification of hazard is not a part of the HAZARD ANALYSIS.		IEC 60601-1-4:2000
HAZARDOUS SITUATION	Circumstance in which people, property or the environment are exposed to one or more hazard(s). [ISO/IEC Guide 51:1999, definition 3.6]		ISO 14971:2000
HEAD/FOOT PANEL ASSEMBLY	Assemblies mounted to BED end which may be used as handles to push the BED.		IEC 60601-2-38 /A1:1999
HEAD RF TRANSMIT COIL	A VOLUME RF TRANSMIT COIL suitable for use in MR EQUIPMENT for a MAGNETIC RESONANCE EXAMINATION of the head of PATIENTS.		IEC 60601-2-33:2002
HEAD SAR	SAR averaged over the mass of the PATIENTS head and over a specified time.		IEC 60601-2-33:2002
HEATING DEVICE	EQUIPMENT intended to supply heat to the whole or part of the body of a PATIENT by means of heated BLANKETS, PADS, MATTRESSES, and fluid-filled MATTRESSES.		IEC 60601-2-35:1996
HIGH FREQUENCY SURGICAL EQUIPMENT; HF SURGICAL EQUIPMENT	MEDICAL ELECTRICAL EQUIPMENT including its associated ACCESSORIES intended for the performance of surgical operations, such as the CUTTING or COAGULATION of biological tissue by means of high frequency (HF) currents.		IEC 60601-2-2:1998 IEC 60601-2-18/A1:2000
HIGH HEAT TRANSFER	Thermal characteristic of a HEATING DEVICE as determined according to Annex CC or Annex DD.		IEC 60601-2-35:1996
HIGH PRESSURE GAS INPUT PORT	Input port to which gas may be supplied at a PRESSURE greater than 100 kPa. [ISO 4135:1995, definition 4.2.10 modified]		IEC 60601-2-12:2001

Term	Definition	Reference	Used in IEC
HIGH VOLTAGE	Any voltage over 1 000 V a.c. or over 1 500 V d.c. or 1 500 V peak value.	NG.04.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
HIGH-CONTRAST RESOLUTION	See SPATIAL RESOLUTION		IEC 61223-2-6:1994
HIGH-VOLTAGE CABLE CONNECTION	EQUIPMENT designed for use in RADIOLOGY.	rm-20-18	IEC 60601-2-7:1998
HIGH-VOLTAGE GENERATOR	In an X-RAY GENERATOR, combination of all components for control and production of the electrical energy to be supplied to an X-RAY TUBE, usually consisting of a HIGH-VOLTAGE TRANSFORMER ASSEMBLY and a control assembly.	rm-21-01	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
HIGH-VOLTAGE TRANSFORMER ASSEMBLY	In a HIGH-VOLTAGE GENERATOR, assembly of the high-voltage transformer and other high-voltage circuit components.	rm-21-15	IEC 60601-2-8:1999
HYDRAULIC TEST PRESSURE	PRESSURE applied to test a vessel or part of it for compliance with Clause 45 of IEC 60601-1:1988.	NG.11.01	IEC 60601-1:1988 IEC 60601-1/A2:1995
IEC 60601 TEST LEVEL	IMMUNITY TEST LEVEL specified in 36.202 by this standard or a Particular Standard.		IEC 60601-1-2:2001
IMAGE DISPLAY DEVICE	Device capable of displaying images from an input signal provided by an imaging system. NOTE Definition from IEC 61223-2-4: HARD COPY CAMERA: Device producing non-erasable images on a sheet of material from an input signal provided by an imaging system.	rm-80-08	IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996
IMAGE DISTORTION	As a characteristic of an XR _{II} , variation of the magnification of the image of an object. IMAGE DISTORTION is expressed with respect to a reference magnification (CENTRAL MAGNIFICATION) and as a function of either position (DIFFERENTIAL RADIAL IMAGE DISTORTION) or size (INTEGRAL IMAGE DISTORTION) of the object.		IEC 61262-4:1994
IMAGE MATRIX	Arrangement of MATRIX ELEMENTS in a preferentially Cartesian coordinate system.	rm-32-55	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001

Term	Definition	Reference	Used in IEC
IMAGE PLANE	A plane assigned to a plane in the OBJECT SLICE. NOTE Usually, the IMAGE PLANE is the mid-plane of the corresponding OBJECT SLICE.		IEC 61675-1:1998 IEC 61675-2:1998
IMAGE RECEPTION AREA	In RADIOLOGY, surface on which an X-RAY PATTERN is received.	rm-37-16	IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60806:1984 IEC 61217:2002 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61331-2:1994
IMAGE RECEPTION PLANE	Plane containing the greatest dimensions of the IMAGE RECEPTION AREA.	rm-37-15	IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 61217:2002 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
IMAGE RECEPTOR PLANE IN X-RAY IMAGE INTENSIFIER TUBES	The image receptor plane of an X-RAY IMAGE INTENSIFIER TUBE is taken in this collateral standard IEC 60601-1-3:1994 to be the plane containing the largest selectable IMAGE RECEPTION AREA. NOTE In accordance with this convention, the position of the image receptor plane and thus also the FOCAL SPOT TO IMAGE RECEPTOR DISTANCE, are considered to be unaffected by the selection of different magnification modes.		IEC 60601-1-3:1994
IMMUNITY (to a disturbance)	The ability of an EQUIPMENT and/or system to perform without DEGRADATION in the presence of an electromagnetic disturbance (IEV 161-01-20, modified).		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
IMMUNITY (TO A DISTURBANCE)	Ability of an EQUIPMENT or SYSTEM to perform without DEGRADATION in the presence of an ELECTROMAGNETIC DISTURBANCE [IEV 161-01-20, modified]		IEC 60601-1-2:2001
IMMUNITY LEVEL	Maximum level of a given ELECTROMAGNETIC DISTURBANCE incident on a particular device, EQUIPMENT or system for which it remains capable of operating at a required degree of performance. [IEV 161-03-14]	IEV 161-03-14	IEC 60601-1-2:2001
IMMUNITY TEST LEVEL	Level of a test signal used to simulate an ELECTROMAGNETIC DISTURBANCE when performing an IMMUNITY test. [IEV 161-04-41]		IEC 60601-1-2 2001

Term	Definition	Reference	Used in IEC
IN VITRO COUNTING SYSTEM	Instrument designed to estimate the ACTIVITY of radioactive substances in a sample. NOTE IN VITRO COUNTING SYSTEMS are usually equipped with a scintillation or semi-conductor detector.		IEC 61948-1:2001
IN VIVO COUNTING SYSTEM	Instruments designed to directly measure the ACTIVITY of radioactive substances in the body.		IEC 61948-1:2001
INCUBATOR	An EQUIPMENT having a BABY COMPARTMENT which is provided with the means to control the environment of the baby primarily by heated air within the BABY COMPARTMENT.		IEC 60601-2-19/A1:1996
INCUBATOR TEMPERATURE	Temperature of the air at a point 10 cm above the centre of the mattress surface in the BABY COMPARTMENT (see Figure 102, point A).		IEC 60601-2-19/A1:1996
INDICATED VALUE	Value of a quantity derived from the SCALE READING of an instrument after applying scale factors.	rm-73-10	IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61223-2-9:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
INDICATED VALUE	The value of a quantity derived from the SCALE READING of an instrument together with any scale factors indicated on the CONTROL PANEL of the instrument. Recommended replacement: rm-73-10		IEC 61676:2002
INDICATED VALUE	The value of a quantity derived from the SCALE READING of an instrument together with any scale factors indicated on the CONTROL PANEL of the instrument. NOTE The INDICATED VALUE is equivalent to the "uncorrected observations" shown in Figure 1 of IEC 60731. Recommended replacement: rm-73-10		IEC 60731/A1:2002
INDICATED VALUE	Value of a quantity derived from the SCALE READING of an instrument together with any scale factors indicated on the CONTROL PANEL of the instrument. Recommended replacement: rm-73-10		IEC 60580:2000 IEC 61674 /A1:2002
INDIRECT RADIOGRAM	RADIOGRAM obtained after TRANSFER of the information.	rm-32-04	IEC 60601-2-1/A1:2002 IEC 61223-2-9:1999
INDIRECT RADIOGRAPHY	RADIOGRAPHY in which the recording is effected after TRANSFER of the information obtained at an IMAGE RECEPTION AREA.	rm-41-08	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-9:1999 IEC 61223-3-1:1999
INDIRECT RADIOSCOPY	RADIOSCOPY in which the images are presented after TRANSFER of the information so that they can be viewed from outside the RADIATION BEAM.	rm-41-03	IEC 60601-1-3:1994 IEC 61223-1:1993 IEC 61223-2-5:1994 IEC 61223-2-9:1999 IEC 61223-3-1:1999

Term	Definition	Reference	Used in IEC
INDUCED RADIOACTIVITY	RADIOACTIVITY of material caused by IRRADIATION.	rm-12-14	IEC 60601-2-1/A1:2002
INFANT PHOTOTHERAPY EQUIPMENT	IRRADIATION EQUIPMENT which emits in the main RADIATION SPECTRUM in the range between 400 nm to 550 nm for reducing the concentration of bilirubin in the body of infants.		IEC 60601-2-50:2000
INFANT RADIANT WARMER	An electrically powered device with a radiant heating source intended to maintain the thermal balance of an infant PATIENT by direct radiation of energy in the infra-red region of the electromagnetic spectrum.		IEC 60601-2-21/ A1:1996
INFLATING GAS	FRESH GAS that may also power the VENTILATOR.		IEC 60601-2-12:2001
INFLATING GAS INPUT PORT	Input port to which INFLATING GAS is supplied. [ISO 4135:1995, definition 4.2.11] NOTE An input port is a port to which gas is supplied under positive pressure and through which the gas is driven by this pressure. The gas may be supplied either at a controlled pressure or at a controlled flow.		IEC 60601-2-12:2001
INFLOW	The phase during which the peritoneal cavity is filled. NOTE The term fill is commonly used as a synonym for inflow.		IEC 60601-2-39:1999
INFLUENCE QUANTITY	Any external quantity that may affect the performance of an instrument. Recommended replacement: IEC 60580		IEC 60731/A1:2002
INFLUENCE QUANTITY	Any external quantity that may affect the performance of an instrument (e. g. ambient temperature, RADIATION QUALITY etc.).		IEC 60580:2000
INFLUENCE QUANTITY	Any external quantity that may affect the performance of an instrument (e.g. ambient temperature etc.) and any property of the X-RAY EQUIPMENT under test that needs to be taken into account in using the instrument FOR NON-INVASIVE MEASUREMENT of X-RAY TUBE VOLTAGE (e.g. range of X-RAY TUBE VOLTAGE, ANODE ANGLE, ANODE material, TOTAL FILTRATION etc.). Recommended replacement: IEC 60580		IEC 61676:2002
INFORMATION TECHNOLOGY EQUIPMENT (ITE)	EQUIPMENT designed for the purpose of: a) receiving data from an external source (such as a data input line or via a keyboard); b) performing some processing functions on the received data (such as computation, data transformation or recording, filing, sorting, storage, TRANSFER of data); c) providing a data output (either to other EQUIPMENT or by the reproduction of data or images). NOTE This definition includes electrical or electronic units or systems which predominantly generate a multiplicity of periodic binary PULSED electrical or electronic WAVEFORMS and are designed to perform data processing functions such as word processing, electronic computation, data transformation, recording, filing, sorting, storage, retrieval and TRANSFER, and reproduction of data as images. [IEV 161-05-04]	rm-80-09	IEC 60601-1-2:2001 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999 IEC 62083:2000
INFREQUENT USE DEFIBRILLATOR	Term used to describe a DEFIBRILLATOR designed to endure less than 2 500 discharges.		IEC 60601-2-4:2002
INFUSION CONTROLLER	EQUIPMENT intended to regulate the flow of liquid into the PATIENT under positive pressure generated by gravitational force.		IEC 60601-2-24:1998

Term	Definition	Reference	Used in IEC
INFUSION PUMP	EQUIPMENT intended to regulate the flow of liquids into the PATIENT under positive pressure generated by the pump. The INFUSION PUMP may be of: – type 1: continuous infusion flow only; – type 2: non-continuous flow only; – type 3: discrete delivery of a BOLUS; – type 4: type 1 combined with type 3 and/or type 2 in the same EQUIPMENT; – type 5: PROFILE PUMP.		IEC 60601-2-24:1998
INFUSION PUMP FOR AMBULATORY USE	EQUIPMENT intended for the controlled infusion of liquids into the PATIENT and intended to be carried continuously by the PATIENT.		IEC 60601-2-24:1998
INHERENT FILTRATION	QUALITY EQUIVALENT FILTRATION due to the irremovable materials through which the RADIATION BEAM passes before emerging from a RADIATION SOURCE ASSEMBLY or from components thereof. For an X-RAY TUBE ASSEMBLY, the INHERENT FILTRATION is expressed in thickness of a reference material which, at a specified voltage and WAVEFORM, gives the same RADIATION QUALITY in terms of first HALF-VALUE LAYER.	rm-13-46	IEC 61223-3-1:1999 IEC 61267:1994
INHIBITION	Disabling or SILENCING and disabling an ALARM until revoked intentionally.		IEC 60601-2-23:1999 IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-49:2001 IEC 60601-2-51:2003
INHIBITION (DISABLED)	State in which an ALARM SYSTEM or part of an ALARM SYSTEM can not annunciate ALARM SIGNALS. NOTE 1 INHIBITION may apply to an individual ALARM CONDITION, to a group of ALARM CONDITIONS, or to the entire ALARM SYSTEM of the EQUIPMENT. NOTE 2 INHIBITION may be invoked by the OPERATOR or by the EQUIPMENT (for instance, in a warm-up mode or when no PATIENT is connected). NOTE 3 The duration of inhibition is always indefinite. Only direct action by the OPERATOR or a change in the EQUIPMENT caused by the OPERATOR (for instance, the end of a warm-up mode or when a PATIENT is connected) will revoke INHIBITION.		IEC 60601-2-12:2001
INITIAL CONSTANCY TEST FILM	Film containing the RADIOGRAM of the step wedge part of the TEST DEVICE.		IEC 61223-2-7:1999
INITIAL REFERENCE FILM	Film with an optical density resulting from processing a non-irradiated film under specific conditions prepared during the initial CONSTANCY TEST.		IEC 61223-2-7:1999
INITIAL X-RAY TUBE VOLTAGE	In a capacitor discharge X-RAY GENERATOR, X-RAY TUBE VOLTAGE at the beginning of the LOADING of the X-RAY TUBE.	rm-36-05	IEC 60601-1-3:1994
INITIATION	In RADIO THERAPY, commencing IRRADIATION from the READY STATE when the READY STATE has been attained by carrying out selection and confirming the operating conditions and not by INTERRUPTION OF IRRADIATION.		IEC 60601-2-17/A1:1996
INPUT APERTURE	The aperture that determines the cross-sectional area of a RADIATION BEAM.		IEC 61262-5:1994
INPUT SCREEN	In an electro-optical vacuum device, layer forming the IMAGE RECEPTION AREA.	rm-32-47	IEC 60601-1-3:1994 IEC 61223-3-1:1999 IEC 61262-5:1994

Term	Definition	Reference	Used in IEC
INSTRUCTIONS FOR USE	Those parts of ACCOMPANYING DOCUMENTS giving the necessary information for safe and proper use and operation of the EQUIPMENT.	rm-82-02	IEC 60601-1-3:1994 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-17/ A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60731/A1:2002 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61331-3:1998 IEC 61674 /A1:2002 IEC 62083:2000
INSTRUMENT ACCURACY	Ratio of the most probable MEASURED VALUE over the TRUE VALUE.		IEC 61303:1994
INSTRUMENT PARAMETER	Any internal property of an instrument that may affect the performance of this instrument.	rm-80-03	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 /A1:2002
INSTRUMENT PARAMETER	Any INTERNAL property of an instrument that may affect the performance of the instrument.		IEC 61676:2002
INTEGRAL IMAGE DISTORTION	IMAGE DISTORTION for a circular TEST DEVICE placed in the ENTRANCE PLANE symmetrically about the CENTRAL AXIS. Integral image distortion is a function of the radius of this circular TEST DEVICE.		IEC 61262-4:1994

Term	Definition	Reference	Used in IEC
INTEGRAL MAGNIFICATION	As a characteristic of XRIs, the ratio of the diameter in the OUTPUT IMAGE to the actual diameter of a circular TEST DEVICE placed in the ENTRANCE PLANE symmetrically about the CENTRAL AXIS. INTEGRAL MAGNIFICATION is a function of the radius of this circular TEST DEVICE.		IEC 61262-4:1994
INTEGRATED PATIENT MONITORING/COMMUNICATIONS SYSTEMS CONTROL SIDE RAIL	See 2.1.103. CONTROL SIDE RAIL with the addition of PATIENT/OPERATOR station communication control, and/or PATIENT television/radio entertainment control, and/or PATIENT room lighting control, and/or PATIENT egress detection system, etc.		IEC 60601-2-38 /A1:1999
INTENDED USE / INTENDED PURPOSE	Use of a product, process or service in accordance with the specifications, instructions and information provided by the MANUFACTURER.		ISO 14971:2000
INTENSIFYING SCREEN	Layer of material used in DIRECT RADIOGRAPHY to convert the incident X-RADIATION or gamma radiation into radiation more suitable for the radiation-sensitive emulsion of the RADIOGRAPHIC FILM.	rm-32-38	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 60806:1984 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61331-2:1994
INTERCHANGEABLE ANAESTHETIC VAPOUR DELIVERY DEVICE	OPERATOR detachable ANAESTHETIC VAPOUR DELIVERY DEVICE designed to be used with specific EQUIPMENT from different MANUFACTURERS.		IEC 60601-2-13:2003
INTERCONNECTION CONDITIONS	Conditions that shall be fulfilled for safe use when an energized ENDOSCOPE or energized ENDOSCOPICALLY-USED ACCESSORY is used with an ENDOSCOPE.		IEC 60601-2-18 /A1:2000
INTERCONNECTION TERMINAL DEVICE	TERMINAL DEVICE by which internal connections within EQUIPMENT or between EQUIPMENT parts are made.	NG.07.09	IEC 60601-1:1988 IEC 60601-1/A2:1995

Term	Definition	Reference	Used in IEC
INTERLOCK	Device preventing the start or the continued operation of EQUIPMENT unless certain predetermined conditions prevail.	rm-83-05	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-17/ A1:1996 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001
INTERMEDIATE RATE	<ul style="list-style-type: none"> – For VOLUMETRIC INFUSION PUMPS and VOLUMETRIC INFUSION CONTROLLERS, set the rate to 25 ml/h; – for drip-rate INFUSION PUMPS and drip-rate infusion controllers, set the rate to 20 drops/minute; – for SYRINGE PUMPS, set the rate to 5 ml/h; – for SPECIAL USE EQUIPMENT and INFUSION PUMPS for ambulatory use, set the rate specified by the MANUFACTURER as typical for the EQUIPMENT. 		IEC 60601-2-24:1998
INTERMITTENT MODE	For an X-RAY GENERATOR, mode of LOADING an X-RAY TUBE where the electric energy is supplied to the tube in single, intermittent or pulsed LOADINGS, as for example in RADIOGRAPHY, CINERADIOGRAPHY.	rm-36-41	IEC 60601-1-3:1994 IEC 60601-2-7:1998
INTERMITTENT OPERATION	Operation in a series of specified identical cycles, each cycle being composed of a period of operation under normal load, without the specified limits of temperature being exceeded, following by a rest period with the EQUIPMENT running idle or switched off.	NG.10.06	IEC 60601-1:1988 IEC 60601-1/A2:1995
INTERNAL ELECTRICAL POWER SOURCE	Power source intended to provide the electrical power necessary to operate EQUIPMENT and which is incorporated in that EQUIPMENT.	NG.01.09	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-12:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
INTERNAL DISCHARGE CIRCUIT	Circuit within the DEFIBRILLATOR which discharges the ENERGY STORAGE DEVICE without energizing the DEFIBRILLATOR ELECTRODES.		IEC 60601-2-4:2002
INTERNALLY POWERED EQUIPMENT	EQUIPMENT able to operate from an INTERNAL ELECTRICAL POWER SOURCE.	NG.02.29	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-26:2002 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
INTERRUPTION	In RADIOTHERAPY, stopping IRRADIATION prior to TERMINATION (of IRRADIATION) with the possibility of CONTINUATION without re-confirmation of operating conditions (i.e. return to READY STATE).		IEC 60601-2-17 /A1:1996

Term	Definition	Reference	Used in IEC
INTERRUPTION (of IRRADIATION)/to interrupt (IRRADIATION)	Stopping of/to stop IRRADIATION and movements with the possibility of continuing without reselecting operating conditions (i.e. a return to the READY STATE).	rm-33-18	IEC 60601-2-11:1997 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999
INTERSTITIAL RADIOTHERAPY	RADIOTHERAPY with SEALED RADIOACTIVE SOURCES implanted within the TARGET VOLUME.	rm-42-53	IEC 60601-2-17 /A1:1996
INTERVENTIONAL REFERENCE POINT	For INTERVENTIONAL X-RAY EQUIPMENT, specified point on the REFERENCE AXIS used as a reference location for the indication of PATIENT-incident AIR KERMA and AIR KERMA RATE.	rm-73-19	IEC 60601-2-43:2000
INTERVENTIONAL X-RAY EQUIPMENT	X-RAY EQUIPMENT for RADIOSCOPICALLY GUIDED INTERVENTIONAL PROCEDURES.	rm-31-11	IEC 60601-2-43:2000
INTRACAVITARY RADIOTHERAPY	RADIOTHERAPY in which a RADIATION BEAM or one or more RADIOACTIVE SOURCES, with or without BEAM APPLICATORS or SOURCE APPLICATORS, are introduced into a body cavity through a natural or artificial opening.	rm-42-04	IEC 60601-2-17 /A1:1996
INTRINSIC ENERGY RESOLUTION	The FWHM of the full energy ABSORPTION peak in the INTRINSIC ENERGY SPECTRUM for a specified RADIONUCLIDE.		IEC 60789:1992
INTRINSIC ENERGY SPECTRUM	The measured histogram of PULSE heights for the DETECTOR HEAD without COLLIMATOR (the PULSE height should be expressed as corresponding energy).		IEC 60789:1992
INTRINSIC ERROR	Deviation of the MEASURED VALUE (i.e. the INDICATED VALUE, corrected to REFERENCE CONDITIONS) from the CONVENTIONAL TRUE VALUE under STANDARD TEST CONDITIONS.	rm-73-16	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/ A1:2002 IEC 61676:2002
INTRINSIC LINE SPREAD FUNCTION	The LSF measured with a collimated LINE SOURCE in front of the DETECTOR HEAD without COLLIMATOR.		IEC 60789:1992
INTRINSIC NON-UNIFORMITY OF RESPONSE	The NON-UNIFORMITY OF RESPONSE of the DETECTOR HEAD without COLLIMATOR.		IEC 60789:1992 IEC 61948-2:2001
INTRINSIC SPATIAL NON-LINEARITY	The spatial non-LINEARITY of the DETECTOR HEAD without COLLIMATOR.		IEC 60789:1992
INVASIVE MEASUREMENT	Measurement of the X-RAY TUBE VOLTAGE by external connection of a suitable meter or a high resistance divider.		IEC 61676:2002
IONIZATION CHAMBER	Ionization detector consisting of a CHAMBER filled with a suitable gas, in which an electric field, insufficient to induce gas multiplication, is provided for the collection at the ELECTRODES of charges associated with ions and the ELECTRONS produced in the SENSITIVE VOLUME of the detector by IONIZING RADIATION.	rm-51-03	IEC 60601-2-9:1996 IEC 60976 /A1:2000 IEC 61223-2-11:1999 IEC 61267:1994 IEC 61303:1994

Term	Definition	Reference	Used in IEC
IONIZATION CHAMBER	<p>Detector consisting of a CHAMBER filled with a suitable medium, usually gaseous, in which an electric field, insufficient to induce charge multiplication, is provided for the collection at the ELECTRODES of charges associated with ions and the ELECTRONS produced in the SENSITIVE VOLUME of the detector by IONIZING RADIATION.</p> <p>NOTE For use with DOSE AREA PRODUCT METERS, IONIZATION CHAMBERS are constructed in such a way as to allow the air inside the measuring volume to communicate freely with the atmosphere. Sealed CHAMBERS are not suitable for use with DOSE AREA PRODUCT METERS, because the necessary wall thickness of a sealed CHAMBER may cause an unacceptable energy dependence of the RESPONSE and because the long term stability of sealed CHAMBERS is not guaranteed.</p> <p>Recommended replacement: rm-51-03</p>		IEC 60580:2000
IONIZATION CHAMBER TEST SOURCE	RADIOACTIVE SOURCE used for the determination of the long-term stability of an IONIZATION CHAMBER. The half-life of the source shall be greater than five years and the effects of any radioactive contaminants shall be such that the indication by the device over a period of five years would not deviate by more than 0,5 % after decay correction for the known half-life of the principal RADIONUCLIDE.		IEC 61303:1994
IONIZING RADIATION	Radiation consisting of directly or indirectly ionizing particles of a mixture of both. By convention ultraviolet radiation is excluded.	rm-11-02	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976 /A1:2000 IEC 61223-2-7:1999 IEC 61262-1:1994 IEC 61303:1994 IEC 61331-1:1994
IONIZING RADIATION SHIELD	Component designed to attenuate the passage of IONIZING RADIATION.		IEC 61303:1994

Term	Definition	Reference	Used in IEC
IRRADIATION	<p>Exposing of a living being or matter to radiation. In RADIOLOGY, exposing of a living being or matter to IONIZING RADIATION.</p> <p>Thus:</p> <ul style="list-style-type: none"> - X-IRRADIATION; - gamma IRRADIATION; - ELECTRON IRRADIATION; - NEUTRON IRRADIATION. 	rm-12-09	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-17 /A1:1996 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/A1:2000 IEC 61217:2002 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-3:1994 IEC 61331-3:1998 IEC 62083:2000
IRRADIATION	<p>Actual TREATMENT of the PATIENT, it is regarded as commencing when the RADIOACTIVE SOURCES reach their intended positions in the SOURCE APPLICATORS and as ceasing when they leave at the end of TREATMENT. These transit times are explicitly from the TREATMENT TIME.</p> <p>Recommended replacement: rm-12-09</p>		IEC 60601-2-17/ A1:1996
IRRADIATION FIELD SIZE	In RADIO THERAPY, dimensions of an area in a plane perpendicular to the RADIATION BEAM AXIS at a specified distance from the RADIATION SOURCE or at a specified depth in the irradiated object and defined by specified isodose lines.	rm-37-11	IEC 60601-2-11:1997
IRRADIATION SWITCH	In RADIOLOGICAL EQUIPMENT, control device provided to initiate and/or stop IRRADIATION.	rm-30-03	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000

Term	Definition	Reference	Used in IEC
IRRADIATION TIME	Duration of an IRRADIATION determined according to specific methods, usually the time a rate of a RADIATION QUANTITY exceeds a specified level.	rm-36-11	IEC 60336:1993 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-4:2000 IEC 62083:2000
IRRADIATION TIME	Generally the IRRADIATION TIME is measured in terms of LOADING TIME as the time interval between: <ul style="list-style-type: none"> – the instant that the X-RAY TUBE VOLTAGE has risen for the first time to a value of 75 % of the peak value, and – the instant at which it finally drops below the same value. For systems in which LOADING is controlled by electronic switching of the HIGH VOLTAGE, using a grid in an electronic tube or in the X-RAY TUBE, the LOADING TIME may be determined as the time interval between the instant when the TIMING DEVICE generates the signal to start the IRRADIATION and the instant when it generates the signal to terminate the IRRADIATION. For systems in which LOADING is controlled by simultaneous switching in the primaries of both the high-voltage circuit and the heating supply for the filament of the X-RAY TUBE, the LOADING TIME shall be determined as the time interval between the instant when the X-RAY TUBE CURRENT first rises above 25 % of its maximum value and the instant when it finally falls below the same value. Recommended replacement: rm-36-11		IEC 60601-2-7:1998
IRRADIATION TIME	Generally the IRRADIATION TIME is measured in terms of LOADING TIME as the time interval between: <ul style="list-style-type: none"> – the instant that the X-RAY TUBE VOLTAGE has risen for the first time to a value of 75 % of the peak value, and – the instant at which it finally drops below the same value. Recommended replacement: rm-36-11		IEC 60601-2-45:2001
IRRADIATION TIME	Duration of IRRADIATION determined according to specific methods, usually the time during which the rate of a RADIATION QUANTITY exceeds a specified level. Recommended replacement: rm-36-11		IEC 60580:2000
IRRADIATION TREATMENT PRESCRIPTION	Quantitative description of all the TREATMENT PARAMETERS that determine the IRRADIATION to be delivered.		IEC 60601-2-17/ A1:1996
ISOCENTRE	In RADIOLOGICAL EQUIPMENT with several modes of movement of the REFERENCE AXIS around a common centre, centre of the smallest sphere through which the RADIATION BEAM AXIS passes.	rm-37-32	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60976 /A1:2000 IEC 61217:2002

Term	Definition	Reference	Used in IEC
ISOCENTRIC	When used in combination with RADIOLOGICAL techniques or EQUIPMENT, refers to the use or presence of an ISOCENTRE.		IEC 60976 /A1:2000
ISOCENTRIC EQUIPMENT	EQUIPMENT for RADIOTHERAPY designed and constructed in such a manner that it has an ISOCENTRE.		IEC 60976/A1:2000
ISOCENTRIC TREATMENT	In RADIOTHERAPY, TREATMENT of a PATIENT in which the position of the TARGET VOLUME is referred to the ISOCENTRE.		IEC 60976/A1:2000
ISOPLANATIC REGION	Region where the form of the POINT SPREAD FUNCTION is constant within specified accuracy.		IEC 61262-7:1995
KEEP OPEN RATE (KOR)	Low predetermined rate(s) to which the EQUIPMENT reverts under specified conditions with the object of keeping the PATIENT LINE open. NOTE The abbreviation KVO (Keep-Vein-Open Rate) is commonly used as a synonym of KOR.		IEC 60601-2-24:1998
KERMA	Letter symbol: <i>K</i> . Kinetic energy released in material by IONIZING RADIATION. KERMA is determined as the quotient of dE_{tr} by dm , where dE_{tr} is the sum of the initial kinetic energies of all the charged ionizing particles liberated by uncharged ionizing particles in a material of mass dm : $K = \frac{dE_{tr}}{dm}$ The unit of KERMA is the joule per kilogram (J.kg ⁻¹). The special name of the unit of KERMA is the gray (Gy). The earlier unit of KERMA was the rad, 1 rad being equal to 10 ⁻² J.kg ⁻¹ .	rm-13-10	IEC 60601-2-17/ A1:1996 IEC 60601-2-9:1996 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996
KERMA RATE	Letter symbol: \dot{K} . KERMA per unit time. KERMA RATE is determined as the quotient of dK by dt , where dK is the increment of KERMA in the time interval dt : $\dot{K} = \frac{dK}{dt}$ A unit of KERMA RATE is any quotient of the gray or its multiples or submultiples by a suitable unit of time (Gy.s ⁻¹ , mGy.h ⁻¹ , etc.). Thus: – AIR KERMA RATE.	rm-13-13	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-17/A1:1996 IEC 60806:1984 IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61267:1994 IEC 61331-1:1994
LARGE EQUIPMENT OR SYSTEM	EQUIPMENT or SYSTEM that cannot fit within a 2 m x 2 m x 2,5 m volume, excluding cables; this includes distributed SYSTEMS.		IEC 60601-1-2:2001
LATCHED ALARM	An ALARM, the visual and auditory manifestation of which does not stop when the parameter returns to a value which no longer exceeds the ALARM LIMIT or when the abnormal PATIENT condition does not exist any longer.		IEC 60601-2-23:1999 IEC 60601-2-34:2000

Term	Definition	Reference	Used in IEC
LATCHED ALARM	An ALARM, the visual and auditory manifestation of which does not stop when the parameter (which caused the ALARM) returns to a value which no longer exceeds the ALARM LIMIT or if the abnormal PATIENT condition does not exist any longer.		IEC 60601-2-30:1999
LATCHED ALARM	An ALARM, the visual and auditory manifestation of which does not stop when the ALARM CONDITION no longer exists.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
LEAD	ELECTRODE and LEAD WIRE combination(s) used for a certain recording of ECG. Examples: Einthoven limb lead II, Unipolar chest lead V5. [IEC 60601-2-25:1999, definition 2.103, modified]		IEC 60601-2-47:2001
LEAD(S)	ELECTRODE combination used for a certain ECG recording.		IEC 60601-2-25 /A1:1999 IEC 60601-2-26:2002 IEC 60601-2-27:1994 IEC 60601-2-51:2003
LEAD(S)	Combination(s) of ELECTRODES and LEAD WIRES used for a certain ECG recording (see also Table 110).		IEC 60601-2-51:2003
LEAD EQUIVALENT	Letter symbol: δ_{Pb} . ATTENUATION EQUIVALENT expressed in thickness of lead as reference material. NOTE For protection against IONIZING RADIATION it is unnecessary for a material containing a significant amount of lead to specify the RADIATION QUALITY.	rm-13-38	IEC 61331-1:1994 IEC 61331-3:1998
LEAKAGE CURRENT	Current that is not functional. The following LEAKAGE CURRENTS are defined: EARTH LEAKAGE CURRENT, ENCLOSURE LEAKAGE CURRENT and PATIENT LEAKAGE CURRENT.	NG.05.03	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-26:2002 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
LEAD SELECTOR	System to select certain LEADS and TEST.		IEC 60601-2-25 /A1:1999
LEAD SELECTOR	System to select LEADS.		IEC 60601-2-27:1994
LEAD SELECTOR	System to select certain LEADS and CAL.		IEC 60601-2-51:2003
LEAD WIRE(S)	Cable connected between the ELECTRODE and the AMBULATORY RECORDER.		IEC 60601-2-47:2001
LEAD WIRE(S)	Cable(s) connected between ELECTRODE(S) and the ELECTROCARDIOGRAPH.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
LEAKAGE CURRENT	Any current in the signal path arising in the detector and/or MEASURING ASSEMBLY which is not produced by ionization in the RADIATION DETECTOR. Recommended replacement: NG.05.03		IEC 61674/A1:2002
LEAKAGE CURRENT	Any current in the signal path arising in the detector and/or MEASURING ASSEMBLY which is not produced by ionization in the IONIZATION CHAMBER. Recommended replacement: NG.05.03		IEC 60580:2000
LEAKAGE CURRENT (CHAMBER ASSEMBLY)	Any current in the signal path arising in the CHAMBER ASSEMBLY which is not produced by ionization in the measuring volume. NOTE It is distinguished from ZERO DRIFT or ZERO SHIFT which arise in the MEASURING ASSEMBLY.		IEC 60731/A1:2002
LEAKAGE RADIATION	IONIZING RADIATION which has passed through the PROTECTIVE SHIELDING of a RADIATION SOURCE as well as that which, for some types of X-RAY GENERATORS, has passed through the RADIATION APERTURE before and after LOADING (for example one containing a grid controlled X-RAY TUBE).	rm-11-15	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60601-2-28:1993
LEGIBLE	Displayed qualitative or quantitative information, values, functions, and/or markings discernible or identifiable to an OPERATOR with 6-6 (20/20) vision (corrected if necessary) from a distance of 1 m at a light level of 215 lux, when viewing the information, markings, etc perpendicular to and including 15° above, below, left and right of the normal line of sight of the OPERATOR.		IEC 60601-2-13:2003
LIFE-SUPPORTING EQUIPMENT or SYSTEM	EQUIPMENT or SYSTEM that includes at least one FUNCTION that is intended to actively keep alive or resuscitate PATIENTS and the failure of which to comply with the requirements of 36.202.1 j) is likely to lead to serious injury or death of a PATIENT.		IEC 60601-1:1988
LIFTING POLE	Device suspended above the BED intended to allow the PATIENT to change position by gripping it.		IEC 60601-2-38 /A1:1999
LIGHT DETECTOR	RADIATION DETECTOR sensitive to visible radiation (light).		IEC 61262-7:1995
LIGHT EMISSION PART	That part of the insertion portion of an ENDOSCOPE surrounding the light emission window, delineated as follows: The area of the surface of the insertion portion within three times the maximum diameter of the insertion portion, measured at the tip (distal cover removed) for forward viewing ENDOSCOPES or the centre of the light emission window for side viewing ENDOSCOPES, measured in both longitudinal directions from the centre of the light emission window, but with a minimum of 10 mm and a maximum of 25 mm.		IEC 60601-2-18 /A1:2000
LIGHT FIELD	In EQUIPMENT emitting IONIZING RADIATION, area illuminated by light, being the locus of points at which the illumination exceeds a specific or specified level, simulating the RADIATION FIELD.	rm-37-09	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-44:2002 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999

Term	Definition	Reference	Used in IEC
LIGHT FIELD CENTRE	(Ifc) Point of maximum illuminance in the light field (lighted area). It is the reference point for light field size and distribution measurements.		IEC 60601-2-41:2000
LIGHT FIELD DIAMETER	(d ₁₀) Diameter of a circle around the LIGHT FIELD CENTRE (point of CENTRAL ILLUMINANCE) where the illuminance reaches 10 % of E _c .		IEC 60601-2-41:2000
LIGHT FIELD-INDICATOR	In RADIOLOGICAL EQUIPMENT, device to delineate by means of visible light the extent of the field to be irradiated.	rm-37-31	IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60976 /A1:2000 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61331-3:1998
LIMITED X-RAY TUBE VOLTAGE	In an X-ray installation, a NOMINAL X-RAY TUBE VOLTAGE limited for a particular combination.	rm-36-04	IEC 60613:1989
LIMITS OF VARIATION	Maximum VARIATION of a PERFORMANCE CHARACTERISTIC y, permitted by this standard. If LIMITS OF VARIATION are stated as ± L %, the VARIATION Δy/y, expressed as a percentage, shall remain in the range from – L % to + L %.	rm-73-17	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 A1:2002
LIMITS OF VARIATION	The maximum VARIATION of a PERFORMANCE CHARACTERISTIC y, permitted by this standard. If the LIMITS OF VARIATION are stated as ± L % the VARIATION Δy/y, expressed as a percentage, shall remain in the range from – L % to + L %.		IEC 61676:2002
LINE OF RESPONSE (LOR)	The axis of the PROJECTION BEAM. NOTE In PET, it is the line connecting the centres of two opposing detector elements operated in coincidence.		IEC 61675-1:1998
LINE PAIR RESOLUTION	Highest spatial frequency of the specified line-group test pattern imaged under specified conditions which is distinguishable in the image. The unit is lp/mm. NOTE Another term for LINE PAIR RESOLUTION used in literature is SPATIAL RESOLUTION. Recommended replacement: SPATIAL RESOLUTION rm-32-65		IEC 61223-3-4:2000
LINE PAIR RESOLUTION	Highest spatial frequency of the specified line-group test pattern imaged under specified conditions which is distinguishable in the image. The unit is lp/mm. NOTE LINE PAIR RESOLUTION is used here as a practical substitute for SPATIAL RESOLUTION. Recommended replacement: SPATIAL RESOLUTION rm-33-56		IEC 61223-3-1:1999
LINE SOURCE	Straight RADIOACTIVE SOURCE approximating a δ-function in two dimensions and being constant (uniform) in the third dimension.	rm-33-09	IEC 61675-1:1998 IEC 61675-2:1998
LINE SPREAD FUNCTION (ABBREVIATION LSF)	Normalized distribution of irradiance in the image of an incoherently radiating LINE SOURCE. The LINE SPREAD FUNCTION only exists in an ISOPLANATIC REGION, see ISO 9334. NOTE The Fourier transform of the line function is the ONE-DIMENSIONAL OPTICAL TRANSFER FUNCTION for the orientation perpendicular to the direction of the LINE SOURCE. Recommended replacement: rm-73-01		IEC 61262-7:1995

Term	Definition	Reference	Used in IEC
LINE SPREAD FUNCTION (LSF)	Letter symbol L. In an imaging system, distribution of the intensity from a LINE SOURCE along a straight line in a specified IMAGE PLANE where the straight line is normal to the image of the LINE SOURCE.	rm-73-01	IEC 60789:1992 IEC 61675-1:1998 IEC 61675-3:1998
LINEAR GRID	ANTI-SCATTER GRID composed of highly absorbing strips and highly transmitting interspaces which are parallel in their longitudinal direction.		IEC 60627:2001
LINEAR RANGE	Range of input signals within which the imaging system exhibits LINEARITY within specified accuracy, see ISO 9334. NOTE The range of input signals indicating the LINEAR RANGE of the imaging system should be specified by minimum and maximum levels.		IEC 61262-7:1995
LINEARITY	Property of an imaging system in that the image of a weighted sum of objects is identical to the similarly weighted sum of images of individual objects.		IEC 61262-7:1995
LIQUID SCINTILLATION COUNTER	Counting system utilizing a liquid scintillator in which the radioactive material is distributed. NOTE Usually the LIQUID SCINTILLATION COUNTER is used for measuring samples with β -emitting RADIONUCLIDES.		IEC 61948-1:2001
LITHOTRIPSY	Comminution or fragmentation of calculi.		IEC 60601-2-36:1997
LIVE	State of a part which, when connection is made to that part, can cause a current exceeding the allowable LEAKAGE CURRENT (specified in NG.19.03) for the part concerned to flow from that part to earth or from that part to an ACCESSIBLE PART of the same EQUIPMENT.	NG.01.10	IEC 60601-1:1988 IEC 60601-1/A2:1995 IEC 60601-2-51:2003
LOADING	In an X-RAY GENERATOR, act of supplying electrical energy to the ANODE of an X-RAY TUBE.	rm-36-09	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60806:1984 IEC 61223-2-6:1994 IEC 61223-2-10:1999

Term	Definition	Reference	Used in IEC
LOADING FACTOR	Factor influencing by its value the X-RAY TUBE LOAD, for example X- ray tube current, LOADING TIME, equivalent ANODE INPUT POWER, X-RAY TUBE VOLTAGE and PERCENTAGE RIPPLE.	rm-36-01	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
LOADING STATE	For an X-RAY GENERATOR, state from the end of the READY STATE, when the intended function of the generator is initiated, until the end of the LOADING of the X-RAY TUBE.	rm-36-40	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001

Term	Definition	Reference	Used in IEC
LOADING TIME	Time, determined according to a specific method, during which the ANODE INPUT POWER is applied to the X-RAY TUBE.	rm-36-10	IEC 60336:1993 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000
LOCAL RADIAL MAGNIFICATION	As a characteristic of XRIIs, the ratio of the length in the OUTPUT IMAGE to the actual length of a small TEST DEVICE placed in the ENTRANCE PLANE symmetrically about a given point and oriented radially to the CENTRAL AXIS. LOCAL RADIAL MAGNIFICATION is a function of position of this TEST DEVICE in the ENTRANCE PLANE.		IEC 61262-4:1994
LOCAL RF TRANSMIT COIL	An RF transmit coil other than a VOLUME RF TRANSMIT COIL. The LOCAL RF TRANSMIT COIL can be a coil for spectroscopy.		IEC 60601-2-33:2002
LOCAL SAR	SAR averaged over any 10 g of tissue of the PATIENT body and over a specified time.		IEC 60601-2-33:2002
LOCALIZATION DEVICE	Device used to determine the position of the calculi in (three-dimensional) space.		IEC 60601-2-36:1997
LONG TERM AUTOMATIC MODE	A mode in which a timer, set by the OPERATOR, initiates the measurements.		IEC 60601-2-30:1999
LOW CONTRAST RESOLUTION	Lowest contrast detail object of a specified shape and area that can be resolved from an uniform background.	rm-32-56	IEC 61223-3-1:1999
LOW CONTRAST RESOLUTION	The lowest contrast detail object of a specified object that can be resolved from an uniform background. Recommended replacement: IEC 61223-3-1		IEC 61223-3-4:2000
LOW HEAT TRANSFER	Thermal characteristic of a HEATING DEVICE as determined according to Annex CC or Annex DD.		IEC 60601-2-35:1996
LOW POWER EQUIPMENT	EQUIPMENT having a RATED OUTPUT POWER not exceeding 10 W.		IEC 60601-2-3/A1:1998
LOW VOLTAGE	Line-to-line or line-to-neutral voltage that is less than or equal to 1 000 V a.c. or 1 500 V d.c.		IEC 60601-1-2:2001
LOW-FREQUENCY DROP (abbreviation LFD)	Difference between unity and the value of the MODULATION TRANSFER FUNCTION close to zero spatial frequency. NOTE With currently known XRIIs, significant veiling glare is present. This is apparent as a steep drop in the MTF curve slightly above zero spatial frequency. For the purpose of this international standard IEC 61262-7:1995 the spatial frequency at which the LFD is to be determined, is chosen to be 0,1 mm ⁻¹ .		IEC 61262-7:1995
LOW-PRESSURE GAS INPUT PORT	Input port to which gas is supplied at a pressure not exceeding 100 kPa. [ISO 4135:1995, definition 4.2.14]		IEC 60601-2-12:2001
LUMINAIRE FOR DIAGNOSIS	Luminaire to illuminate the body of the PATIENT locally in order to support diagnosis or TREATMENT which could be interrupted without any hazard for the PATIENT in case of failure of the light. It is not intended to be used in operating rooms. See Table 101.		IEC 60601-2-41:2000

Term	Definition	Reference	Used in IEC
LUMINANCE DISTRIBUTION	In an ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER, spatial VARIATION of luminance over the area of the OUTPUT IMAGE under specific conditions.	rm-32-45	IEC 61262-3:1994
LUMINANCE NON-UNIFORMITY	For an XRII, the difference of luminance between the CENTRE OF THE OUTPUT IMAGE and locations near the periphery of the OUTPUT IMAGE under specific conditions, expressed as a percentage of the luminance at the CENTRE OF THE OUTPUT IMAGE.		IEC 61262-3:1994
MAGNETIC RESONANCE (MR)	Resonant absorption of electromagnetic energy by an ensemble of atomic particles situated in a magnetic field.		IEC 60601-2-33:2002
MAGNETIC RESONANCE EQUIPMENT (MR EQUIPMENT)	MEDICAL ELECTRICAL EQUIPMENT which is intended for in-vivo MAGNETIC RESONANCE EXAMINATION of a PATIENT. The MR EQUIPMENT comprises all parts in hardware and software from the SUPPLY MAINS to the display monitor. The MR EQUIPMENT is a Programmable Electrical Medical System (PEMS).		IEC 60601-2-33:2002
MAGNETIC RESONANCE EXAMINATION (MR EXAMINATION)	Process of acquiring data by MAGNETIC RESONANCE from a PATIENT.		IEC 60601-2-33:2002
MAGNETIC RESONANCE SYSTEM (MR SYSTEM)	Ensemble of MR EQUIPMENT, ACCESSORIES including means for display, control, energy supplies, and the CONTROLLED ACCESS AREA, where provided.		IEC 60601-2-33:2002
MAINS CONNECTOR	Part of an APPLIANCE COUPLER integral with or intended to be attached to a flexible cord which is intended to be connected to the SUPPLY MAINS. A MAINS CONNECTOR is intended to be inserted into the APPLIANCE INLET of EQUIPMENT.	NG.07.10	IEC 60601-1:1988 IEC 60601-1/A2:1995
MAINS PART	Entirety of all parts of EQUIPMENT intended to have a CONDUCTIVE CONNECTION with the SUPPLY MAINS. For the purpose of this definition, the PROTECTIVE EARTH CONDUCTOR is not regarded as a part of the MAINS PART.	NG.01.12	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-44:2002 IEC 60601-2-45:2001
MAINS PLUG	Part integral with or intended to be attached to a power SUPPLY CORD of EQUIPMENT, to be inserted into a FIXED MAINS SOCKET OUTLET.	NG.07.11	IEC 60601-1:1988 IEC 60601-1/A2:1995
MAINS TERMINAL DEVICE	TERMINAL DEVICE by which the electrical connection to the SUPPLY MAINS is made.	NG.07.12	IEC 60601-1:1988 IEC 60601-1/A2:1995
MAINS VOLTAGE	Voltage of a SUPPLY MAINS between two line conductors of a polyphase system or voltage between the line conductor and the neutral conductor of a single-phase system.	NG.04.02	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003
MAJOR SURGICAL LUMINAIRE	Single luminaire in the PATIENT environment which is FAIL SAFE and provides an adequate CENTRAL ILLUMINANCE to illuminate locally the body of the PATIENT. It is intended to support the TREATMENT and diagnosis, and to be used in operating rooms. See Table 101.		IEC 60601-2-41:2000

Term	Definition	Reference	Used in IEC
MAMMOGRAPHIC ANTI-SCATTER GRID	FOCUSED GRID specially designed for mammography. NOTE In this Standard the term "general purpose ANTI-SCATTER GRID" is used to describe any ANTI-SCATTER GRID not specially designed for mammography.		IEC 60627:2001
MAMMOGRAPHIC STEREOTACTIC DEVICE	Device for three-dimensional localization of a point within the breast, and for mechanically guided placement of a needle or position marker for such purposes as fine-needle aspiration, core biopsy and pre-surgical localization. The localization is based on radiographic images of an immobilized breast acquired at different known angles. Such a device may be a dedicated system or an ACCESSORY for mammographic X-RAY EQUIPMENT.	rm-35-20	IEC 60601-2-45:2001
MANUAL DEFIBRILLATOR	DEFIBRILLATOR capable of being manually operated by the OPERATOR for selection of energy, charging and discharging.		IEC 60601-2-4:2002
MANUAL MODE	A mode of operation in which the heater is either at a fixed level or a proportion of its maximum output set by the USER.		IEC 60601-2-21/A1:1996
MANUAL MODE	A mode in which the OPERATOR has full control of the INITIATION of each measurement.		IEC 60601-2-30:1999
MANUAL VENTILATION PORT	Port to which a device may be connected for manual inflation of the lungs. [ISO 4135:1995, definition 4.2.15 modified]		IEC 60601-2-12:2001

Term	Definition	Reference	Used in IEC
MANUFACTURER	<p>Organization or individual who produces an EQUIPMENT.</p> <p>(Term without definition in IEC 60788)</p>	MR-121-01 (rm-85-03)	<p>IEC 60522:1999</p> <p>IEC 60580:2000</p> <p>IEC 60601-1-3:1994</p> <p>IEC 60601-1-4:2000</p> <p>IEC 60601-2-1 /A1:2002</p> <p>IEC 60601-2-7:1998</p> <p>IEC 60601-2-8:1999</p> <p>IEC 60601-2-9:1996</p> <p>IEC 60601-2-11:1997</p> <p>IEC 60601-2-29:1999</p> <p>IEC 60601-2-33:2002</p> <p>IEC 60601-2-43:2000</p> <p>IEC 60601-2-44:2002</p> <p>IEC 60601-2-45:2001</p> <p>IEC 60627:2001</p> <p>IEC 60731/A1:2002</p> <p>IEC 61217:2002</p> <p>IEC 61223-2-7:1999</p> <p>IEC 61223-2-9:1999</p> <p>IEC 61223-2-10:1999</p> <p>IEC 61223-2-11:1999</p> <p>IEC 61223-3-1:1999</p> <p>IEC 61223-3-3:1996</p> <p>IEC 61223-3-4:2000</p> <p>IEC 61262-7:1995</p> <p>IEC 61267:1994</p> <p>IEC 61331-1:1994</p> <p>IEC 61331-2:1994</p> <p>IEC 61331-3:1998</p> <p>IEC 61674/A1:2002</p> <p>IEC 62083:2000</p>
MANUFACTURER	<p>Natural or legal person with responsibility for the design, manufacture, packaging or labelling of a medical device, assembling a system, or adapting a medical device before it is placed on the market and/or put into service, regardless of whether these operations are carried out by that person himself or on his behalf by a third party.</p>		ISO 14971:2000
MATCHED LOAD	<p>Resistive load normally in the range 50 Ω to 75 Ω, which, when replacing the APPLICATOR, results in a voltage standing wave ratio (VSWR) not exceeding 1,5 in the APPLICATOR connecting cable or waveguide.</p>		IEC 60601-2-6:1984

Term	Definition	Reference	Used in IEC
MATRIX ELEMENT	Smallest unit of an IMAGE MATRIX, which is assigned in location and size to a certain volume element of the object (VOXEL).	rm-32-58	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
MATTRESS	HEATING DEVICE providing resilient support to the whole body of a PATIENT.		IEC 60601-2-35:1996
MATTRESS SUPPORT PLATFORM	Structural surface on which the PATIENT sleeping surface (for example mattress) rests in NORMAL USE. The MATTRESS SUPPORT PLATFORM articulates or changes positions to facilitate various therapeutic, diagnostic and convenience positions. (See Figures 101 and 112.)		IEC 60601-2-38/A1:1999
MAXIMUM ANODE HEAT CONTENT	Maximum permissible ANODE HEAT CONTENT.	rm-36-27	IEC 60601-2-28:1993 IEC 60613:1989
MAXIMUM CONTINUOUS HEAT DISSIPATION	Highest value of the X-RAY TUBE ASSEMBLY INPUT POWER which can be applied to an X-RAY TUBE ASSEMBLY continuously under specified conditions without exceeding the MAXIMUM X-RAY TUBE ASSEMBLY HEAT CONTENT.	rm-36-34	IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-44:2002 IEC 60613:1989
MAXIMUM ENERGY	Highest RADIATION ENERGY contained in a beam of polyenergetic radiation.	rm-13-32	IEC 60601-1-3:1994 IEC 60601-2-45:2001
MAXIMUM GRADIENT SLEW RATE	The rate of change of the gradient obtained by switching the GRADIENT UNIT between its maximum specified gradient strengths G_{+max} and G_{-max} in the shortest possible ramp time obtainable under normal scan conditions.		IEC 60601-2-33:2002
MAXIMUM INFUSION PRESSURE	Maximum PRESSURE which can be generated by the EQUIPMENT under conditions of total occlusion at the end of the PATIENT LINE.		IEC 60601-2-24:1998
MAXIMUM LIMITED PRESSURE (P_{LIMmax})	Highest PRESSURE at the PATIENT CONNECTION PORT during NORMAL USE and under a SINGLE FAULT CONDITION.		IEC 60601-2-12:2001
MAXIMUM PEAK VOLTAGE	Maximum value of the X-RAY TUBE VOLTAGE in a specified time interval. The unit of this quantity is the volt (V).		IEC 61676:2002
MAXIMUM PERMISSIBLE WORKING PRESSURE	PRESSURE specified by the MANUFACTURER or by the inspection authority or competent person(s) in the report of the most recent examination.	NG.11.02	IEC 60601-1:1988 IEC 60601-1/A2:1995
MAXIMUM TOLERABLE RISK	Value of RISK which is specified as the maximum which may be permitted. NOTE The value may be specified for the PEMS as a whole or for a particular hazard.		IEC 60601-1-4:2000
MAXIMUM TRACKING RATE	Maximum PULSE RATE at which the PULSE GENERATOR will respond on a 1:1 basis to a triggering signal.		IEC 60601-2-31/A1:1998
MAXIMUM TRACKING RATE	Maximum ventricular pacing rate in response to sensed arterial ACTIVITY.		IEC 60601-2-31/A1:1998
MAXIMUM WORKING PRESSURE (P_wmax)	Highest PRESSURE at the PATIENT CONNECTION PORT during NORMAL USE, irrespective of the setting of controls, other than the control intended to adjust this PRESSURE. NOTE Even if not adjustable, this maximum is equal to or less than the MAXIMUM LIMITED PRESSURE.		IEC 60601-2-12:2001
MAXIMUM X-RAY TUBE ASSEMBLY HEAT CONTENT	Maximum permissible X-RAY TUBE ASSEMBLY HEAT CONTENT under specific ambient conditions.	rm-36-31	IEC 60601-2-28:1993 IEC 60613:1989
MEAN CT NUMBER	Mean value of the COMPUTED TOMOGRAPHY NUMBERS of all PIXELS within a certain defined region of interest.		IEC 61223-2-6:1994

Term	Definition	Reference	Used in IEC
MEAN PEAK VOLTAGE	Mean value of all X-RAY TUBE VOLTAGE peaks during a specified time interval. The unit of this quantity is the volt (V).		IEC 61676:2002
MEASURED VALUE	Estimate of the TRUE VALUE of a quantity, derived from the INDICATED VALUE of a meter after applying all relevant CORRECTION FACTORS.	rm-73-08	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61303:1994
MEASURED VALUE	The best estimate of the TRUE VALUE of a quantity, being derived from the INDICATED VALUE of an instrument together with the application of all relevant CORRECTION FACTORS and the CALIBRATION FACTOR. NOTE The MEASURED VALUE is the “final result of measurement” shown in Figure 1 of IEC 60731:2002. Recommended replacement: rm-73-08		IEC 60731:2002
MEASURED VALUE	Best estimate of the TRUE VALUE of a quantity, derived from the INDICATED VALUE of an instrument together with the application of all relevant CORRECTION FACTORS.		IEC 61674/A1:2002
MEASURED VALUE	Value of a physical quantity derived by applying all relevant corrections to an INDICATED VALUE. Recommended replacement: rm-73-08		IEC 60580:2000
MEASURED VALUE	The best estimate of the CONVENTIONAL TRUE VALUE of a quantity, being derived from the INDICATED VALUE of an instrument together with the application of all relevant CORRECTION FACTORS. NOTE The CONVENTIONAL TRUE VALUE will usually be the value determined by the WORKING STANDARD with which the instrument under test is being compared. Recommended replacement: rm-73-08		IEC 61676:2002
MEASURING ASSEMBLY	Device to convert the output from the IONIZATION CHAMBER into a form suitable for the display of the value(s) of DOSE AREA PRODUCT or DOSE AREA PRODUCT RATE.		IEC 60580:2000
MEASURING ASSEMBLY	A device to convert the output from the RADIATION DETECTOR into a form suitable for display, control or storage of the values of ABSORBED DOSE, ABSORBED DOSE RATE or any dose-related quantities. It includes all electrical circuits in use during the period of PATIENT contact up to and including any SEPARATION DEVICE(S).		IEC 60601-2-9:1996
MEASURING ASSEMBLY	A device to measure the charge (or current) from the IONIZATION CHAMBER and convert it into a form suitable for displaying the values of dose or KERMA (or their corresponding rates). Recommended replacement: IEC 60601-2-9:1996		IEC 60731/A1:2002

Term	Definition	Reference	Used in IEC
MEASURING ASSEMBLY	Device to convert the output from the DETECTOR ASSEMBLY into a form suitable for the display of the value(s) of AIR KERMA, AIR KERMA LENGTH or AIR KERMA RATE. Recommended replacement: IEC 60601-2-9:1996		IEC 61674/A1:2002
MECHANICAL INDEX	MECHANICAL INDEX is given by $MI \equiv \frac{p_{ra} f_{awf}^{-1/2}}{C_{MI}}$ where $C_{MI} = 1 \text{ MPa MHz}^{-1/2}$; p_{ra} is the ATTENUATED PEAK-RAREFACTIONAL PRESSURE in megapascals; f_{awf} is the ACOUSTIC WORKING FREQUENCY in megahertz. Symbol: <i>MI</i> . Unit: None.		IEC 60601-2-37:2001
MEDICAL DEVICE	Any instrument, apparatus, appliance, material or other article, whether used alone or in combination, including the software necessary for its proper application, intended by the MANUFACTURER to be used for human beings for the purpose of – diagnosis, prevention, monitoring, TREATMENT or alleviation of disease, – diagnosis, monitoring, TREATMENT, alleviation of, or compensation for, an injury or handicap, – investigation, replacement or modification of the anatomy or of a physiological process, – control of conception, and which does not achieve its principal intended action in or on the human body by pharmacological, immunological or metabolic means, but which may be assisted in its function by such means. [ISO 13485:1996, definition 3.1]		ISO 14971:2000
MEDICAL DIAGNOSTIC RADIOLOGY	Medical diagnosis using IONIZING RADIATION.	rm-40-04	IEC 60601-1-3:1994 IEC 60601-2-43:2000 IEC 60806:1984 IEC 61223-2-1:1993

Term	Definition	Reference	Used in IEC
MEDICAL ELECTRICAL EQUIPMENT (hereinafter referred to as EQUIPMENT)	<p>Electrical EQUIPMENT, provided with not more than one connection to a particular SUPPLY MAINS and intended to diagnose, treat, or monitor the PATIENT under MEDICAL SUPERVISION and which makes physical or electrical contact with the PATIENT and/or transfers energy to or from the PATIENT and/or detects such energy transfer to or from the PATIENT.</p> <p>The EQUIPMENT includes those accessories as defined by the MANUFACTURER which are necessary to enable the NORMAL USE of the EQUIPMENT.</p>	NG.02.15	IEC 60601-1/A2:1995 IEC 60601-1:1988 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-13:2003 IEC 60601-2-33:2002 IEC 60601-2-51:2003 IEC 60731 /A1:2002 IEC 61217:2002 IEC 61674/A1:2002 IEC 62083:2000
MEDICAL ELECTRICAL EQUIPMENT	<p>Electrical EQUIPMENT, provided with not more than one connection to a particular SUPPLY MAINS and intended to diagnose, treat, or monitor the PATIENT under MEDICAL SUPERVISION and which makes physical or electrical contact with the PATIENT and/or transfers energy to or from the PATIENT and/or detects such energy transfer to or from the PATIENT.</p> <p>Under the scope of this Particular Standard EQUIPMENT means HAEMODIALYSIS, HAEMODIAFILTRATION and/or HAEMOFILTRATION EQUIPMENT.</p>		IEC 60601-2-16:1998
MEDICAL ELECTRICAL EQUIPMENT	<p>Electrical EQUIPMENT, provided with not more than one connection to a particular SUPPLY MAINS and intended to diagnose, treat, or monitor the PATIENT under MEDICAL SUPERVISION and which makes physical or electrical contact with the PATIENT and/or transfers energy to or from the PATIENT and/or detects such energy transfer to or from the PATIENT.</p> <p>Under the scope of this Particular Standard EQUIPMENT means PERITONEAL DIALYSIS EQUIPMENT.</p>		IEC 60601-2-39:1999
MEDICAL ELECTRICAL EQUIPMENT	<p>Electrical EQUIPMENT, provided with one or more connections to particular SUPPLY MAINS and intended to diagnose, treat, or monitor the PATIENT under MEDICAL SUPERVISION and which makes physical or electrical contact with the PATIENT and/or transfers energy to or from the PATIENT and/or detects such energy transfer to or from the PATIENT.</p> <p>See Figure 101 describing the possible SUPPLY MAINS for SURGICAL LUMINAIRES.</p>		IEC 60601-2-41:2000
MEDICAL ELECTRICAL SYSTEM		NG-2.203	IEC 60601-1-4:2000
MEDICAL ELECTRICAL SYSTEM	Totality of more than one item of MEDICAL ELECTRICAL EQUIPMENT or of MEDICAL ELECTRICAL EQUIPMENT in combination with other non-medical electrical EQUIPMENT that by COUPLING behaves as a unit with specified functions.		IEC 60601-2-13:2003
MEDICAL ELECTRICAL SYSTEM	<p>Combination of items of EQUIPMENT, at least one of which must be MEDICAL ELECTRICAL EQUIPMENT and interconnected by FUNCTIONAL CONNECTION or use of a MULTIPLE PORTABLE SOCKET-OUTLET.</p> <p>NOTE EQUIPMENT when mentioned in connection with a SYSTEM, should be taken to include EQUIPMENT.</p>		IEC 60601-1 /A2:1995 IEC 60601-1-2:2001
MEDICAL RADIOLOGICAL EXAMINATION	Medical examination using effects of IONIZING RADIATION.	rm-41-24	IEC 60580:2000

Term	Definition	Reference	Used in IEC
MEDICAL RADIOLOGY	Branch of RADIOLOGY applied to human and veterinary medicine as well as to dentistry and chiropractic.	rm-40-03	IEC 60601-2-43:2000
MEDICAL SUPERVISION	Adequate medical management of PATIENTS who may be at risk from some parameters of EXPOSURE to the MR EQUIPMENT, either because of the medical condition of the PATIENT, the levels of EXPOSURE or a combination,		IEC 60601-2-33:2002
MICROWAVE THERAPY EQUIPMENT	EQUIPMENT for the TREATMENT of the PATIENT by means of a propagated electromagnetic field in the frequency range of more than 300 MHz but not exceeding 30 GHz.		IEC 60601-2-6:1984
MID POINT AVERAGE TEMPERATURE	(T_M) The TEST DEVICE AVERAGE TEMPERATURE of the TEST DEVICE positioned at the mid point of the EQUIPMENT mattress. (See Figure 102.)		IEC 60601-2-21/A1:1996
MINIMUM BREAKING LOAD	Maximum load where Hooke's Law is applicable.	NG.11.03	IEC 60601-1/A2:1995
MINIMUM EFFECTIVE RANGE	The MINIMUM EFFECTIVE RANGE is the smallest permitted range of INDICATED VALUES for which an instrument complies with a stated performance.		IEC 61676:2002
MINIMUM LIMITED PRESSURE (P_{LIMmin})	Lowest PRESSURE at the PATIENT CONNECTION PORT during NORMAL USE and under a SINGLE FAULT CONDITION. NOTE This PRESSURE may be sub-atmospheric.		IEC 60601-2-12:2001
MINIMUM RATE	Lowest rate selectable by the OPERATOR, but not less than 1 ml/h. NOTE For INFUSION PUMPS FOR AMBULATORY USE it is the lowest selectable rate.		IEC 60601-2-24:1998
MINIMUM RATED RANGE	Least range of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER over which the instrument shall operate within the specified LIMITS OF VARIATION in order to comply with this standard.		IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/ A1:2002
MINOR SURGICAL LUMINAIRE (TREATMENT luminaire)	Single luminaire in the PATIENT environment which provides an adequate CENTRAL ILLUMINANCE to illuminate the body of the PATIENT locally. It is intended to be used in operating rooms for diagnosis and TREATMENT which can be interrupted without any hazard for the PATIENT in case of failure of the light. See Table 101.		IEC 60601-2-41:2000
MINUTE VOLUME (\dot{V})	Volume of gas per minute entering or leaving the lungs of the PATIENT.		IEC 60601-2-12:2001
MOBILE EQUIPMENT	TRANSPORTABLE EQUIPMENT intended to be moved from one location to another between periods of use while supported by its own wheels or equivalent means.	NG.02.16	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001
MOBILE OPERATING TABLE	An OPERATING TABLE intended to be moved from one location to another.		IEC 60601-2-46:1998
MODE OF OPERATION	For INTERVENTIONAL X-RAY EQUIPMENT, the technical state defined by a configuration of several predetermined LOADING FACTORS, technique factors or other settings for RADIOSCOPY or RADIOGRAPHY, selectable simultaneously by the operation of a single control. NOTE 1 Selection of a particular mode does not necessarily define the values of all the parameters affecting its use. NOTE 2 Values defined by selection of a particular mode are not necessarily invariable during its use.		IEC 60601-2-43:2000

Term	Definition	Reference	Used in IEC
MODEL OR TYPE REFERENCE	Combination of figures, letters or both used to identify a particular model of EQUIPMENT.	NG.12.02	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-4:2000
MODES OF OPERATION WITH CONTINUED DISPLAY	An X-RAY IMAGING ARRANGEMENT operating with continued display is regarded in this collateral standard IEC 60601-1-3:1994 as an X-RAY IMAGING ARRANGEMENT for RADIOLOGY if means are provided for automatic repetition of irradiation.		IEC 60601-1-3:1994
MODULATION TRANSFER FUNCTION (abbreviation MTF)	Modulus of the ONE-DIMENSIONAL OPTICAL TRANSFER FUNCTION. NOTE The MTF is defined in ISO 9334 as the modulus of the OPTICAL TRANSFER FUNCTION. For the purpose of this international standard IEC 61262-7:1995, this definition is more appropriate. Recommended replacement: rm-73-05		IEC 61262-7:1995
MODULATION TRANSFER FUNCTION (MTF)	Letter symbol: M. Fourier transform of the LINE SPREAD FUNCTION. For a symmetrical line spread function, the MODULATION TRANSFER FUNCTION is the normalized Fourier transform using the equation: $M(v) = \frac{\int_{-\infty}^{+\infty} L(x) \cos 2\pi v x dx}{\int_{-\infty}^{+\infty} L(x) x dx}$ where: v is the spatial frequency, L is the LINE SPREAD FUNCTION, x is the abscissa.	rm-73-05	IEC 60336:1993 IEC 60789:1992 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000
MOMENTARY CONTACT SWITCH	Control device which initiates and maintains operation of operating elements only as long as the control (actuator) is actuated. The manual control (actuator) returns automatically to the stop position when released. MOMENTARY CONTACT SWITCHES are also known as "hold-to-run control devices".		IEC 60601-2-38/ A1:1999
MONITOR	Part of a DEFIBRILLATOR providing a visual display of the electrical ACTIVITY of the PATIENT'S heart. NOTE The term is used within this Particular Standard to distinguish such a monitor from one which forms a separate EQUIPMENT in its own right even in cases where the separate stand-alone monitor is able to provide synchronization signals to the DEFIBRILLATOR, used as basis for AED rhythm recognition detection or providing control signals to the DEFIBRILLATOR.		IEC 60601-2-4:2002
MONITORING DEVICE	Device which continuously or repeatedly measures and indicates the value of a variable to the OPERATOR.		IEC 60601-2-13:2003

Term	Definition	Reference	Used in IEC
MOVING BEAM RADIOTHERAPY	RADIOTHERAPY with continuous displacement of the RADIATION SOURCE relative to the PATIENT during the IRRADIATION.	rm-42-41	IEC 60601-2-11:1997 IEC 60976/A1:2000 IEC 61217:2002
MOVING BEAM RADIOTHERAPY	RADIOTHERAPY with any planned displacement of the RADIATION FIELD or PATIENT relative to each other or with any planned change of ABSORBED DOSE distribution. Recommended replacement: rm-42-41		IEC 60601-2-1/A1:2002
MOVING GRID	ANTI-SCATTER GRID used in an ACCESSORY that enables that ANTI-SCATTER GRID to be moved, when irradiated by a RADIATION BEAM, in order to avoid the imaging of the absorbing strips and the consequent loss of information.	rm-32-15	IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-2:1996
MOVING GRID	ANTI-SCATTER GRID used in an ACCESSORY that enables the ANTI-SCATTER GRID to be moved, when irradiated by a RADIATION BEAM, in order to avoid the imaging of the absorbing strips and the consequent loss of information.		IEC 60627:2001
MTF ANALYZER	Instrument, including relay optics and software, capable of performing measurements of the MODULATION TRANSFER FUNCTION.		IEC 61262-7:1995
MULTI-DETECTOR COUNTER	Instrument consisting of an array of WELL-TYPE DETECTORS to determine the ACTIVITY in multiple samples simultaneously.		IEC 61948-1:2001
MULTI-PURPOSE ULTRASONIC EQUIPMENT	Ultrasonic EQUIPMENT which is intended for more than one clinical application.		IEC 60601-2-37:2001
MULTICHANNEL ELECTROCARDIOGRAPH	EQUIPMENT for the simultaneous recording of several ECG LEADS. This EQUIPMENT may also provide facilities for phonocardiography and PULSE recording, etc.		IEC 60601-2-25 A1:1999
MULTICHANNEL ELECTROCARDIOGRAPH	EQUIPMENT for the simultaneous recording of two or more ECG LEADS. This EQUIPMENT may also provide facilities for phonocardiography and PULSE recording, etc.		IEC 60601-2-51:2003
MULTIFUNCTION PATIENT MONITORING EQUIPMENT	A modular or pre-configured device including more than one PHYSIOLOGICAL MONITORING UNIT designed to collect information from a single PATIENT and process it for monitoring purposes and to generate ALARMS.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
MULTIPLE FUNCTION	Measurement of more than one physiological parameter.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
MULTIPARAMETER PATIENT MONITORING EQUIPMENT	Stationary or MOBILE EQUIPMENT powered by an electrical power source and including one or more physiological monitoring units designed to collect information from a PATIENT, process it and generate ALARMS.		IEC 60601-2-23:1999
MULTIPLE WINDOW SPATIAL REGISTRATION	The measured position of a source as a function of the PULSE amplitude analyzer window setting.		IEC 60789:1992
NARROW BEAM	RADIATION BEAM of a solid angle as small as possible for measuring a desired RADIATION QUANTITY thus minimizing the contribution of SCATTERED RADIATION and ensuring, if relevant, the lateral electronic equilibrium.	rm-37-22	IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
NARROW BEAM CONDITION	Arrangement for the measurement of a RADIATION QUANTITY in a NARROW BEAM of IONIZING RADIATION.	rm-37-23	IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61267:1994
NATIONAL STANDARD	A standard recognized by an official national decision as the basis for fixing the value in that country of all other standards of the given quantity.		IEC 60731/A1:2002
NET OPTICAL DENSITY	Density above FILM BASE PLUS FOG DENSITY.		IEC 61223-2-10:1999
NEUTRAL ELECTRODE	Electrode of a relatively large area for connection to the body of the PATIENT, intended to provide a return path for the high frequency current with such a low current density in the body tissue that physical effects such as unwanted burns are avoided. NOTE The NEUTRAL ELECTRODE is also known as plate, plate electrode, passive, return or dispersive electrode.		IEC 60601-2-2:1998
NEUTRAL ELECTRODE	Reference point for differential amplifiers and/or interference suppression circuits, not forming part of any ELECTROCARDIOGRAPH LEAD. [IEC 60601-2-25:1999, definition 2.107]		IEC 60601-2-25:1993 IEC 60601-2-27:1994 IEC 60601-2-47:2001
NEUTRAL ELECTRODE	ELECTRODE used as a common mode reference for differential amplifiers and/or interference suppression which is not involved in an EQUIPMENT ELECTRODE combination.		IEC 60601-2-26:2002
NEUTRAL ELECTRODE	Reference point for differential amplifiers and/or interference suppression circuits. Any ELECTROCARDIOGRAPHIC LEAD is independent of the potential of this reference point.		IEC 60601-2-51:2003
NEUTRON	Elementary particle having no electric charge, a rest mass of $1,67492 \times 10^{-27}$ kg, and a mean life of about 1 000 s.	rm-11-17	IEC 60601-2-1/A1:2002
NOISE	VARIATION OF COMPUTED TOMOGRAPHY NUMBERS from a mean value in a defined area in the image of a uniform substance. The magnitude of NOISE is indicated by the standard deviation of the COMPUTED TOMOGRAPHY NUMBERS of a uniform substance in the region of interest.		IEC 61223-2-6:1994
NOISE	Unwanted signals of any frequency present in the ELECTROCARDIOGRAM.		IEC 60601-2-51:2003
NOMINAL (value)	Value quoted for reference purposes which is subject to agreed tolerances, for example, NOMINAL MAINS VOLTAGE, NOMINAL diameter of a screw.	NG.12.03	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-44:2002
NOMINAL ANODE INPUT POWER	Highest constant ANODE INPUT POWER that can be applied for a single X-RAY TUBE LOAD in a specific LOADING TIME.	rm-36-23	IEC 60336:1993 IEC 60601-2-28:1993 IEC 60613:1989

Term	Definition	Reference	Used in IEC
NOMINAL ELECTRIC POWER	For a HIGH-VOLTAGE GENERATOR, highest constant electric power which can be delivered for a single X-RAY TUBE LOAD in a specific LOADING TIME.	rm-36-19	IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001
NOMINAL ENERGY	for ELECTRON radiation, energy stated by the MANUFACTURER to characterize the RADIATION BEAM. This energy is approximately equal to the most probable energy at the surface of the measuring PHANTOM, $E_{p,0}$ (see ICRU Report 35: Section 3.3; Energy, $E_{p,0}$); for X-RADIATION, the energy stated by the MANUFACTURER to characterize the RADIATION BEAM.	rm-13-56	IEC 60601-2-1/A1:2002 IEC 62083:2000
NOMINAL ENERGY	As a characteristic of medical ELECTRON accelerators, RADIATION ENERGY describing: – for X-RADIATION the energy of the ELECTRONS striking the TARGET, and for ELECTRON radiation the energy of the ELECTRONS in the USEFUL BEAM at the PHANTOM surface in the NORMAL TREATMENT DISTANCE. Recommended replacement: rm-13-56		IEC 60976/ A1:2000
NOMINAL ENTRANCE FIELD SIZE	For an ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER, ENTRANCE FIELD SIZE that would be achieved with a parallel beam of IONIZING RADIATION.	rm-32-44	IEC 61223-3-1:1999
NOMINAL ENTRANCE FIELD SIZE	The ENTRANCE FIELD SIZE of the XRII that would be achieved with a parallel beam of IONIZING RADIATION with the RADIATION SOURCE approaching infinity. Recommended replacement: rm-32-44		IEC 61262-1:1994
NOMINAL FOCAL SPOT VALUE	Dimensionless numerical value having a specific relation to the dimensions of the effective spot of an X-RAY TUBE, measured under specific conditions.	rm-20-14	IEC 60336:1993 IEC 60601-2-28:1993 IEC 60613:1989 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-6:1994 IEC 61262-7:1995
NOMINAL IMAGE SIZE	The product of the linear dimension of a small OBJECT in the ENTRANCE PLANE and the CENTRAL MAGNIFICATION.		IEC 61262-6:1994
NOMINAL SHORTEST IRRADIATION TIME	For HIGH-VOLTAGE GENERATORS with AUTOMATIC CONTROL SYSTEMS which vary the IRRADIATION TIME, shortest IRRADIATION TIME for which a required constancy of the controlled RADIATION QUANTITY is maintained.	rm-36-12	IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61223-3-1:1999
NOMINAL TOMOGRAPHIC SECTION THICKNESS	In CT SCANNERS the TOMOGRAPHIC SECTION THICKNESS which is selected and indicated on the CONTROL PANEL.		IEC 60601-2-44:2002
NOMINAL TOMOGRAPHIC SECTION THICKNESS	In CT SCANNERS the TOMOGRAPHIC SECTION THICKNESS which is selected and indicated on the CONTROL PANEL. NOTE In helical scanning the thickness of a reconstructed image depends on the helical reconstruction algorithm and pitch, and hence this thickness may not equal the NOMINAL TOMOGRAPHIC SECTION THICKNESS. The thickness of the reconstructed image may be indicated or selected prior to the helical scan.		IEC 60601-2-44:2002

Term	Definition	Reference	Used in IEC
NOMINAL SENSITIVITY	The ratio of the change in TRANSDUCER output to a change of the value of the PRESSURE at any selected pressure range.		IEC 60601-2-34:2000
NOMINAL TOMOGRAPHIC SLICE THICKNESS	In EQUIPMENT for COMPUTED TOMOGRAPHY, SLICE THICKNESS selected and indicated at the CONTROL PANEL. Recommended replacement: NOMINAL TOMOGRAPHIC SECTION THICKNESS		IEC 61223-2-6:1994
NOMINAL X-RAY TUBE VOLTAGE	Highest permitted X-RAY TUBE VOLTAGE for specific operating conditions.	rm-36-03	IEC 60336:1993 IEC 60522:1999 IEC 60601-2-7:1998 IEC 60601-2-8,1999 IEC 60601-2-28:1993 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60806:1984 IEC 61267:1994
NON-FLAMMABLE ANAESTHETIC AGENTS	(IEC 60601-1)		IEC 60601-2-13:2003
NON-INTERCHANGEABLE ANAESTHETIC VAPOUR DELIVERY DEVICE	ANAESTHETIC VAPOUR DELIVERY DEVICE designed to be used only with EQUIPMENT specified by the MANUFACTURER. NOTE These devices may or may not be OPERATOR-detachable.		IEC 60601-2-13:2003
NON-ISOCENTRIC	When used in combination with RADIOLOGICAL techniques or EQUIPMENT, refers to conditions without the use of, or to the absence of, an ISOCENTRE.		IEC 60976/ A1:2000
NON-LATCHED ALARM	An ALARM, the visual and auditory manifestation of which stops when the parameter (which caused the ALARM) returns to a value which no longer exceeds the ALARM LIMIT or if the abnormal PATIENT condition does not exist any longer.		IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-23:1999
NON-LATCHED ALARM	An ALARM, the auditory or visual and auditory manifestations of which stop when the ALARM CONDITION no longer exists.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
NON-LATCHING ALARM SIGNAL	ALARM SIGNAL that automatically stops ANNUNCIATING when its associated ALARM CONDITION no longer exists		IEC 60601-2-13:2003
NON-LINEARITY	Deviation from LINEARITY, quantified as follows: on each range the half full SCALE READING M is taken as a reference; the input signal Q required to produce this REFERENCE SCALE READING is measured. At another SCALE READING m produced by an input signal q , the percentage deviation from LINEARITY is given by: $100 \cdot ((m \cdot Q / M \cdot q) - 1)$ NOTE 1 For a MEASURING ASSEMBLY set to the "dose" mode, the input signal is electric charge; NOTE 2 For a MEASURING ASSEMBLY set to the "dose rate" mode, the input signal is electric current.		IEC 60731/A1:2002
NON-IMPLANTABLE PULSE GENERATOR	MEDICAL ELECTRICAL EQUIPMENT with an INTERNAL ELECTRICAL POWER SOURCE which is intended for use outside the body and which produces a periodic electrical PULSE intended to stimulate the heart through a LEAD (or combination of a LEAD and PATIENT CABLE).		IEC 60601-2-31/ A1:1998

Term	Definition	Reference	Used in IEC
NON-INVASIVE MEASUREMENT	Measurement of X-RAY TUBE VOLTAGE by analysis of the emitted radiation.		IEC 61676:2002
NON-IRRADIATED CONSTANCY TEST FILM	Film with an optical density resulting from processing a non-irradiated film under specific conditions.		IEC 61223-2-7:1999
NON-SCANNING MODE	Mode of operation of an ULTRASONIC DIAGNOSTIC EQUIPMENT that involves a sequence of ultrasonic PULSES which give rise to ultrasonic scan lines that follow the same acoustic path.		IEC 60601-2-37:2001
NON-SCREEN FILM	In DIRECT RADIOGRAPHY, RADIOGRAPHIC FILM to be used without an INTENSIFYING SCREEN.	rm-32-35	IEC 60336:1993 IEC 60806:1984 IEC 61223-2-1:1993 IEC 61223-3-4:2000 IEC 61262-3:1994
NON-UNIFORMITY OF RESPONSE	In a RADIONUCLIDE imaging device, differences in COUNT RATE between small areas of specified dimensions within the DETECTOR FIELD OF VIEW when a uniform plane source parallel to the detector face and of dimensions larger than its ENTRANCE FIELD is used.	rm-34-26	IEC 60789:1992 IEC 61948-2:2001
NORMAL CONDITION	Condition in which all means provided for protection against SAFETY HAZARDS are intact.	NG.10.07	IEC 60601-1/ A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-17 A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
NORMAL OPERATING MODE	Mode of operation of the MR EQUIPMENT in which none of the outputs have a value that may cause physiological stress to PATIENTS.		IEC 60601-2-33:2002
NORMAL POSITION	The position of the OPERATING TABLE top with all sections set in the horizontal position.		IEC 60601-2-46:1998
NORMAL SENSITIVITY	SENSITIVITY of 10 mm per mV.		IEC 60601-2-25/A1:1999 IEC 60601-2-51:2003
NORMAL TREATMENT DISTANCE	For ELECTRON IRRADIATION, specified distance measured along the axis of the beam from the VIRTUAL SOURCE of ELECTRONS to the ENTRANCE SURFACE. For X-IRRADIATION, specified distance measured along the axis of the beam from the VIRTUAL SOURCE of X-RADIATION to the ISOCENTRE or, in EQUIPMENT without an ISOCENTRE, to a specified plane.	rm-33-16	IEC 60601-2-8,:1999 IEC 60976 /A1:2000 IEC 61217:2002
NORMAL TREATMENT DISTANCE	A specified distance measured along the RADIATION BEAM AXIS from the RADIATION SOURCE to the ISOCENTRE or, for EQUIPMENT without an ISOCENTRE, to a specified plane. Recommended replacement: IEC 60976, IEC 61217:2002		IEC 60601-2-11:1997

Term	Definition	Reference	Used in IEC
NORMAL TREATMENT DISTANCE (abbreviation: NTD)	<p>For ELECTRON IRRADIATION, specified distance measured along the REFERENCE AXIS from the ELECTRON radiation window to the distal end of the ELECTRON beam APPLICATOR or to a specified plane;</p> <p>FOR X-IRRADIATION, specified distance measured along the REFERENCE AXIS from the front surface of the TARGET to the ISOCENTRE or, for EQUIPMENT without an ISOCENTRE, to a specified plane.</p> <p>Recommended replacement: IEC 60976, IEC 61217:2002</p>		<p>IEC 60601-2-1/A1:2002</p> <p>IEC 60601-2-29:1999</p>
NORMAL USE	<p>Use and operation, as well as transport and storage between periods of use, according to the INSTRUCTIONS FOR USE or for the obvious intended purpose.</p>	rm-82-04	<p>IEC 60336:1993</p> <p>IEC 60522:1999</p> <p>IEC 60601-1-3:1994</p> <p>IEC 60601-2-7:1998</p> <p>IEC 60601-2-11:1997</p> <p>IEC 60601-2-28:1993</p> <p>IEC 60601-2-43:2000</p> <p>IEC 60601-2-44:2002</p> <p>IEC 60601-2-45:2001</p> <p>IEC 60976 /A1:2000</p> <p>IEC 61223-3-1:1999</p> <p>IEC 61223-3-4:2000</p> <p>IEC 61262-1:1994</p> <p>IEC 61262-2:1994</p> <p>IEC 61262-3:1994</p> <p>IEC 61262-4:1994</p> <p>IEC 61262-5:1994</p> <p>IEC 61262-6:1994</p> <p>IEC 61262-7:1995</p> <p>IEC 61331-3:1998</p> <p>IEC 62083:2000</p>
NORMAL USE	<p>Operation, including routine inspection and adjustments by the OPERATOR, and STAND-BY, according to the INSTRUCTIONS FOR USE.</p>	NG.10.08	<p>IEC 60601-1/A2:1995</p> <p>IEC 60601-1-4:2000</p> <p>IEC 60601-2-1/A1:2002</p> <p>IEC 60601-2-11:1997</p> <p>IEC 60601-2-12:2001</p> <p>IEC 60601-2-13:2003</p> <p>IEC 60601-2-17/A1:1996</p> <p>IEC 60601-2-29:1999</p> <p>IEC 60601-2-32:1994</p> <p>IEC 60601-2-51:2003</p>

Term	Definition	Reference	Used in IEC
NORMALIZED SLICE SENSITIVITY	SLICE SENSITIVITY divided by the AXIAL SLICE WIDTH (EW) for that slice.		IEC 61675-1:1998
NORMALIZED VOLUME SENSITIVITY	VOLUME SENSITIVITY divided by the AXIAL FIELD OF VIEW of the tomograph or the PHANTOM length, whichever is the smaller.		IEC 61675-2:1998
NUCLEAR MEDICINE	Use of unsealed RADIONUCLIDES for diagnostic and therapeutic purposes.	rm-40-06	IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61303:1994
OBJECT PROGRAMMED CONTROL	In an X-RAY GENERATOR, mode of operation in which (a) semi-permanently pre-set combination(s) of LOADING FACTORS is (are) pre-selected depending upon the object to be irradiated, usually for diagnostic purposes.	rm-36-44	IEC 60601-2-7:1998
OBJECT SLICE	A slice in the object. The physical property of this slice that determines the measured information is displayed in the tomographic image.	rm-32-59	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
OBJECTIVE EVIDENCE	Information which can be proven true, based on facts obtained through observation, measurement, TEST or other means. [ISO 8402:1994, definition 2.19]		ISO 14971:2000
OBLIQUE CROSS GRID	CROSS GRID in which the directions of the absorbing strips form an angle other than 90°.		IEC 60627:2001
OCCLUSION ALARM THRESHOLD (PRESSURE)	Value of the physical quantity at which the occlusion ALARM is activated.		IEC 60601-2-24:1998
OFFSET	Deviation of the position of the PROJECTION of the COR (X'_p) from $X_p = 0$.		IEC 61675-2:1998 IEC 61948-2:2001
ONE-DIMENSIONAL OPTICAL TRANSFER FUNCTION (abbreviation 1-OTF)	Section of the OPTICAL TRANSFER FUNCTION through the origin in a given orientation.		IEC 61262-7:1995
ONE-PEAK HIGH-VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR for operation on a single-phase supply that delivers an unrectified output voltage, or a rectified output voltage with one peak during each cycle of the supply.	rm-21-02	IEC 60601-2-7:1998 IEC 60613:1989
OPERATING CABLE	A PATIENT supporting table for general, surgical/medical procedures.		IEC 60601-2-46:1998
OPERATING CONDITIONS FOR NOMINAL X-RAY TUBE VOLTAGE	NOMINAL X-RAY TUBE VOLTAGE is defined in IEC 60788 (rm-36-03) as the highest permitted X-RAY TUBE VOLTAGE for specific operating conditions. In this collateral standard, if specific operating conditions are not stated, it is to be assumed that the value referenced is unconditional and is thus the highest X-RAY TUBE VOLTAGE permitted for NOMINAL use of the item under consideration. Such a value cannot be higher, but is sometimes lower, than values permitted for certain separate subassemblies or parts of the item.	rm-36-49	IEC 60601-1-3:1994
OPERATING CONDITIONS FOR NOMINAL X-RAY TUBE VOLTAGE	NOMINAL X-RAY TUBE VOLTAGE is defined in IEC 60788 (rm-36-03) as the highest permitted X-RAY TUBE VOLTAGE for specific operating conditions. In this standard, if specific operating conditions are not stated, it is to be assumed that the value referenced is unconditional and is thus the highest X-RAY TUBE VOLTAGE permitted for NOMINAL USE of the item under consideration. Such a value cannot be higher, but is sometimes lower, than values permitted for certain separate subassemblies or parts of the item.		IEC 60601-2-45:2001

Term	Definition	Reference	Used in IEC
OPERATING CONDITIONS FOR NOMINAL X-RAY TUBE VOLTAGE	<p>NOMINAL X-RAY TUBE VOLTAGE is defined in IEC 60788 (rm-36-03) as the highest permitted X-RAY TUBE VOLTAGE for specific operating conditions. In this standard IEC 60601-2-7:1998, if specific operating conditions are not stated, it is to be assumed that the value referenced is unconditional and is thus the highest X-RAY TUBE VOLTAGE permitted for NORMAL USE of the item under consideration. Such a value cannot be higher, but is sometimes lower, than values permitted for certain separate subassemblies or parts of the item.</p> <p>Recommended: Definition from IEC 60601-1-3</p>		IEC 60601-2-7:1998
OPERATING FREQUENCY	Fundamental frequency of a signal, electrical or non-electrical, that is set in an EQUIPMENT or SYSTEM intended to control a physiological parameter.		IEC 60601-1-2:2001
OPERATOR	Person utilizing an EQUIPMENT individually with or without the aid of an assistant, who controls some or all functions of the EQUIPMENT in his presence.	rm-85-02	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-37:2001 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60731/A1:2002 IEC 60976/A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-9:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61331-2:1994 IEC 61331-3:1998 IEC 61674 /A1:2002 IEC 62083:2000

Term	Definition	Reference	Used in IEC
OPERATOR	Person handling EQUIPMENT. Recommended replacement: rm-85-02	NG.12.17	IEC 60601-1/ A2:1995 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-26:2002 IEC 60601-2-32:1994 IEC 60601-2-47:2001 IEC 60601-2-51:2003
OPERATOR'S POSITION	Intended location and orientation of the OPERATOR with respect to the EQUIPMENT for NORMAL USE according to the instructions for use.		IEC 60601-2-12:2001
OPTICAL TRANSFER FUNCTION (abbreviation OTF)	Two-dimensional Fourier transform of the imaging system's POINT SPREAD FUNCTION, see ISO 9334. NOTE For the OPTICAL TRANSFER FUNCTION to have significance, it is essential that the imaging system is working in its LINEAR RANGE, and that an ISOPLANATIC REGION is considered.		IEC 61262-7:1995
ORGAN COUNTING SYSTEM	Instrument used for radiation detection of incorporated radioactive substances in specific organs or regions of the body.		IEC 61948-1:2001
ORTHOGONAL CROSS GRID	CROSS GRID in which the directions of the absorbing strips form an angle of 90°.		IEC 60627:2001
OUTFLOW	The phase during which the peritoneal cavity is emptied. NOTE The term drain is commonly used as a synonym for outflow.		IEC 60601-2-39:1999
OUTPUT CIRCUIT	All conductive parts used to couple radio-frequency power from the generator to the APPLICATORS, including conductive (inaccessible) parts of the APPLICATORS and their connecting cables.		IEC 60601-2-3 /A1:1998
OUTPUT IMAGE	In an electro-optical vacuum device, light image generated in the OUTPUT SCREEN.	rm-32-49	IEC 61223-2-1:1993 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
OUTPUT POWER	Time-average ultrasonic power radiated by a TREATMENT HEAD of EQUIPMENT into an approximately free field under specified conditions in a specified medium, preferably in water (see 3.5 of IEC 61161). [IEC 61689, definition 3.31]		IEC 60601-2-5:2000
OUTPUT POWER	Time-average power radiated by an ULTRASONIC TRANSDUCER into an approximately free-field under specified conditions in a specified medium, preferably water. Symbol: <i>P</i> . Unit: milliwatts, mW.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
OUTPUT SCREEN	In an electro-optical vacuum device, layer in which the ELECTRON pattern is converted into a light image.	rm-32-48	IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-7:1995
OVARY SHIELD	PROTECTIVE DEVICE intended to protect the gonads of a female PATIENT.	rm-64-07	IEC 61331-3:1998
OVERALL UNCERTAINTY	Uncertainty associated with the MEASURED VALUE, i.e. it represents the bounds within which the ERROR OF MEASUREMENT is estimated to lie. NOTE For the purpose of this standard IEC 60731/A1:2002 the OVERALL UNCERTAINTY may be taken as the EXPANDED UNCERTAINTY corresponding to a confidence level of 95 %.		IEC 60731/A1:2002
OVERALL UNCERTAINTY	Quadrature combination of the random and non-random uncertainties at the 68 % confidence limits. Recommended replacement: IEC 61674		IEC 61303:1994
OVERALL UNCERTAINTY	Uncertainty associated with the MEASURED VALUE, i.e. representing the bounds within which the ERROR OF MEASUREMENT is estimated to lie.		IEC 61674/ A1:2002
OVERLOAD TOLERANCE	Maximum input-circuit voltage which does not alter the functioning of the ELECTROCARDIOGRAPH.		IEC 60601-2-51:2003
OVER-BLANKET	BLANKET to be used over a PATIENT.		IEC 60601-2-35:1996
OVER-CURRENT RELEASE	PROTECTIVE DEVICE which causes a circuit to open with or without delay, when the current in the device exceeds a predetermined value.	NG.09.07	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-45:2001
OXYGEN RICH ENVIRONMENT	An environment in which partial pressure of oxygen is greater than 275 hPa.		IEC 60601-2-13:2003
PAD	HEATING DEVICE which can be bent but not folded.		IEC 60601-2-35:1996
PARALLEL GRID	LINEAR GRID in which the planes of the absorbing strips are parallel to each other and perpendicular to the incident face.		IEC 60627:2001
PARALLEL HOLE COLLIMATOR	COLLIMATOR with a number of apertures, the axes of which are parallel.		IEC 60789:1992
PART LEAKAGE CURRENT	Current flowing from a SINGLE FUNCTION through the PATIENT to the remaining SINGLE FUNCTION(S) of the same APPLIED PART under NORMAL CONDITION.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
PARTIAL BODY SAR	SAR averaged over the mass of the PATIENT'S body that is exposed by the VOLUME RF TRANSMIT COIL and over a specified time.		IEC 60601-2-33:2002
PARTICLE ACCELERATOR	EQUIPMENT for accelerating charged particles such as ELECTRONS, protons, deuterons and alpha particles to kinetic energies higher than corresponding to the voltage applied. Thus: – ELECTRON accelerator.	rm-23-01	IEC 60601-2-1/A1:2002 IEC 60976/A1:2000 IEC 61217:2002 IEC 62083:2000
PASSWORD	For EQUIPMENT under the control of a PROGRAMMABLE ELECTRONIC SUBSYSTEM (PESS), sequence of keystrokes that permits OPERATOR access for NORMAL USE or to reset INTERLOCKS and, with a different sequence of keystrokes, permits access for adjustment and maintenance.		IEC 60601-2-1/A1:2002 IEC 62083:2000

Term	Definition	Reference	Used in IEC
PATIENT	Living being (person or animal) undergoing medical or dental investigation or TREATMENT.	NG.12.04	IEC 60580:2000 IEC 60601-1/A2:1995 IEC 60601-1-4:2000 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-26:2002 IEC 60601-2-32:1994 IEC 60601-2-47:2001 IEC 60601-2-51:2003 IEC 60731/A1:2002 IEC 61674/A1:2002
PATIENT	Person or animal undergoing medical examination or TREATMENT. For purposes of RADIOLOGICAL PROTECTION, a person or animal is a PATIENT only during the intentional application of IONIZING RADIATION to that person or animal. Recommended replacement: NG.12.04	rm-62-03	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-17 A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61267:1994 IEC 61331-2:1994 IEC 61331-3:1998 IEC 672083:2000

Term	Definition	Reference	Used in IEC
PATIENT	An infant who is being treated by means of visible radiation. Recommended replacement: NG 12.04		IEC 60601-2-50:2000
PATIENT ANATOMY MODEL/ANATOMY MODELLING	All physical and anatomical parameters required to plan a course of RADIOTHERAPY for a particular PATIENT. The process of establishing the PATIENT ANATOMY MODEL is referred to as "ANATOMY MODELLING".		IEC 62083:2000
PATIENT AUXILIARY CURRENT	Current flowing in the PATIENT in NORMAL USE between parts of the APPLIED PART and not intended to produce a physiological effect, for example, bias current of an amplifier, current used in impedance plethysmography.	NG.05.04	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
PATIENT CABLE	Multiwire cable and associated connector(s) to connect the ELECTRODES to the ELECTROCARDIOGRAPH. Recommended replacement: generalized term that suits all 3 definitions of PATIENT CABLE		IEC 60601-2-25 /A1:1999 IEC 60601-2-51:2003
PATIENT CABLE	Multiwire cable and associated connector(s) to connect the ELECTRODES to the AMBULATORY RECORDER. [IEC 60601-2-25:1999, definition 2.109] Recommended replacement: generalized term that suits all 3 definitions of PATIENT CABLE		IEC 60601-2-26:2002 IEC 60601-2-47:2001
PATIENT CABLE	Device attached to the terminals of a non-implantable PULSE GENERATOR so that the distance between it and the pacing LEAD can be increased. Recommended replacement: generalized term that suits all 3 definitions of PATIENT CABLE		IEC 60601-2-31 /A1:1998
PATIENT CIRCUIT	Any electrical circuit which contains one or more PATIENT CONNECTIONS. PATIENT CIRCUITS include all conductive parts which are not insulated from the PATIENT CONNECTIONS to the extent necessary to comply with the dielectric strength requirements or which are not separated from the PATIENT CONNECTIONS to the extent necessary to comply with the CREEPAGE DISTANCE and AIR CLEARANCE requirements.	NG.01.15	IEC 60601-1/A2:1995
PATIENT CONNECTION	Every individual part of the APPLIED PART through which current can flow between the PATIENT and the EQUIPMENT in NORMAL CONDITION or SINGLE FAULT CONDITION.	NG.01.23	IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-51:2003
PATIENT CONNECTION PORT (OF THE VENTILATOR BREATHING SYSTEM)	Port of the VENTILATOR BREATHING SYSTEM to which the PATIENT can be connected. [ISO 4135:1995, definition 4.2.16] NOTE Interface between the VENTILATOR BREATHING SYSTEM and the PATIENT.		IEC 60601-2-12:2001
PATIENT ELECTRODE	Means in contact with a specified part of the body to detect heart action voltage in combination with another means. [IEC 60601-2-25:1999, definition 2.104]		IEC 60601-2-47:2001
PATIENT END	That end of the PATIENT LINE where connection to the PATIENT takes place.		IEC 60601-2-24:1998
PATIENT ENVIRONMENT	IEC 601-1-1 2.202		IEC 60601-2-9:1996

Term	Definition	Reference	Used in IEC
PATIENT EXTRAPMENT	The ability for a PATIENT to insert his / her head, neck or chest cavity into a permanent opening in the BED and/or its ACCESSORIES or a temporary opening created during NORMAL USE and from which the PATIENT cannot remove that portion of his/her anatomy.		IEC 60601-2-38 /A1:1999
PATIENT LEAKAGE CURRENT	Current flowing from the APPLIED PART via the PATIENT to earth or flowing from the PATIENT via an F-type APPLIED PART to earth originating from the unintended appearance of a voltage from an external source on the PATIENT.	NG.05.06	IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-51:2003
PATIENT LINE	That part of the ADMINISTRATION SET between the EQUIPMENT and the PATIENT.		IEC 60601-2-24:1998
PATIENT SUPPORT	In RADIOLOGICAL EQUIPMENT, component such as a table top or arm rest, serving to support the PATIENT in order to allow the part of his body which is to be irradiated to be positioned or to be displaced.	rm-30-02	IEC 60601-1-3:1994 IEC 60601-2-11:1997 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61217:2002 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61267:1994
PATIENT SUPPORT	The assembly of EQUIPMENT that supports the PATIENT. Recommended replacement: rm-30-02		IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
PATIENT SURFACE	In RADIOLOGY, surface through which the radiation enters the body of the PATIENT.	rm-37-18	IEC 60601-1-3:1994 IEC 60601-2-43:2000 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61331-3:1998
PEAK-RAREFACTIONAL ACOUSTIC PRESSURE	Maximum of the modulus of the negative instantaneous acoustic pressure in an acoustic field during an acoustic repetitions period. Symbol: p_r . Unit: megapascals, MPa.		IEC 60601-2-37:2001
PENDANT CONTROL	Means, used by either PATIENT or OPERATOR, to control the drives that activate various BED functions.		IEC 60601-2-38 A1:1999

Term	Definition	Reference	Used in IEC
PENETRATIVE QUALITY	Depth in a PHANTOM most distant from its surface at which the ABSORBED DOSE is 80 % of the maximum ABSORBED DOSE both measured on the radiation axis in a specified RADIATION FIELD and with the surface of the PHANTOM at a specified distance.		IEC 60976/A1:2000
PENUMBRA	In RADIOLOGY, spatial region around the RADIATION BEAM where the value of radiation flux is between two specified or specific fractions of the value that is measured in the RADIATION BEAM AXIS, these two values being measured in a same cross-section. NOTE The existence of such spatial regions can be due to one or more of the following phenomena: <ul style="list-style-type: none"> – EXTRA-FOCAL RADIATION; – SCATTERED RADIATION; – absence of lateral electronic equilibrium; – pair production; – geometry of the RADIATION SOURCE and of the BEAM LIMITING SYSTEM. 	rm-37-08	IEC 60976/A1:2000 IEC 62083:2000
PERCENTAGE RIPPLE	For a HIGH-VOLTAGE GENERATOR, ratio of the difference between the highest and the lowest values of a rectified voltage WAVEFORM during a cycle of the supply to the highest value, expressed as a percentage.	rm-36-17	IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-44:2002 60601-2-45:2001 IEC 60613:1989 IEC 61267:1994 IEC 61331-1:1994
PERCENTAGE RIPPLE IN CONSTANT POTENTIAL HIGH-VOLTAGE GENERATORS	Unless otherwise stated, it is to be assumed that for a HIGH-VOLTAGE GENERATOR to be regarded as a CONSTANT POTENTIAL HIGH-VOLTAGE GENERATOR, the PERCENTAGE RIPPLE of its output voltage (under the relevant conditions) does not exceed 4. Recommended replacement: rm-36-17		IEC 60601-2-7:1998 IEC 60601-2-45:2001
PERFORMANCE CHARACTERISTIC	One of the quantities used to define the performance of an instrument (e.g. RESPONSE, LEAKAGE CURRENT).	rm-72-05	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/A1:2002
PERFORMANCE CHARACTERISTIC	One of the quantities used to define the performance of an instrument (e.g. RESPONSE). Recommended replacement: IEC 60731, IEC 61674		IEC 61676:2002
PERITONEAL DIALYSIS	A process whereby DIALYSING SOLUTION is introduced into the peritoneal cavity of the PATIENT and is subsequently removed.		IEC 60601-2-39:1999
PERITONEAL DIALYSIS EQUIPMENT	EQUIPMENT used to perform PERITONEAL DIALYSIS.		IEC 60601-2-39:1999
PERMANENT FILTRATION	The QUALITY EQUIVALENT FILTRATION effected in an X-RAY TUBE ASSEMBLY by permanently fixed materials intercepting the X-ray beam, that are not intended to be removed for any application and are not provided with means for removal in NORMAL USE.		IEC 60522:1999

Term	Definition	Reference	Used in IEC
PERMANENTLY INSTALLED EQUIPMENT	EQUIPMENT that is electrically connected to the SUPPLY MAINS by means of a permanent connection which can only be detached by the use of a TOOL.	NG.02.17	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
PHANTOM	In MEDICAL RADIOLOGY, object behaving in essentially the same manner as tissue, with respect to ABSORPTION or SCATTERING of the IONIZING RADIATION in question. PHANTOMS are used, for example, for simulating practical conditions of measurement: <ul style="list-style-type: none"> – for purposes of RADIATION PROTECTION; – for evaluation the performances of diagnostic systems with respect to the radiation or to the object; – for dosimetry. 	rm-54-01	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/ A1:2000 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61267:1994
PHANTOM	Device, intended to simulate parts of the PATIENT for test purposes.		IEC 60601-2-6:1984
PHOTON	Stable elementary particle, quantum of electromagnetic radiation.	rm-11-19	IEC 61223-2-10:1999
PHYSIOLOGICAL ALARM	Signal which either indicates that a monitored physiological parameter is out of the specified limits or indicates an abnormal PATIENT condition.		IEC 60601-2-23:1999 IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-49:2001 IEC 60601-2-51:2003
PHYSIOLOGICAL MONITORING UNIT	A part of the EQUIPMENT whose purpose is to collect information relating to (a) physiological function(s) and to process it for monitoring and summary diagnostic purposes.		IEC 60601-2-49:2001 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
PHYSICAL POINT SPREAD FUNCTION	For tomographs, a two-dimensional point function in planes perpendicular to the PROJECTION BEAM at specified distances from the detector. NOTE The PHYSICAL POINT SPREAD FUNCTION characterizes the purely physical imaging performance of the tomographic device independent from, e.g. sampling, image reconstruction and image processing, but dependent on the COLLIMATOR. A PROJECTION BEAM is characterized by the entirety of all PHYSICAL POINT SPREAD FUNCTIONS as a function of distance along its axis.		IEC 61675-1:1998 IEC 61675-2:1998
PHYSIOLOGICAL SIMULATION FREQUENCY	Fundamental frequency of a signal, electrical or non-electrical, used to simulate a physiological parameter such that the EQUIPMENT or SYSTEM will operate in a manner consistent with use on a PATIENT.		IEC 60601-1-2:2001
PILE UP EFFECT	False measurement of the PULSE amplitude, due to the ABSORPTION of two or more gamma rays, reaching the same RADIATION DETECTOR within the RESOLVING TIME.		IEC 61675-1:1998
PINHOLE CAMERA	Assembly of EQUIPMENT used to obtain a FOCAL SPOT PINHOLE RADIOGRAM on RADIOGRAPHIC FILM.	rm-71-02	IEC 60336:1993 IEC 61223-3-1:1999 IEC 61223-3-4:2000
PIN-HOLE COLLIMATOR	COLLIMATOR with one small aperture in a plane in front of the RADIATION DETECTOR ASSEMBLY.		IEC 60789:1992
PIXEL	MATRIX ELEMENT in a two-dimensional IMAGE MATRIX.	rm-32-60	IEC 61675-1:1998 IEC 61675-2:1998
PLAYBACK EQUIPMENT	EQUIPMENT for monitoring and documenting functions into which data from the RECORDER is fed. NOTE This EQUIPMENT is usually stationary and commonly includes computing facilities.		IEC 60601-2-47:2001
POINT SOURCE	RADIOACTIVE SOURCE approximating a δ -function in all three dimensions.	rm-34-36	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998 IEC 61948-2:2001
POINT SPREAD FUNCTION (PSF)	Normalized distribution of irradiance in the image of a POINT SOURCE, see ISO 9334.		IEC 61262-7:1995
POINT SPREAD FUNCTION (PSF)	Scintigraphic image of a POINT SOURCE. Recommended replacement: IEC 61262-7		IEC 61675-1:1998 IEC 61675-2:1998
PORTABLE EQUIPMENT	TRANSPORTABLE EQUIPMENT intended to be moved from one location to another while used or between periods of use while being carried by one or more persons.	NG.02.18	IEC 60601-1/A2:1995 IEC 60601-2-32:1994 IEC 60601-2-51:2003
PORTABLE EQUIPMENT	TRANSPORTABLE EQUIPMENT intended to be moved from one location to another while in use of between periods of use, by one or more persons or by other means. Recommended replacement: NG.02.18		IEC 60601-2-24:1998
POSITIONING DEVICE	Device which brings the calculi into coincidence with the TARGET LOCATION.		IEC 60601-2-36:1997
POSITIONING TIME	((see DETECTOR POSITIONING TIME))		IEC 61675-2:1998
POSITRON EMISSION TOMOGRAPH	Tomographic device, which detects the ANNIHILATION RADIATION of positron emitting RADIONUCLIDES by COINCIDENCE DETECTION.		IEC 61675-1:1998

Term	Definition	Reference	Used in IEC
POSITRON EMISSION TOMOGRAPHY (PET)	EMISSION COMPUTED TOMOGRAPHY utilizing the ANNIHILATION RADIATION of positron emitting RADIONUCLIDES by COINCIDENCE DETECTION.		IEC 61675-1:1998
POST-VENTRICULAR ATRIAL REFRACTORY PERIOD (PVARP)	Period after a ventricular event (whether sensed or paced), in which there is no sensing in the atrium.		IEC 60601-2-31/A1:1998
POST-VENTRICULAR ATRIAL REFRACTORY PERIOD (PVARP)	Period after a ventricular event (whether sensed or paced), during which synchronous ventricular pacing is disabled, regardless of any atrial event.		IEC 60601-2-31/A1:1998
POTENTIAL EQUALIZATION CONDUCTOR	Conductor providing a connection between EQUIPMENT and the potential equalization busbar of the electrical installation.	NG.06.06	IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
POWER SUPPLY	Any source of energy, other than that generated directly by the human body or by gravity, that makes the device function.		IEC 60601-2-13:2003
POWER SUPPLY CORD	Flexible cord, fixed to or assembled with EQUIPMENT for mains supply purposes	NG.07.17	IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
PRACTICAL PEAK VOLTAGE (PPV)	<p>The PRACTICAL PEAK VOLTAGE \hat{U} is defined as:</p> $\hat{U} = \frac{\int_{U_{\min}}^{U_{\max}} p(U) \cdot w(U) \cdot U dU}{\int_{U_{\min}}^{U_{\max}} p(U) \cdot w(U) dU} \quad \text{with} \quad \int_{U_{\min}}^{U_{\max}} p(U) dU = 1$ <p>where $p(U)$ is the distribution function for the voltage U and $w(U)$ is a weighting function. U_{\max} is the highest voltage in the interval, and U_{\min} is the lowest voltage in the interval. The unit of the quantity PRACTICAL PEAK VOLTAGE is the volt (V).</p> <p>NOTE Additional information on the PRACTICAL PEAK VOLTAGE, the weighting function $w(U)$ and the distribution function $p(U)$ is provided in Annex B. Using this weighting function $w(U)$ the PRACTICAL PEAK VOLTAGE will be defined as the constant potential which produces the same AIR KERMA contrast behind a specified PHANTOM as the non-dc voltage under test.</p>		IEC 61676:2002
PRACTICAL RANGE	For ELECTRON radiation, depth in a PHANTOM with its surface at the NORMAL TREATMENT DISTANCE, for which on the DEPTH DOSE chart the extrapolation of the steepest fall-off section of the ABSORBED DOSE distribution along the RADIATION BEAM AXIS intercepts the extrapolated tail of the ABSORBED DOSE distribution.		IEC 60976/ A1:2000

Term	Definition	Reference	Used in IEC
PREPARATORY STATE	State of EQUIPMENT for setting essential operating conditions, if in the STAND-BY STATE the setting of these conditions is not possible.	rm-84-04	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999
PRESSURE (overpressure)	PRESSURE above atmospheric (gauge pressure).	NG.11.04	IEC 60601-1/A2:1995 IEC 60601-2-28:1993 IEC 60601-2-33:2002 IEC 60601-2-44:2002
PRESSURE PULSE	Acoustic wave emitted by the LITHOTRIPSY EQUIPMENT.		IEC 60601-2-36:1997
PRESSURE PULSE COUPLING	Any means allowing transition of the PRESSURE PULSE from the EQUIPMENT into the PATIENT.		IEC 60601-2-36:1997
PRIMARY DOSE MONITORING SYSTEM	DOSE MONITORING SYSTEM which is intended to terminate IRRADIATION when a pre-selected value is reached.	rm-33-03	IEC 60601-2-1/A1:2002 IEC 60976/A1:2000
PRIMARY PROTECTIVE SHIELDING	PROTECTIVE SHIELDING for attenuating RESIDUAL RADIATION.	rm-64-02	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60601-2-45:2001
PRIMARY RADIATION	IONIZING RADIATION emitted directly by the TARGET or by a RADIOACTIVE SOURCE.	rm-11-06	IEC 60601-2-44:2002 IEC 60627:2001 IEC 61223-2-11:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
PRIMARY TIMER	The CONTROLLING TIMER which is intended to terminate IRRADIATION at the pre-selected time.		IEC 60601-2-11:1997
PRIMARY/SECONDARY (timer) COMBINATION	Combination of two timers in which one is arranged to be the PRIMARY TIMER and the other is to be the SECONDARY TIMER.	rm-21-11	IEC 60601-2-8:1999 IEC 60601-2-11:1997
PRIMARY/SECONDARY DOSE MONITORING COMBINATION	Utilization of two DOSE MONITORING SYSTEMS where one is arranged to be the PRIMARY and the other the SECONDARY DOSE MONITORING SYSTEM.	rm-33-17	IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999
PRIMARY-SECONDARY DOSE MONITORING SYSTEM	Combination of two DOSE MONITORING SYSTEMS in which one is arranged to be the PRIMARY DOSE MONITORING SYSTEM and the other is to be the SECONDARY DOSE MONITORING SYSTEM. Recommended replacement: PRIMARY/SECONDARY DOSE MONITORING COMBINATION		IEC 60976/A1:2000
PROCEDURE	Specific way to perform an ACTIVITY. [ISO 8402:1994, definition 1.3]		ISO 14971:2000
PROCESS	Set of inter-related resources and activities which transform inputs into outputs. [ISO 8402:1994, definition 1.2]		ISO 14971:2000
PROFILE PUMP	EQUIPMENT intended for controlled infusion of liquids into the PATIENT by means of a programmed sequence of delivery rates.		IEC 60601-2-24:1998

Term	Definition	Reference	Used in IEC
PROGRAMMABLE ELECTRICAL MEDICAL SYSTEM (PEMS)	MEDICAL ELECTRICAL EQUIPMENT or MEDICAL ELECTRICAL SYSTEM containing one or more PROGRAMMABLE ELECTRONIC SUBSYSTEM.	rm-80-04	IEC 60601-1-4:2000 IEC 62083:2000
PROGRAMMABLE ELECTRONIC SUBSYSTEM (PESS)	System based on one or more central processing units, including their software and interfaces.	rm-80-05	IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
PROGRAMMABLE ELECTRONIC SYSTEM (abbreviation: PES)	Term used to cover systems incorporating a wide range of programmable devices including microprocessors, programmable controllers, programmable logic controllers and other computer based devices. These devices may contain one or more central processing units connected to sensors and/or actuators, for the purpose of control, protection or monitoring.		IEC 60601-2-11:1997
PROJECTION	Transformation of a three-dimensional object into its two-dimensional image or of a two-dimensional object into its one-dimensional image, by integrating the physical property which determines the image along the direction of the PROJECTION BEAM. NOTE This process is mathematically described by line integrals in the direction of PROJECTION and called the Radon-transform.	rm-32-61	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
PROJECTION ANGLE	Angle at which the PROJECTION is measured or acquired.	rm-32-62	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
PROJECTION BEAM	Determines the smallest possible volume in which the physical property which determines the image is integrated during the measurement process. Its shape is limited by the SPATIAL RESOLUTION in all three dimensions. NOTE The PROJECTION BEAM mostly has the shape of a long thin cylinder or cone. In POSITRON EMISSION TOMOGRAPHY, it is the SENSITIVE VOLUME between two detector elements operated in coincidence.		IEC 61675-1:1998
PROJECTION BEAM	Determines the smallest possible volume in which the physical property which determines the image is integrated during the measurement process. Its shape is limited by the SPATIAL RESOLUTION in all three dimensions. NOTE In SPECT the PROJECTION BEAM usually has the shape of a long thin diverging cone. Recommended replacement: IEC 61675-1:1998		IEC 61675-2:1998
PROPERLY INSTALLED	Condition in which at least the relevant instructions concerning installation given by the MANUFACTURER in the ACCOMPANYING DOCUMENTS are observed.	NG.10.09	IEC 60601-1/A2:1995
PROTECTED AREA	Defined area within an area under surveillance or within a CONTROLLED AREA which is protected by STRUCTURAL SHIELDING or by distance so that the level of radiation is lower than is required for the total area of which it is a part.	rm-63-06	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60601-2-43:2000
PROTECTIVE BARRIER	PROTECTIVE SHIELDING in the form of attenuating material provided for RADIOLOGICAL PROTECTION.	rm-64-04	IEC 60601-2-45:2001

Term	Definition	Reference	Used in IEC
PROTECTIVE COVER	Part of an ENCLOSURE or guard provided to prevent accidental access to parts which might be hazardous if contacted.	NG.01.17	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
PROTECTIVE DEVICE	In RADIOLOGY, device for the purpose of RADIOLOGICAL PROTECTION. Thus: – protective clothing; – protective apron; – protective skirt; – protective glove; – mobile protective barrier.	rm-64-05	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 61223-1:1993 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998
PROTECTION DEVICE	No definition - Recommended replacement: rm-64-05	NG.09.08	IEC 60601-2-8:1999
PROTECTION DEVICE	Device which, without intervention of the OPERATOR, protects the PATIENT from hazardous output due to incorrect delivery of energy or substances. Recommended replacement: rm-64-05		IEC 60601-2-13:2003
PROTECTIVE EARTH CONDUCTOR	Conductor to be connected between the PROTECTIVE EARTH TERMINAL and an external protective earthing system.	NG.06.07	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
PROTECTIVE EARTH TERMINAL	Terminal connected to conductive parts of CLASS I EQUIPMENT for SAFETY purposes. This terminal is intended to be connected to an external protective earthing system by a PROTECTIVE EARTH CONDUCTOR.	NG.06.08	IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
PROTECTIVE GLASS PLATE	PROTECTIVE DEVICE of an optical quality suitable for transmitting visual images.		IEC 61331-2:1994
PROTECTIVE GLASS PLATE TYPE SC	PROTECTIVE GLASS PLATE of high optical quality with specified ATTENUATION properties used in DIRECT RADIOSCOPY for observation of the image in the FLUORESCENT SCREEN.		IEC 61331-2:1994
PROTECTIVE GLASS PLATE TYPE VI	PROTECTIVE GLASS PLATE of low optical quality with specified ATTENUATION properties used to provide optically clear and transparent PROTECTIVE SHIELDING.		IEC 61331-2:1994

Term	Definition	Reference	Used in IEC
PROTECTIVE GONAD APRON	Protective apron worn by the PATIENT to protect the region of the gonads as an alternative to the use of a SCROTUM SHIELD or an OVARY SHIELD; see rm-64-05 of IEC 60788.		IEC 61331-3:1998
PROTECTIVE MITTEN	Protective glove with open palm and separated thumb used where full perception of touch is essential.		IEC 61331-3:1998
PROTECTIVE SHIELDING	In RADIOLOGY, material that limits the extent of the RADIATION BEAM or attenuates STRAY RADIATION. NOTE PROTECTIVE SHIELDING may include materials provided for RADIOLOGICAL PROTECTION, or devices or materials provided for other purposes, which attenuate IONIZING RADIATION.	rm-64-01	IEC 60580:2000 IEC 60601-1-3:1994 IEC 61331-2:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997
PROTECTIVE SYSTEM	An automatic system which senses a specified parameter (or parameters), or a constructional feature, specifically designed to protect the PATIENT against SAFETY HAZARDS which may arise.		IEC 60601-2-16:1998 EC 60601-2-39:1999
PROTECTIVELY EARTHED	Connected to the PROTECTIVE EARTH TERMINAL for protective purposes by means complying with the requirements of this standard IEC 60601-1:1988.	NG.06.09	IEC 60601-1/A2:1995 IEC 60601-2-51:2003
PRUDENT-USE STATEMENT	Affirmation of the principle advising avoidance of primarily high EXPOSURE levels and secondarily long EXPOSURE times while acquiring necessary clinical information.		IEC 60601-2-37:2001
PUBLIC MAINS NETWORKS	LOW VOLTAGE electricity power lines to which all categories of consumers have access.		IEC 60601-1-2:2001
PULSE AMPLITUDE ANALYZER PULSE WINDOW	Range of input signal amplitudes for which the analyzer delivers an output signal.	rm-34-23	IEC 60789:1992 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998
PULSE BEAM-WIDTH	Distance between two points, on a specified surface in a specified direction passing through the point of maximum PULSE-PRESSURE-SQUARED INTEGRAL (p_i) in that surface, at which the PULSE-PRESSURE-SQUARED INTEGRAL is the specified fraction of the maximum value in that surface. Symbol: d_{-6} (for PULSE BEAM-WIDTH defined at -6 dB). Unit: centimetres, cm.		IEC 60601-2-37:2001
PULSE DURATION	Time interval beginning at the first time the pressure amplitude exceeds a REFERENCE VALUE and ending at the last time the pressure amplitude returns to that value. The REFERENCE VALUE is equal to the sum of the minimum pressure amplitude and 10 % of the difference between the maximum and minimum pressure amplitude. [IEC 61689, definition 3.35] NOTE The above definition from IEC 61689 differs from that of 3.30 of IEC 61102 to account for incomplete modulation.		IEC 60601-2-5:2000
PULSE DURATION	The duration of the output PULSE WAVEFORM at 50 % of the maximum amplitude.		IEC 60601-2-10 /A1:2001
PULSE DURATION	1,25 times the interval between the time when the time integral of intensity in an acoustic PULSE at a point reaches 10 % and when it reaches 90 % of the PULSE-INTENSITY INTEGRAL. Symbol: t_d . Unit: seconds, s.		IEC 60601-2-37:2001
PULSE DURATION	The duration of the electrical stimulus pulse WAVEFORM at 50 % of the peak amplitude.		IEC 60601-2-40:1998
PULSE REPETITION PERIOD	Absolute value of the time interval after which the same characteristics of a periodic WAVEFORM recur (see 5.3.2.1 of IEC 60469-1). [IEC 61689, definition 3.36]		IEC 60601-2-5:2000
PULSE REPETITION RATE	Inverse of the time interval between two successive acoustic PULSES. Symbol: p_{rr} . Unit: hertz, Hz.		IEC 60601-2-37:2001

Term	Definition	Reference	Used in IEC
PULSE-AVERAGE INTENSITY	Ratio of the PULSE-INTENSITY INTEGRAL I_{pi} to the PULSE DURATION t_d . Symbol: I_{pa} . Unit: watts per square centimetre, $W\ cm^{-2}$.		IEC 60601-2-37:2001
PULSE-INTENSITY INTEGRAL	Time integral of instantaneous intensity at a particular point in an acoustic field integrated over the acoustic PULSE WAVEFORM. Symbol: I_{pi} . Unit: millijoules per centimetre squared, mJ/cm^2 .		IEC 60601-2-37:2001
PULSE-PRESSURE-SQUARED INTEGRAL	Time integral of the square of the instantaneous acoustic pressure at a particular point in an acoustic field integrated over the acoustic PULSE WAVEFORM. Symbol: p_i . Unit: Pascal squared second, Pa^2s .		IEC 60601-2-37:2001
QUALIFIED PERSON	Person recognized by a competent authority as having the requisite knowledge and training to perform specified duties.	rm-85-04	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 62083:2000
QUALIFIED PERSON	Person competent in any relevant discipline by virtue of his training, knowledge and experience to perform required duties.		IEC 60601-2-17 /A1:1996
QUALITY ASSURANCE	Planned and systematic actions necessary to provide adequate confidence by ensuring that a product or service will satisfy given requirements for quality.	rm-70-05	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999
QUALITY ASSURANCE PROGRAMME	Detailed instruction for carrying out actions of QUALITY ASSURANCE for individual items of EQUIPMENT, systems of EQUIPMENT or facilities, including quality administrative elements and quality control techniques.	rm-70-06	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
QUALITY CONTROL	Operational techniques and activities that are used to fulfil requirements for quality.	rm-70-07	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999
QUALITY CONTROL	Part of the QUALITY ASSURANCE in nuclear medicine including tests of instruments with appropriate test methods. NOTE Includes both ACCEPTANCE TESTING and ROUTINE TESTING.		IEC 61948-1:2001

Term	Definition	Reference	Used in IEC
QUALITY EQUIVALENT FILTRATION	Quantitative indication of the FILTRATION effected by one or several layer(s) of reference material(s) which, if substituted in a beam of specified RADIATION QUALITY under NARROW BEAM CONDITION for the material under consideration, give(s) the same RADIATION QUALITY as gives the material under consideration. The QUALITY EQUIVALENT FILTRATION is expressed in suitable submultiples of the metre together with the reference material(s) and the RADIATION QUALITY of the incident beam.	rm-13-45	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61267:1994
QUALITY EQUIVALENT FILTRATION	Quantity indicating for a material or an object the effect of its FILTRATION, expressed as the thickness of a particular reference material, whose FILTRATION is found to have the same effect on RADIATION QUALITY under specific conditions of measurement. Recommended replacement: rm-13-45		IEC 60580:2000
QUANTITY INDEX	For X-RADIATION, the ratio of the ABSORBED DOSE measured at a depth of 20 cm to that measured at a depth of 10 cm. The detector is at the NORMAL TREATMENT DISTANCE. The measurement is made in a PHANTOM on the RADIATION BEAM AXIS for a RADIATION FIELD of 10 cm x 10 cm.		IEC 60976 /A1:2000
QUANTUM ABSORPTION EFFICIENCY	The number of PHOTONS incident at the input of a RADIATION DETECTOR that yield a signal at the output of the RADIATION DETECTOR divided by the total number of incident PHOTONS.		IEC 61262-5:1994
QUENCH	Transition of the electrical conductivity of a coil that is carrying a current from a superconducting state to normal conductivity, resulting in rapid boil-off of fluid cryogen and decay of the magnetic field.		IEC 60601-2-33:2002
RADIATION SOURCE TO SKIN DISTANCE	In RADIOTHERAPY, distance from the surface of the RADIATION source to the ENTRANCE SURFACE.	rm-37-14	IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997
RADIATION SPECTRUM	Distribution of a RADIATION QUANTITY with respect to RADIATION energy. Thus: – X-ray spectrum; – gamma-ray spectrum.	rm-13-34	IEC 60601-2-28:1993 IEC 60627:2001 IEC 60976 /A1:2000 IEC 61223-2-11:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61267:1994
RADIATION TYPE	Nature of the waves or corpuscles comprising the RADIATION, for example whether the RADIATION is X-RADIATION or ELECTRON RADIATION.	rm-11-23	IEC 60601-2-1/A1:2002 IEC 60976 /A1:2000
RADIAL RESOLUTION	TRANSVERSE RESOLUTION along a line passing through the position of the source and the SYSTEM AXIS.	rm-34-37	IEC 61675-1:1998 IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
RADIATION	<p>Propagation of emitted energy through space or through a material medium in the form of waves or in the form of kinetic energy of particles.</p> <p>NOTE When unqualified, the term RADIATION usually refers</p> <ul style="list-style-type: none"> – to electromagnetic radiations according to frequency or origin such as: radiofrequency radiation, infra-red radiation, visible radiation (light), ultraviolet radiation, X-radiation, gamma radiation; – to corpuscular radiations according to particles or origin such as: alpha radiation, beta radiation, ELECTRON radiation, NEUTRON radiation. 	rm-11-01	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60806:1984 IEC 60976 /A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-3:1998 IEC 62083:2000
RADIATION APERTURE	Aperture in the PROTECTIVE SHIELDING of a RADIATION SOURCE or in a beam limiting device, that is intended to give passage to the RADIATION BEAM.	rm-37-26	IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 61223-3-1:1999

Term	Definition	Reference	Used in IEC
RADIATION BEAM	<p>In RADIOLOGY, spatial region limited in solid angle and containing a flux of IONIZING RADIATION originating from a RADIATION SOURCE that is considered as a POINT SOURCE. Leakage radiation and SCATTERED RADIATION are considered not to form a RADIATION BEAM.</p> <p>Thus:</p> <ul style="list-style-type: none"> - X-ray beam; - gamma-ray beam; - ELECTRON beam; - NEUTRON beam. 	rm-37-05	<p>IEC 60522:1999</p> <p>IEC 60601-1-3:1994</p> <p>IEC 60601-2-1/A1:2002</p> <p>IEC 60601-2-7:1998</p> <p>IEC 60601-2-8:1999</p> <p>IEC 60601-2-11:1997</p> <p>IEC 60601-2-32:1994</p> <p>IEC 60601-2-43:2000</p> <p>IEC 60601-2-44:2002</p> <p>IEC 60601-2-45:2001</p> <p>IEC 60627:2001</p> <p>IEC 60806:1984</p> <p>IEC 60976/ A1:2000</p> <p>IEC 61217:2002</p> <p>IEC 61223-2-4:1994</p> <p>IEC 61223-2-5:1994</p> <p>IEC 61223-2-6:1994</p> <p>IEC 61223-2-7:1999</p> <p>IEC 61223-2-9:1999</p> <p>IEC 61223-2-10:1999</p> <p>IEC 61223-2-11:1999</p> <p>IEC 61223-3-1:1999</p> <p>IEC 61223-3-2:1996</p> <p>IEC 61223-3-3:1996</p> <p>IEC 61223-3-4:2000</p> <p>IEC 61262-2:1994</p> <p>IEC 61262-3:1994</p> <p>IEC 61262-5:1994</p> <p>IEC 61262-6:1994</p> <p>IEC 61267:1994</p> <p>IEC 61331-1:1994</p> <p>IEC 61331-3:1998</p> <p>IEC 62083:2000</p>

Term	Definition	Reference	Used in IEC
RADIATION BEAM AXIS	<p>For a symmetrical RADIATION BEAM, line through the centre of the RADIATION SOURCE and half way between the effective edges of the beam limiting device. Usually, the RADIATION BEAM AXIS coincides within required tolerances with the REFERENCE AXIS of the RADIATION SOURCE.</p> <p>Thus:</p> <ul style="list-style-type: none"> – X-ray beam axis; – gamma-ray beam axis; – NEUTRON beam axis; – ELECTRON beam axis. 	rm-37-06	IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-2-7:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61267:1994
RADIATION CONDITION	<p>Description of RADIATION FIELDS by a set of electrical and geometrical parameters like X-RAY TUBE VOLTAGE, TOTAL FILTRATION and geometrical arrangements.</p> <p>NOTE The term RADIATION CONDITION refers to a description of RADIATION FIELDS and not to a particular set-up for testing of EQUIPMENT.</p>	rm-13-59	IEC 60627:2001 IEC 61267:1994
RADIATION DETECTOR	EQUIPMENT, generally sub-assembly, or substance which, in the presence of radiation, provides by either direct or indirect means a signal or other indication suitable for use in measuring one or more quantities of the incident radiation.	rm-51-01	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60976/ A1:2000 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
RADIATION DETECTOR	<p>Element which transduces AIR KERMA, AIR KERMA length or AIR KERMA RATE into a measurable electrical signal. It may be either an IONIZATION CHAMBER or a semi-conductor detector:</p> <p>1) IONIZATION CHAMBER: Ionization detector consisting of a CHAMBER filled with air, in which an electric field insufficient to induce gas multiplication is provided for the collection, at the ELECTRODES, of charges associated with the ions and ELECTRONS produced in the SENSITIVE VOLUME of the detector by IONIZING RADIATION. The CHAMBER is constructed in such a way as to allow the air inside the measuring volume to communicate freely with the atmosphere so that corrections to the RESPONSE for changes in air density need to be made.</p> <p>2) Vented CHAMBER: An IONIZATION CHAMBER constructed in such a way as to allow the air inside the measuring volume to communicate freely with the atmosphere so that corrections to the RESPONSE for changes in air density need to be made.</p> <p>NOTE Sealed CHAMBERS are not suitable, because the necessary wall thickness of a sealed CHAMBER may cause an unacceptable energy dependence of the RESPONSE and because the long term stability of sealed CHAMBERS is not guaranteed.</p> <p>3) Semi-conductor detector: Either a) and/or b):</p> <p>a) semi-conductor device operating in the shorted junction mode that utilizes the production and motion of excess free charge carriers in the semi-conductor for the detection and measurement of incident IONIZING RADIATION;</p> <p>b) scintillator material optionally coupled to a semi-conductor photodiode operating in the shored junction mode, in which assembly incident IONIZING RADIATION is first converted to light and then to an electrical signal.</p> <p>Recommended replacement: rm-51-01</p>		IEC 61674 /A1:2002
RADIATION DETECTOR	<p>For this standard IEC 60601-2-9:1996 this is defined as the electrically operated element which directly transduces ABSORBED DOSE, ABSORBED DOSE RATE or any other dose related quantity into a measurable electrical signal.</p> <p>Recommended replacement: rm-51-01</p>		IEC 60601-2-9:1996
RADIATION DETECTOR ASSEMBLY	<p>In a RADIONUCLIDE imaging device, assembly with one or more RADIATION DETECTORS the electrical output signals of which are used to form a RADIOLOGICAL IMAGE .</p>	rm-34-11	IEC 60601-2-9:1996 IEC 60789:1992 IEC 61675-3:1998
RADIATION ENERGY	<p>In RADIOLOGY, quantity indicating the energy that a PHOTON or other particle is carrying, except its rest energy. The unit of RADIATION ENERGY is the ELECTRONVOLT (eV), 1 eV being equal to $1,60219 \times 10^{-19}$ J.</p> <p>Thus:</p> <ul style="list-style-type: none"> - X-ray energy; - gamma ray energy. 	rm-13-29	IEC 60613:1989 IEC 60601-2-29:1999 IEC 60976/ A1:2000 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
RADIATION FIELD	<p>Area on a surface intersected by a RADIATION BEAM within which the radiation intensity exceeds a specific or specified level.</p> <p>Thus:</p> <ul style="list-style-type: none"> - X-ray field; - gamma-ray field; - ELECTRON field; - NEUTRON field. 	rm-37-07	IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-11:1997 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60806:1984 IEC 60976 /A1:2000 IEC 61217:2002 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61267:1994 IEC 62083:2000
RADIATION HEAD	Structure from which the RADIATION BEAM emerges.	rm-20-06	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60976/ A1:2000 IEC 61217:2002

Term	Definition	Reference	Used in IEC
RADIATION METER	<p>In RADIOLOGY, assembly designed to measure quantities concerned with IONIZING RADIATION (ACTIVITY, EXPOSURE RATE, etc.), and including one or several RADIATION DETECTORS and associated sub-assemblies or basic function units.</p> <p>Thus:</p> <ul style="list-style-type: none"> – kermameter; – KERMA ratemeter; – area KERMA product meter; – EXPOSURE METER; – EXPOSURE ratemeter; – area EXPOSURE product meter. 	rm-50-01	<p>IEC 60601-2-9:1996 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000</p>
RADIATION OUTPUT	AIR KERMA per CURRENT TIME PRODUCT (mGy/mAs) at a given distance from the FOCAL SPOT in the primary X-ray beam.	rm-13-57	<p>IEC 61223-3-1:1999 IEC 61223-3-4:2000</p>
RADIATION PROTECTION	<p>Limitation to an acceptable level of:</p> <ul style="list-style-type: none"> – radiation hazard; – damage to material attributable to radiation. 	rm-60-02	<p>IEC 60601-1-3:1994 IEC 60601-2-11:1997 IEC 60601-2-43:2000 IEC 61331-2:1994</p>
RADIATION QUALITY	<p>Characteristic of IONIZING RADIATION determined by the spectral distribution of a RADIATION QUANTITY with respect to RADIATION ENERGY.</p> <p>NOTE For various purposes concerning X-RADIATION, practical approximations of RADIATION QUALITY are expressed in terms of variables such as:</p> <ul style="list-style-type: none"> a) HIGH VOLTAGE with PERCENTAGE RIPPLE and TOTAL FILTRATION; b) first HALF-VALUE LAYER for specified HIGH VOLTAGE with its PERCENTAGE RIPPLE; c) first HALF-VALUE LAYER and TOTAL FILTRATION; d) the first HALF-VALUE LAYER and the quotient of the first HALF-VALUE LAYER by the second HALF-VALUE LAYER; e) equivalent energy. 	rm-13-28	<p>IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60806:1984 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61331-1:1994 IEC 61331-2:1994 IEC 62083:2000</p>

Term	Definition	Reference	Used in IEC
RADIATION QUALITY	RADIATION CONDITION whereby the RADIATION FIELD only comprises an insignificant amount of SCATTERED RADIATION. NOTE This definition takes preference over that given in IEC 60788.		IEC 60627:2001 IEC 61267:1994
RADIATION QUALITY	For a specific type of radiation, the description of any characteristic that depends on its energy spectrum. NOTE For the purposes of this international standard, a practical approximation of RADIATION QUALITY is expressed as the quotient of the first HALF-VALUE LAYER and the second HALF-VALUE LAYER. Recommended replacement: rm-13-28		IEC 60580:2000
RADIATION QUANTITIES AND UNITS	This collateral standard IEC 60601-1-3:1994 uses the quantity AIR KERMA in preference to EXPOSURE. The unit of AIR KERMA is the gray (Gy). An AIR KERMA of 1 Gy corresponds to an EXPOSURE of $2,97 \times 10^{-2}$ C kg ⁻¹ .		IEC 60601-1-3:1994
RADIATION QUANTITY	Letter symbol: Φ . At a given point of space, the number dN of particles incident during a given time interval on a suitably small sphere centred at that point divided by the cross-sectional area da of the sphere. $\Phi = \frac{dN}{da}$	rm-13-01	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 61331-1:1994
RADIATION QUANTITY FOR NOMINAL SHORTEST IRRADIATION TIME	The definition of NOMINAL SHORTEST IRRADIATION TIME refers to a required constancy of a RADIATION QUANTITY. In this standard the RADIATION QUANTITY concerned is AIR KERMA.	rm-13-58	IEC 60601-2-7:1998 IEC 60601-2-45:2001
RADIATION SOURCE	RADIOACTIVE SOURCE or part of EQUIPMENT capable of emitting IONIZING RADIATION.	rm-20-01	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60976 /A1:2000 IEC 61217:2002 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-3:1998 IEC 62083:2000

Term	Definition	Reference	Used in IEC
RADIATION SOURCE ASSEMBLY	<p>Assembly of components comprising:</p> <ul style="list-style-type: none"> – the RADIATION SOURCE, – the means providing protection against IONIZING RADIATION and, where applicable, against electric shock, – the BEAM LIMITING SYSTEM. <p>Thus:</p> <ul style="list-style-type: none"> – X-ray source assembly; – gamma-ray source assembly; – RADIONUCLIDE source assembly. 	rm-20-05	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60806:1984 IEC 61223-1:1993 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994
RADIO FREQUENCY (RF)	<p>Frequency in the portion of the electromagnetic spectrum that is between the audio-frequency portion and the infrared portion; frequency useful for radio transmission.</p> <p>NOTE The limits are generally accepted to be 9 kHz to 3 000 GHz.</p>		IEC 60601-1-2:2001
RADIOACTIVE HALF-LIFE	<p>Letter symbol: T. For a single radioactive decay process, the time required for the ACTIVITY to decrease to half its value.</p> <p>NOTE For a RADIONUCLIDE, the RADIOACTIVE HALF-LIFE T is related to the decay constant λ by the expression:</p> $T = \frac{L_n 2}{\lambda} = \frac{0,693}{\lambda}$	rm-13-20	IEC 61675-1:1998 IEC 62083:2000
RADIOACTIVE IMPURITY	RADIONUCLIDES in a RADIOACTIVE SOURCE other than the principal RADIONUCLIDE.		IEC 61303:1994
RADIOACTIVE SOURCE	Quantity of radioactive material having both an ACTIVITY and a specific ACTIVITY above specific levels.	rm-20-02	IEC 60601-2-17/A1:1996 IEC 61303:1994 IEC 61675-1:1998 IEC 61675-2:1998 IEC 62083:2000
RADIOACTIVE SOURCE TRAIN	A sequence of SEALED RADIOACTIVE SOURCES, possibly separated by non-radioactive spacers, either permanently combined or selected prior to each IRRADIATION, and used in AFTERLOADING EQUIPMENT. The RADIOACTIVE SOURCE TRAIN is usually selected to give a specified dose distribution.		IEC 60601-2-17/A1:1996

Term	Definition	Reference	Used in IEC
RADIOACTIVE STANDARD SOURCE	General term used to refer to the standard sources listed below.		IEC 61303:1994
RADIOACTIVITY	Property of certain nuclides of spontaneously emitting particles or gamma radiation, or of emitting X-RADIATION following orbital ELECTRON capture or of undergoing spontaneous fission.	rm-12-13	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 61303:1994
RADIOGRAM	In RADIOLOGY, RECORD of an X-RAY PATTERN.	rm-32-02	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60806:1984 IEC 60976/ A1:2000 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 62083:2000

Term	Definition	Reference	Used in IEC
RADIOGRAPHIC CASSETTE	Light-tight receptacle with a radiation-transparent front cover, intended to house one or more stationary RADIOGRAPHIC FILMS, usually with one or more INTENSIFYING SCREENS.	rm-35-14	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 60806:1984 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-6:1994 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61331-2:1994
RADIOGRAPHIC CASSETTE HOLDER	Recommendation: Do not use as defined term Reason: Self-explaining, in none of the 4 standards applying the term is a definition missed by the reader.	rm-35-18	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 61217:2002 IEC 61223-2-10:1999

Term	Definition	Reference	Used in IEC
RADIOGRAPHIC FILM	Sheet or roll material consisting of a transparent carrier covered with radiation-sensitive emulsion on one or usually both sides and designed for use in DIRECT RADIOGRAPHY.	rm-32-32	IEC 60336:1993 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-45:2001 IEC 60806:1984 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61331-2:1994
RADIOGRAPHIC RATING	For the operation of an X-RAY TUBE, specified combination of conditions and LOADING FACTORS, under which the specified limits of loadability of the X-RAY TUBE are attained.	rm-36-36	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-28:1993 IEC 60601-2-45:2001 IEC 60613:1989
RADIOGRAPHY	Technique for obtaining, recording, and optionally processing directly or after TRANSFER, information contained in an X-RAY PATTERN at an IMAGE RECEPTION AREA.	rm-41-06	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 61223-1:1993 IEC 61223-2-7:1999 IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000

Term	Definition	Reference	Used in IEC
RADIOLOGICAL	Referring to IONIZING RADIATION, its generation and application for scientific, medical and technical purposes.	rm-40-02	IEC 60601-1-3:1994 IEC 60601-2-11:1997 IEC 60601-2-43:2000 IEC 61223-2-10:1999 IEC 61331-3:1998
RADIOLOGICAL EQUIPMENT	EQUIPMENT designed for use in RADIOLOGY.	rm-20-19	IEC 61331-2:1994
RADIOLOGICAL INSTALLATION	Installed RADIOLOGICAL EQUIPMENT including all means for its intended operation. Thus: – gamma-ray installation; – X-ray installation (IEC 60613:1989) (IEC 61223-1:1993).	rm-20-24	IEC 60613:1989 IEC 61223-1:1993 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61331-2:1994
RADIOLOGICAL IMAGE	Information obtained by using IONIZING RADIATION presented as an image suitable for medical diagnosis.	rm-32-05	IEC 61223-2-1:1993 IEC 61675-3:1998
RADIOLOGICAL PROTECTION	RADIATION PROTECTION with respect to IONIZING RADIATION.	rm-60-03	IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001
RADIOLOGY	Science of IONIZING RADIATION and its application.	rm-40-01	IEC 61223-2-10:1999 IEC 61223-3-1:1999 IEC 61267:1994
RADIOMETRIC PARAMETERS	NOTE See IEC 60050(845).		IEC 60601-2-50:2000

Term	Definition	Reference	Used in IEC
RADIONUCLIDE	Radioactive nuclide.	rm-11-22	IEC 60601-2-11:1997 IEC 60601-2-17 /A1:1996 IEC 61303:1994 IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998 IEC 61948-1:2001 IEC 61948-2:2001 IEC 62083:2000
RADIONUCLIDE BEAM THERAPY EQUIPMENT	Thus: – gamma beam therapy EQUIPMENT.	rm-24-01	IEC 60601-2-11:1997 IEC 61217:2002 IEC 62083:2000
RADIONUCLIDE CALIBRATOR	Device for measuring the ACTIVITY of a radioactive sample.		IEC 61303:1994
RADIONUCLIDE FACTOR	Factor, dependent on the RADIONUCLIDE, by which the RESPONSE of the system must be multiplied in order to obtain the correct ACTIVITY reading of a source which has been placed in the IONIZATION CHAMBER.		IEC 61303:1994
RADIOSCOPIC SCREEN	FLUORESCENT SCREEN used for DIRECT RADIOSCOPY.	rm-32-31	IEC 60601-1-3:1994
RADIOSCOPICALLY GUIDED INVASIVE PROCEDURE	Invasive procedure (involving the introduction of a device, such as a needle or a catheter into the body of the PATIENT) using radioscopic imaging as the principal means of guidance.		IEC 60601-2-43:2000
RADIOSCOPICALLY GUIDED INTERVENTIONAL PROCEDURE	RADIOSCOPICALLY GUIDED INVASIVE PROCEDURES intended to effect TREATMENT on the medical condition of the PATIENT.	rm-31-12	IEC 60601-2-43:2000
RADIOSCOPY	Technique for obtaining continuously or periodically a sequence of X-RAY PATTERNS and presenting them simultaneously and continuously as visible images.	rm-41-01	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-9:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61223-3-4:2000

Term	Definition	Reference	Used in IEC
RADIOTHERAPY	Medical therapy essentially consisting of one or more TREATMENTS by IONIZING RADIATION.	rm-40-05	IEC 60522:1999 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-9:1996 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60976 /A1:2000 IEC 61217:2002 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 62083:2000
RADIOTHERAPY SIMULATOR	An EQUIPMENT which uses X-RAY EQUIPMENT to simulate physically a therapeutic RADIATION BEAM so that the TREATMENT VOLUME to be irradiated during RADIOTHERAPY can be localized and the size of the therapeutic RADIATION FIELD can be confirmed. Recommended replacement: IEC 60601-2-29		IEC 61217:2002
RADIOTHERAPY SIMULATOR	EQUIPMENT that uses X-RAY EQUIPMENT to simulate geometrically parameters of movements and RADIATION FIELDS of RADIOTHERAPY equipment so as to assist with the planning of PATIENT TREATMENTS.		IEC 60601-2-29:1999
RADIOTHERAPY TREATMENT PLANNING SYSTEM (RTPS)	A device, usually a PROGRAMMABLE ELECTRONIC SYSTEM including its associated peripherals, that is used to simulate the application of radiation to a PATIENT for a proposed RADIOTHERAPY TREATMENT. It usually, but not necessarily, provides estimations of ABSORBED DOSE distribution in human tissue using a particular algorithm or algorithms. These algorithms provide simulations of radiation that is typically from, but not necessarily limited to, medical ELECTRON accelerators, gamma beam therapy EQUIPMENT or RADIOACTIVE SOURCES when brachytherapy is planned.		IEC 62083:2000
RADIUS OF ROTATION	Distance between the SYSTEM AXIS and the COLLIMATOR FRONT FACE.	rm-34-38	IEC 61675-2:1998 IEC 61948-2:2001
RANDOM COINCIDENCE	Result of COINCIDENCE DETECTION in which both participating PHOTONS emerge from different positron annihilations.		IEC 61675-1:1998
RANDOM UNCERTAINTY	Observed standard deviation of a set of repeated MEASURED VALUES.		IEC 61303:1994
RATED (value)	Value assigned by the MANUFACTURER to a quantity characteristic of the EQUIPMENT.	NG.12.08	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001
RATED FIELD SIZE	Size of the USEFUL BEAM at the IONIZATION CHAMBER within which the IONIZATION CHAMBER performs to its specification.		IEC 60580:2000
RATED LENGTH	Length along the axis of the CT DETECTOR within which the detector performs to its specification.		IEC 61674 /A1:2002
RATED LOAD	The value of non-reactive load resistance that results in the maximum HFOUTPUT POWER from each operating mode of the HF SURGICAL EQUIPMENT.		IEC 60601-2-2:1998

Term	Definition	Reference	Used in IEC
RATED OUTPUT POWER	The power in watts produced when the HF output is fed into the RATED LOAD.		IEC 60601-2-2:1998
RATED OUTPUT POWER	Maximum radio-frequency power assigned by the MANUFACTURER, averaged over a period of 1 s, which can be delivered to the load specified in Clause 50.		IEC 60601-2-3 /A1:1998
RATED OUTPUT POWER	Maximum OUTPUT POWER of the EQUIPMENT at any RATED MAINS VOLTAGE. [IEC 61689, definition 3.32]		IEC 60601-2-5:2000
RATED OUTPUT POWER	Value of the maximum high-frequency power averaged over at least 1 s which can be fed into a MATCHED LOAD.		IEC 60601-2-6:1984
RATED RANGE (of use)	Range of values of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER within which the instrument will operate within the LIMITS OF VARIATION. Its limits are the maximum and minimum RATED values. NOTE The EFFECTIVE RANGE of use is referred to as RATED RANGE in this standard.		IEC 60580:2000
RATED RANGE (of use)	Range of values of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER within which the instrument will operate within the LIMITS OF VARIATION. Its limits are the maximum and minimum RATED values. NOTE Referred to as RATED RANGE in this standard IEC 60731/A1:2002.		IEC 60731/A1:2002 IEC 61674/A1:2002
RATED RANGE (of use)	The range of values of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER within which the instrument will operate within the LIMITS OF VARIATION. Its limits are the maximum and minimum RATED values. The minimum RATED RANGE is the least range of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER within which the instrument shall operate within the specified LIMITS OF VARIATION in order to comply with this standard IEC 61676:2002 Recommended replacement: IEC 61674, IEC 60731		IEC 61676:2002
READY STATE	State of EQUIPMENT in which all conditions, such as carrying out of confirming operations and any other satisfaction of INTERLOCKS are prevailing so that the intended operation of such EQUIPMENT can be initiated by a single action.	rm-84-05	IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-17 /A1:1996 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976 /A1:2000
RECONSTRUCTIVE TOMOGRAPHY	TOMOGRAPHY in which information obtained from the object is recorded for constructing images of layers in the object by processing.	rm-41-19	IEC 60336:1993 IEC 60601-2-7:1998 IEC 61223-1:1993 IEC 61223-2-1:1993
RECORD	Document which furnishes objective evidence of activities performed or results achieved. [ISO 8402:1994, definition 3.15]		ISO 14971:2000
RECORDING ELECTROCARDIOGRAPH	MEDICAL ELECTRICAL EQUIPMENT intended for the production of ECG RECORDS.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
RECOVERY COEFFICIENT	Measured (image) ACTIVITY concentration of an active volume divided by the true ACTIVITY concentration of that volume, neglecting ACTIVITY CALIBRATION FACTORS. NOTE For the actual measurement, the true ACTIVITY concentration is replaced by the measured ACTIVITY concentration in a large volume.		IEC 61675-1:1998
REDUNDANT (timer) COMBINATION	Combination of two CONTROLLING TIMERS in which both are arranged to terminate IRRADIATION at the pre-selected time.	rm-33-13	IEC 60601-2-8:1999 IEC 60601-2-11:1997
REDUNDANT DOSE MONITORING SYSTEMS	Utilization of two DOSE MONITORING SYSTEMS where both systems are arranged to terminate IRRADIATION according to the pre-selected number of dose monitoring units.	rm-33-14	IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999
REDUNDANT DOSE MONITORING COMBINATION	Combination of two DOSE MONITORING SYSTEMS in which both systems are arranged to terminate IRRADIATION according to the preselected number of DOSE MONITOR UNITS. Recommended replacement: REDUNDANT DOSE MONITORING COMBINATION		IEC 60976/ A1:2000
REFERENCE AIR KERMA	AIR KERMA of the primary X-ray beam measured under specific conditions and expressed as an equivalent value at the interventional reference point. REFERENCE AIR KERMA RATE, AIR KERMA RATE expressed as above. REFERENCE AIR KERMA (rate), used for brevity where either REFERENCE AIR KERMA OR REFERENCE AIR KERMA RATE apply, according to the context.		IEC 60601-2-43:2000
REFERENCE AXIS	For a RADIATION SOURCE, line in the REFERENCE DIRECTION through the centre of the RADIATION SOURCE.	rm-37-03	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60806:1984 IEC 60976/A1:2000 IEC 61217:2002 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
REFERENCE CONDITIONS	Conditions under which all INFLUENCE QUANTITIES and INSTRUMENT PARAMETERS have their REFERENCE VALUES.	rm-70-12	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 /A1:2002 IEC 61676:2002
REFERENCE DATA	A set of data measured immediately after ACCEPTANCE TESTING, using test methods designed for ROUTINE TESTING.		IEC 61948-1:2001 IEC 61948-2:2001

Term	Definition	Reference	Used in IEC
REFERENCE DIRECTION	For a RADIATION SOURCE, specified direction to which characteristics such as TARGET ANGLE, RADIATION FIELD, and specifications with respect to the imaging quality of the RADIATION SOURCE, are referenced.		IEC 60336:1993 IEC 60806:1984 IEC 61223-2-11:1999 IEC 61267:1994
REFERENCE INDICATED VALUE	The INDICATED VALUE at which the CALIBRATION FACTOR of an instrument is determined.		IEC 60731/A1:2002
REFERENCE PLANE	In diagnostic X-RAY EQUIPMENT for an EFFECTIVE FOCAL SPOT, plane perpendicular to the REFERENCE DIRECTION containing the point at which the REFERENCE AXIS intersects with the ACTUAL FOCAL SPOT. By convention, the point of intersection forms the centre of the EFFECTIVE FOCAL SPOT.	rm-37-04	IEC 60336:1993 IEC 60601-2-44:2002
REFERENCE POINT ACCORDING TO GOLDBERGER	Reference point at an average potential of two limbs (e.g. average of L and F).		IEC 60601-2-51:2003
REFERENCE POINT (of a CHAMBER)	Point of an IONIZATION CHAMBER, which during the calibration of the CHAMBER, is brought to coincidence with the point at which the CONVENTIONAL TRUE VALUE is specified.		IEC 60731/A1:2002 IEC 61267:1994
REFERENCE POINT (of a RADIATION DETECTOR)	Point of a RADIATION DETECTOR which, during the calibration of the detector, is brought to coincidence with the point at which the CONVENTIONAL TRUE VALUE is specified.		IEC 61674/A1:2002
REFERENCE SCALE READING	The SCALE READING corresponding to the REFERENCE INDICATED VALUE		IEC 60731/A1:2002
REFERENCE VALUE	Particular value of an INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) chosen for the purpose of reference, i.e. the value of an INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) at which the CORRECTION FACTOR for dependence on that INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) is unity.	rm-72-06	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/A1:2002
REFERENCE VALUE	Particular value of an INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) chosen for the purposes of reference i.e. the value of an INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) at which the CORRECTION FACTOR for dependence on that INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) is unity. Recommended replacement: rm-72-06		IEC 61676:2002
REFERENCE VOLUME	Volume throughout which the RADIONUCLIDE of a RADIOACTIVE STANDARD SOURCE is distributed.		IEC 61303:1994
REFERENCE-CLASS DOSIMETER	DOSIMETER whose performance and stability are sufficient for it to be used to calibrate other DOSIMETERS.		IEC 60731/A1:2002
REGION OF CONTROL	That part of the EQUIPMENT within which flow regulation, flow shut-off or air detection occurs, within the body of the EQUIPMENT or remotely.		IEC 60601-2-24:1998
REGION OF INTEREST (ROI)	Localized part of an image, which is of particular interest at a given time.	rm-32-63	IEC 61223-2-6:1994 IEC 61223-3-1:1999
REINFORCED INSULATION	Single insulation system applied to LIVE parts which provides a degree of protection against electric shock equivalent to DOUBLE INSULATION under the conditions specified in this standard IEC 60601-1:1995.	NG.03.07	IEC 60601-1/A2:1995 IEC 60601-2-51:2003
RELATIVE INTRINSIC ERROR	Ratio of the INTRINSIC ERROR to the CONVENTIONAL TRUE VALUE.	rm-73-18	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/A1:2002
RELATIVE INTRINSIC ERROR	The ratio of the INTRINSIC ERROR to the CONVENTIONAL TRUE VALUE.		IEC 61676:2002

Term	Definition	Reference	Used in IEC
RELATIVE SURFACE DOSE	Ratio of the ABSORBED DOSE on the RADIATION BEAM AXIS at the depth of 0,5 mm to the maximum ABSORBED DOSE on the RADIATION BEAM AXIS, both measured in a PHANTOM with its surface at a specified distance.	rm-13-60	IEC 60601-2-11:1997 IEC 60976 /A1:2000
RELATIVE SURFACE DOSE	Ratio of the ABSORBED DOSE on the REFERENCE AXIS, at the depth of 0,5 mm, to the maximum ABSORBED DOSE on the REFERENCE AXIS, both measured in a PHANTOM with its surface at a specified distance. Recommended replacement IEC 60601-2-11:1997, IEC 60976		IEC 60601-2-1/A1:2002
RESERVE ELECTRICAL POWER SOURCE	Part of the MEDICAL ELECTRICAL EQUIPMENT that temporarily supplies power to the electrical system in the event of an interruption of the primary electrical supply.		IEC 60601-2-13:2003
RESIDUAL RADIATION	In MEDICAL RADIOLOGY, that part of the RADIATION BEAM which remains after having passed the plane of the IMAGE RECEPTION AREA and any relevant radiation measuring device, or, in RADIOTHERAPY, which emerges from the part of the body being intentionally irradiated.	rm-11-14	IEC 60601-1-3:1994 IEC 60601-2-29:1999
RESIDUAL RISK	RISK identified by hazard analysis which remains after RISK MANAGEMENT has been completed. Recommended replacement: ISO/IEC Guide 51,1999, definition 3.9		IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999
RESIDUAL RISK	RISK remaining after protective measures have been taken. [ISO/IEC Guide 51:1999, definition 3.9]		ISO 14971:2000
RESOLUTION OF THE DISPLAY	Smallest change of SCALE READING to which a numerical value can be assigned without further interpolation: for an analogue display, the resolution is the smallest fraction of a scale interval that can be determined by an observer under specified conditions; for a digital display, the resolution is the smallest significant increment of the reading.	rm-32-64	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674/ A1:2002
RESOLVING TIME	Smallest time interval which must elapse between the occurrence of two consecutive input signals to a device in order that it be capable of fulfilling its function for each of them separately.	rm-34-22	IEC 60789:1992 IEC 61675-1:1998
RESPIRATORY PRESSURE	PRESSURE at the PATIENT CONNECTION PORT.		IEC 60601-2-12:2001
RESPONSE	The quotient of the INDICATED VALUE divided by the CONVENTIONAL TRUE VALUE.		IEC 61676:2002
RESPONSE	For a CHAMBER ASSEMBLY with an associated MEASURING ASSEMBLY, it is the quotient of the INDICATED VALUE divided by the CONVENTIONAL TRUE VALUE at the position of the REFERENCE POINT of the IONIZATION CHAMBER. For a MEASURING ASSEMBLY on its own it is the quotient of the INDICATED VALUE divided by the input charge or current. For an IONIZATION CHAMBER on its own it is the quotient of the ionization charge or current divided by the CONVENTIONAL TRUE VALUE. Recommended replacement: IEC 60580:2000		IEC 60601-2-9:1996 IEC 60731/A1:2002
RESPONSE	Quotient of the INDICATED VALUE by the CONVENTIONAL TRUE VALUE. Recommended replacement: IEC 60580:2000		IEC 60580:2000 IEC 61674 /A1:2002
RESPONSE time	The time taken for a SCALE READING to reach and remain within a specified deviation from its final steady value, after a sudden change in the quantity being measured.	rm-13-60	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 /A1:2002
RESPONSE TIME	Time required to display a 10 % to 90 % RESPONSE to a change of partial pressure as measured in Clause 7. NOTE Different gases may have different RESPONSE TIME.		IEC 60601-3-1:1996

Term	Definition	Reference	Used in IEC
RHYTHM RECOGNITION DETECTOR (RRD)	A system that analyzes the ECG and identifies whether a cardiac rhythm is shockable. The algorithm in an AED is designed for SENSITIVITY and specificity for the detection of arrhythmias for which a defibrillation shock is clinically indicated. May be referred to as RRD.		IEC 60601-2-4:2002
RISK	Probable rate of occurrence of a hazard causing HARM, and the degree of SEVERITY of the HARM. Recommended replacement: ISO/IEC Guide 51:1999, definition 3.2		IEC 60601-1-4:2000 IEC 62083:2000
RISK	Combination of the probability of occurrence of HARM and the SEVERITY of that HARM. [ISO/IEC Guide 51:1999, definition 3.2]		ISO 14971:2000
RISK ANALYSIS	Systematic use of available information to identify hazards and to estimate the RISK. [ISO/IEC Guide 51:1999, definition 3.10]		ISO 14971:2000
RISK ASSESSMENT	Overall process comprising a RISK ANALYSIS and a RISK EVALUATION. [ISO/IEC Guide 51:1999, definition 3.12]		ISO 14971:2000
RISK CONTROL	Process through which decisions are reached and protective measures are implemented for reducing risks to, or maintaining risks within, specified levels.		ISO 14971:2000
RISK EVALUATION	Judgement, on the basis of RISK ANALYSIS, of whether a RISK which is acceptable has been achieved in a given context based on the current values of society. NOTE Based on ISO/IEC Guide 51:1999, definitions 3.11 and 3.7.		ISO 14971:2000
RISK MANAGEMENT	Systematic application of management policies, procedures and practices to the tasks of analyzing, evaluating and controlling RISK.		ISO 14971:2000
RISK MANAGEMENT FILE	That part of the quality RECORDS required by this standard IEC 60601-1-4:2000. Recommended replacement: ISO 14971:2000		IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-29:1999 IEC 62083:2000
RISK MANAGEMENT FILE	Set of RECORDS and other documents, not necessarily contiguous, that are produced by a RISK MANAGEMENT process.		ISO 14971:2000
RISK MANAGEMENT SUMMARY	Document, which provides traceability for each hazard and each cause of the hazard to the RISK ANALYSIS and to the VERIFICATION that the RISK of the hazard is controlled. NOTE This document may be held on paper or on electronic media.		IEC 60601-1-4:2000
ROUTINE MONITORING	Routine PATIENT monitoring which is carried out by responsible personal such as the OPERATOR and staff of the MR EQUIPMENT and consisting of audio and/or visual contact, as appropriate with the PATIENT during the MR EXAMINATION.		IEC 60601-2-33:2002
ROUTINE TEST	TEST of a piece of EQUIPMENT or its components which is repeated at specified intervals, to establish and document changes from the initial status described by REFERENCE DATA. NOTE A ROUTINE TEST could be carried out by the USER with simple methods and EQUIPMENT.		IEC 61948-1:2001 IEC 61948-2:2001
ROUTINE TEST	TEST carried out on all instruments of a production or delivery batch.		IEC 60731/A1:2002
RUCK-RESISTANT BLANKET	BLANKET having a construction of such rigidity that rucking of the flexible part is unlikely.		IEC 60601-2-35:1996

Term	Definition	Reference	Used in IEC
SAFE WORKING LOAD	Maximum load on an EQUIPMENT or EQUIPMENT part that can be permitted according to a declaration of the supplier or such an EQUIPMENT or EQUIPMENT part if his instructions for installation and use are followed.	NG.11.05	IEC 60601-1/A2:1995
SAFETY	Freedom from unacceptable RISK. [ISO/IEC Guide 51:1999, definition 3.1]		IEC 60601-1-4:2000 IEC 62083:2000 ISO 14971:2000
SAFETY DEVICE	Means which protect the PATIENT and/or OPERATOR from a hazardous force due to excessive travel or from the fall of a suspended mass in the event of failure of a means of suspension.	NG.11.06	IEC 60601-1/A2:1995 IEC 60601-2-32:1994
SAFETY EXTRA-LOW VOLTAGE (SELV)	Voltage which does not exceed a NOMINAL value of 25 V a.c. or 60 V d.c. at RATED supply voltage on the transformer or converter, between conductors in an earth-free circuit which is isolated from the SUPPLY MAINS by a SAFETY EXTRA-LOW VOLTAGE TRANSFORMER or by a device with an equivalent separation.	NG.04.03	IEC 60601-1/A2:1995 IEC 60601-2-41:2000
SAFETY EXTRA-LOW VOLTAGE TRANSFORMER	Transformer with an output-winding which is electrically separated from earth and the body of the transformer by at least BASIC INSULATION and which is electrically separated from the input-winding by an insulation at least equivalent to DOUBLE INSULATION or REINFORCED INSULATION and which is designed to supply SAFETY EXTRA-LOW VOLTAGE circuits.	NG.08.03	IEC 60601-1/A2:1995
SAFETY FACTOR	The ratio between the MINIMUM BREAKING LOAD and SAFE WORKING LOAD.	NG.11.08	IEC 60601-1/A2:1995 IEC 60601-2-32:1994 IEC 60601-2-43:2000
SAFETY HAZARD	Potentially detrimental effect on the PATIENT, other persons, animals, or the surroundings, arising directly from EQUIPMENT. Recommended delineation of the defined terms HARM and HAZARD: – HARM when speaking of the detrimental effect; – HAZARD when speaking of the source that causes the effect.	NG.12.18	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-13:2003 IEC 60601-2-26:2002 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003 IEC 62083:2000
SAFETY HAZARD	Potentially detrimental effect on the PATIENT, other persons, animals, or the surroundings, arising directly from MEDICAL ELECTRICAL EQUIPMENT. Recommended delineation of the defined terms HARM and HAZARD: HARM when speaking of the detrimental effect HAZARD when speaking of the source that causes the effect		IEC 60601-1-4:2000 IEC 62083:2000
SAFETY INTEGRITY	Likelihood of a SAFETY-related system satisfactorily performing the required SAFETY functions under all the stated conditions within a stated period of time.		IEC 60601-1-4:2000
SAMPLE CHANGER	Counting system with a WELL-TYPE DETECTOR and a mechanism for automatically changing samples in the well of the detector.		IEC 61948-1:2001

Term	Definition	Reference	Used in IEC
SAMPLE VOLUME CHARACTERISTIC	Function relating the instrument reading and the sample volume for a specified container at a specified position in the IONIZATION CHAMBER.		IEC 61303:1994
SCALE READING	Value displayed by an instrument before applying scale factors.	rm-73-09	IEC 60601-2-17 /A1:1996 IEC 60976/ A1:2000
SCANNING MODE	Mode of operation of an ULTRASONIC DIAGNOSTIC EQUIPMENT that involves a sequence of ultrasonic PULSES which give rise to scan lines that do not follow the same acoustic path.		IEC 60601-2-37:2001
SCATTER FRACTION (SF)	Ratio between SCATTERED TRUE COINCIDENCES and the sum of scattered plus UNSCATTERED TRUE COINCIDENCES for a given experimental set-up.		IEC 61675-1:1998
SCATTERED FRACTION (SF)	Ratio between the number of scattered PHOTONS and the sum of scattered plus unscattered PHOTONS for a given experimental set-up.		IEC 61675-2:1998
SCATTERED RADIATION	IONIZING RADIATION emitted by interaction of IONIZING RADIATION with matter, the interaction being accompanied by a reduction in RADIATION ENERGY and/or by a change in direction of the radiation.	rm-11-13	IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60806:1984 IEC 60976/ A1:2000 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61267:1994 IEC 61331-3:1998
SCATTERED TRUE COINCIDENCE	TRUE COINCIDENCE where at least one participating PHOTON was scattered before the COINCIDENCE DETECTION.		IEC 61675-1:1998
SCATTERING	Process in which a change in direction or energy of an incident particle or incident radiation is caused by a collision with a particle or a system of particles.	rm-12-03	IEC 60806:1984 IEC 61223-2-10:1999
SCREEN FILM	In DIRECT RADIOGRAPHY, RADIOGRAPHIC FILM with relatively high SENSITIVITY to the radiation emitted by fluorescence of an INTENSIFYING SCREEN.	rm-32-36	IEC 61223-2-1:1993 IEC 61223-2-7:1999
SCROTUM SHIELD	PROTECTIVE DEVICE intended to protect by ENCLOSURE the gonads of a male PATIENT.	rm-64-06	IEC 61331-3:1998
SEALED RADIOACTIVE SOURCE	RADIOACTIVE SOURCE sealed in a container or having a bonded cover, the container or cover being such as to prevent contact with, and dispersion of, the radioactive material under the conditions of use and wear for which it was designed.	rm-20-03	IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996
SEARCH COIL	A small diameter coil used in a compliance test to measure GRADIENT OUTPUT.		IEC 60601-2-33:2002
SECOND LEVEL CONTROLLED OPERATING MODE	Mode of operation of the MR EQUIPMENT in which one or more outputs reach a value that may produce significant RISK for PATIENTS, for which explicit ethical approval is required (i.e. a human studies protocol approved to local requirements).		IEC 60601-2-33:2002

Term	Definition	Reference	Used in IEC
SECONDARY DOSE MONITORING SYSTEM	DOSE MONITORING SYSTEM which is intended to terminate IRRADIATION in the event of failure of the PRIMARY DOSE MONITORING SYSTEM.	rm-33-04	IEC 60601-2-1/A1:2002 IEC 60976 /A1:2000
SECONDARY TIMER	The CONTROLLING TIMER which is intended to terminate IRRADIATION in the event of failure of the PRIMARY TIMER.		IEC 60601-2-11:1997
SELECTED ENERGY	Energy which the DEFIBRILLATOR is intended to deliver, as determined by the setting of a manual control or by an automatic protocol.		IEC 60601-2-4:2002
SELF-RESETTING THERMAL CUT-OUT	THERMAL CUT-OUT which automatically restores the current after the relevant part of EQUIPMENT has cooled.	NG.09.10	IEC 60601-1/A2:1995
SENSITIVE VOLUME	Part of a detector sensitive to radiation and used for detection.	rm-51-07	IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-9:1996 IEC 60601-2-45:2001 IEC 61223-2-6:1994 IEC 61267:1994 IEC 61331-1:1994
SENSITIVITY			IEC 61675-2:1998
SENSITIVITY	Ratio of the amplitude of a recording to the amplitude of the signal producing it, expressed in mm/mV.		IEC 60601-2-25 /A1:1999 IEC 60601-2-27:1994 IEC 60601-2-51:2003
SENSITIVITY PROFILE	Relative RESPONSE of a system for COMPUTED TOMOGRAPHY as a function of position along a line perpendicular to the TOMOGRAPHIC PLANE.	rm-13-61	IEC 60601-2-44:2002 IEC 61223-2-6:1994
SEPARATE MONITORING ELECTRODES	ELECTRODES applied to the PATIENT for the purpose of monitoring the PATIENT. These ELECTRODES are not used to apply defibrillation PULSES to the PATIENT.		IEC 60601-2-4:2002
SEPARATION DEVICE	Definition 2.203 of IEC 601-1-1		IEC 60601-2-9:1996
SERIAL CHANGER	Device permitting the taking of a series of RADIOGRAMS on a single or on several RADIOGRAPHIC FILMS by means of a manually or automatically operated transport mechanism for the film or the RADIOGRAPHIC CASSETTE. NOTE SERIAL CHANGER was earlier used as a synonym for SPOTFILM DEVICE, now it is the general concept.	rm-31-04	IEC 61223-2-9:1999
SERIAL LOAD RATING	Highest permitted X-RAY TUBE LOAD given by the relationship between ANODE INPUT POWER and LOADING TIME for the total of a specified series of individual X-RAY TUBE LOADS with specified LOADING FACTORS.	rm-36-38	IEC 60601-2-28:1993 IEC 60613:1989

Term	Definition	Reference	Used in IEC
SERIAL NUMBER	Number and/or other designation used to identify an individual unit of a certain model of EQUIPMENT.	NG.12.09	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-51:2003 IEC 60627:2001 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000
SERIAL RADIOGRAPHY	RADIOGRAPHY in which the information is obtained and recorded in a regular or irregular series of LOADINGS with equal or unequal LOADING FACTORS.	rm-41-09	IEC 60601-2-7:1998
SET TEMPERATURE	Desired APPLIED PART INTERFACE temperature.		IEC 60601-2-23:1999
SEVERITY	Qualitative measure of the possible consequences of a HAZARD. Recommended replacement: ISO 14971		IEC 60601-1-4:2000
SEVERITY	Measure of the possible consequences of a HAZARD.		ISO 14971:2000
SHADOW DILUTION	Ability of the EQUIPMENT to minimise the impact of shadows in the working area due to the partial obstruction by the OPERATOR of the emitted light.		IEC 60601-2-41:2000
SHADOW SHIELD	PROTECTIVE DEVICE to intercept the RADIATION BEAM in the areas of the gonads, to be used when a SCROTUM SHIELD and an OVARY SHIELD cannot be used.		IEC 61331-3:1998
SHORT TERM AUTOMATIC MODE	A mode in which as many automatic measurements as possible are made within a specified time period.		IEC 60601-2-30:1999
SHORT-TIME OPERATION	Operation under normal load for a specified period, starting from COLD CONDITION without the specified limits of temperature being exceeded, the intervals between each period of operation being sufficient to allow the EQUIPMENT to cool down to COLD CONDITION.	NG.10.10	IEC 60601-1/A2:1995
SHORT-WAVE THERAPY EQUIPMENT	EQUIPMENT for the TREATMENT of the PATIENT by EXPOSURE to electric or magnetic fields produced by the operation of the EQUIPMENT with frequencies between 3 MHz and 45 MHz.		IEC 60601-2-3 /A1:1998
SHUTTER	In RADIOLOGICAL EQUIPMENT, device to open or close the RADIATION APERTURE or to move the RADIATION SOURCE so as to enable or prevent the passage of a RADIATION BEAM.	rm-24-02	IEC 60601-2-11:1997
SIDE RAIL	Rail mounted to both sides of the BED which, when located in the "up" position, identifies the edge of the MATTRESS SUPPORT PLATFORM and by doing so, reduces the RISK of the PATIENT accidentally slipping or rolling off the mattress.		IEC 60601-2-38/A1:1999
SIGNAL INPUT PART	Part of EQUIPMENT, not being an APPLIED PART, intended to receive input signal voltages or currents from other EQUIPMENT, for example, for display, recording or data processing.	NG.01.18	IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
SIGNAL OUTPUT PART	Part of EQUIPMENT, not being an APPLIED PART, intended to deliver output signal voltages or currents to other EQUIPMENT, for example, for display, recording or data processing.	NG.01.19	IEC 60601-1/A2:1995 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
SIGNIFICANT ZONE OF OCCUPANCY	For X-RAY EQUIPMENT, zone with specified boundaries within an area under surveillance or within a CONTROLLED AREA, other than a PROTECTED AREA, that is significant because of the assumed need for persons to occupy it during IRRADIATION.	rm-63-07	IEC 60601-1-3:1994 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 61331-3:1998
SILENCE	The stopping of an auditory ALARM manifestation by OPERATOR action.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
SILENCE, SILENCED	State of temporary duration in which the ALARM SYSTEM or part of the ALARM SYSTEM does not annunciate an audible ALARM signal.		IEC 60601-2-13:2003
SILENCE/RESET	The stopping of an auditory or auditory and visual ALARM manifestation and re-enabling system RESPONSE to an ALARM CONDITION.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
SILENCING	Stopping an auditory ALARM manifestation by manual action.		IEC 60601-2-23:1999 IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-51:2003
SILENCING/RESET	Stopping a visual and/or auditory ALARM manifestation and re-enabling the EQUIPMENT RESPONSE to an abnormal PATIENT condition.		IEC 60601-2-23:1999 IEC 60601-2-34:2000
SILENCING/RESET	The stopping of a visual and/or auditory ALARM manifestation and re-enabling of the EQUIPMENT'S RESPONSE to an abnormal PATIENT condition.		IEC 60601-2-30:1999
SINGLE CHAMBER	Relating to either atrium or ventricle.		IEC 60601-2-31/A1:1998
SINGLE CHANNEL ELECTROCARDIOGRAPH	EQUIPMENT for the recording of one ECG LEAD at a time.		IEC 60601-2-25/A1:1999 IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
SINGLE FAULT CONDITION	Condition in which a single means for protection against a SAFETY HAZARD in EQUIPMENT is defective or a single external abnormal condition is present.	NG.10.11	IEC 60601-1/A2:1995 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-17/A1:1996 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-51:2003
SINGLE FUNCTION	Measurement of one physiological parameter. NOTE Examples of physiological functions are body temperature, ECG, invasive and non-invasive blood pressure etc.		IEC 60601-2-49:2001 IEC 60601-2-51:2003
SINGLE GAMMA-RAY PHOTON PULSE	The number of light PHOTONS emitted by the OUTPUT SCREEN of the XR11 attributable to the interaction of one gamma-ray PHOTON of specific energy in the INPUT SCREEN of the XR11.		IEC 61262-5:1994
SINGLE LOAD RATING	Highest permitted X-RAY TUBE LOAD given by a relationship between constant ANODE INPUT POWER and LOADING TIME for one loading under specified conditions.	rm-36-37	IEC 60601-2-28:1993 IEC 60613:1989
SINGLE PHOTON EMISSION COMPUTED TOMOGRAPHY (SPECT)	Emission computed tomograph utilizing single PHOTON detection of gamma-ray emitting RADIONUCLIDES.	rm-41-25	IEC 61675-2:1998 IEC 61948-2:2001
SINGLES RATE	COUNT RATE measured without COINCIDENCE DETECTION, but with energy discrimination.		IEC 61675-1:1998
SINOGRAM	Two-dimensional display of all one-dimensional PROJECTIONS of an OBJECT SLICE, as a function of the PROTECTION ANGLE. The PROJECTION angle is displayed on the ordinate. The linear PROJECTION coordinate is displayed on the abscissa.	rm-32-68	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
SITE TEST	After installation, TEST of an individual device or EQUIPMENT to establish compliance with specified criteria. Recommended replacement: ACCEPTANCE TEST rm-70-01		IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997
SIX-PEAK HIGH-VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR for operation on a three-phase supply that delivers a rectified output voltage with six peaks during each cycle of the supply.	rm-21-04	IEC 60601-2-7:1998 IEC 60601-2-45:2001
SKIN TEMPERATURE	The temperature of the skin of the baby at a point on which the SKIN TEMPERATURE SENSOR is placed.		IEC 60601-2-19 /A1:1996 IEC 60601-2-20 /A1:1996

Term	Definition	Reference	Used in IEC
SKIN TEMPERATURE SENSOR	A sensing device intended to measure the baby's SKIN TEMPERATURE.		IEC 60601-2-19 /A1:1996 IEC 60601-2-20 /A1:1996
SKIN TEMPERATURE SENSOR	A sensing device including the link with the EQUIPMENT intended to measure the infant's SKIN TEMPERATURE.		IEC 60601-2-21 /A1:1996
SLICE SENSITIVITY	Ratio of COUNT RATE as measured on the SINOGRAM to the ACTIVITY concentration in the PHANTOM. NOTE 1 In SPECT the measured counts are not numerically corrected for scatter by subtracting the SCATTER FRACTION. NOTE 2 In PET, the measured counts are numerically corrected for scatter by subtracting the SCATTER FRACTION.	rm-34-41	IEC 61675-1:1998 IEC 61675-2:1998
SLICE THICKNESS	Full width at half-maximum of the SENSITIVITY PROFILE in the centre of the scan field.		IEC 61223-2-6:1994
SLIT CAMERA	Assembly of EQUIPMENT used to obtain a FOCAL SPOT SLIT RADIOGRAM on RADIOGRAPHIC FILM.	rm-71-01	IEC 60336:1993 IEC 61223-3-1:1999 IEC 61223-3-4:2000
SOFT TISSUE THERMAL INDEX	THERMAL INDEX related to soft tissues. Symbol: <i>T/S</i> . Unit: None. NOTE 1 See DD 5.1 and the following for methods of determination of the SOFT TISSUE THERMAL INDEX. NOTE 2 For the purposes of this document, soft tissue includes all body tissues and fluids but excludes skeletal tissues.		IEC 60601-2-37:2001
SOURCE APPLICATOR	In brachy RADIOTHERAPY, device to bring one or more RADIATION SOURCES into the intended positions. A SOURCE APPLICATOR may include PROTECTIVE SHIELDING.	rm-25-04	IEC 60601-2-17 /A1:1996
SOURCE CARRIER	In EQUIPMENT for RADIONUCLIDE beam therapy, component located within the RADIATION HEAD to which a capsule is fixed.	rm-24-03	IEC 60601-2-11:1997
SOURCE DRIVE MECHANISM	In EQUIPMENT for remotely controlled after-loading, mechanism which drives one or more SEALED RADIOACTIVE SOURCES out of, and back into, a STORAGE CONTAINER.	rm-25-03	IEC 60601-2-17 /A1:1996
SOURCE TO ENTRANCE PLANE DISTANCE (abbreviation SED)	The distance between the FOCAL SPOT of the X-RAY TUBE and the ENTRANCE PLANE of the XRIL.		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
SPATIAL NONLINEARITY	The deviations of the image of a straight LINE SOURCE from a straight line.		IEC 60789:1992
SPATIAL RESOLUTION	Ability to concentrate the count density distribution in the image of a POINT SOURCE to a point.	rm-32-65	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61675-3:1998

Term	Definition	Reference	Used in IEC
SPATIAL RESOLUTION (in CT EQUIPMENT)	<p>(see HIGH-CONTRAST RESOLUTION): In EQUIPMENT for COMPUTED TOMOGRAPHY, the ability to resolve different objects in the displayed image, when the difference in ATTENUATION between the objects and the background is large compared to NOISE.</p> <p>NOTE 1 Normally a difference in ATTENUATION coefficient between the object and the background resulting in a difference of the respective COMPUTED TOMOGRAPHY NUMBERS of several hundred Hounsfield units is regarded as large enough.</p> <p>NOTE 2 HIGH-CONTRAST RESOLUTION is an alternate name for SPATIAL RESOLUTION.</p>		IEC 61223-2-6:1994
SPATIAL-PEAK TEMPORAL-AVERAGE INTENSITY	<p>Maximum value of the TEMPORAL-AVERAGE INTENSITY in a specified plane at a specified distance z from the TRANSDUCER. Symbol: $I_{zpta}(z)$. Unit: milliwatts per centimetre squared, mW-cm⁻².</p> <p>NOTE In this Standard, the restricted definition from 3.49 of IEC 61102 relating to a specified plane is used.</p>		IEC 60601-2-37:2001
SPECIAL PURPOSE GRADIENT SYSTEM	<p>A gradient system suitable for use in MR EQUIPMENT for a special purpose. An example of a SPECIAL PURPOSE GRADIENT SYSTEM is a gradient system that can be incorporated in MR EQUIPMENT to allow special examination of the head of the PATIENT.</p>		IEC 60601-2-33:2002
SPECIAL USE EQUIPMENT	<p>EQUIPMENT in which the delivery rate is set by the OPERATOR and indicated by the EQUIPMENT in units other than those defined in 2.101 to 2.106.</p>		IEC 60601-2-24:1998

Term	Definition	Reference	Used in IEC
specific	When used in combination with parameters or conditions: referring to a particular value or standardized arrangement, usually to those required in an IEC standard or a legal requirement.	rm-74-01	IEC 60336:1993 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-28:1993 IEC 60601-2-32:1994 IEC 60601-2-44:2002 IEC 60613:1989 IEC 60627:2001 IEC 60806:1984 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 62083:2000
SPECIFIC ABSORPTION RATE (SAR)	RADIO FREQUENCY power absorbed per unit of mass of an object (W/kg).		IEC 60601-2-33:2002

Term	Definition	Reference	Used in IEC
specified	When used in combination with parameters or conditions: referring to a value or arrangement to be chosen for the purpose under consideration and indicated usually in ACCOMPANYING DOCUMENTS.	rm-74-02	IEC 60336:1993 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 60601-2-44:2002 IEC 60613:1989 IEC 60627:2001 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998 IEC 62083:2000
specified	When used with parameters or conditions: refers to a value or arrangement to be chosen for the purpose under consideration and indicated usually in ACCOMPANYING DOCUMENTS. Recommended replacement: rm-74-02		IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61262-7:1995
SPECIFIED ENERGY RESPONSE	This is the RESPONSE of an IONIZATION CHAMBER calculated or measured for that type of CHAMBER as a function of RADIATION QUALITY.		IEC 60731/A1:2002

Term	Definition	Reference	Used in IEC
SPEED INDEX	For CONSTANCY TESTS in X-RAY EQUIPMENT, the specific value of optical density in an area of the RADIOGRAM produced by a constant EXPOSURE to a light source. NOTE The value of SPEED INDEX normally is established at an optical density in the range from 0,8 to 1,2 above that of film base plugs fog density.	rm-32-66	IEC 61223-2-1:1993 IEC 61223-2-7:1999 IEC 61223-2-10:1999
SPOTFILM DEVICE	Device for taking one or more RADIOGRAMS for which the choice of object and moment is made during RADIOSCOPY. NOTE A RADIOGRAPHIC CASSETTE HOLDER attached to a radioscopy device is not considered as a spot-film device.	rm-31-05	IEC 60601-1-3:1994 IEC 60601-2-32:1994 IEC 61223-2-11:1999 IEC 61223-3-1:1999
SQUEEZING and SHEARING POINTS (FOR FINGERS and HANDS)	Points where the spacing between moveable parts of the BED when in positions of NORMAL USE fail to maintain a clearance of less than or equal to 8 mm, or greater than or equal to 25 mm.		IEC 60601-2-38/ A1:1999
STABILITY CHECK DEVICE	A device which enables the stability of RESPONSE of the MEASURING ASSEMBLY and/or CHAMBER ASSEMBLY to be checked. NOTE The STABILITY CHECK DEVICE may be a purely electrical device, or a source, or it may include both. Recommended replacement: IEC 60580:2000		IEC 60731/A1:2002
STABILITY CHECK DEVICE	Device, either separate or integral part of the diagnostic DOSIMETER, which enables the stability of the RESPONSE of the RADIATION DETECTOR and/or MEASURING ASSEMBLY to be checked. NOTE The STABILITY CHECK DEVICE may be a purely electrical device, or a RADIATION SOURCE, or it may include both. Recommended replacement: IEC 60580:2000		IEC 61674/ A1:2002
STABILITY CHECK DEVICE	Device, either separate or integral part of the DOSE AREA PRODUCT METER, which enables the stability of the RESPONSE of the IONIZATION CHAMBER and/or MEASURING ASSEMBLY to be checked. NOTE The STABILITY CHECK DEVICE may be a purely electrical device.		IEC 60580:2000
STABILIZATION TIME	Time taken for a stated performance characteristic to reach and remain within a specified deviation from its final steady value, after the DOSIMETER has been switched on (and, if the RADIATION DETECTOR is an IONIZATION CHAMBER, after the polarizing voltage has been applied).		IEC 61674 /A1:2002
STABILIZATION TIME	Time taken for a stated PERFORMANCE CHARACTERISTIC to reach and remain within a specified deviation from its final steady value, after the DOSE AREA PRODUCT METER has been switched on and after the polarizing voltage has been applied to the IONIZATION CHAMBER. Recommended replacement: IEC 61674		IEC 60580:2000
STABILIZATION TIME	The time taken for a stated PERFORMANCE CHARACTERISTIC to reach and remain within a specified deviation from its final steady value after the MEASURING ASSEMBLY has been switched on (or the polarizing voltage has been applied to the IONIZATION CHAMBER). Recommended replacement: IEC 61674		IEC 60731/A1:2002

Term	Definition	Reference	Used in IEC
STABILIZATION TIME	Time taken for a stated PERFORMANCE CHARACTERISTIC to reach and remain within a specified deviation from its final steady value, after the DOSIMETER has been switched on (and, if the RADIATION DETECTOR is an IONIZATION CHAMBER, after the polarizing voltage has been applied). Recommended replacement: IEC 61674		IEC 61674 /A1:2002
STANDARD	An instrument which defines, represents physically, maintains or reproduces the unit of measurement of a quantity (or a multiple or submultiple of that unit) in order to transfer it to other instruments by comparison.		IEC 60731/A1:2002 IEC 61674 /A1:2002
STANDARD MEASUREMENT DEPTH	For the measurement of characteristics of a beam of IONIZING RADIATION, specified depth in a PHANTOM.		IEC 60976 /A1:2000
STANDARD TEST CONDITIONS	Conditions under which all INFLUENCE QUANTITIES and INSTRUMENT PARAMETERS have their STANDARD TEST VALUES.	rm-70-08	IEC 60580:2000 IEC 60731/A1:2002 IEC 61674 /A1:2002 IEC 61676:2002
STANDARD TEST VALUES	A value, values, or range of values of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER, which is / are permitted when carrying out calibrations or tests on another INFLUENCE QUANTITY or INSTRUMENT PARAMETER.	rm-72-07	IEC 60731/A1:2002 IEC 61676:2002
STANDARD TEST VALUES	Value(s), or range of values of an INFLUENCE QUANTITY or INSTRUMENT PARAMETER which are permitted when carrying out calibrations or tests on another INFLUENCE QUANTITY or INSTRUMENT PARAMETER. Recommended replacement: IEC 60976		IEC 60580:2000 IEC 61674 /A1:2002
STANDARDIZATION VOLTAGE	Voltage step recorded for amplitude calibration purposes.		IEC 60601-2-25/A1:1999
STAND-BY	Mode of operation in which the EQUIPMENT is operational except that the ENERGY STORAGE DEVICE is not yet charged.		IEC 60601-2-4:2002
STAND-BY STATE	State of EQUIPMENT after a preconditioning which is indispensable or customary, before the intended operation of such EQUIPMENT can be initiated.	rm-84-03	IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-29:1999 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60976 /A1:2000
STAR PATTERN CAMERA	Assembly of EQUIPMENT used to obtain a FOCAL SPOT STAR RADIOGRAM on RADIOGRAPHIC FILM.	rm-71-03	IEC 60336:1993
STAR PATTERN RESOLUTION LIMIT	As a characteristic of the FOCAL SPOT of an X-RAY TUBE, lowest spatial frequency which cannot be imaged under specific measuring conditions.		IEC 60336:1993
STATIC LOAD	Maximum LOADING of a part excluding any LOADING caused by acceleration or deceleration of masses. Where a load is divided over several parallel supporting parts and the distribution over these parts is not determined unequivocally, the least favorable possibility shall be considered.	NG.11.07	IEC 60601-1/A2:1995
STATIONARY EQUIPMENT	Either FIXED EQUIPMENT or EQUIPMENT which is not intended to be moved from one place to another.	NG.02.21	IEC 60601-1/A2:1995

Term	Definition	Reference	Used in IEC
STATIONARY GRID	ANTI-SCATTER GRID used in such a way that it does not move in relation to the RADIATION BEAM.	rm-32-14	IEC 60627:2001 IEC 61223-2-10:1999 IEC 61223-3-2:1996
STATIONARY RADIOTHERAPY	RADIOTHERAPY without displacement of the RADIATION SOURCE relative to the PATIENT during the IRRADIATION.	rm-42-31	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997
STATUS TEST	TEST carried out to establish the functional status of EQUIPMENT at a given time.	rm-70-09	IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999
STEADY TEMPERATURE CONDITION	The condition reached when the INCUBATOR TEMPERATURE does not vary by more than 1° C over a period of one hour (see Figure 101).		IEC 60601-2-19 /A1:1996
STEADY TEMPERATURE CONDITION	The condition reached when the TRANSPORT INCUBATOR TEMPERATURE does not vary by more than 2° C over a period of one hour (see Figure 101).		IEC 60601-2-20 /A1:1996
STEADY TEMPERATURE CONDITION	A condition which is reached when the temperature, measured at the centre of the TEST DEVICE positioned on the mid point of the EQUIPMENT mattress, does not vary by more than 1° C over a period of 1 h.		IEC 60601-2-21 /A1:1996
STERILE HANDLE	Device maintaining a sterile area in order to handle it under aseptic conditions when attached to the EQUIPMENT.		IEC 60601-2-41:2000
STERILIZABLE EQUIPMENT	EQUIPMENT parts which come into contact with the PATIENT during NORMAL USE and which may be sterilized in accordance with MANUFACTURER'S instructions.		IEC 60601-2-9:1996
STIMULATOR	EQUIPMENT for the application of electric currents via ELECTRODES in direct contact with the PATIENT for the diagnosis and/or therapy of neuromuscular disorders.		IEC 60601-2-10 /A1:2001
STORAGE CONTAINER	Container for one or more RADIOACTIVE SOURCES, which provides protection against IONIZING RADIATION while the sources are not in use.	rm-25-01	IEC 60601-2-17 /A1:1996
STORED ENERGY	Energy which is stored in the DEFIBRILLATOR ENERGY STORAGE DEVICE.		IEC 60601-2-4:2002
STRAY RADIATION	For IONIZING RADIATION, all radiation except that of the specified RADIATION BEAM under consideration, but including its RESIDUAL RADIATION	rm-11-12	IEC 60601-1-3:1994 IEC 60601-2-/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61331-3:1998

Term	Definition	Reference	Used in IEC
STRIP FREQUENCY	Letter symbol: <i>N</i> , unit: cm ⁻¹ . Number of absorbing strips per unit length of a LINEAR GRID. NOTE This term replaces the previous term STRIPS PER CENTIMETRE.		IEC 60627:2001
STRIPS PER CENTIMETRE	Letter symbol: <i>N</i> . For a LINEAR GRID, number of absorbing STRIPS PER CENTIMETRE.	rm-32-16	IEC 60627:2001
STRUCTURAL SHIELDING	PROTECTIVE SHIELDING forming part of the building structure of a RADIOLOGICAL INSTALLATION.	rm-64-03	IEC 60601-2-43:2000
SUBSTITUTION FLUID	A fluid which during HF or HDF is administered to the PATIENT via the EXTRACORPOREAL CIRCUIT.		IEC 60601-2-16:1998
SUPERFICIAL RADIOTHERAPY	RADIOTHERAPY of superficial tissues of the body usually at a depth not exceeding 1 cm.	rm-42-01	IEC 60601-2-17 /A1:1996
SUPPLEMENTARY INSULATION	Independent insulation applied in addition to BASIC INSULATION in order to provide protection against electric shock in the event of a failure of BASIC INSULATION.	NG.03.08	IEC 60601-1/A2:1995
SUPPLY EQUIPMENT	EQUIPMENT which supplies electrical power to one or more items of EQUIPMENT.	NG.01.21	IEC 60601-1/A2:1995
SUPPLY LINE	That part of the ADMINISTRATION SET between the liquid supply and the EQUIPMENT.		IEC 60601-2-24:1998
SUPPLY MAINS	Permanently installed power source which may also be used to supply electrical apparatus that is outside the scope of this standard IEC 60601-1:1988. This also includes permanently installed battery systems in ambulances and the like.	NG.12.10	IEC 60601-1/ A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-17 A1:1996 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60601-2-47:2001 IEC 60601-2-51:2003 IEC 60731/A1:2002 IEC 61674/A1:2002
SUPPLY UNIT	That part of ENDOSCOPIC EQUIPMENT directly connected to an ENDOSCOPE, supplying functions necessary for the ENDOSCOPE to produce the intended view or image, for example illumination or signal processing.		IEC 60601-2-18 /A1:2000
SURFACE DOSE	ABSORBED DOSE, including that caused by BACK-SCATTERING, at a point of the ENTRANCE SURFACE of the irradiated object, usually on the RADIATION BEAM AXIS.	rm-13-50	IEC 60601-2-11:1997 IEC 60976 /A1:2000
SURGICAL LUMINAIRE	A generic term applicable to minor SURGICAL LUMINAIRES, major SURGICAL LUMINAIRES and SURGICAL LUMINAIRE SYSTEMS.		IEC 60601-2-41:2000
SURGICAL LUMINAIRE SYSTEM	Combination of several SURGICAL LUMINAIRES to illuminate the body of the PATIENT locally. It is FAIL SAFE and provides an adequate CENTRAL ILLUMINANCE. It is intended to support the TREATMENT and diagnosis, and to be used in operating rooms. See Table 101. (Example: A proved FAIL SAFE combination of two or more minor SURGICAL LUMINAIRES is a SURGICAL LUMINAIRE SYSTEM.)		IEC 60601-2-41:2000
SUSPENDED	State of an ALARM SYSTEM where OPERATOR action has temporarily caused an otherwise enabled ALARM SYSTEM to disable all auditory or all auditory and visual ALARM SIGNALS for a fixed interval.		IEC 60601-2-12:2001

Term	Definition	Reference	Used in IEC
SUSPENSION	Disabling, or SILENCING and disabling, an ALARM temporarily.		IEC 60601-2-23:1999 IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-49:2001 IEC 60601-2-51:2003
SYNCHRONIZER	Device allowing the DEFIBRILLATOR discharge to be synchronized with a specific phase of the cardiac cycle.		IEC 60601-2-4:2002
SYRINGE PUMP	EQUIPMENT intended for controlled infusion of liquids into the PATIENT by means of one or more single action syringe(s) or similar container(s) (e.g. where the cartridge is emptied by pushing on its plunger) and in which the delivery rate is set by the OPERATOR and indicated by the EQUIPMENT in volume per unit of time.		IEC 60601-2-24:1998
SYSTEM AXIS	Axis of symmetry characterized by geometrical and physical properties of the arrangement of the system. NOTE The SYSTEM AXIS of a GAMMA CAMERA with rotating detectors is the axis of rotation. For a circular POSITRON EMISSION TOMOGRAPH, the SYSTEM AXIS is the axis through the centre of the detector ring For tomographs with rotating detectors it is the axis of rotation.	rm-34-42	IEC 61675-1:1998 IEC 61675-2:1998 IEC 61948-2:2001
SYSTEM LINEARITY	Function relating the observed and predicted ACTIVITY values when the ACTIVITY of a specified RADIOACTIVE SOURCE is varied.		IEC 61303:1994
SYSTEM NON-UNIFORMITY OF RESPONSE	The NON-UNIFORMITY OF RESPONSE of the DETECTOR HEAD with COLLIMATOR.	rm-34-43	IEC 60789:1992 IEC 61948-2:2001
SYSTEM SENSITIVITY	With a specified COLLIMATOR and PULSE amplitude analyzer window, the ratio of the COUNT RATE of the DETECTOR HEAD to the RADIOACTIVITY of a plane source of specific dimensions and containing a specified radio nuclide placed perpendicular to and centred on the COLLIMATOR AXIS under specified conditions.	rm-34-44	IEC 60789:1992 IEC 61948-2:2001
TANGENTIAL RESOLUTION	TRANSVERSE RESOLUTION in the direction orthogonal to the direction of RADIAL RESOLUTION.		IEC 61675-1:1998 IEC 61675-2:1998
TAPERED GRID	LINEAR GRID in which the height of the absorbing strips decreases as the distance between the absorbing strips and the TRUE CENTRAL LINE increases. This decrease is symmetrical about the TRUE CENTRAL LINE.		IEC 60627:2001
TARGET	Part of an X-RAY TUBE or a PARTICLE ACCELERATOR onto which is directed a beam of accelerated particles to produce IONIZING RADIATION or other particles.	rm-20-08	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-1/A1:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60806:1984 IEC 60976 /A1:2000 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61262-7:1995 IEC 61267:1994

Term	Definition	Reference	Used in IEC
TARGET ANGLE	Acute angle between the plane of the ACTUAL FOCAL SPOT and the REFERENCE AXIS.	rm-20-11	IEC 60601-2-28:1993 IEC 61223-3-1:1999
TARGET MARKER	Location in space where the MANUFACTURER intends the OPERATOR to locate the calculi.		IEC 60601-2-36:1997
TARGET LOCATION	Marker which is used to indicate the TARGET LOCATION.		IEC 60601-2-36:1997
TARGET VOLUME	In RADIOTHERAPY, region in the PATIENT, to which it is desired to deliver an ABSORBED DOSE.	rm-37-20	IEC 60601-2-17 /A1:1996 IEC 60976 /A1:2000 IEC 62083:2000
TECHNICAL ALARM	Signal which indicates that an EQUIPMENT is not capable of accurately monitoring or no longer monitors the PATIENT'S condition.		IEC 60601-2-23:1999
TECHNICAL ALARM	A signal which indicates that the EQUIPMENT or part(s) of the EQUIPMENT is not capable of accurately monitoring the PATIENT'S condition.		IEC 60601-2-30:1999 IEC 60601-2-34:2000 IEC 60601-2-49:2001 IEC 60601-2-51:2003
TELERADIOTHERAPY	RADIOTHERAPY with a large RADIATION SOURCE TO SKIN DISTANCE, usually not less than 50 cm.	rm-42-23	IEC 60601-2-11:1997 IEC 61217:2002
TEMPERATURE LIMITER	Means of limiting the temperature of the APPLIED PART INTERFACE.		IEC 60601-2-23:1999
TEMPORAL-AVERAGE INTENSITY	Time-average of the instantaneous intensity at a particular point in an acoustic field. Symbol: $I_{ta}(z)$. Unit: milliwatts per centimetre squared, mW / cm ² .		IEC 60601-2-37:2001
TEMPORAL-MAXIMUM INTENSITY	In the case of an amplitude modulated wave, this is the ratio of the TEMPORAL MAXIMUM OUTPUT POWER to the EFFECTIVE RADIATING AREA. [IEC 61689, definition 3.41, modified]		IEC 60601-2-5:2000
TEMPORAL-MAXIMUM OUTPUT POWER	In the case of an amplitude modulated wave, this is a function of the actual OUTPUT POWER, the temporal-peak acoustic pressure and the r.m.s. acoustic pressure and is determined as specified in IEC 61689. [conforms to 3.34 of IEC 61689]		IEC 60601-2-5:2000
TENTH-VALUE LAYER	Thickness of a specified material which attenuates under BROAD BEAM CONDITIONS X-RADIATION or gamma radiation with a particular RADIATION ENERGY or with a particular spectrum to an extent such that the KERMA RATE, EXPOSURE RATE or ABSORBED DOSE RATE is reduced to one-tenth of the value that is measured without the material. The TENTH-VALUE LAYER is expressed in suitable submultiples of the metre together with the material.	rm-13-43	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997
TERMINAL DEVICE	Part of EQUIPMENT by which electrical connection is made; it may contain several individual contacts.	NG.07.16	IEC 60601-1/A2:1995
TERMINATION (of IRRADIATION)/ to terminate (IRRADIATION)	Stopping of/to stop IRRADIATION with no possibility of re-starting without the re-selection of all operating conditions, (i.e. returning/to return to the PREPARATORY STATE): when the pre-selected value of elapsed time is reached; or: by deliberate manual act; by the operation of an INTERLOCK; by pre-selected value of GANTRY angular position in MOVING BEAM RADIOTHERAPY.		IEC 60601-2-11:1997

Term	Definition	Reference	Used in IEC
TERMINATION (of IRRADIATION)	In RADIOTHERAPY, stopping or preventing further IRRADIATION with no possibility of re-starting without re-selection or re-confirmation of operating conditions. Recommended replacement: IEC 60601-2-11:1997		IEC 60601-2-17/A1:1996
TERMINATION of IRRADIATION /to terminate IRRADIATION	Stopping of/to stop IRRADIATION and movements, with not possibility of restarting without the reselection of all operation conditions (i.e. returning/to return to the PREPARATORY STATE). NOTE Events that terminate IRRADIATION and stop movements include the following events: – when the pre-selected value of DOSE MONITOR UNITS is reached, – when the pre-selected value of elapsed time is reached, – a deliberate manual act, – the operation of an INTERLOCK, in MOVING BEAM RADIOTHERAPY, when the pre-selected value of an angular or linear dimension is exceeded. Recommended replacement: IEC 60601-2-11:1997		IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-29:1999
TERMINATION of IRRADIATION /to terminate IRRADIATION	Stopping of IRRADIATION without the possibility of restarting without reselection of all operation conditions (that means return to the PREPARATORY STATE): – when the pre-selected value of DOSE MONITOR UNITS is reached, or – when the pre-selected value of elapsed time is reached, or – by deliberate manual act, or – by the operation of an INTERLOCK, or – by pre-selected value of GANTRY angular position in MOVING BEAM RADIOTHERAPY.		IEC 60976/A1:2000
TEST	Facility enabling the STANDARDIZATION VOLTAGE or zero voltage to be recorded in place of the electrocardiogram.		IEC 60601-2-25 /A1:1999
TEST	Other designation for cal.		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
TEST DEVICE	For TESTS requiring an X-RAY PATTERN, specific structure of one or more suitable materials to be placed in a RADIATION BEAM in order to produce such a pattern.	rm-71-04	IEC 60601-2-45:2001 IEC 61223-1:1993 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994
TEST DEVICE	A totally mat blackened disc used as a reproducible receiver of radiant energy during testing of the INFANT RADIANT WARMER. Recommended replacement: rm-71-04		IEC 60601-2-21/A1:1996
TEST DEVICE AVERAGE TEMPERATURE	(T_1 , T_2 , T_3 , T_4 or T_M) The average temperature reading taken during a STEADY TEMPERATURE CONDITION at regular intervals at the centre of a TEST DEVICE.		IEC 60601-2-21/A1:1996
TEST LOAD	An array of five TEST DEVICES used in a specified configuration (see Figure 102) for performance tests of the INFANT RADIANT WARMER.		IEC 60601-2-21/ A1:1996
THERMAL CUT-OUT	Device which, during abnormal operation, limits the temperature of EQUIPMENT or of parts of it, by automatically opening the circuit or by reducing the current, and which is so constructed that its setting cannot be altered by the OPERATOR.	NG.09.12	IEC 60601-1/A2:1995 IEC 60601-2-28:1993
THERMAL INDEX	Ratio of attenuated acoustic power at a specified point to the attenuated acoustic power required to raise the temperature at that point in a specific tissue model by 1° C. Symbol: T_I . Unit: None.		IEC 60601-2-37:2001
THERMOSTAT	A temperature sensing control which is intended to keep a temperature between two particular values under normal operating conditions and which may have provision for setting by the OPERATOR.	NG.09.13	IEC 60601-1/A2:1995
THREE-DIMENSIONAL RECONSTRUCTION	In THREE-DIMENSIONAL RECONSTRUCTION, the lines of RESPONSE are not restricted to being perpendicular to the SYSTEM AXIS. So, a LINE OF RESPONSE may pass several transverse slices. Consequently, transverse slices cannot be reconstructed independent of each other. Each slice has to be reconstructed utilizing the full three-dimensional data set.		IEC 61675-1:1998

Term	Definition	Reference	Used in IEC
<i>TIME CONSTANT</i>	The time taken for the output WAVEFORM step to decay to 1/e (37 %) of the initial amplitude. It is used to define the low frequency RESPONSE of an a.c. coupled amplifier to a d.c. step input. NOTE This definition is derived from a first order network.		IEC 60601-2-51:2003
TIME RATE OF CHANGE OF THE MAGNETIC FIELD (dB/dt)	Rate of change of the magnetic flux density with time (T/s).		IEC 60601-2-33:2002
TIMING DEVICE	Device integrating and/or presenting time elapsed during an EQUIPMENT function and optionally changing the state of operation at the end of a predetermined time interval.	rm-83-03	IEC 60601-2-7:1998 IEC 60601-2-17/A1:1996 IEC 61223-3-4:2000
TISSUE EQUIVALENT MATERIAL	Material which absorbs and scatters a specified IONIZING RADIATION to the same degree as a particular biological tissue.	rm-35-16	IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-2-11:1999 IEC 61223-3-1:1999
TOMOGRAPHIC PLANE	The geometric plane perpendicular to the axis of rotation.		IEC 60601-2-44:2002
TOMOGRAPHIC SECTION	The volume over which TRANSMISSION data of X-RADIATION are collected in a single axial scan. NOTE In a CT SCANNER with multiple detector elements along the z-axis, it is the volume over which data are collected by a single acquisition channel (selected grouping of elements) and not the total volume irradiated.		IEC 60601-2-44:2002
TOMOGRAPHIC SECTION THICKNESS	The FULLWIDTH AT HALF MAXIMUM of the SENSITIVITY PROFILE taken at the iso-centre of a TOMOGRAPHIC SECTION.		IEC 60601-2-44:2002
TOMOGRAPHIC VOLUME	Ensemble of all volume elements which contribute to the measured PROJECTIONS for all PROJECTION angles. NOTE For a rotating GAMMA CAMERA with a circular field of view, the TOMOGRAPHIC VOLUME is a sphere provided that the RADIUS OF ROTATION is larger than the radius of the field of view. For a rectangular field of view, the TOMOGRAPHIC VOLUME is a cylinder.		IEC 61675-2:1998
TOMOGRAPHIC VOLUME	Juxtaposition of all volume elements which contribute to the measured PROJECTIONS for all PROJECTION angles. Recommended replacement: IEC 61675-2:1998		IEC 61675-1:1998
TOMOGRAPHY	RADIOGRAPHY of one or more layers within an object.	rm-41-15	IEC 61223-1:1993 IEC 61223-3-1:1999 IEC 61675-1:1998 IEC 61675-2:1998

Term	Definition	Reference	Used in IEC
TOOL	Extra-corporeal object which may be used to secure or release fasteners or to make adjustments.	NG.12.12	IEC 60601-1/A2:1995 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-17 /A1:1996 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60731/A1:2002 IEC 61674 /A1:2002
TOTAL COINCIDENCES	Sum of all coincidences detected.		IEC 61675-1:1998
TOTAL FIELD OF VIEW	Dimensions (three-dimensional) of the TOMOGRAPHIC VOLUME.		IEC 61675-1:1998 IEC 61675-2:1998
TOTAL FILTRATION	The total of INHERENT FILTRATION and ADDITIONAL FILTRATION.	rm-13-48	IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994

Term	Definition	Reference	Used in IEC
TOTAL IRRADIANCE FOR BILIRUBIN	(E _{BI}) The irradiance equal to the evaluated irradiance in the range between 400 nm and 550 nm, given by an integration $E_{bi} = \int_{400nm}^{550nm} E_{\lambda}(\lambda) d\lambda$ unit: W/m ² where E _λ (λ) is the measured irradiance at an individual wavelength (λ).		IEC 60601-2-50:2000
TOTAL LOAD	Sum of the STATIC LOAD and the forces caused by acceleration and deceleration occurring in NORMAL CONDITION.	NG.11.09	IEC 60601-1/A2:1995
TRACEABLE RADIOACTIVE STANDARD SOURCE	RADIOACTIVE SOURCE that has been calibrated by comparing it to a CERTIFIED RADIOACTIVE STANDARD SOURCE or to another TRACEABLE RADIOACTIVE STANDARD SOURCE of the same RADIONUCLIDE.		IEC 61303:1994
TRANSCUTANEOUS OXYGEN AND CARBON DIOXIDE PARTIAL PRESSURE MONITORING EQUIPMENT	Device and associated TRANSDUCERS for the monitoring and/or recording of partial pressures of oxygen and carbon dioxide at the skin surface.		IEC 60601-3-1:1996
TRANSCUTANEOUS PARTIAL PRESSURE MONITORING EQUIPMENT	Device and associated TRANSDUCERS for the monitoring of partial pressures of oxygen and/or carbon dioxide at the skin surface.		IEC 60601-2-23:1999
TRANSDUCER	Device for converting the partial pressure of a gas into a signal for monitoring or recording.		IEC 60601-2-23:1999 IEC 60601-3-1:1996
TRANSDUCER	Device for converting pressure into an electrical signal for monitoring or measuring.		IEC 60601-2-34:2000 IEC 60601-2-51:2003
TRANSDUCER ASSEMBLY	TRANSDUCER housing (probe), any associated electronic circuitry and any liquids contained in the housing and the integral cable which connects the TRANSDUCER probe to an ULTRASOUND console.		IEC 60601-2-37:2001
TRANSFER	Displacement of information optionally including its transformation or conversion.	rm-84-02	IEC 61262-7:1995
TRANSMEMBRANE PRESSURE (TMP)	Hydrostatic pressure exerted across a semi-permeable membrane. NOTE For practical reasons the mean TMP is generally expressed as either: a) the difference between the arithmetic means of inlet and outlet PRESSURES of the blood and DIALYSING FLUID compartments of a DIALYSER, or b) the difference between the arithmetic mean of the inlet and outlet PRESSURES of the blood compartment and the filtrate PRESSURE of a haemofilter or a haemoconcentrator.		IEC 60601-2-16:1998
TRANSMISSION	In RADIOLOGY, passage of IONIZING RADIATION through, and emergence from, matter essentially in the direction of its incidence, without or after interaction with that matter.	rm-12-10	IEC 60336:1993 IEC 60627:2001 IEC 61223-2-9:1999 IEC 61223-3-1:1999 IEC 61262-7:1995 IEC 62083:2000

Term	Definition	Reference	Used in IEC
TRANSMISSION CHAMBER	Ionization detector containing one or more SENSITIVE VOLUMES and suitable to transmit the entire RADIATION BEAM and which has negligible effects on the RADIATION BEAM.	rm-51-04	IEC 60601-2-7:1998
TRANSMISSION DETECTOR	RADIATION DETECTOR through which the RADIATION BEAM passes.		IEC 60601-2-1/A1:2002
TRANSMISSION KERMA (TRANSMISSION KERMA RATE)	AIR KERMA (AIR KERMA RATE) in the central X-ray beam behind the specified attenuating layer.		IEC 61223-3-1:1999
TRANSMISSION OF PRIMARY RADIATION	Letter symbol: T_p . Characteristic of an object, evaluated as the ratio of the MEASURED VALUE of the quantity or rate of PRIMARY RADIATION with the object placed in a RADIATION BEAM to that with the object removed from the beam, under specific measuring conditions.		IEC 60627:2001
TRANSMISSION OF SCATTERED RADIATION	Letter symbol: T_s . Characteristic of an object, evaluated as the ratio of the MEASURED VALUE of the quantity or rate of SCATTERED RADIATION with the object placed in a RADIATION BEAM to that with the object removed from the beam, under specific measuring conditions.		IEC 60627:2001
TRANSMISSION OF TOTAL RADIATION	Letter symbol: T_t . Characteristic of an object, evaluated as the ratio of the MEASURED VALUE of the quantity or rate of total RADIATION with the object placed in a RADIATION BEAM to that with the object removed from the beam, under specific measuring conditions.		IEC 60627:2001
TRANSMISSION RATIO	Ratio of the value of a specified RADIATION QUANTITY in the centre of a beam of specified RADIATION QUALITY and under specified geometrical conditions after passage through a material to the value which would be present at the same position without this material in the beam.	rm-13-41	IEC 62083:2000
TRANSMIT PATTERN	Combination of a specific set of TRANSDUCER beam-forming characteristics (determined by the transmit aperture size, apodization shape, and relative timing/phase delay pattern across the aperture, resulting in a specific focal length and direction), and an electrical drive WAVEFORM of a specific fixed shape but variable amplitude.		IEC 60601-2-37:2001
TRANSPORT INCUBATOR	TRANSPORTABLE EQUIPMENT that is equipped with a BABY COMPARTMENT and a TRANSPORTABLE ELECTRICAL POWER SOURCE with the means to control the environment of the baby primary by heated air within the BABY COMPARTMENT, and suitable for the safe conveyance of a baby.		IEC 60601-2-20 /A1:1996
TRANSPORT INCUBATOR TEMPERATURE	Temperature of the air at a point 10 cm above the centre of the mattress surface in the BABY COMPARTMENT (see Figure 102, point A).		IEC 60601-2-20 /A1:1996
TRANSPORTABLE ELECTRICAL POWER SOURCE	A rechargeable battery and battery charger intended to provide the electrical power necessary to operate the TRANSPORT INCUBATOR.		IEC 60601-2-20 /A1:1996
TRANSPORTABLE EQUIPMENT	EQUIPMENT which is intended to be easily moved from one place to another whether or not connected to a supply and without an appreciable restriction or range. Examples: MOBILE EQUIPMENT and PORTABLE EQUIPMENT. According to IEC 60601-1/A1:1991, replace the first paragraph of 2.2.23 of IEC 60601-1:1988 by the following: EQUIPMENT which is intended to be moved from one place to another whether or not connected to a supply and without an appreciable restriction of range.	NG.02.23	IEC 60601-1/A2:1995 IEC 60601-2-7:1998 IEC 60601-2-45:2001 IEC 60601-2-51:2003
TRANSPORTER	A device intended for the transportation of the table top, with or without a PATIENT in place, to or from the base or pedestal of an OPERATING TABLE, or the transportation of the table top complete with the base, again with or without the PATIENT in place. NOTE This does not include devices intended to simply transport the PATIENT from one location to another without the transfer of parts associated with an OPERATING TABLE.		IEC 60601-2-46:1998
TRANSVERSE FIELD MAGNET	Magnet for which the field is at right angles to the axial direction of the PATIENT.		IEC 60601-2-33:2002

Term	Definition	Reference	Used in IEC
TRANSVERSE FIELD OF VIEW	Dimensions of a slice through the TOMOGRAPHIC VOLUME, perpendicular to the SYSTEM AXIS. For a circular TRANSVERSE FIELD OF VIEW it is described by its diameter. NOTE For non-cylindrical TOMOGRAPHIC VOLUMES the TRANSVERSE FIELD OF VIEW may depend on the axial position of the slice.		IEC 61675-1:1998 IEC 61675-2:1998
TRANSVERSE POINT SPREAD FUNCTION	Reconstructed two-dimensional point spread function in a tomographic IMAGE PLANE. NOTE In TOMOGRAPHY, the TRANSVERSE POINT SPREAD FUNCTION can also be obtained from a LINE SOURCE located parallel to the SYSTEM AXIS.		IEC 61675-1:1998 IEC 61675-2:1998
TRANSVERSE RESOLUTION	SPATIAL RESOLUTION in a reconstructed plane perpendicular to the SYSTEM AXIS.		IEC 61675-1:1998 IEC 61675-2:1998
TRANSVERSE TOMOGRAPHY	In TRANSVERSE TOMOGRAPHY the three-dimensional object is sliced by physical methods, e.g. collimation, into a stack of OBJECT SLICES, which are considered as being two-dimensional and independent from each other. The transverse IMAGE PLANES are perpendicular to the SYSTEM AXIS.		IEC 61675-1:1998 IEC 61675-2:1998
TREATMENT	The application of a prescribed procedure, or a part thereof, for therapeutic purposes.		IEC 60601-2-11:1997
TREATMENT CONTROL PANEL	In RADIOTHERAPY, CONTROL PANEL from which the IRRADIATION of PATIENTS is controlled.	rm-33-05	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 60601-2-29:1999
TREATMENT FIELD	In RADIOTHERAPY, area at the PATIENT'S surface which is to be irradiated.		IEC 60601-2-11:1997
TREATMENT HEAD	Assembly comprising an ULTRASONIC TRANSDUCER and associated parts for local application of ULTRASOUND to the PATIENT. NOTE A TREATMENT HEAD is also referred to as an APPLICATOR.		IEC 60601-2-5:2000
TREATMENT PARAMETER	Factor which describes one aspect of the IRRADIATION of a PATIENT during RADIOTHERAPY, such as RADIATION ENERGY, ABSORBED DOSE, TREATMENT TIME.		IEC 60601-2-17/A1:1996
TREATMENT PLAN/TREATMENT PLANNING	All PATIENT and dosimetric information that is intended for use by appropriately QUALIFIED PERSONS for the purpose of prescribing or administering RADIOTHERAPY TREATMENT. A TREATMENT PLAN includes information transmitted to other EQUIPMENT for which the use of the information for prescribing or administering IRRADIATION is indirect. A printed or plotted TREATMENT PLAN is referred to as a TREATMENT PLAN report.		IEC 62083:2000
TREATMENT ROOM	In RADIOTHERAPY, room in which IONIZING RADIATION is administered to the PATIENT, and which has the required structural means for RADIATION PROTECTION and for mechanical support.	rm-20-23	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-17/A1:1996 IEC 61217:2002
TREATMENT TIME	In RADIOTHERAPY, the time between INITIATION and TERMINATION of IRRADIATION, excluding any time in the READY STATE after INTERRUPTION.		IEC 60601-2-17/A1:1996
TREATMENT VOLUME	In RADIOTHERAPY, region in the PATIENT, to which the prescribed ABSORBED DOSE is delivered.	rm-37-21	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60976/ A1:2000

Term	Definition	Reference	Used in IEC
TRENDELENBURG	With the MATTRESS SUPPORT PLATFORM in the flat position, tilting of the entire MATTRESS SUPPORT PLATFORM a minimum of 12° so that the PATIENT'S head is lower than the circulatory centre point of the body.		IEC 60601-2-38/A1:1999
TRIXEL	MATRIX ELEMENT in a three-dimensional IMAGE MATRIX. Recommended replacement: VOXEL		IEC 61675-1:1998 IEC 61675-2:1998
TRUE CENTRAL LINE	For a PARALLEL GRID: line on the incident face in the direction of the absorbing strips and passing through the centre of the grid area For a FOCUSED GRID: perpendicular PROJECTION onto the incident face of the grid, of the line into which the planes of the absorbing strips converge. For a TAPERED GRID: line on the incident face in the direction of the absorbing strips and lying within a symmetry plane of the grid structure. NOTE A CROSS GRID has two TRUE CENTRAL LINES.		IEC 60627:2001
TRUE COINCIDENCE	Result of COINCIDENCE DETECTION of two gamma events originating from the same positron annihilation.		IEC 61675-1:1998
TRUE COUNT RATE	COUNT RATE that would be observed if the RESOLVING TIME of the device were zero.	rm-34-20	IEC 60789:1992 IEC 61675-1:1998
TRUE VALUE	Value of the physical quantity to be measured by an instrument.	rm-73-07	IEC 60580:2000 IEC 61303:1994 IEC 61674 /A1:2002
TRUE VALUE	The value of the physical quantity to be measured by an instrument. NOTE The TRUE VALUE is equivalent to the "value of measurement" shown in Figure 1 of IEC 60731. Recommended replacement: rm-73-07		IEC 60731/A1:2002
TUBE VOLTAGE (X-ray)	Potential difference applied to an X-RAY TUBE between the CATHODE, i.e. the ELECTRON emitter, and the ANODE. Recommended replacement: rm-36-02		IEC 61674 /A1:2002
TWELVE-PEAK HIGH VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR for operation on a three-phase supply that delivers a rectified output voltage with twelve peaks during each cycle of the supply.	rm-21-05	IEC 60601-2-7:1998 IEC 60601-2-45:2001
TWO-PEAK HIGH VOLTAGE GENERATOR	HIGH-VOLTAGE GENERATOR for operation on a single-phase supply that delivers a rectified output voltage with two peaks during each cycle of the supply.	rm-21-03	IEC 60601-2-7:1998 IEC 60613:1989
TWO-DIMENSIONAL RECONSTRUCTION	In TWO-DIMENSIONAL RECONSTRUCTION, the data are rebinned prior to reconstruction into SINOGRAMS, which are the PROJECTION data of transverse slices, which are considered being independent of each other and being perpendicular to the SYSTEM AXIS. So, each event will be assigned, in the axial direction, to that transverse slice passing the midpoint of the corresponding LINE OF RESPONSE. Any deviation from perpendicular to the SYSTEM AXIS is neglected. The data are then reconstructed by two-dimensional methods, i.e. each slice is reconstructed from its associated SINOGRAM, independent of the rest of the data set. NOTE This is the STANDARD method of reconstruction for POSITRON EMISSION TOMOGRAPHS using small axial acceptance angles, i.e. utilizing septa. For POSITRON EMISSION TOMOGRAPHS using large axial acceptance angles, i.e. without septa, this method is also called "single slice rebinning".		IEC 61675-1:1998

Term	Definition	Reference	Used in IEC
TYPE B APPLIED PART	APPLIED PART complying with the specified requirements of this standard IEC 60601-1/A2:1995 to provide protection against electric shock, particularly regarding allowable LEAKAGE CURRENT and marked with symbol 1, Table DII, of Appendix D. NOTE TYPE B APPLIED PARTS are not suitable for DIRECT CARDIAC APPLICATION.	NG.01.24	IEC 60601-1/A2:1995 IEC 60601-2-1/A1:2002 IEC 60601-2-9:1996 IEC 60601-2-17 /A1:1996 IEC 60601-2-26:2002 IEC 60601-2-29:1999 IEC 60601-2-47:2001 IEC 60601-2-51:2003
TYPE B EQUIPMENT	EQUIPMENT providing a particular degree of protection against electric shock, particularly regarding: – allowable LEAKAGE CURRENT, – reliability of the protective earth connection (if present).	NG.02.24	IEC 60601-2-44:2002
TYPE BF APPLIED PART	F-type APPLIED PART complying with the specified requirements of this standard IEC 60601-1/A2:1995 to provide a higher degree of protection against electric shock than that provided by type B APPLIED PARTS and marked with symbol 2, Table DII, of Appendix D. NOTE TYPE BF APPLIED PARTS are not suitable for DIRECT CARDIAC APPLICATION.	NG.01.25	IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
TYPE CF APPLIED PART	F-type APPLIED PART complying with the specified requirements of this standard IEC 60601-1/A2:1995 to provide a higher degree of protection against electric shock than that provided by TYPE BF APPLIED PARTS and marked with symbol 3, Table DII, of Appendix D.	NG.01.26	IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-26:2002 IEC 60601-2-47:2001 IEC 60601-2-51:2003
TYPE TEST	TEST normally carried out on a single instrument of each design. NOTE The purpose of the TYPE TEST is to verify whether or not the design of the instrument renders it capable of meeting the requirements of the specification. Recommended replacement: IEC 60601-2-1, IEC 60601-2-11 and IEC 60601-2-8		IEC 60731/A1:2002
TYPE TEST	For a particular design of device or EQUIPMENT, a TEST by the MANUFACTURER to establish compliance with specified criteria.		IEC 60601-2-1/A1:2002 IEC 60601-2-8:1999 IEC 60601-2-11:1997
ULTRAFILTRATION	The process of fluid removal from the PATIENT'S blood across the DIALYSER.		IEC 60601-2-16:1998
ULTRASONIC DIAGNOSTIC EQUIPMENT	MEDICAL ELECTRICAL EQUIPMENT which is intended for in vivo ultrasonic and monitoring examination for obtaining a medical diagnosis. NOTE See also definition 3.11 of IEC 61157: medical diagnostic ultrasonic EQUIPMENT (or system) - combination of the ULTRASOUND instrument console and the TRANSDUCER ASSEMBLY making up a complete diagnostic system.		IEC 60601-2-37:2001 IEC 60601-2-18 /A1:2000
ULTRASONIC MEDICAL DIAGNOSTIC EQUIPMENT AND MONITORING EQUIPMENT	((See ULTRASONIC DIAGNOSTIC EQUIPMENT))		IEC 60601-2-18 /A1:2000

Term	Definition	Reference	Used in IEC
ULTRASONIC PHYSIOTHERAPY EQUIPMENT	EQUIPMENT for the generation and application of ULTRASOUND to a PATIENT for therapeutic purposes. NOTE Essentially the EQUIPMENT comprises a generator of electric high-frequency power and a TRANSDUCER for converting this to ULTRASOUND.		IEC 60601-2-5:2000
ULTRASONIC TRANSDUCER	Device capable of converting electrical energy to mechanical energy and/or mechanical energy to electrical energy, both within the ultrasonic frequency range.		IEC 60601-2-37:2001
ULTRASONIC TRANSDUCER	Device capable of converting electrical energy to mechanical energy within the ultrasonic frequency range. Recommended replacement: IEC 60601-2-37		IEC 60601-2-5:2000
ULTRASOUND	Acoustic oscillation whose frequency is above the high-frequency limit of audible sound (about 16 kHz) (see IEV 801-21-04 [IEC 61689, definition 3.45]).		IEC 60601-2-5:2000
UNATTENUATED BEAM	X-ray beam incident on the PATIENT or PHANTOM.		IEC 61674/A1:2002
UNATTENUATED BEAM QUALITY	RADIATION QUALITY of the X-ray beam incident on the PATIENT or PHANTOM in the absence of the PATIENT or PHANTOM, i.e. in free air.		IEC 61674/A1:2002
UNDER-BLANKET	BLANKET to be used under a PATIENT.		IEC 60601-2-35:1996
UNIFORM CONSTANCY TEST FILM	Film containing the RADIOGRAM of the homogeneous FILTER part of the TEST DEVICE.		IEC 61223-2-7:1999
UNIFORMITY	Consistency of the COMPUTED TOMOGRAPHY NUMBERS of the image of a homogeneous material across the scan field.		IEC 61223-2-6:1994
UNIFORMITY G_2 OF THE TOTAL IRRADIANCE FOR BILIRUBIN	The ratio of the lowest TOTAL IRRADIANCE FOR BILIRUBIN $E_{bi\ min}$ to the highest TOTAL IRRADIANCE FOR BILIRUBIN $E_{bi\ max}$ on the EFFECTIVE SURFACE AREA, given by the expression $G_2 = E_{bi\ min}/E_{bi\ max}$		IEC 60601-2-50:2000
UNSCATTERED TRUE COINCIDENCE	The difference between TRUE COINCIDENCES and SCATTERED TRUE COINCIDENCES.		IEC 61675-1:1998
UNWANTED RADIATION	Microwave radiation which is not incident on the PATIENT for TREATMENT purpose.		IEC 60601-2-6:1984
USEFUL BEAM	All X-rays which emerge through a cone defined by the focus point and the specified aperture of its PROTECTIVE SHIELDING or of its beam-limiting device. Recommended replacement: rm-37-05 RADIATION BEAM		IEC 60580:2000
USEFUL ENTRANCE FIELD SIZE	The ENTRANCE FIELD SIZE measured at the ENTRANCE PLANE of the XRII at a specified SED.		IEC 61262-1:1994
USEFUL FIELD	Cross section of the USEFUL BEAM, perpendicular to its specified direction at a specified distance from the FOCAL SPOT or at a specified plane of measurement.		IEC 60580:2000

Term	Definition	Reference	Used in IEC
USER	When used in an IEC standard on electromedical EQUIPMENT, organization or individual responsible for the use and maintenance of the EQUIPMENT.	rm-85-01	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-1-4:2000 IEC 60601-2-1/A1:2002 IEC 60601-2-7:1998 IEC 60601-2-11:1997 IEC 60601-2-17 /A1:1996 IEC 60601-2-29:1999 IEC 60601-2-33:2002 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 60731/A1:2002 IEC 60976/ A1:2000 IEC 61217:2002 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61267:1994 IEC 61331-3:1998 IEC 61674/A1:2002 IEC 62083:2000

Term	Definition	Reference	Used in IEC
USER	Authority responsible for the use and maintenance of EQUIPMENT. Recommended replacement: rm-85-01	NG.12.13	IEC 60601-1/A2:1995 IEC 60601-2-9:1996 IEC 60601-2-12:2001 IEC 60601-2-13:2003 IEC 60601-2-51:2003
VALIDATION	Process of evaluating a PEMS or a component of a PEMS during or at the end of the development process, to determine whether it satisfies the requirements for its intended use.		IEC 60601-1-4:2000
VARIATION	The relative difference, $\Delta y/y$, between the values of a PERFORMANCE CHARACTERISTIC, y , when one INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) successively assumes two specified values, the other INFLUENCE QUANTITIES (and INSTRUMENT PARAMETERS) being kept constant at the STANDARD TEST VALUES (unless other values are specified).		IEC 61674 /A1:2002
VARIATION	The relative difference, $\Delta y/y$, between the values of a PERFORMANCE CHARACTERISTIC y , when one INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) assumes successively two values, the other INFLUENCE QUANTITIES (and INSTRUMENT PARAMETERS) being kept constant at the STANDARD TEST VALUES (unless other values are specified). Recommended replacement: IEC 61674		IEC 60731/A1:2002
VARIATION	Relative difference, $\Delta y/y$, between the values of a PERFORMANCE CHARACTERISTIC, y , when one INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) successively assumes two specified values, the other INFLUENCE QUANTITIES (and INSTRUMENT PARAMETERS) being kept constant at the STANDARD TEST VALUES (unless other values are specified). Recommended replacement: IEC 61674		IEC 60580:2000
VARIATION	The relative difference $\Delta y/y$, between the values of a PERFORMANCE CHARACTERISTIC y , when one INFLUENCE QUANTITY (or INSTRUMENT PARAMETER) assumes successively two specified values, the other INFLUENCE QUANTITIES (and INSTRUMENT PARAMETERS) being kept constant at the STANDARD TEST VALUES (unless other values are specified). Recommended replacement: IEC 61674		IEC 61676:2002
VEILING GLARE INDEX (abbreviation VGI)	The reciprocal of the CR.		IEC 61262-6:1994
VENOUS PART	Part of the EXTRACORPOREAL CIRCUIT between the outlet of the DIALYSER and the PATIENT.		IEC 60601-2-16:1998
VENOUS PRESSURE	The PRESSURE measured in the EXTRACORPOREAL CIRCUIT between the outlet from the DIALYSER and the return to the PATIENT.		IEC 60601-2-16:1998
VENTILATOR	Automatic EQUIPMENT that is intended to augment or provide ventilation of the lungs of the PATIENT when connected to the airway of the PATIENT.		IEC 60601-2-12:2001
VENTILATOR BREATHING SYSTEM (VBS)	Breathing system bounded by the LOW PRESSURE GAS INPUT PORT(S), the LOW PRESSURE GAS INPUT PORT(S) and the PATIENT CONNECTION PORT, together with the LOW PRESSURE GAS INPUT PORT(S), if these are provided. [ISO 4135:1995, definition 4.1.6 modified]		IEC 60601-2-12:2001
VERIFICATION	Process of evaluating a PEMS or a component of a PEMS to determine whether the products of a given development phase satisfy the specified requirements imposed at the start of that phase. Recommended replacement: ISO 8402:1994, definition 2.17		IEC 60601-1-4:2000

Term	Definition	Reference	Used in IEC
VERIFICATION	Confirmation by examination and provision of objective evidence that specified requirements have been fulfilled. NOTE In design and development, VERIFICATION concerns the process of examining the result of a given ACTIVITY to determine conformity with the stated requirement for that ACTIVITY. [ISO 8402:1994, definition 2.17]		ISO 14971:2000
VIRTUAL SOURCE	Point from which the RADIATION appears to originate.	rm-37-01	IEC 60976 /A1:2000
VISUAL STIMULATOR	Parts of EQUIPMENT or system for the application of electromagnetic radiation in the visible spectrum from a TRANSDUCER to the eyes of the PATIENT, for the evoking of biopotentials or other action.		IEC 60601-2-40:1998
VOLTAGE RIPPLE	The VOLTAGE RIPPLE at the X-RAY TUBE, r , is expressed as a percentage of the peak voltage, U_{\max} , over a specified time interval. This is expressed by the equation: $r = \frac{U_{\max} - U_{\min}}{U_{\max}} \cdot 100\%$ where U_{\max} is the highest voltage in the interval, and U_{\min} is the lowest voltage in the interval.		IEC 61676:2002
VOLUME RF TRANSMIT COIL	An RF transmit coil suitable for use in MR EQUIPMENT that produces a homogeneous RF field over an extended volume encompassed by the coil. The VOLUME RF TRANSMIT COIL can be a WHOLE BODY RF TRANSMIT COIL, a HEAD RF TRANSMIT COIL or a RF transmit coil designed for homogeneous EXPOSURE of a specific part of the body. A single loop coil enclosing the body or a part of the body is considered to be a VOLUME RF TRANSMIT COIL (example: single loop wrist coil).		IEC 60601-2-33:2002
VOLUME SENSITIVITY	Sum of the individual slice sensitivities.		IEC 61675-1:1998 IEC 61675-2:1998
VOLUMETRIC INFUSION CONTROLLER	INFUSION CONTROLLER in which the delivery rate is set by the OPERATOR and indicated by the EQUIPMENT in volume per unit of time.		IEC 60601-2-24:1998
VOLUMETRIC INFUSION PUMP	INFUSION PUMP in which the delivery rate is set by the OPERATOR and indicated by the EQUIPMENT in volume per unit of time, but excluding SYRINGE PUMPS.		IEC 60601-2-24:1998
VOXEL	Volume element in the object which is assigned to a MATRIX ELEMENT in the IMAGE MATRIX (two-dimensional or three-dimensional). The dimensions of the VOXEL are determined by the dimensions of the corresponding MATRIX ELEMENT via the appropriate scale factors and by the systems SPATIAL RESOLUTION in all three dimensions.		IEC 61675-1:1998 IEC 61675-2:1998
WARNING SIGNAL	Means of signalling a predetermined state of a physiological parameter or EQUIPMENT.		IEC 60601-2-23:1999
WATER KERMA	KERMA measured in a mass of water.	rm-13-12	IEC 60601-2-8:1999
WAVE RECOGNITION POINTS	REFERENCE POINTS on the time axis of the ECG WAVEFORM for interval and amplitude measurements on an ECG cycle: – P-ONSET: beginning of the P-wave (atrial depolarisation); – P-OFFSET: end of the P-wave; – QRS-ONSET: beginning of the QRS-complex (ventricular depolarisation); – QRS-OFFSET: end of the QRS-complex; – T-OFFSET: end of the T-wave (end of ventricular repolarisation).		IEC 60601-2-51:2003

Term	Definition	Reference	Used in IEC
WAVEFORM	The variations in magnitude of an electrical signal (in either voltage or current) as a function of time appearing in a PATIENT CIRCUIT.		IEC 60601-2-10 /A1:2001
WAVEFORM	The variations in magnitude of an electrical stimulus output (in either voltage or current) as a function of time appearing in the APPLIED PART of the electrical STIMULATOR.		IEC 60601-2-40:1998
WEDGE FILTER	FILTER which effects stepless change in TRANSMISSION over all or a part of the RADIATION FIELD.	rm-35-10	IEC 60601-2-1/A1:2002 IEC 60601-2-11:1997 IEC 60601-2-29:1999 IEC 60976 /A1:2000 IEC 61217:2002 IEC 62083:2000
WEDGE FILTER ANGLE	On an isodose curve passing through the RADIATION BEAM AXIS at STANDARD MEASUREMENT DEPTH, the angle defined by the slope of the line joining two points equidistant from the RADIATION BEAM AXIS and half the width of the geometrical field apart.	rm-33-19	IEC 60601-2-11:1997 IEC 60976/A1:2000
WEDGE FILTER FACTOR	Ratio of the ABSORBED DOSE on the RADIATION BEAM AXIS at the STANDARD MEASUREMENT DEPTH with and without the WEDGE FILTER present in the RADIATION BEAM.		IEC 60976/A1:2000
WELL-COUNTER	Instrument utilizing nearly 4π geometry counting with a WELL-TYPE DETECTOR into which the sample can be inserted.		IEC 61948-1:2001
WELL-TYPE DETECTOR	In vitro measuring instrument utilizing a detector with a well to detect PHOTONS from a sample inserted into the well of the detector.		IEC 61948-1:2001
WHOLE BODY GRADIENT SYSTEM	A gradient system suitable for use in WHOLE BODY MR EQUIPMENT.		IEC 60601-2-33:2002
WHOLE BODY MAGNET	Magnet suitable for use in WHOLE BODY MR EQUIPMENT.		IEC 60601-2-33:2002
WHOLE BODY MAGNETIC RESONANCE EQUIPMENT (WHOLE BODY MR EQUIPMENT)	MR EQUIPMENT of sufficient size to allow whole body MR EXAMINATION and partial body MR EXAMINATION of adult PATIENTS. It may be equipped with VOLUME RF TRANSMIT COILS, LOCAL RF TRANSMIT COILS and with a SPECIAL PURPOSE GRADIENT SYSTEM.		IEC 60601-2-33:2002
WHOLE BODY RF TRANSMIT COIL	A VOLUME RF TRANSMIT COIL of sufficient size for whole body examinations of adult PATIENTS.		IEC 60601-2-33:2002
WHOLE BODY SAR	SAR averaged over the total mass of the PATIENT'S body and over a specified time.		IEC 60601-2-33:2002
WHOLEBODY COUNTER	Instrument for estimating the amount of RADIONUCLIDES in the body and, if possible, identifying the RADIONUCLIDES and estimating the spatial distribution of RADIONUCLIDES and their ACTIVITIES within the body. WHOLE BODY COUNTERS have a high SENSITIVITY that is essentially independent of the distribution of ACTIVITY in the body. For minimizing the detection threshold, appropriate shielding of background RADIATION is necessary.		IEC 61948-1:2001
WHOLEBODY IMAGING DEVICE	EQUIPMENT for scintigraphy, employing one or two DETECTOR HEAD(S), in which the image is formed by linear motion of the DETECTOR HEAD(S) and the object relative to each other.		IEC 61948-2:2001
WORKING STANDARD	A standard which is traceable to the NATIONAL STANDARD.		IEC 60731/A1:2002

Term	Definition	Reference	Used in IEC
WORKLOAD	<p>Letter symbol: <i>W</i>. Measure in suitable units of the degree of use of EQUIPMENT generating IONIZING RADIATION.</p> <p>NOTE For diagnostic X-RAY EQUIPMENT, the WORKLOAD is expressed in coulombs (C) per week, in milliamperere seconds (mAs) per week or milliamperere minutes (mAmin) per week (1 C = 10³ mAs = 16,66 mAmin). Usually, the WORKLOAD is determined from the average of the weekly sums of the products of X-RAY TUBE CURRENT and corresponding switch-on times. For therapeutic X-RAY EQUIPMENT, WORKLOAD is expressed in KERMA per week in the RADIATION BEAM at 1 m from the source.</p>	rm-61-03	IEC 60601-1-3:1994 IEC 61223-2-10:1999
X-RAY EQUIPMENT	EQUIPMENT consisting of a combination of an X-RAY GENERATOR, ASSOCIATED EQUIPMENT and accessories.	rm-20-20	IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-29:1999 IEC 60601-2-32:1994 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60627:2001 IEC 61223-1:1993 IEC 61223-2-1:1993 IEC 61223-2-4:1994 IEC 61223-2-5:1994 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-3:1998

Term	Definition	Reference	Used in IEC
X-RAY GENERATOR	Combination of all components provided for the generation and control of X-RADIATION, comprising at least the HIGH-VOLTAGE GENERATOR interconnected with an X-ray source assembly.	rm-20-17	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 61223-2-1:1993 IEC 61223-3-1:1999 IEC 61223-3-4:2000 IEC 61267:1994
X-RAY IMAGE INTENSIFIER	Device which converts an X-RAY PATTERN into a corresponding light pattern using an additional supply of energy for intensification.	rm-32-39	IEC 60601-2-32:1994 IEC 60601-2-33:2002 IEC 61217:2002 IEC 61223-2-1:1993 IEC 61223-2-9:1999 IEC 61223-3-1:1999 IEC 61223-3-3:1996 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994
X-RAY IMAGE INTENSIFIER TUBE	Electro-optical vacuum device with an INPUT SCREEN in optical contact with a photocATHODE, in which an ELECTRON pattern is formed and then, using an additional supply of energy for intensification, converted into a light image in the OUTPUT SCREEN.	rm-32-41	IEC 60601-1-3:1994 IEC 61267:1994

Term	Definition	Reference	Used in IEC
X-RAY IMAGE RECEPTOR	Device, such as a FLUORESCENT SCREEN of RADIOGRAPHIC FILM, intended to convert an X-RAY PATTERN into a visible image either directly or indirectly.	rm-32-29	IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-45:2001 IEC 61217:2002 IEC 61223-2-9:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61267:1994
X-RAY IMAGING ARRANGEMENT	In X-RAY EQUIPMENT, arrangement of RADIATION SOURCE and X-RAY IMAGE RECEPTOR for a specified RADIOLOGICAL technique.	rm-20-21	IEC 60601-1-3:1994
X-RAY PATTERN	Information contained in a beam of IONIZING RADIATION the distribution of intensity of which has been modulated by the object passed.	rm-32-01	IEC 60601-1-3:1994 IEC 60627:2001 IEC 60806:1984 IEC 61262-1:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
X-RAY THERAPY	RADIOTHERAPY with X-RADIATION using X-RAY TUBE VOLTAGES up to about 300 kV.	rm-42-12	IEC 60976/A1:2000

Term	Definition	Reference	Used in IEC
X-RAY TUBE	<p>Evacuated vessel for the production of X-RADIATION by the bombardment of a TARGET, usually contained in an ANODE, with ELECTRONS accelerated from a CATHODE by an electric field.</p> <p>Thus:</p> <ul style="list-style-type: none"> - rotating ANODE X-RAY TUBE; - double focus X-RAY TUBE. 	rm-22-03	IEC 60336:1993 IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-28:1993 IEC 60601-2-33:2002 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60806:1984 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994
X-RAY TUBE	<p>A high-vacuum hollow vessel for the production of X-RADIATION by the bombardment of a TARGET by a beam of ELECTRONS accelerated by a potential difference.</p> <p>Recommended replacement: rm-22-03</p>		IEC 60336:1993

Term	Definition	Reference	Used in IEC
X-RAY TUBE ASSEMBLY	X-RAY TUBE HOUSING with an X-RAY TUBE installed.	rm-22-01	IEC 60336:1993 IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60806:1984 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000 IEC 61267:1994
X-RAY TUBE ASSEMBLY COOLING CURVE	Curve showing the X-RAY TUBE ASSEMBLY HEAT CONTENT with zero X-RAY TUBE ASSEMBLY INPUT POWER as a function of time beginning after a LOADING when the X-RAY TUBE ASSEMBLY HEAT CONTENT is equal to the MAXIMUM X-RAY TUBE ASSEMBLY HEAT CONTENT.	rm-36-33	IEC 60601-2-28:1993 IEC 60613:1989
X-RAY TUBE ASSEMBLY HEAT CONTENT	Momentary value of the heat contained in the X-RAY TUBE ASSEMBLY.	rm-36-30	IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989
X-RAY TUBE ASSEMBLY HEATING CURVE	Curve showing the X-RAY TUBE ASSEMBLY HEAT CONTENT as a function of LOADING TIME, under specified LOADING conditions.	rm-36-32	IEC 60601-2-28:1993 IEC 60613:1989
X-RAY TUBE ASSEMBLY INPUT POWER	Mean power applied to an X-RAY TUBE ASSEMBLY for all purposes before, during and after LOADING, including power applied to the stator of a rotating ANODE X-RAY TUBE, to the filament and to any other device included in the X-RAY TUBE ASSEMBLY.	rm-36-25	IEC 60613:1989

Term	Definition	Reference	Used in IEC
X-RAY TUBE CURRENT	Electric current of the ELECTRON beam incident on the TARGET of an X-RAY TUBE. Usually, the X-RAY TUBE CURRENT is expressed by its mean value in milliamperes (mA).	rm-36-07	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-4:2000
X-RAY TUBE HEAD	X-ray source assembly containing the HIGH-VOLTAGE TRANSFORMER ASSEMBLY.	rm-20-07	IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60601-2-45:2001
X-RAY TUBE HOUSING	Container for an X-RAY TUBE providing protection against electric shock and against X-RADIATION and having a RADIATION APERTURE. It may optionally contain additional components.	rm-22-02	IEC 60336:1993 IEC 60522:1999 IEC 60601-1-3:1994 IEC 60601-2-8:1999 IEC 60601-2-28:1993 IEC 60806:1984
X-RAY TUBE LOAD	Electrical energy supplied to an X-RAY TUBE expressed by a combination of values of LOADING FACTORS.	rm-36-21	IEC 60336:1993 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-44:2002 IEC 60613:1989 IEC 61223-3-2:1996

Term	Definition	Reference	Used in IEC
X-RAY TUBE VOLTAGE	Potential difference applied to an X-RAY TUBE between the ANODE and the CATHODE. Usually, X-RAY TUBE VOLTAGE is expressed by its peak value in kilovolts (kV).	rm-36-02	IEC 60336:1993 IEC 60522:1999 IEC 60580:2000 IEC 60601-1-3:1994 IEC 60601-2-7:1998 IEC 60601-2-8:1999 IEC 60601-2-29:1999 IEC 60601-2-43:2000 IEC 60601-2-44:2002 IEC 60601-2-45:2001 IEC 60613:1989 IEC 60627:2001 IEC 60806:1984 IEC 61223-2-6:1994 IEC 61223-2-7:1999 IEC 61223-2-9:1999 IEC 61223-2-10:1999 IEC 61223-2-11:1999 IEC 61223-3-1:1999 IEC 61223-3-2:1996 IEC 61223-3-3:1996 IEC 61223-3-4:2000 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-6:1994 IEC 61262-7:1995 IEC 61267:1994 IEC 61331-1:1994 IEC 61331-2:1994 IEC 61331-3:1998
X-RAY TUBE VOLTAGE	Potential difference applied to an X-RAY TUBE between the ANODE and the CATHODE. The unit of this quantity is the volt (V). Recommended replacement: rm-36-02		IEC 61676:2002

Term	Definition	Reference	Used in IEC
XRII	An abbreviation for ELECTRO-OPTICAL X-RAY IMAGE INTENSIFIER		IEC 61262-1:1994 IEC 61262-2:1994 IEC 61262-3:1994 IEC 61262-4:1994 IEC 61262-5:1994 IEC 61262-6:1994 IEC 61262-7:1995
zero APPLICATOR	In a system which includes an INTERLOCK against IRRADIATION without a beam APPLICATOR, means to bypass the INTERLOCK.		IEC 60601-2-11:1997
ZERO DRIFT (MEASURING ASSEMBLY)	A continuous change in the near zero SCALE READING of the MEASURING ASSEMBLY in the "measure" condition with no signal present.		IEC 60580:2000 IEC 60731:1997
ZERO FILTER	In a system which includes an INTERLOCK against IRRADIATION without added FILTER, means to bypass this INTERLOCK.	rm-35-06	IEC 60601-2-8:1999 IEC 60601-2-11:1997
ZERO SHIFT (MEASURING ASSEMBLY)	A sudden change in the near zero SCALE READING of the MEASURING ASSEMBLY when the setting control is changed from the "zero" condition to the "measure" condition, with no signal present.		IEC 60731/A1:2002

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